Check for updates

OPEN ACCESS

EDITED BY Tamotsu Kamishima, Hokkaido University, Japan

REVIEWED BY Rong Lu, Fudan University, China Songtao Ai, Radiology/Shanghai Ninth Hospital, China

*correspondence Xiaokai Li 🖂 lxkmoon@126.com

RECEIVED 16 August 2024 ACCEPTED 15 October 2024 PUBLISHED 29 October 2024

CITATION

Cheng Y and Li XK (2024) Advanced quantitative magnetic resonance imaging of lower extremity muscle microtrauma after marathon: a mini review. Front. Sports Act. Living 6:1481731. doi: 10.3389/fspor.2024.1481731

COPYRIGHT

© 2024 Cheng and Li. This is an open-access article distributed under the terms of the **Creative Commons Attribution License (CC BY)**. The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.

Advanced quantitative magnetic resonance imaging of lower extremity muscle microtrauma after marathon: a mini review

Yu Cheng and Xiaokai Li*

School of Sports and Health, Shanghai University of Sport, Shanghai, China

This article reviews the existing literature and outlines recent advances in quantitative Magnetic Resonance Imaging (MRI) techniques for the assessment of lower extremity muscle microtrauma following a marathon. Single-modality quantitative MRI techniques include T2 mapping to assess the dynamics of muscle inflammatory edema and variability at the site of injury, Diffusion Tensor Imaging (DTI) to detect subclinical changes in muscle injury, Intravoxel Incoherent Motion (IVIM) imaging to provide simultaneous information on perfusion and diffusion in muscle tissue without the need for intravenous contrast, and Magnetic Resonance Spectroscopy (MRS) to noninvasively detect intramyocellular lipid (IMCL) content in muscle before and after marathon exercise to explain the use of fatty acids as an energy source in skeletal muscle during long-distance running. As well as Chemical Exchange Saturation Transfer (CEST) is particularly suitable for detecting changes in free creatine, pH values and lactate concentrations in muscles before and after exercise, providing a more detailed picture of muscle physiology and chemistry. These metabolic MRI methods enhance the understanding of biochemical alterations occurring in muscles pre- and post-exercise. Multimodal techniques combine different modalities to provide a comprehensive evaluation of muscle structural and functional changes. These advanced techniques aim to better assess microtrauma and guide clinical treatment, though further validation with larger studies is needed to establish their potential over traditional qualitative methods.

KEYWORDS

magnetic resonance imaging, marathon, muscle, microtrauma, lower extremity

1 Introduction

Marathon is a popular pastime and sporting activity, with over 30 million people participating annually across the globe, many of whom are novice runners (1). However, prolonged running (e.g., full marathons, mountain ultra-marathons) tends to lead to organism fatigue and induces motor microtrauma in the muscles of the lower limbs, with common microstructural changes including cellular swelling, loss of membrane integrity, inflammation and fiber tearing (2–5). Although traditional imaging techniques such as Ultrasonography and x-ray offer some advantages in the assessment of sports injuries, with Ultrasonography allowing real-time visualization of soft tissues and x-rays being widely used in skeletal assessment, they have limitations in detecting deeper microstructural changes in muscle and early injury. In contrast, Quantitative Magnetic Resonance Imaging (QMRI) provides higher soft tissue contrast and sensitivity, enabling the assessment of microstructural physiological and biochemical changes in lower limb muscle injuries, which are often not detectable by conventional imaging techniques (6, 7). Whereas detecting changes at the microscopic molecular level in lower limb muscles may be useful for injury prevention, injury assessment in athletes or active individuals, while minimizing injury risk and rehabilitation time (8, 9). Currently, researchers (10-12) are using advanced quantitative imaging techniques to characterize ultramicro changes, monitor recovery, and estimate return-to-exercise time in lower extremity muscle kinesiology injuries in order to avoid gross anatomical damage due to repetitive microtrauma. Therefore, this article focuses on outlining recent advances in advanced quantitative magnetic resonance imaging techniques in assessing lower extremity muscle microtrauma after marathon exercise and directions for future research.

2 Materials and methods

A comprehensive literature search was conducted using computerized systems in PubMed, Google Scholar, and China National Knowledge Infrastructure (CNKI) databases. The search utilized specific keywords pertinent to the research questions, as outlined in Table 1. This search encompassed both Chinese and English literature published from 1998 to 2024. Initially, a total of 5,862 articles were identified.

After screening the titles and abstracts, 5,712 articles were deemed irrelevant. The remaining articles underwent a full-text review, which resulted in the inclusion of 21 articles for analysis¹. The inclusion criteria were defined as follows: studies must focus on marathon-related muscle injuries and utilize quantitative magnetic resonance imaging techniques. Studies that did not meet these criteria or were not published in peer-reviewed journals were excluded.

3 Results and discussion

3.1 General findings

In studies assessing lower extremity muscle microtrauma after marathon exercise, quantitative MRI techniques have now evolved from single-modality applications to advanced multimodal assessment methods. Single-modality quantitative MRI techniques include T2 mapping, Diffusion-weighted MRI (dMRI), Magnetic Resonance Spectroscopy (MRS) and Chemical Exchange Saturation Transfer (CEST). Multi-modal quantitative MRI techniques include combining information from different modalities and single-scan multicontrast imaging methods (Synthetic MRI, SyMRI). Their respective advantages, disadvantages, and potential clinical applications are summarized in Table 2.

3.2 Single-modality quantitative MRI techniques

3.2.1 T2 mapping

Magnetic resonance T2 mapping is a commonly used method to quantify motor physiologic impairments in lower extremity muscles. The technique obtains multiple T2-weighted images (T2WI) using a series of different echo times (TE) and fitting them with mono-exponential or multi-exponential models to obtain T2 values, and also generates pseudo-color maps for a more objective assessment of the T2 relaxation time of muscle tissue (13). T2 relaxation time is highly sensitive to changes in the overall water content of muscle tissue and to intra- and extracellular water redistribution (14-16). Under normal conditions, T2 values are low due to the orderly arrangement of collagen fibers and the structural integrity of cell membranes in muscle. When the muscle underwent intense exercise, the water content and freedom of skeletal muscle cells increased, resulting in the extension of T2 value. This change reflects microscopic changes in muscle tissue that may occur as a result of pathological conditions such as inflammation and edema (11, 17).

In two recent studies (18, 19) the dynamics of T2 values in the hamstring muscle before and after marathon exercise were quantified by the T2 mapping technique; the results showed a significant prolongation of the muscle's T2 values after exercise compared with those before exercise, suggesting that marathon running may induce inflammatory edema in the hamstring muscle. In another study (10), T2 values of foot muscles before and after 22 college students participated in a full marathon were also analyzed using the T2 mapping technique; the results showed that the T2 values of all extrinsic and some intrinsic foot muscles (plantar flexors) were significantly elevated on day 1 after the race compared to the pre-race period, and that the T2 values were gradually restored to the baseline level by day 8 after the race; moreover, changes in the T2 values of extrinsic foot. In addition, the changes in T2 values of external muscles of the foot (flexor digitorum longus and flexor pollicis longus) between precompetition and post-competition day 1 were directly related to the corresponding changes in the arch height ratio. This indicates that T2 mapping can accurately reflect the differences in foot muscle injuries caused by full marathon, and the changes in T2 values are reversible, suggesting that micro-injuries of foot muscles can be recovered. Therefore, T2 mapping can be used to quantitatively assess the changes and differences of lower limb muscle inflammatory edema caused by marathon exercise, and may be used to estimate the time to resume marathon participation and the risk of re-injury.

3.2.2 dMRI

dMRI is an imaging technique that reflects microstructural changes by detecting the diffusion properties of water molecules within tissues. It holds significant potential for application in

¹The included articles are marked by an asterisk (*) in the reference list.

TABLE 1 Literature search keywords.

Concepts (AND)	Magnetic resonance imaging	Marathon	Muscle	Microtrauma
Keywords (OR)	Magnetic resonance imaging	Marathon running	Muscles	Wounds and injuries
			Muscle	Injury
				Microtrauma
	MRI	Marathon	Muscle, skeletal	Microinjury
			Skeletal muscle	Damage
	Quantitative magnetic resonance imaging			Microdamage
	QMRI			

TABLE 2 Strengths, limitations and clinical potential of different quantitative MRI techniques in the assessment of lower limb muscle injuries after marathon running.

Technique	Strengths	Limitations	Potential applications	
T2 mapping	Highly sensitive to changes in overall tissue water content and to intra- and extracellular water redistribution	Lack of standardization, e.g., establishment of normal values for T2 in muscle tissue, image acquisition and analysis processes	Assessing the dynamics of muscle inflammatory edema and difference in site of injury Estimated time for individuals to return to play and	
	Can be applied to conventional MRI equipment		risk of re-injury	
DTI	Observation and tracking of fiber bundle orientation and microstructure within the muscle	Difficulty balancing signal-to-noise ratio, resolution and acceptable scan time	Fiber bundle length, pinnation angle, and curvature can be calculated algorithmically to reflect biomechanical properties to a certain extent Assessment of subclinical microinjuries in lower limb muscles induced by different types of marathon exercise	
	Detection of subclinical changes in lower limb muscles after long-distance running, e.g., minor tears in muscle fibers, abnormal diffusion of water molecules	Lack of multi-center comparisons		
IVIM	No need for intravenous contrast Also provides information on perfusion and	The effect of marathon exercise on muscle microcirculatory perfusion is unclear	IVIM, based on multiband acceleration technology, greatly reduces scanning time and is expected to be	
MRS	diffusion in tissues Non-invasive detection of intramyocellular lipid content in muscle, which may have a U-shaped relationship with marathon running intensity	Long scanning time High requirements for spatial homogeneity of the static magnetic field, hardware stability, and scanning technology Selectable CEST technology	applied in routine clinical monitoring Adjustment of exercise or rehabilitation programs based on muscle metabolism to optimize treatment results	
Multi-modal MRI techniques	Comprehensive information on muscle structure and function can be provided by combining information from different modalities or applying SyMRI techniques	Combining different modal imaging techniques requires longer scanning times	Multiple sets of quantitative parameters can comprehensively detect microscopic changes in muscles before and after exercise, accurately reflecting the degree of injury and monitoring the recovery process	

sports medicine, particularly in the assessment of muscle injuries related to marathon running. dMRI encompasses various imaging modalities, with this paper focusing on Diffusion Tensor Imaging (DTI) and Intravoxel Incoherent Motion Imaging (IVIM), discussing in detail their application in the evaluation of lower limb muscle injuries following marathon exercise.

3.2.2.1 DTI

DTI is based on the stochastic Brownian motion of water molecules in living tissues, and a diffusion-sensitive gradient field is applied in multiple directions to quantify the anisotropy of water molecule diffusion, and to observe and track the orientation of fiber bundles and the microstructure within the muscles of the lower extremities. Under normal conditions, the diffusive motion of water molecules in tissues is blocked by intact cell membranes, allowing water molecules to move in the direction of the long axis of the muscle fibers, and the muscle fibers are aligned in an orderly fashion (12). After marathon running, lower limb muscles may show subclinical changes (8), such as minor tears in muscle fibers and disruption of cell membrane integrity, leading to enhanced free diffusion of water molecules and increased free water content between muscle fibers. Subclinical changes of muscle fibers that could not be detected by conventional T2WI sequences can be demonstrated by DTI technique, e.g., minor tears in muscle fibers, abnormal diffusion of water molecules, and are usually manifested as a fractional anisotropy (FA) of the muscle on the image is significantly decreased and mean diffusivity (MD) and apparent diffusion coefficient (ADC) values are increased (20–22). DTI measurements of lower limb muscles can be performed using 1.5T or 3T MRI equipment, and technical adjustments in sequence design (e.g., using b-values between 400 and 600 s/mm² and at least 12 diffusion gradient directions) are usually required to obtain accurate measurements (8, 12, 20).

Furthermore, the available evidence is inconsistent. A recent study of 20 mountain ultra-marathoners found (23) that both T2 and T2* values of the quadriceps were significantly higher after the race compared with before the race and did not return to baseline levels after 48–72 h; this suggests that mountain ultra-marathons may lead to recurrent eccentric contractions and exposure of the quadriceps muscles of the lower limb to high mechanical stress, which in turn lead to quadriceps injuries that

10.3389/fspor.2024.1481731

are not easy to recover from. In contrast, a study of 17 amateur marathoners participating in a half-marathon showed (20) that DTI measurements (thigh muscle group FA values) changed reversibly before, 3 h, and 3 days after exercise, demonstrating that running on a flat and non-gradient surface is less susceptible to lower limb muscle kinematic injuries. Therefore, DTI is promising for detecting subclinical changes in lower limb muscles and monitoring recovery after different marathon runs. However, the use of DTI measurements as markers in the clinical setting remains challenging due to the difficulty of balancing signal-to-noise ratio, resolution, and acceptable scanning time, and also the need for reference values and large samples for prospective studies.

3.2.2.2 IVIM

IVIM is a noninvasive MRI technique that utilizes multiple b-value dMRI to separate and quantify "true diffusion" and "pseudodiffusion" information of water molecule movement and microcirculatory perfusion in tissues (24). "Based on a biexponential model, perfusion and diffusion components can be determined simultaneously in lower limb muscle tissue (25)." A small prospective study involving 16 healthy recreational marathon runners (18) showed that the IVIM microvascular perfusion fraction f of the popliteus muscle was significantly higher 2-3 h after participation in a half-marathon compared with the pre-run period, suggesting an increase in blood perfusion. However, another study of 109 athletes with acute hamstring injuries showed (26) that a modified DTI sequence scan of the IVIM model of the bilateral thighs, performed 7 days after injury, revealed significant differences in all IVIM-DTI diffusion parameters (e.g., FA, MD) between the injured side and the contralateral healthy muscle, with the exception of the perfusion fraction, f. To enable routine clinical monitoring of hamstring injuries, this study also proposed an IVIM-DTI method using a multiband acceleration technique, which reduced the scanning time from 11 min 08 s to 3 min 40 s without compromising the sensitivity of the quantitative outcome parameters to hamstring injuries. Thus, the effect of marathon exercise on lower limb muscle microcirculatory perfusion is unclear. Future studies need to analyze larger longitudinal sample sizes by IVIM or IVIM-DTI sequences with multiband acceleration techniques to make routine clinical monitoring of marathon exercise-induced lower extremity microinjuries possible.

3.2.3 MRS and CEST

MRS is an examination method based on the principle of MRI, which identifies and quantifies different chemical substances and their contents by utilizing small differences in the resonance frequencies of atomic nuclei in different chemical environments within the body to distinguish between different chemical shifts. This technology allows for non-invasive detection of energy metabolism in living muscle tissue. Currently, MRS studies of the effects of marathon running on lower limb muscle metabolism have focused on both ¹H-MRS and ³¹P-MRS, which can be measured using 1.5T, 3T, or mobile MRI equipment (27–29). But there is little evidence in the literature that MRS Images muscle

damage after marathon running. A small prospective study (30) involving 12 male runners with regular endurance training examined the effects of marathons of varying intensities and durations on muscle; the study measured intramyocellular lipid (IMCL) content in the tibialis anterior and soleus muscles before and after exercise with the ¹H-MRS, and the results showed that the content of IMCL in the tibialis anterior muscle and soleus muscle decreased significantly with the increase of the duration of moderate intensity marathon running. However, when the intensity was higher and the duration was similar, the IMCL content did not decrease significantly. In another more interesting study (31), IMCL content in the tibialis anterior muscle was measured pre- and mid-race in 22 regular endurance runners participating in a multi-stage ultra-marathon using a mobile ¹H-MRS, and the results showed a significant increase in IMCL values compared to the pre-run period during higherintensity, longer-duration aerobic exercise. Thus, in regular endurance runners, lower limb muscle IMCL content may have a U-shaped relationship with intensity and duration of marathon running. IMCL content at different intensities and durations of marathon running is critical in explaining the role of fatty acids as a source of energy within skeletal muscle and in relation to insulin sensitivity. However, the high requirements of MRS for spatial homogeneity of static magnetic field, hardware stability, and complex scanning techniques, especially ³¹P-MRS, which requires additional hardware equipment and software for transmitting/receiving at the appropriate resonance frequencies, limit its clinical application in studying the effects of marathon running on lower limb muscles. In addition, ¹H-MRS and ³¹P-MRS cannot measure free creatine (Cr) in energy metabolism (32), whereas the emerging CEST technology can measure changes in free Cr (32, 33), pH values (34), and lactate concentrations (35) in human leg muscles before and after mild to moderate exercise. CEST is a non-invasive, high-resolution biochemical imaging tool that uses specific pulses to saturate hydrogen protons in macromolecules and then exchanges the saturated signal with hydrogen protons in surrounding free water. This allows for measuring the difference in free water signals to indirectly reflect macromolecule concentrations. Therefore, future research could consider using CEST technology to monitor the impact of marathons on lower limb muscle metabolites, which may provide new insights into muscle microtrauma.

3.3 Multi-modal quantitative MRI techniques

At present, in order to fully analyze the imaging mechanism of the lower limb muscle microtrauma caused by marathon, multimodal quantitative MRI technology is adopted in the research. Through the combination of different modes or the multicontrast imaging of a single scan, the muscle structure and function are comprehensively analyzed from multiple angles. For example, in a study of 20 extreme mountain ultra-marathon runners (23), the quadriceps muscle was automatically segmented

(36) by a T1 3D sequence based on the Dixon algorithm to quantify its volume, and based on this T1 structure image, the proton density fat fraction (PDFF), T2*, and internal magnetic susceptibility (χ) have been simultaneously calculated using 3D spoiled gradient echo sequence, and muscle T2 values were quantified by a 2D multiecho T2-weighted spin-echo sequence. Combined multimodal analyses of quadriceps structure, energy reserve status, and cellular water content revealed significant increases in T2 and T2* values and a slight increase in quadriceps volume from 48 to 72 h post-competition, whereas PDFF and χ remained relatively stable, suggesting that the multimodal quantification technique may reveal that extreme eccentric loading runs place significant biomechanical stresses on the quadriceps muscle that translate into a pronounced inflammatory burden. However, the combination of different modal techniques tends to add additional scan time and is limited in clinical applications.

SyMRI techniques greatly reduce scan time by allowing multiple sequences of contrast-weighted images to be acquired in a single image acquisition. For example, in a study of 24 amateur marathon runners (37), knee joints were scanned using SyMRI using a multi-delay multi-echo sequence. Conventional contrast weighted images such as T1WI, T2WI, proton density weighted imaging (PDWI) and short time inversion recovery (STIR), as well as quantitative maps T1, T2 and corresponding relaxation rates R1 (1/T1), R2 (1/T2) and proton density (PD) were obtained within 8 min and 5 s. The results showed that T1, T2, and PD values were elevated in the periprosthetic muscle subregion of the knee joint in most subjects compared to the pre-race period within 48 h after the marathon, and decreased after 1 month of rest (37). In conclusion, the various quantitative parameters obtained from the SyMRI technique effectively detect microscopic changes in muscles before and after marathon exercise, offering a valuable tool for the future monitoring of muscle-related diseases.

4 Conclusion

The microtrauma caused by marathon exercise to lower limb muscles is manifested in imaging as a diversity of microstructural and functional changes. Quantitative single-modality MRI techniques such as T2 mapping, DTI, IVIM, MRS and CEST are effective in capturing changes in inflammatory edema, subclinical alterations, microcirculatory perfusion, and energy metabolism in muscles, and provide a powerful tool for quantitative assessment of sports injuries. However, the limitations of single-modal techniques may not fully reveal the whole picture of sports injuries in some cases. By combining information of different modes or SyMRI technology, multi-modal quantitative MRI technology can more comprehensively analyze the structural and functional damage of lower limb muscles caused by marathon exercise, especially in extreme mountain ultra-marathon high-intensity exercise, providing important biomechanical and inflammatory burden indicators. However, a major problem is the lack of standardization in the process of clinical conversion of both single-modal and multimodal MRI techniques. Therefore, prospective longitudinal studies with large sample sizes are necessary to determine standardized processes for these technologies.

Future studies should further explore the potential application of quantitative MRI to observe the longitudinal trends of marathon runners after lower extremity muscle injury by plotting curves through the time axis (x-axis) and quantitative measurements (e.g., T2, T2* values, diffusion, perfusion parameters, and metabolite content) on the y-axis, in an attempt to determine the threshold for safe return to play; such quantitative thresholds would help clinicians, compared with traditional MRI assessments, to physicians to more accurately assess marathoners' return-to-play time and risk of reinjury (38). In addition, prospective longitudinal studies should expand the sample size to cover different types of marathon events and diverse athlete populations to validate the accuracy and reliability of these techniques in a wider range of applications. Meanwhile, attention should be paid to the potential application of multimodal techniques such as SyMRI-based techniques, exploring their advantages in rapid scanning and comprehensive analysis, aiming at efficient and accurate sports injury monitoring and assessment, and providing a more reliable basis for rehabilitation and re-injury risk prediction in athletes or active individuals.

Author contributions

YC: Data curation, Formal Analysis, Investigation, Methodology, Writing – original draft, Writing – review & editing. XKL: Supervision, Writing – original draft, Writing – review & editing.

Funding

The author(s) declare financial support was received for the research, authorship, and/or publication of this article. Funding was provided by the Ruijin Hospital, Shanghai Jiaotong University School of Medicine. Project: Sub-projects of major R&D projects of the Ministry of Science and Technology of China, Project Number: 2023YFC2410704. This grant was awarded to XKL.

Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

Publisher's note

All claims expressed in this article are solely those of the authors and do not necessarily represent those of their affiliated organizations, or those of the publisher, the editors and the reviewers. Any product that may be evaluated in this article, or claim that may be made by its manufacturer, is not guaranteed or endorsed by the publisher.

References

1. Horga LM, Henckel J, Fotiadou A, Di Laura A, Hirschmann AC, Hart AJ. Magnetic resonance imaging of the hips of runners before and after their first marathon run: effect of training for and completing a marathon. *Orthop J Sports Med.* (2021) 9(7):23259671211010405. doi: 10.1177/23259671211010405

2. Petersen K, Hansen CB, Aagaard P, Madsen K. Muscle mechanical characteristics in fatigue and recovery from a marathon race in highly trained runners. *Eur J Appl Physiol.* (2007) 101(3):385–396. doi: 10.1007/s00421-007-0504-x

3. Howatson G, van Someren KA. The prevention and treatment of exercise-induced muscle damage. *Sports Med.* (2008) 38(6):483–503. doi: 10.2165/00007256-200838060-00004

4. Inami T, Nakagawa K, Yonezu T, Fukano M, Higashihara A, Iizuka S, et al. Tracking of time-dependent changes in muscle hardness after a full marathon. *J Strength Cond Res.* (2019) 33(12):3431. doi: 10.1519/JSC.00000000002495

5. Petersen J, Thorborg K, Nielsen MB, Budtz-Jørgensen E, Hölmich P. Preventive effect of eccentric training on acute hamstring injuries in men's soccer. *Am J Sports Med.* (2011) 39(11):2296–303. doi: 10.1177/0363546511419277

 Biglands JD, Grainger AJ, Robinson P, Tanner SF, Tan AL, Feiweier T, et al. MRI in acute muscle tears in athletes: can quantitative T2 and DTI predict return to play better than visual assessment? *Eur Radiol.* (2020) 30(12):6603–13. doi: 10.1007/ s00330-020-06999-z

7. Kawai T, Takahashi M, Takamoto K, Bito I. Hamstring strains in professional rugby players result in increased fascial stiffness without muscle quality changes as assessed using shear wave elastography. *J Bodyw Mov Ther.* (2021) 27:34–41. doi: 10.1016/j.jbmt.2021.03.009

8. *Hooijmans MT, Monte JRC, Froeling M, van den Berg-Faay S, Aengevaeren VL, Hemke R, et al. Quantitative MRI reveals microstructural changes in the upper leg muscles after running a marathon. *J Magn Reson Imaging*. (2020) 52(2):407–17. doi: 10.1002/jmri.27106

 Rubin EB, Schmidt AM, Koff MF, Kogan F, Gao K, Majumdar S, et al. Advanced MRI approaches for evaluating common lower extremity injuries in basketball players: current and emerging techniques. J Magn Reson Imaging. (2024) 59(6):1902–13. doi: 10.1002/jmri.29019

10. *Fukano M, Nakagawa K, Higashihara A, Inami T, Narita T. Damage and recovery of the intrinsic and extrinsic foot muscles from running a full marathon. *Scand J Med Sci Sports.* (2023) 33(8):1486–93. doi: 10.1111/sms.14377

11. *Zhang RX, Yu H, Zhang P, Li JJ, Ren CC, Zhao J. Analysis of the characteristics of MRI T2 value changes of the muscles around the knee joint before and after the race in amateur marathon runners based on T2 mapping. *Zhonghua Yi Xue Za Zhi.* (2022) 102(9):648–53. doi: 10.3760/cma.j.cn112137-20210626-01448

12. *Froeling M, Oudeman J, Strijkers GJ, Maas M, Drost MR, Nicolay K, et al. Muscle changes detected with diffusion-tensor imaging after long-distance running. *Radiology*. (2015) 274(2):548–62. doi: 10.1148/radiol.14140702

13. Crema MD, Roemer FW, Marra MD, Burstein D, Gold GE, Eckstein F, et al. Articular cartilage in the knee: current MR imaging techniques and applications in clinical practice and research. *Radiographics.* (2011) 31(1):37–61. doi: 10.1148/rg. 311105084

14. *Maeo S, Ando Y, Kanehisa H, Kawakami Y. Localization of damage in the human leg muscles induced by downhill running. *Sci Rep.* (2017) 7(1):5769. doi: 10. 1038/s41598-017-06129-8

15. Patten C, Meyer RA, Fleckenstein JL. T2 mapping of muscle. Semin Musculoskelet Radiol. (2003) 7:297–307. doi: 10.1055/s-2004-815677

16. Fulford J, Eston RG, Rowlands AV, Davies RC. Assessment of magnetic resonance techniques to measure muscle damage 24 h after eccentric exercise. *Scand J Med Sci Sports.* (2015) 25(1):e28–39. doi: 10.1111/sms.12234

17. Mathur S, Vohra RS, Germain SA, Forbes S, Bryant ND, Vandenborne K, et al. Changes in muscle T2 and tissue damage following downhill running in mdx mice. *Muscle Nerve.* (2011) 43(6):878–86. doi: 10.1002/mus.21986

18. *Shu D, Zhang C, Dai S, Wang S, Liu J, Ding J. Acute effects of foam rolling on hamstrings after half-marathon: a muscle functional magnetic resonance imaging study. *Front Physiol.* (2021) 12:1–12. doi: 10.3389/fphys.2021.723092

19. *Higashihara A, Nakagawa K, Inami T, Fukano M, Iizuka S, Maemichi T, et al. Regional differences in hamstring muscle damage after a marathon. *PLoS One.* (2020) 15(6):e0234401. doi: 10.1371/journal.pone.0234401

20. *Zhou J, Zhang L, Chen LL, Lin XY, Zheng XZ, Yao WZ, et al. Diffusion tensor imaging in quantitative evaluation on thigh muscle of male amateur marathon runners

after running a half marathon. Zhonghua Yi Xue Za Zhi. (2022) 102(9):642–7. doi: 10. 3760/cma.j.cn112137-20210716-01591

21. Zeng PE, Zhou YL, Jian Y. Progress of functional MRI in muscle injury. Int J Med Radiol. (2019) 42(2):189–92. doi: 10.19300/j.2019.Z6630

22. *Zhang L. Preliminary magnetic resonance imaging study on the effects of marathon on human thigh muscles. Dissertation/master's thesis. Hangzhou: Hangzhou Normal University (2020).

23. *Nguyen HT, Grenier T, Leporq B, Le Goff C, Gilles B, Grange S, et al. Quantitative magnetic resonance imaging assessment of the quadriceps changes during an extreme mountain ultramarathon. *Med Sci Sports Exerc.* (2021) 53 (4):869–81. doi: 10.1249/MSS.00000000002535

24. Le Bihan D, Breton E, Lallemand D, Aubin ML, Vignaud J, Laval-Jeantet M. Separation of diffusion and perfusion in intravoxel incoherent motion MR imaging. *Radiology.* (1988) 168(2):497–505. doi: 10.1148/radiology.168.2.3393671

25. Adelnia F, Shardell M, Bergeron CM, Fishbein KW, Spencer RG, Ferrucci L, et al. Diffusion-weighted MRI with intravoxel incoherent motion modeling for assessment of muscle perfusion in the thigh during post-exercise hyperemia in younger and older adults. *NMR Biomed.* (2019) 32(5):e4072. doi: 10.1002/nbm.4072

26. *Rauh SS, Suskens JJM, Monte JR, Smithuis F, Gurney-Champion OJ, Tol JL, et al. Accelerated IVIM-corrected DTI in acute hamstring injury: towards a clinically feasible acquisition time. *Eur Radiol Exp.* (2024) 8(1):38. doi: 10.1186/ s41747-024-00437-1

27. Baguet A, Everaert I, Hespel P, Petrovic M, Achten E, Derave W. A new method for non-invasive estimation of human muscle fiber type composition. *PLoS One.* (2011) 6(7):e21956. doi: 10.1371/journal.pone.0021956

28. *Mäurer J, Konstanczak P, Söllner O, Ehrenstein T, Knollmann F, Wolff R, et al. Muscle metabolism of professional athletes using 31P-spectroscopy. *Acta Radiol.* (1999) 40(1):73-7. doi: 10.1080/02841859909174407

29. *Schütz UH, Schmidt-Trucksäss A, Knechtle B, Machann J, Wiedelbach H, Ehrhardt M, et al. The transeurope footrace project: longitudinal data acquisition in a cluster randomized mobile MRI observational cohort study on 44 endurance runners at a 64-stage 4,486km transcontinental ultramarathon. *BMC Med.* (2012) 10(1):78. doi: 10.1186/1741-7015-10-78

30. *Brechtel K, Niess AM, Machann J, Rett K, Schick F, Claussen CD, et al. Utilisation of intramyocellular lipids (IMCLs) during exercise as assessed by proton magnetic resonance spectroscopy (1H-MRS). *Horm Metab Res.* (2001) 33:63–6. doi: 10.1055/s-2001-12407

31. *König S, Jockenhöfer C, Billich C, Beer M, Machann J, Schmidt-Trucksäss A. Long distance running—can bioprofiling predict success in endurance athletes? *Med Hypotheses*. (2021) 146:110474. doi: 10.1016/j.mehy.2020.110474

32. *Kogan F, Haris M, Debrosse C, Singh A, Nanga RP, Cai K, et al. In vivo chemical exchange saturation transfer imaging of creatine (CrCEST) in skeletal muscle at 3T. *J Magn Reson Imaging*. (2014) 40(3):596–602. doi: 10.1002/jmri.24412

33. *Kogan F, Haris M, Singh A, Cai K, Debrosse C, Nanga RPR, et al. Method for high-resolution imaging of creatine in vivo using chemical exchange saturation transfer. *Magn Reson Med.* (2014) 71(1):164–72. doi: 10.1002/mrm.24641

34. *Rerich E, Zaiss M, Korzowski A, Ladd ME, Bachert P. Relaxation-compensated CEST-MRI at 7 T for mapping of creatine content and pH—preliminary application in human muscle tissue in vivo. *NMR Biomed.* (2015) 28(11):1402–12. doi: 10.1002/ nbm.3367

35. *DeBrosse C, Nanga RPR, Bagga P, Nath K, Haris M, Marincola F, et al. Lactate chemical exchange saturation transfer (LATEST) imaging in vivo: a biomarker for LDH activity. *Sci Rep.* (2016) 6(1):19517. doi: 10.1038/srep19517

36. Gilles B, Bourguignon C de, Croisille P, Millet G, Beuf O, Viallon M. Automatic Segmentation for Volume Quantification of Quadriceps Muscle Head: A Longitudinal Study in Athletes Enrolled in Extreme Mountain Ultra-Marathon. Singapore: ISMRM: International Society for Magnetic Resonance in Medicine (2016). Available online at https://hallirmm.ccsd.cnrs.fr/lirmm-01383144.

37. *Wu WH, Zhu HM, Zhu TT, Hu F, Guo YK, Li SL, et al. Monitoring changes of the muscles around the knee joint in amateur marathon athletes using synthetic magnetic resonance imaging: a preliminary stud. *Chin J Magn Reson Imaging.* (2023)14(7):98–102+120. doi: 10.12015/issn

38. Hayashi D, Roemer FW, Tol JL, Heiss R, Crema MD, Jarraya M, et al. Emerging quantitative imaging techniques in sports medicine. *Radiology*. (2023) 308(2):e221531. doi: 10.1148/radiol.221531