#### Check for updates

#### OPEN ACCESS

EDITED BY Emiliano Cè, University of Milan, Italy

#### REVIEWED BY

Clayton L. Camic, Northern Illinois University, United States Takafumi Ando, National Institute of Advanced Industrial Science and Technology (AIST), Japan

\*CORRESPONDENCE Naomi Omi,

RECEIVED 17 October 2023 ACCEPTED 23 January 2024 PUBLISHED 15 February 2024

🖂 omi.naomi.gn@u.tsukuba.ac.jp

#### CITATION

Ogata H, Negishi Y, Koizumi N, Nagayama H, Kaneko M, Kiyono K and Omi N (2024), Individually optimized estimation of energy expenditure in rescue workers using a tri-axial accelerometer and heart rate monitor. *Front. Physiol.* 15:1322881. doi: 10.3389/fphys.2024.1322881

#### COPYRIGHT

© 2024 Ogata, Negishi, Koizumi, Nagayama, Kaneko, Kiyono and Omi. This is an openaccess article distributed under the terms of the **Creative Commons Attribution License (CC BY)**. The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.

# Individually optimized estimation of energy expenditure in rescue workers using a tri-axial accelerometer and heart rate monitor

# Hitomi Ogata<sup>1</sup>, Yutaro Negishi<sup>2</sup>, Nao Koizumi<sup>2</sup>, Hisashi Nagayama<sup>2</sup>, Miki Kaneko<sup>3</sup>, Ken Kiyono<sup>3</sup> and Naomi Omi<sup>2</sup>\*

<sup>1</sup>Graduate School of Humanities and Social Sciences, Hiroshima University, Hiroshima, Japan, <sup>2</sup>Faculty of Health and Sport Sciences, University of Tsukuba, Tsukuba, Japan, <sup>3</sup>Graduate School of Engineering Science, Osaka University, Toyonaka, Japan

**Objectives:** This study aimed to provide an improved energy expenditure estimation for heavy-load physical labor using accelerometer data and heart rate (HR) measured by wearables and to support food preparation and supply management for disaster relief and rescue operations as an expedition team.

**Methods:** To achieve an individually optimized estimation for energy expenditure, a model equation parameter was determined based on the measurements of physical activity and HR during simulated rescue operations. The metabolic equivalent of task (MET), which was measured by using a tri-axial accelerometer and individual HR, was used, where two (minimum and maximum) or three (minimum, intermediate, and maximum) representative reference points were selected for each individual model fitting. In demonstrating the applicability of our approach in a realistic situation, accelerometer-based METs and HR of 30 males were measured using the tri-axial accelerometer and wearable HR during simulated rescue operations over 2 days.

**Results:** Data sets of 27 rescue operations (age:34.2  $\pm$  7.5 years; body mass index (BMI):22.9  $\pm$  1.5 kg/m<sup>2</sup>) were used for the energy expenditure estimation after excluding three rescue workers due to their activity type and insufficient HR measurement. Using the combined approach with a tri-axial accelerometer and HR, the total energy expenditure increased by 143% for two points and 133% for three points, compared with the estimated total energy expenditure using only the accelerometer-based method.

**Conclusion:** The use of wearables provided a reasonable estimation of energy expenditure for physical workers with heavy equipment. The application of our approach to disaster relief and rescue operations can provide important insights into nutrition and healthcare management.

#### KEYWORDS

rescue operations, metabolic equivalent of task, disaster simulation training, estimation equation, wearable

# 1 Introduction

An accurate estimation of energy expenditure can provide important information and guidelines for nutrition and healthcare management of physical workers. In particular, disaster relief and rescue teams must prepare and transport their food supplies in advance. The higher the degree of energy deficiency, the lower the energy expenditure in activity, especially during highintensity physical activity, and the more significant the decrease in energy expenditure (Martin et al., 2011). Based on the studies conducted by the U.S. military, the lack of energy promotes muscle damage and muscle soreness, decreases the performance of physical activities (Margolis et al., 2014), causes weight loss and a greater percentage of muscle mass loss than fat mass (Berryman et al., 2017), decreased immune function (T lymphocyte response) (Kramer et al., 1997), and decreased cardiac function (altered left ventricular diastolic function) (Planer et al., 2012). Therefore, the total amount of food supplied must be sufficient to meet the nutritional needs of the body and to maintain the energy required for high-intensity physical activity. However, energy expenditure estimation methods for such workers have not been well established, and the energy expenditure during such operations remains unclear.

With recent advancements in sensor technologies, portable devices are becoming smaller, capable of longer data collection (because of their storage and battery lives), multidimensional, and more sensitive (Chen et al., 2012). Many movement sensors can be used to measure human physical activities, including electromechanical switches (for heel strike detection), mercury switches, pedometers, inclinometers, gyroscopes, goniometers (for angles or postures), accelerometers, and even global positioning systems (GPS) (Chen et al., 2012). Among these devices, accelerometers are currently the most widely used sensors for human physical activity monitoring in clinical and free-living settings (Chen et al., 2012) because of their small size, noninvasiveness, and relatively low cost (Plasqui and Westerterp, 2007). Moreover, accelerometers can easily estimate the amount of energy expenditure during high-intensity physical activities, except for heavy equipment and static load activities (Bouten et al., 1997). However, discriminating movements during daily low-intensity physical activities and estimating the appropriate energy expenditure remain a challenge (Ndahimana and Kim, 2017). Some tri-axial accelerometers have shown potential application in estimating the amount of energy expenditure during low-intensity physical activities, such as sitting, standing, housework, and walking, which are important for estimating total energy expenditure (Midorikawa et al., 2007; Yamada et al., 2009; Ohkawara et al., 2011). When measuring the total energy expenditure in field validation studies (double-labeled water (DLW), which is the gold standard for measuring total energy expenditure in the field), high correlations with the total energy expenditure estimate were found in most activity monitors (Van Remoortel et al., 2012). However, these correlations are to a large extent driven by subject characteristics, body weight, age, and height, which are important predictors of total energy expenditure (Plasqui et al., 2005). Based on previous reports, only 19% of the total energy expenditure is accounted for by physical activity in healthy subjects (Plasqui et al., 2005) and in patients with coronary heart disease (Ades et al., 2005) in a field setting. Previous research demonstrated that wearable devices, such as movement sensors, do not accurately represent energy expenditure measured by the DLW (Murakami et al., 2019; Willis et al., 2022). Several studies have also compared the DLW method to the total energy expenditure estimated by using accelerometers. The total energy expenditure using an accelerometer in patients with reduced pulmonary function, particularly chronic obstructive pulmonary disease, is underestimated by 11% compared with the DLW (Sato et al., 2021). Even the total energy expenditure of people who are not engaged in heavy physical activity is underestimated compared with that of accelerometer. A wristmounted motion sensor accounts for 78% of the variation of total energy expenditure using the DLW during the free-living period and 62% during the training period (Kinnunen et al., 2019). The total energy expenditure using an accelerometer in firefighters under normal working conditions is underestimated by 33% compared with the DLW (Touno et al., 2003). In the literature, the total energy expenditure by the accelerometer is underestimated compared with the DLW (Touno et al., 2003; Kinnunen et al., 2019; Murakami et al., 2019; Sato et al., 2021; Willis et al., 2022) despite the difference between wrist-mounted and waist/chest-worn accelerometers (Kinnunen et al., 2019). Therefore, the energy expenditure estimation for heavy equipment and static load activities has an underestimation bias, although accelerometerbased methods are convenient and applicable to real-world situations (Touno et al., 2003).

Various wearable devices to monitor heart rate (HR) have been developed, such as wristwatches, ear clips, and undershirts, and some devices can measure HR accurately. These devices can record HR noninvasively, with minimal technical effort and without the constraints of laboratory conditions (Karmen et al., 2019; Isakadze and Martin, 2020). The HR increases almost proportionally to exercise intensity and intra-individual oxygen uptake (% VO2 max), and its dynamics can influence a number of different factors, such as body temperature, food intake, body posture, and individual cardiorespiratory fitness level (Hill and Trowbridge, 1998). However, the use of HR wearable devices, most of which are wrist-worn devices, may underestimate energy expenditure and provide inaccurate measures of energy expenditure compared with reference standard criterion measures, including direct calorimetry and indirect calorimetry (Fuller et al., 2020; Chevance et al., 2022). Summarizing the total energy expenditure by most of the aforementioned devices, such as accelerometer, HR, GPS, and combined motion sensors, provides a more accurate estimation of energy expenditure at light-to-moderate intensities; by contrast, underestimation increases at very light and higher intensity activities (Aparicio-Ugarriza et al., 2015).

A previous review reported that adding indicators such as HR and heat flux values to acceleration values as a method of estimating daily energy expenditure and physical activity has not significantly improved the system (Van Remoortel et al., 2012). Nevertheless, focusing on the HR that can be measured with a wearable device can address the underestimation of energy expenditure by using only a tri-axial accelerometer because HR can relate intensity to energy expenditure. This study aimed to provide an energy expenditure estimation method using wearables to support food preparation and supply management, particularly for expedition rescue team workers with heavy equipment and static loads. By combining the characteristics of tri-axial accelerometers and HR monitor information, we evaluated the relationship between accelerometerbased physical activity and HR and provided an individually optimized energy expenditure estimation equation (model). Providing an equation/model to predict energy expenditure would promote the estimation of energy expenditure in the field, which is not measurable in the laboratory. As an application of this approach, the energy expenditure of rescue operations was estimated while mimicking large-scale disasters.

# 2 Materials and methods

#### 2.1 Subjects

This study included 30 males (age:  $34.2 \pm 7.3$  years; body mass index (BMI):  $23.1 \pm 1.7$  kg/m<sup>2</sup>) who participated in a 2-day disaster simulation training (i.e., rescue operations were unaware of the training protocol). Note that some of the firefighters of our previously reported paper were included in the present study (Koizumi et al., 2021). This study was approved by the local ethics committee of the University of Tsukuba (approval number: tai-28-66), conducted in accordance with the principles set forth in the Declaration of Helsinki, and the subjects were informed of and agreed to the details of this study. In addition, detailed explanations were given to each training director and participating organizationaffiliated institution regarding the purpose and content of the experiment, and the experiment was started only after obtaining agreement.

## 2.2 Simulated rescue operations

Rescue operation training was conducted from November 30 to 1 December 2018, in Kanagawa Prefecture, Japan. The mean temperature of the 2-day training was 12.8°C (8.5°C–18.3°C), with humidity of 55.5%. The main activities were as follows: rescue activity training in a skyscraper, in a gas leak accident, in a collapsed building, at a sediment-related disaster site, in the event of many injured people on the subway, from vehicles, and in a tunnel collapse accident; fire-extinguishing activity training in an industrial complex fire.

# 2.3 Measurements

#### 2.3.1 Accelerometer

Figure 1 shows flow chart of calculating energy expenditure. A tri-axial accelerometer (Active style Pro HJA-750C, 23 g, 40 mm  $\times$  52 mm  $\times$  12 mm; Omron Healthcare Co., Ltd., Kyoto, Japan) (Ohkawara et al., 2011; Nagayoshi et al., 2019; Nishida et al., 2020) was inserted into the chest pocket, located near the waist area (approximately 10 cm above the belt). The accelerometer was covered with a vinyl material and fixed in the chest pocket with adhesive tape to avoid the influence of liquid matter (e.g., water) in fire-extinguishing activities. The basic metabolic rate was calculated automatically when weight, height, age, and sex were entered, which was calculate using Ganpule's formula (Ganpile et al., 2007). The accelerometer was programmed to save the metabolic equivalent of

task (MET) once every 10 s using a built-in Omron's algorithm (Oshima et al., 2010; Ohkawara et al., 2011). MET is defined as the ratio of the metabolic rate during an activity to the metabolic rate at rest (Jetté et al., 1990). Next, each transformed data point (METs) was converted into units of activity energy expenditure in kcal/min (Oshima et al., 2010; Ohkawara et al., 2011) to understand the amount of energy intake, and the data were divided and aggregated for each activity (see Section 2.3.2 Recording paper).

#### 2.3.2 Recording paper

A recording paper was distributed, and rescue squads were asked to describe the activities that they performed during the disaster simulation training. This recording paper was used to classify the types and times of activities.

#### 2.3.3 HR monitor

R–R intervals were measured by electrocardiogram signals using wearable HR sensors (WHS-1, myBeat, 14 g, 39 mm × 37 mm × 9 mm; Union Tool Co., Tokyo, Japan) (Arikawa et al., 2020). The HR sensor was placed on a shirt with attached conductive fiber electrodes (Kurabo Industries Ltd., Osaka, Japan, Figure 2). The HR per minute [beats per minute (bpm)] was estimated using the median of instantaneous HRs during a 1min period to reduce the effect of the outliers presented in R–R interval data. If the absolute difference of the successive R–R intervals was larger than 200 ms, then the detected R–R interval was classified as an outlier using R version 3.6.0 (R Foundation for Statistical Computing, Vienna, Austria; http://www.R-project.org/). The percentage of the outlier R–R interval for each individual was also calculated.

#### 2.3.4 Estimation equation (model)

A percent of HR reserve (%HRR) provides a good approximation (almost linear relation) of  $\dot{VO}_2$  reserve ( $(\dot{VVO}_2)$ ) was shown in the previous studies (Swain et al., 1998; Strath et al., 2000), and an HR-based equation can provide a reliable estimation of the METs (Swain et al., 1998; Strath et al., 2000). % HRR is defined as follows:

$$\% HRR = \frac{HR_{activity} - HR_{rest}}{HR_{max} - HR_{rest}} \times 100$$

where  $HR_{activity}$  is the recorded HR during the activity;  $HR_{rest}$  is the HR while sitting at rest, and HRmax is the maximum HR as estimated by the Karvonen equation, (220 bpm—age) bpm.  $\%\dot{VO}_2$  reserve is defined as follows:

$$\% \dot{\mathrm{VO}}_{2}\mathrm{R} = \frac{\dot{\mathrm{VO}}_{2\mathrm{act}} - \dot{\mathrm{VO}}_{2\mathrm{rest}}}{\dot{\mathrm{VO}}_{2\mathrm{max}} - \dot{\mathrm{VO}}_{2\mathrm{rest}}} \times 100,$$

where  $\dot{V}O_{2activity}$  is the recorded  $\dot{V}O_2$  during the activity;  $\dot{V}O_{2rest}$  is the  $\dot{V}O_2$  while sitting at rest, and  $\dot{V}O_{2max}$  is the maximum  $\dot{V}O_2$  as estimated by the equation proposed by Jackson et al. (1990). By assuming %HRR  $\approx \% \dot{V}O_2 R$  and dividing the numerator and denominator of the  $\% \dot{V}O_2 R$  by the  $\dot{V}O_{2rest}$ , we obtain the following equation:

$$\frac{\mathrm{HR}_{\mathrm{act}} - \mathrm{HR}_{\mathrm{rest}}}{\mathrm{HR}_{\mathrm{max}} - \mathrm{HR}_{\mathrm{rest}}} = \frac{\frac{\mathrm{VO}_{2\mathrm{act}}}{\mathrm{VO}_{2\mathrm{rest}}} - 1}{\frac{\mathrm{VO}_{2\mathrm{rest}}}{\mathrm{VO}_{\mathrm{rest}}} - 1} = \frac{\mathrm{METS}_{\mathrm{act}} - 1}{\mathrm{METS}_{\mathrm{max}} - 1}$$



# Accelerometer

Active style Pro HJA-750C (Omron Healthcare Co., Ltd., Kyoto, Japan)

#### Default

Estimated MET every 10 s using a built-in Omron's algorithms (Ohkawara et al., 2011; Oshima et al., 2010)

## #1: Setting (calculating basal metabolic rate)

To calculate the basal metabolic rate (BMR) with subject's data (age, sex, weight, and height) automatically using the Ganpules's formula (Ganpile et al., 2007)

#### #2: Download data

Using a dedicated application

#### #3: Converted the MET to kcal/min

Using Ohkawara et al and Ohshima et al's algorithms (Ohkawara et al., 2011; Oshima et al., 2010)

# HR monitor



WHS-1, myBeat (Union Tool Co., Tokyo, Japan)

**#1: Setting** Measured R-R interval

#### #2: Download data

Using a dedicated application

#### #3: Estimated HR per minute (bpm)

Calculating the median of instantaneous HRs during a 1-min period (outlier defined the absolute difference of the successive R-R intervals was larger than 200 ms) using R.

#### #4: Divided and aggregated for each activity Using recording paper

#### #5: Check HR and METs data

Check the trends in HR and METs for each activity and picked up activities that cause a discrepancy between HR and MET.

#### #6: Estimation equation (model)

Select the MET value corresponding to the activity from the MET table (Ainsworth et al., 2011), calculate the 10th percentile, 50th percentile, or 90th percentile of HR during the selected each individual and activity, and create a 2-point or 3-point estimation equation.

The estimation equation and R<sup>2</sup> were calculated using least-square-fitting.

#### #7: Calculate total energy expenditure

Total energy consumption was calculated by summing the following four components, BMR, diet induced thermogenesis (DIT), activity energy expenditure (AEE) estimated by HR, and AEE measured by accelerometer. 1: The BMR and DIT, which are automatically calculated by entering each individual's data into the accelerometer (Ohkawara et al., 2011; Ganpile et al., 2007).

2: By substituting HR during activities into this model (**#6**), it was possible to calculate MET during activities that cause a discrepancy between HR and MET. And then, the MET data converted to kcal using a conversion formula (Ohkawara et al., 2011; Oshima et al., 2010).

**3:** Estimated MET (by measuring accelerometer) during activities other than the above were converted to kcal using a conversion formula (Ohkawara et al., 2011; Oshima et al., 2010).

FIGURE 1

Flow chart of calculating energy expenditure.



#### FIGURE 2

T-shirt attached with conductive fiber electrodes (backside). Stretchy shirts with electrodes were placed in the psoas. The size of the T-shirt was selected on the basis of the physique of the rescue operations.



Based on the abovementioned relation, we obtain the following equation for MET estimation (Strath et al., 2000):

$$METS_{act} = \frac{METS_{max} - 1}{HR_{max} - HR_{rest}} \left(HR_{act} - HR_{rest}\right) + 1$$

Therefore, if we use two reference conditions with different METs, METS<sub>1</sub> and METS<sub>2</sub>, instead of resting and the maximum  $\dot{V}O_2$  condition, then we can obtain a more general equation for MET estimation.

$$METS_{act} = \frac{MET_2 - MET_1}{HR_2 - HR_1} (HR_{act} - HR_1) + METS_1, (*)$$

where  $HR_1$  and  $HR_2$  are the HR recorded during the activity with METS<sub>1</sub> and METS<sub>2</sub>, respectively.

We used two (minimum and maximum) or three (minimum, intermediate, and maximum) representative reference points recorded in each individual (Figure 3) to obtain the parameters,  $(HR_1, MET_1)$ ,  $(HR_2, MET_2)$ , in the MET estimation equation [Eq (\*)] optimized to each individual. The lowest HR, HR<sub>1</sub>, corresponding MET<sub>1</sub> was calculated as follows: 1) the 10th percentile of HR during

napping was calculated as HR1, and 2) we defined the MET1 as 0.95 MET based on the MET table (Garby et al., 1987). We selected the 10th percentile of HR instead of the observed lowest value to attenuate the effect of outliers of the HR measurement. The intermediate HR was calculated as follows: First, the 50th percentile of HR during withdrawal was calculated as the intermediate HR because withdrawal was performed by all groups and was considered to be less affected by tension as it was performed after all activities were completed, and then we defined the intermediate HR as 3.0 MET based on the MET table (Ainsworth et al., 2011). Moreover, the highest HR corresponding to the highest MET during all activities was calculated as follows: First, the 90th percentile of HR was calculated for each rescue operation activity. Although the highest HR would be induced by the activity with the highest MET, we selected the 90th percentile of HR instead of the observed highest value to attenuate the effect of outliers of the HR measurement. Second, activity's METs were defined on the basis of the MET table (Table 1) (Ainsworth et al., 2011), and then the activity with the highest HR was selected. Finally, the parameters, (HR<sub>2</sub>, MET<sub>2</sub>), were estimated for all participants using a least-square-fitting on the abovementioned values.

#### TABLE 1 Activities corresponding to the MET table.

Code	Major heading	Activity <sup>a</sup> (description)	METs
05147	home activities	withdrawal (implied walking, putting away household items, moderate effort)	3.0
11240	occupation	rescue narrow space, rescue activity, rescue search (fire fighter, general)	
11244	occupation	rescue traffic, rescue transport (fire fighter, rescue victim, automobile accident, using pike pole)	
11245	occupation	fire training (fire fighter, raising and climbing ladder with full gear, simulated fire suppression)	
11246	occupation	gas rescue, rescue gas search, rescue gas transport (fire fighter, hauling hoses on ground, carrying/hoisting equipment, breaking down walls, wearing full gear)	
11550	occupation	rescue sediment, rescue tunnel (shoveling, more than 7.3 kg/min, deep digging, vigorous effort)	8.8
17029	walking	rescue activity training in a skyscraper (carrying 22.7-33.6 kg load, upstairs)	10.0

\*Activity represents the rescue operations conducted in this study. The code, major heading, description, and METs, are provided in the MET, table (Ainsworth et al., 2011).



training in a gas leak accident (yellow) and excavation rescue in a narrow space (light orange). Colors were categorized for each activity: gray, nap; orange, meeting; light blue, movement; blue, rest; ocher, eating; light green, standby; green, withdrawal; yellow, gas leak accident; light orange, rescue narrow space; and brown, training preparation.

These two rescue squads were excluded from analysis because one rescue squad was only able to measure their HR for 15% during their nap time, and the activity of another rescue squad did not include withdrawal.

## 2.3.5 Statistical analysis

Data are presented as mean values and standard deviations.

# **3** Results

# 3.1 Typical example of measurements

We measured the physical activity and HR from 8:30 to 11: 00 the next day. Figure 4 represents a typical example of METs and HR during simulated rescue operations (28 years, 173 cm, 72 kg).

#### TABLE 2 Heart rate during each activity.

Activity (METs) <sup>a</sup>	Heart rate (bpm) <sup>b</sup>	n
Nap (0.95 METs)	56.2 ± 13.5	27
Withdrawal (3.0 METs)	$104.8 \pm 17.2$	27
Rescue training from vehicles (6.8 METs)	121.9 ± 24.1	5
Search activity (6.8 METs)	125.4 ± 20.7	10
Rescuer transport (6.8 METs)	132.9 ± 16.9	5
Rescue training in a collapsed building (8.0 METs)	116.7 ± 20.3	15
General firefighting (8.0 METs)	132.5 ± 14.6	5
Excavation rescue search activity (8.8 METs)	128.2 ± 13.8	9
Tunnel accident rescue activity (8.8 METs)	131.2 ± 15.7	4
Rescue activity training in a gas leak accident (9.0 METs)	131.2 ± 21.2	15
General rescue activity (9.0 METs)	135.1 ± 17.8	10
Rescue activity training in a skyscraper (10.0 METs)	154.9 ± 23.9	20

The results are presented as mean values ±SD.

<sup>a</sup>The table shows the activities extracted to create the equations for the relationship between HR, and METs; the figure is based on the MET, table (Garby et al., 1987; Ainsworth et al., 2011). <sup>b</sup>HR, which was computed as the 10th percentile for nap, 50th percentile for withdrawal, and 90th percentile for other activities, is also shown. The number of rescue operations engaged in the activity is depicted as *n*.

The rescue worker engaged in rescue activity training in a gas leak accident (yellow) for 210 min, excavation rescue in narrow space (light orange) for 150 min, and nap (gray) for 330 min. The basic metabolic rate of the rescue worker, which is automatically calculated, was 1,600 kcal, and the total energy expenditure estimated by using the tri-axial accelerometer was 3,723 kcal (from 11:00 to 11:00 the next day). This example underestimated METs in the yellow and light-orange areas because the activities did not show high METs despite an increase in HR. Therefore, METs are more stable than HR during low-intensity activities, particularly during napping.

# 3.2 Calculation of HR for each activity

One rescue worker who conducted excavation rescue search and tunnel accident rescue activities could measure only the first 4 h (deficiency rate was 83.1%). Thus, the rescue worker was excluded from analysis. The percentage of missing HR data for each individual was  $4.7\% \pm 4.4\%$  (range: 0%–15.3%) for 27 rescue squads (age:  $34.2 \pm 7.5$  years; BMI:  $22.9 \pm 1.5$  kg/m<sup>2</sup>). The HR was computed as the 10th percentile for naps, 50th percentile for withdrawal, and 90th percentile for other activities. The number of subjects in each activity is summarized in Table 2. Nap had the lowest HR, and rescue activity training in a skyscraper had the highest HR.

# 3.3 Basic metabolic rate and estimated total energy expenditure by the tri-axial accelerometer

The tri-axial accelerometer automatically calculated the basic metabolic rate, with an average of  $1,545 \pm 92$  kcal, and the estimated

total energy expenditure, with an average of  $3,414 \pm 229$  kcal for 27 rescue squads (from 11:00 to 11:00 the next day).

# 3.4 Estimated total energy expenditure by combining the tri-accelerometer and HR

Figure 4 shows the estimation equation using two points (Figure 5A) created using the 10th percentile of HR during nap (0.95 METs) as the lowest HR and the 90th percentile of HR during rescue activity training in a gas leak accident (9.0 METs). Using three points (Figure 5B), the estimation equation was created using the abovementioned two points plus the intermediate 50th percentile of the HR during withdrawal (3.0 METs). The results showed that HR was higher during rescue training in a gas leak accident (9.0 METs) than during the excavation rescue in a narrow space (6.8 METs). Therefore, we developed an equation to estimate the highest HR for the latter (Figure 4). The energy expenditure calculated using the estimation equation replaced specific rescue activities, such as rescue activity training in a gas leak accident (yellow) and excavation rescue in a narrow space (light orange). The estimated total energy expenditure was 5,456 kcal using the twopoint equation and 4,945 kcal using the three-point equation. The difference between the estimated total energy expenditure by the triaxial accelerometer and that by combining the tri-axial accelerometer and HR was 1,733 kcal using the two-point equation and 1,222 kcal using the three-point equation.

The average value of  $R^2$  in the estimation equation was 0.895 (95% confidence interval: 0.858–0.932) using the three-point equation (minimum, intermediate, and maximum). The average corrected total energy expenditure obtained by the tri-axial accelerometer and HR was 4,871 ± 486 kcal and 4,555 ± 391 kcal, respectively. The average difference between the estimated total energy expenditure by the tri-axial accelerometer and that by



combining the tri-axial accelerometer and HR was  $1,457 \pm 486$  kcal and  $1,140 \pm 410$  kcal, respectively (accounting for an average increase of 143% and 133%, respectively).

# 4 Discussion

In this study, we developed a simple energy expenditure estimation method using wearables (tri-axial accelerometer and HR) for heavy load physical laborers to achieve a reliable estimation of energy expenditure for disaster relief and rescue workers as an expedition team. The relationship between the MET and individual HR in humans was also explored. If the minimum HR is known, then the maximum HR can be largely predicted; therefore, a model with some uniformity can be created without laboratory assessment. The strength of this study depends on the measurement of tri-axial acceleration, which can isolate each activity, capture a wide range of movement, as well as HR for rescue workers who experience various difficulties at the forefront, and estimate the total energy expenditure for each individual using a novel method in the field.

The MET concept, which expresses the intensity of physical activity by the time it corresponds to the resting metabolic rate, represents a simple, practical, and easily understood procedure to express the energy cost of physical activities as a multiple of the resting metabolic rate (Jetté et al., 1990); one MET represents the state of sitting and resting. In the present study, an accelerometer was used to store MET because energy expenditure can be calculated by multiplying the MET by a coefficient and individual body weight. The HR is high under the influence of mental and physical fatigue (Tanaka et al., 2011), stress, tension, and excitement (Cannon, 1929). Many researchers will conduct standardized laboratory assessments of resting and maximal HR before field testing using the submaximal test and/or Yo-Yo intermittent endurance test to determine maximal HR in the field (Sell and Ledesma, 2016). This approach is advantageous because the HR data in the field can be normalized to each individual, and other researchers can easily replicate those standardized tests. However, if only the minimum HR is known in humans, then the maximum HR can be largely predicted, that is, %HRR. Consequently, an estimation equation model with some uniformity can be created. Previous research demonstrated that estimating the total energy expenditure by using only an accelerometer is underestimated compared with the DLW (Touno et al., 2003; Kinnunen et al., 2019; Murakami et al., 2019; Sato et al., 2021; Willis et al., 2022). Therefore, given the nature of accelerometers, accurately measuring the total energy expenditure during heavy equipment or static load activities is difficult (Touno et al., 2003). In the present study, we combined METs and HR to improve underestimation.

METs differ depending on posture; therefore, we hypothesized that the METs during sitting and resting are different. Thus, 0.95 MET was derived from the original paper (Garby et al., 1987) of METs for a nap. We defined the minimum HR as the 10th percentile of nap time because the participating rescue squads operating in a blind training environment where they did not know what to do next slept very differently than usual and slept on their cots. In this study, the average HR during nap was  $68.3 \pm 15.3$  bpm/ min, which may also be affected by the abovementioned factors. The maximum HR was set at the 90th percentile of each rescue operation's activity because the same HR did not last forever, although the same activity was continued. Activity and activity time were classified on the basis of self-reported recording forms; however, the actual time spent waiting was also included, which may have reduced the HR during the activity. Although the training was conducted at relatively low temperatures in winter, the HR, which was set at the 90th percentile for training in winter conditions, may need to be higher because the load on the body is expected to be higher in summer than in winter. As rescue operations include various activities, not all activities can be applied to appropriate METs. However, a positive correlation was observed between METs and HR, indicating that the wearable device could accurately measure HR without burdening the subject. The HR values during multiple activities were consistent with those reported in previous studies (Rodahl, 1989; Parker et al., 2017). Average HRs during all tasks ranged from 110 to 130 bpm (Rodahl, 1989) and from 145 to 109 bpm for steep and flatlands, respectively (Parker et al., 2017). We defined withdrawal as an intermediate HR as it was an activity carried by all groups. In most rescue squad estimation equations, the intermediate point shifts downward. In this study, the METs may not be appropriate because withdrawal includes activities such as carrying heavy loads, moving, and feeling fatigue. Based on the error propagation law, the error in the estimated METS<sub>act</sub> depends on the accuracy of the measurements in METs and HR at the assumed maximum intensity. Improving the accuracy of those measurements with the aid of laboratory measurements is a future challenge.

A previous systematic review reported that tri-axial and multisensory devices tend to be more valid monitors compared with the DLW while adding indicators such as HR and heat flux values to acceleration values to estimate daily energy expenditure, and physical activity has only slightly improved the system (Van Remoortel et al., 2012). In addition, the combination of motion sensor and HR is valid for estimating free-living energy expenditure compared with the DLW, but it is less accurate for an individual assessment (Sliva et al., 2015). Kortelainen et al. (2021) proposed accurate energy expenditure predictions based on a few calibration measurements using a nonlinear (logistic) mixed model for energy expenditure and HR. They found that the logistic mixed model performed better than the linear mixed model when predicting energy expenditure at population level and with calibration. In this study, using the linear model, the result of the estimated equation with three points was 94% (-316 kcal) compared with the results of the two points. Therefore, no moderate-intensity activity that did not affect HR. In addition, using the tri-axial accelerometer method, the estimation equation with two points of total energy expenditure was underestimated by 43% compared with the combined accelerometer and HR. In the present study, we able to improve the underestimation of total energy expenditure, but we could not examine whether it was an overestimation or an accurate assessment. The novel estimation equation of the two points between the METs and HR is simple, and it has high validity as an estimation equation for energy expenditure in the field. Considering its application in the field, the two minimum and maximum estimation equations used in this study are sufficient. In estimating the energy expenditure per activity for a short period, rather than the average energy expenditure for 1 day or several days, combining tri-axial accelerometers and HR was easy and effective. Our research objective was to estimate energy expenditure in a realworld environment. Since our approach was a real-world datadriven study, rather than a traditional experimental design-driven study, there were many limitations on the measurement. Under such real-world, non-uniform, and a priori unforeseeable work environments, we believe that our method gave improved estimation results compared to the results of previous studies that estimated using only acceleration. Also, the results we refer to are the widely-accepted reference values, METs, estimated based on experimental studies in previous studies. Nevertheless, indeed, the values estimated based on experimental studies do not take into account factors such as individual differences, mental load, different types of exercise load, the type of heavy equipment, effects of circadian rhythm, effects of diet, and effects of sleep. It is difficult to conduct an experiment that takes all these factors into account. We also believe that in real-world, non-uniform, and a priori unforeseeable work environments, accurate estimation of individual tasks is difficult, whether using the DLW or other methods. We are sure that the accuracy can be improved by combining it with laboratory studies in the future. Beckner et al. (2023) reported sustained operations for the military personnel are often conducted in a state of negative energy balance and are associated with degraded cognitive performance and mood. In order to prevent such condition, the amount of energy ingested should also be considered in the future. The accuracy of the estimation equation can be further improved by accurately extracting the reference activities of METs. Moreover, estimating energy expenditure for a wide range of age groups, sex, and people with different body sizes, such as obese and overweight, may require an estimation equation with three or more points, instead of just two, in the future.

This study had four limitations. First, we focused only on HR because the measurements were conducted in winter. However, the temperature should also be considered because the HR can quickly increase depending on environmental conditions, particularly during summer. In addition, an equation that considers the circadian rhythm of the heartbeat should be developed. Second, the activities were calculated by applying them to the MET table; however, applying them to special rescue operation activities was difficult because appropriate METs could not be found. Therefore, the validity of METs remains to be examined using the Douglas bag and other methods. Third, we did not consider the diet induced thermogenesis, because it was automatically calculated by entering each individual's data into the accelerometer. Finally, the present study was conducted in the field, and no controls were used to verify the energy expenditure calculations. In the future, the energy expenditure remained to be examined using the Douglas bag and DLW.

In this study, a method to improve energy expenditure estimation for heavy-load physical labor, such as disaster relief and rescue operations, using a tri-axial accelerometer and HR monitor was proposed. Energy expenditure, which was underestimated by accelerometer-based energy expenditure methods, could be compensated by creating an individually optimized estimation equation between METs and individual HR. Furthermore, more detailed measurements were necessary for a large number of rescue operations in a wide range of ranks and firefighter activities in the future.

# Data availability statement

The datasets presented in this study can be found in online repositories. The names of the repository/repositories and accession number(s) can be found below: All data files are available from the figshare database (https://figshare.com/articles/dataset/Estimation\_equation\_model\_/21579168).

# **Ethics statement**

The studies involving humans were approved by the local ethics committee of the University of Tsukuba (approval number: tai-28-66). The studies were conducted in accordance with the local legislation and institutional

requirements. Written informed consent for participation was not required from the participants or the participants' legal guardians/next of kin because detailed explanations were given to each training director and participating organizationaffiliated institution regarding the purpose and content of the experiment, and the experiment was started only after obtaining agreement.

# Author contributions

HO: Conceptualization, Funding acquisition, Writing-original draft. YN: Investigation, Writing-review and editing. NK: Formal Analysis, Investigation, Writing-review and editing. HN: Investigation, Writing-review and editing. MK: Methodology, Writing-review and editing. KK: Data curation, Methodology, Writing-review and editing. NO: Conceptualization, Supervision, Writing-review and editing.

# Funding

The author(s) declare financial support was received for the research, authorship, and/or publication of this article. This work was supported by the Advanced Research Initiative for Human High

# References

Ades, P. A., Savage, P. D., Brochu, M., Tischler, M. D., Lee, N. M., and Poehlman, E. T. (2005). Resistance training increases total daily energy expenditure in disabled older women with coronary heart disease. *J. Appl. Physiol.* 98 (4), 1280–1285. doi:10.1152/japplphysiol.00360.2004

Ainsworth, B. E., Haskell, W. L., Herrmann, S. D., Meckes, N., Bassett, D. R., Jr, Tudor-Locke, C., et al. (2011). 2011 Compendium of Physical Activities: a second update of codes and MET values. *Med. Sci. Sports Exerc* 43 (8), 1575–1581. doi:10.1249/ MSS.0b013e31821ece12

Aparicio-Ugarriza, R., Mielgo-Ayuso, J., Benito, P. J., Pedrero-Chamizo, R., Ara, I., González-Gross, M., et al. (2015). Physical activity assessment in the general population; instrumental methods and new technologies. *Nutr. Hosp.* 31 (Suppl. 3), 219–226. doi:10. 3305/nh.2015.31.sup3.8769

Arikawa, T., Nakajima, T., Yazawa, H., Kaneda, H., Haruyama, A., Obi, S., et al. (2020). Clinical usefulness of new R-R interval analysis using the wearable heart rate sensor WHS-1 to identify obstructive sleep apnea: OSA and RRI analysis using a wearable heartbeat sensor. *J. Clin. Med.* 9 (10), 3359. doi:10.3390/jcm9103359

Beckner, M. E., Lieberman, H. R., Hatch-McChesney, A., Allem, J. T., Niro, P. J., Thompson, L. A., et al. (2023). Effects of energy balance on cognitive performance, risktaking, ambulatory vigilance and mood during simulated military sustained operations (SUSOPS). *Physiol. Behav.* 258, 114010. doi:10.1016/j.physbeh.2022.114010

Berryman, C. E., Sepowitz, J. J., McClung, H. L., Lieberman, H. R., Frrina, E. K., McClung, J. P., et al. (2017). Supplementing an energy adequate, higher protein diet with protein does not enhance fat-free mass restoration after short-term severe negative energy balance. *Appl. Physiol.* 122, 1485–1493. doi:10.1152/japplphysiol. 01039.2016

Bouten, C. V., Koekkoek, K. T., Verduin, M., Kodde, R., and Janssen, J. D. (1997). A triaxial accelerometer and portable data processing unit for the assessment of daily physical activity. *IEEE Trans. Biomed. Eng.* 44 (3), 136–147. doi:10.1109/10.554760

Cannon, W. B. (1929). Bodily changes in pain, hunger, fear and rage: an account of recent research into the function of emotional excitement. 2nd ed. New York: Appleton-Century-Crofts.

Chen, K. Y., Janz, K. F., Zhu, W., and Brychta, R. J. (2012). Re-defining the roles of sensors in objective physical activity monitoring. *Med. Sci. Sports Exerc* 44 (Suppl. 1), S13–S23. doi:10.1249/MSS.0b013e3182399bc8

Chevance, G., Golaszewski, N. M., Tipton, E., Hekler, E. B., Buman, M., Welk, G. J., et al. (2022). Accuracy and precision of energy expenditure, heart rate, and steps measured by combined-sensing Fitbits against reference measures: systematic review and meta-analysis. *JMIR Mhealth Uhealth* 10 (4), e35626. doi:10.2196/35626 Performance (ARIHHP, University of Tsukuba) under Grant [2017, 2018, 2019, 2020, and 2021].

# Acknowledgments

We are extremely grateful to all the firefighters who cooperated with our research.

# Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

# Publisher's note

All claims expressed in this article are solely those of the authors and do not necessarily represent those of their affiliated organizations, or those of the publisher, the editors and the reviewers. Any product that may be evaluated in this article, or claim that may be made by its manufacturer, is not guaranteed or endorsed by the publisher.

Fuller, D., Clowell, E., Low, J., Orychock, K., Tobin, M. A., Simango, B., et al. (2020). Reliability and validity of commercially available wearable devices for measuring steps, energy expenditure, and heart rate: systematic review. *JMIR Mhealth Uhealth* 8 (9), e18694. doi:10.2196/18694

Ganpile, A. A., Tanaka, S., Ishikawa-Takata, K., and Tabata, I. (2007). Interindividual variability in sleeping metabolic rate in Japanese subjects. *Eur. J. Clin. Nutr.* 61 (11), 1256–1261. doi:10.1038/sj.ejcn.1602645

Garby, L., Kurzer, M. S., Lammert, O., and Nielsen, E. (1987). Energy expenditure during sleep in men and women: evaporative and sensible heat losses. *Hum. Nutr. Clin. Nutr.* 41C, 225–233.

Hill, J. O., and Trowbridge, E. L. (1998). Childhood obesity: future directions and research priorities. *Pediatrics* 101 (3 Pt 2), 570–574. doi:10.1542/peds.101.3.570

Isakadze, N., and Martin, S. S. (2020). How useful is the smartwatch ECG? Trends Cardiovasc Med. 30 (7), 442–448. doi:10.1016/j.tcm.2019.10.010

Jackson, A. S., Blair, S. N., Mahar, M. T., Wier, L. T., Ross, R. M., and Stuteville, J. E. (1990). Prediction of functional aerobic capacity without exercise testing. *Med. Sci. Sports Exerc* 22 (6), 863–870. doi:10.1249/00005768-199012000-00021

Jetté, M., Sidney, K., and Blümchen, G. (1990). Metabolic equivalents (METS) in exercise testing, exercise prescription, and evaluation of functional capacity. *Clin. Cardiol.* 13, 555–565. doi:10.1002/clc.4960130809

Karmen, C. L., Reisfel, M. A., McIntyre, M. K., Timmermans, R., and Frishman, W. (2019). The clinical value of heart rate monitoring using an Apple Watch. *Cardiol. Rev.* 27 (2), 60–62. doi:10.1097/CRD.0000000000243

Kinnunen, H., Häkkinen, K., Schumann, M., Karavurta, L., Westerterp, K. R., and Kyröläinen, H. (2019). Training-induced changes in daily energy expenditure: methodological evaluation using wrist-worn accelerometer, heart rate monitor, and doubly labeled water technique. *PLoS One* 14 (7), e0219563. doi:10.1371/journal.pone. 0219563

Koizumi, N., Negishi, Y., Ogata, H., Rakwal, R., and Omi, N. (2021). Estimating total energy expenditure for fire-fighters during large scale disaster response training using a tri-axial accelerometer. *Nutrients* 13 (8), 2789. doi:10.3390/nu13082789

Kortelainen, L., Helske, J., Finni, T., Mehtätalo, L., Tikkanen, O., and Kärkkäinen, S. (2021). A nonlinear mixed model approach to predict energy expenditure from heart rate. *Physiol. Meas.* 42 (3), 035001. doi:10.1088/1361-6579/abea25

Kramer, T. R., Moore, R. J., Shippee, R. L., Friedl, K. E., Martinez-Lopez, L., Chan, M. M., et al. (1997). Effects of food restriction in military training on T-lymphocyte responses. *Int. J. Sports Med.* 18 (Suppl. 1), S84–S90. doi:10.1055/s-2007-972704

Margolis, L. M., Murphy, N. E., Martini, S., Spitz, M. G., Thrane, I., McGraw, S. M., et al. (2014). Effects of winter military training on energy balance, whole-body protein balance, muscle damage, soreness, and physical performance. *Appl. Physiol. Nutr. Metab.* 39, 1395–1401. doi:10.1139/apnm-2014-0212

Martin, C. K., Das, S. K., Lindblad, L., Racette, S. B., McCrory, M. A., Weiss, E. P., et al. (2011). Effect of calorie restriction on the free-living physical activity levels of nonobese humans: results of three randomized trials. *J. Appl. Physiol.* 110, 956–963. doi:10.1152/japplphysiol.00846.2009

Midorikawa, T., Tanaka, S., Kaneko, K., Koizumi, K., Ishikawa-Takata, K., Futami, J., et al. (2007). Evaluation of low-intensity physical activity by triaxial accelerometry. *Obesity* 15 (12), 3031–3038. doi:10.1038/oby.2007.361

Murakami, H., Kawakami, R., Nakae, S., Yamada, Y., Nakata, Y., Ohkawara, K., et al. (2019). Accuracy of 12 wearable devices for estimating physical activity energy expenditure using a metabolic chamber and the doubly labeled water method: validation study. *JMIR Mhealth Uhealth* 7 (8), e13938. doi:10.2196/ 13938

Nagayoshi, S., Oshima, Y., Ando, T., Aoyama, T., Nakae, S., Usui, C., et al. (2019). Validity of estimating physical activity intensity using a triaxial accelerometer in healthy adults and older adults. *BMJ Open Sport Exerc Med.* 5 (1), e000592. doi:10.1136/ bmjsem-2019-000592

Ndahimana, D., and Kim, E. K. (2017). Measurement methods for physical activity and energy expenditure: a review. *Clin. Nutr. Res.* 6 (2), 68–80. doi:10.7762/cnr.2017.6. 2.68

Nishida, Y., Tanaka, S., Nakae, S., Yamada, Y., Morino, K., Kondo, K., et al. (2020). Validity of the use of a triaxial accelerometer and a physical activity questionnaire for estimating total energy expenditure and physical activity level among elderly patients with type 2 diabetes mellitus: CLEVER-DM study. *Ann. Nutr. Metab.* 76 (1), 62–72. doi:10.1159/000506223

Ohkawara, K., Oshima, Y., Hikihara, Y., Ishikawa-Takata, K., Tabata, I., and Tanaka, S. (2011). Real-time estimation of daily physical activity intensity by a triaxial accelerometer and a gravity-removal classification algorithm. *Br. J. Nutr.* 105, 1681–1691. doi:10.1017/S0007114510005441

Oshima, Y., Kawaguchi, K., Tanaka, S., Ohkawara, K., Hikihara, Y., Ishikawa-Takata, K., et al. (2010). Classifying household and locomotive activities using a triaxial accelerometer. *Gait Posture* 31, 370–374. doi:10.1016/j.gaitpost.2010. 01.005

Parker, R., Vitalis, A., Walker, R., Riley, D., and Pearce, H. G. (2017). Measuring wildland fire fighter performance with wearable technology. *Appl. Ergon.* 59, 34–44. doi:10.1016/j.apergo.2016.08.018

Planer, D., Leibowitz, D., Hadid, A., Erlich, T., Sharon, N., Paltiel, O., et al. (2012). The effect of prolonged physical activity performed during extreme caloric deprivation on cardiac function. *PLoS One* 7 (2), e31266. doi:10.1371/journal. pone.0031266

Plasqui, G., Joosen, A. M., Kester, A. D., Goris, A. H., and Westerterp, K. R. (2005). Measuring free-living energy expenditure and physical activity with triaxial accelerometry. *Obes. Res.* 13 (8), 1363–1369. doi:10.1038/oby.2005.165

Plasqui, G., and Westerterp, K. R. (2007). Physical activity assessment with accelerometers: an evaluation against doubly labeled water. *Obesity* 15 (10), 2371-2379. doi:10.1038/oby.2007.281

Rodahl, K. (1989). Physiology of work. London: CRC Press.

Sato, H., Nakamura, H., Nishida, Y., Shirahata, T., Yogi, S., Akagami, T., et al. (2021). Energy expenditure and physical activity in COPD by doubly labelled water method and an accelerometer. *ERJ Open Res.* 7 (2), 00407–02020. doi:10.1183/23120541.00407-2020

Sell, K. M., and Ledesma, A. B. (2016). Heart rate and energy expenditure in division I field hockey players during competitive play. *J. Strength Cond. Res.* 30 (8), 2122–2128. doi:10.1519/JSC.00000000001334

Sliva, A. M., Santos, D. A., Matias, C. N., Júdice, P. B., Magalhães, J. P., Ekelund, U., et al. (2015). Accuracy of a combined heart rate and motion sensor for assessing energy expenditure in free-living adults during a double-blind crossover caffeine trial using doubly labeled water as the reference method. *Eur. J. Clin. Nutr.* 69 (1), 20–27. doi:10.1038/ejcn.2014.51

Strath, S. J., Swartx, A. M., Bassett, D. R., Jr, O'Brien, W. L., King, G. A., and Ainsworth, B. E. (2000). Evaluation of heart rate as a method for assessing moderate intensity physical activity. *Med. Sci. Sports Exerc* 32 (9 Suppl. I), S465–S470. doi:10.1097/ 00005768-200099001-00005

Swain, D. P., Leutholtz, B. C., King, M. E., Haas, L. A., and Branch, J. D. (1998). Relationship between % heart rate reserve and %  $VO_2$  reserve in treadmill exercise. *Med. Sci. Sports Exerc* 30 (2), 318–321. doi:10.1097/00005768-199802000-00022

Tanaka, M., Mizuno, K., Yamaguti, K., Kuratsune, H., Fujii, A., Baba, H., et al. (2011). Autonomic nervous alterations associated with daily level of fatigue. *Behav. Brain Funct.* 7, 46. doi:10.1186/1744-9081-7-46

Touno, M., Hasina, R. H., Ebine, N., Peng, H. Y., Yoshitake, Y., Tanaka, H., et al. (2003). Measurement of total energy expenditure in Japanese Firefighters under normal working condition using the doubly labelled water method. *Jpn. J. Phys. Fit. Sports Med.* 52, 265–274. doi:10.7600/jspfsm1949.52.265

Van Remoortel, H., Giavedoni, S., Raste, Y., Burtin, C., Louvaris, Z., Gimeno-Santos, E., et al. (2012). Validity of activity monitors in health and chronic disease: a systematic review. *Int. J. Behav. Nutr. Phys. Act.* 9, 84. doi:10.1186/1479-5868-9-84

Willis, E. A., Creasy, S. A., Saint-Maurice, P. F., Keadle, S. K., Pontzer, H., Schoeller, D., et al. (2022). Physical activity and total daily energy expenditure in older US adults: constrained versus additive models. *Med. Sci. Sports Exerc* 54 (1), 98–105. doi:10.1249/MSS.00000000002759

Yamada, Y., Yokoyama, K., Noriyasu, R., Osaki, T., Adachi, T., Itoi, A., et al. (2009). Light-intensity activities are important for estimating physical activity energy expenditure using uniaxial and triaxial accelerometers. *Eur. J. Appl. Physiol.* 105 (1), 141–152. doi:10.1007/s00421-008-0883-7