



A dual-tracer method for differentiating transendothelial transport from paracellular leakage *in vivo* and *in vitro*

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Inflammation-induced impaired function of vascular endothelium may cause leakage of plasma proteins that can lead to edema. Proteins may leave the vascular lumen through two main paracellular and transcellular pathways. As the first involves endothelial cell (EC) junction proteins and the second caveolae formation, these two pathways are interconnected. Therefore, it is difficult to differentiate the prevailing role of one or the other pathway during pathology that causes inflammation. Here we present a newly developed dual-tracer probing method that allows differentiation of transcellular from paracellular transport during pathology. This fluorescence-based method can be used *in vitro* to test changes in EC layer permeability and *in vivo* in various animal vascular preparations. The method is based on comparison of low molecular weight molecule (LMWM) transport to that of high molecular weight molecule (HMWM) transport through the EC layer or the vascular wall during physiological and pathological conditions. Since the LMWM will leak through mainly the paracellular and HMWM will move through paracellular (when gaps between the ECs are wide enough) and transcellular pathways, the difference in transport rate (during normal conditions and pathology) of these molecules will indicate the prevailing transport pathway involved in overall protein crossing of vascular wall. Thus, the novel approach of assessing the transport kinetics of different size tracers *in vivo* by intravital microscopy can clarify questions related to identification of target pathways for drug delivery during various pathologies associated with elevated microvascular permeability.

Keywords: cerebrovascular leakage, intravital microscopy, fluorescent dyes

INTRODUCTION

Many inflammatory diseases such as hypertension (Johansson et al., 1978; Miller et al., 1986; Pedrinelli et al., 1999), diabetes (Bonnardel-Phu et al., 1999), and stroke (Hatashita and Hoff, 1990; Laursen et al., 1993; Wardlaw et al., 2003) are accompanied by impaired vascular wall integrity leading to enhanced microvascular leakage. Movement of plasma proteins to interstitium can be particularly detrimental as it is most likely a cause of edema. Proteins may cross endothelium through two main pathways: paracellular and transcellular. Paracellular transport occurs through gaps between endothelial cells (ECs) and involves alterations in tight, gap, and adherence junction proteins (Mehta and Malik, 2006). Transcellular transport occurs through the EC and involves formation of functional caveolae and their mobility (Stan et al., 1999; Stan, 2007). Since caveolae are attached to actin filaments through the protein filamin (Ushio-Fukai and Alexander, 2006) as are tight junction and adherence junction proteins (Mehta and Malik, 2006), and caveolae-mediated transcytosis and paracellular transport are interconnected (Bauer et al., 2005) the prevailing role of one or the other pathway in overall protein transvascular transport is difficult to define. Caveolin-1-null mice that lack caveolae in the endothelium showed increased permeability to albumin in venules and capillaries via the paracellular route (Razani et al., 2001; Miyawaki-Shimizu et al., 2006), suggesting a close crosstalk between transcellular and paracellular pathways in regulating tissue fluid balance.

Albumin, the most abundant plasma protein, constantly crosses the EC barrier in both directions (from the apical to the basal and from the basal to the apical side of cells) and acts as a chaperone for a number of hydrophobic molecules (Mehta and Malik, 2006). It is suggested that movement of albumin occurs through mainly transcellular transport (Mehta and Malik, 2006) since EC gaps are not readily opened to the extent to permit albumin leakage. During various inflammatory stimulations EC gaps open transiently leading to leakage of plasma components (including proteins, e.g., albumin) to the interstitium. However, formation of caveolae may be enhanced and lead to protein transport for a longer duration leading to edema. Thus there is a difference in action between these two transport pathways.

We developed a dual-tracer probing method to differentiate the relative involvement of transcellular and paracellular transport pathways in protein crossing the EC layer and vascular wall during pathology. This method is based on a comparison of leakage of a low molecular weight molecule (LMWM) and a high molecular weight molecule (HMWM; in our case albumin) through cultured mouse brain ECs (MBECs) and mouse pial venules during normal and pathological conditions. To test inflammation-induced possible changes in transcellular and paracellular transport, we used hyperfibrinogenemia (HFg) as the experimental pathology. HFg accompanies many inflammatory diseases such as hypertension (Letcher et al., 1981; Lominadze et al., 1998), diabetes (Lee et al., 2007), stroke (Eidelman and Hennekens, 2003; del Zoppo

et al., 2009), and traumatic brain injury (Pahatouridis et al., 2010). We showed that enhanced blood content of fibrinogen (Fg) compromises EC layer integrity resulting in albumin leakage through cultured EC layer (Tyagi et al., 2008; Muradashvili et al., 2011) and mouse pial venules (Muradashvili et al., 2012). It was found that Fg causes enhanced movement of fluorescently labeled bovine serum albumin (BSA) through both transcellular and paracellular pathways (Tyagi et al., 2008; Muradashvili et al., 2011, 2012). However, the prevailing role of one or the other transport mechanism was not defined.

METHODS

REAGENTS AND ANTIBODIES

Human Fg (FIB-3, depleted of plasminogen, von-Willebrand factor, and fibronectin) was purchased from Enzyme Research Laboratories (South Bend, IN). Alexa Fluor 647-conjugated BSA (BSA-647) was obtained from Invitrogen (Carlsbad, CA). Fluorescein isothiocyanate (FITC) and Lucifer Yellow were from Sigma Aldrich Chemicals Co. (St. Louis, MO).

ANIMALS

In accordance with National Institute of Health Guidelines for animal research, all animal procedures for these experiments were reviewed and approved by the Institutional Animal Care and Use Committee of the University of Louisville.

Male wild type (WT) C57BL/6J mice were from the Jackson Laboratory (Bar Harbor, ME). HFg transgenic mice on C57BL/6J background (strain name: C57BL/6-Tg(Fga,Fgb,Fgg)1Unc/Mmnc; Stock Number 004104) were purchased from Mutant Mouse Regional Resource Center at the University of North Carolina at Chapel Hill (Chapel Hill, NC). For genotyping of HFg mice, DNA was extracted from the tail tip of mice and was amplified by polymerase chain reaction (PCR) using specific primer sequences according to the protocol provided by the Jackson Laboratory and described elsewhere (Gulledge et al., 2001). The primer sequences for HFg were forward 5'-GGC CGT CGA CAT TTA GGT GAC AC-3' and reverse 5'-AGT CAA TTT GGT CAC TAA CC GCC-3'. The primer sequences for WT were forward: 5'-GTG GGA CCA TCA TAA CAT CAC A-3'; reverse: 5'-CTC GCG GCA AGT CTT CAG AGT A-3'. Typical genotype results are presented on **Figure 1**. HFg mice have higher plasma levels of Fg than WT mice (Gulledge et al., 2001, 2003).

Twenty-week old mice (29–32 g) were anesthetized with sodium pentobarbital (70 mg/kg, IP). Supplemental anesthesia was given as required during the experiment. 2% Xylocaine

(AstraZeneca LP, Wilmington, DE) was used for local analgesia. The left carotid artery was cannulated with polyethylene tubing PE-10 for blood pressure monitoring and necessary infusions. The trachea was cannulated to maintain a patent airway. Body temperature of the mouse was kept at $37 \pm 1^\circ\text{C}$ with a heating pad. Mean arterial blood pressure and heart rate were continuously monitored through a carotid artery cannula connected to a transducer and a blood pressure analyzer (CyQ 103/302, Cybersense, Lexington, KY). A tail cuff and a CODA monitor, a non-invasive blood pressure measurement system (Kent Scientific Apparatus, Torrington, CT), were used to monitor mean arterial blood pressure during infusion of dyes.

Brain pial microcirculation was prepared for observations according to the method described previously (Lominadze et al., 2006; Muradashvili et al., 2012).

ENDOTHELIAL CELL CULTURE

Mouse brain ECs were purchased from American Type Culture Collection (ATCC, Manassas, VA). The cells were cultured in complete Dulbecco's modified eagle's medium (DMEM), according to the manufacturer's (ATCC) recommendation, at 37°C with 5% CO_2/air in a humidified environment and were used at the 5th or 6th passage for the experiments.

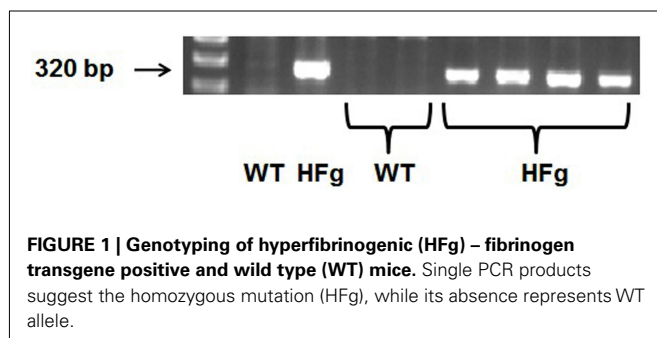
DUAL-TRACER PROBING METHOD

To determine changes in transcellular and paracellular transport mechanisms induced by enhanced blood content of Fg and to define if one of these pathways has a prevailing role during this pathology, we developed a dual-tracer probing method. *In vitro*, leakage of Lucifer yellow (as a LMWM) and Alexa Fluor 647-conjugated BSA (BSA-647) through MBEC layer treated with 4 mg/ml Fg or phosphate-buffered saline (PBS) was studied. *In vivo*, leakage of FITC (as a LMWM) was compared to that of BSA-647 in pial venules of normal WT and HFg mice.

Microvascular leakage

Mouse pial venular leakage was observed as described previously (Lominadze et al., 2006; Muradashvili et al., 2012). Following the surgical preparation and preceding each experiment, there was a 1-h equilibration period. Before each experiment, autofluorescence of the observed area was recorded over a standard range of camera gains. Mixture of 100 μl of FITC (300 $\mu\text{g}/\text{ml}$) and 20 μl of BSA-647 (3.3 mg/ml) in PBS (a total of 120 μl solution) was infused through the carotid artery cannulation. The solution was infused with a syringe pump (Harvard Apparatus, Holliston, MA) at 30 $\mu\text{l}/\text{min}$ speed and allowed to circulate for 10 min (Lominadze et al., 2006; Muradashvili et al., 2012). The pial circulation was surveyed to ensure that there was no spontaneous leakage of BSA-647 in the observed area that would indicate compromised vascular integrity. Venules were identified by observing the topology of the pial circulation and blood flow direction. Images of the selected third-order venular segments were recorded and used as baseline. After obtaining the baseline reading, images of the selected venular segments were recorded at 10, 20, 40, 60, and 120 min.

An epi-illumination system was used to observe intravascular and extravascular FITC and BSA-647. The area of interest was exposed to blue light (488 nm) and then red light (647 nm) for 10–15 s with a power density of $3.5 \mu\text{W}/\text{cm}^2$. The microscope images



were acquired by an electron-multiplying charge-coupled device camera (Quantem 512SC, Photometrics, Tucson, AZ) and image acquisition system (Slidebook 5.0, Intelligent Imaging Innovations, Inc., Philadelphia, PA). The camera output was standardized with a 50 ng/ml fluorescein diacetate standard (Estman Kodak, Rochester, NY) for each experiment. The lamp power and camera gain settings were held constant during experiments, and the camera response was verified to be linear over the range used for these acquisitions. The magnification of the system with Olympus 20×/0.40 (UPlanSApo) objective was determined with a stage micrometer.

Images of the pial venular circulation were analyzed by image analysis software (Image-Pro Plus 7.0, Media Cybernetics, Bethesda, MD). Example of the image analysis for detection of BSA-647 leakage to interstitium is presented on **Figure 2**. In each image, a Line Profile probe (LPP) of 50 μm in length was

positioned in the interstitium adjacent to a venular wall in parallel to the venule (**Figure 2A**) and then in the middle of the venule parallel to the blood stream (**Figure 2B**). Mean fluorescence intensities were measured for each dye (**Figure 2**). Leakage of FITC and BSA-647 to interstitium was assessed by changes in the ratio of fluorescence intensity of each dye in the interstitium to that inside the venule for the respective dye. The results were averaged for each experimental group and presented as percent of baseline. The diameter of each venule under observation was also measured.

Leakage through EC layer

Changes in transcellular and paracellular transport in cultured MBECs were studied using Transwell permeable supports (Corning Inc., Corning, NJ) as previously described (Tyagi et al., 2008; Patibandla et al., 2009). Briefly, the Transwell permeable supports

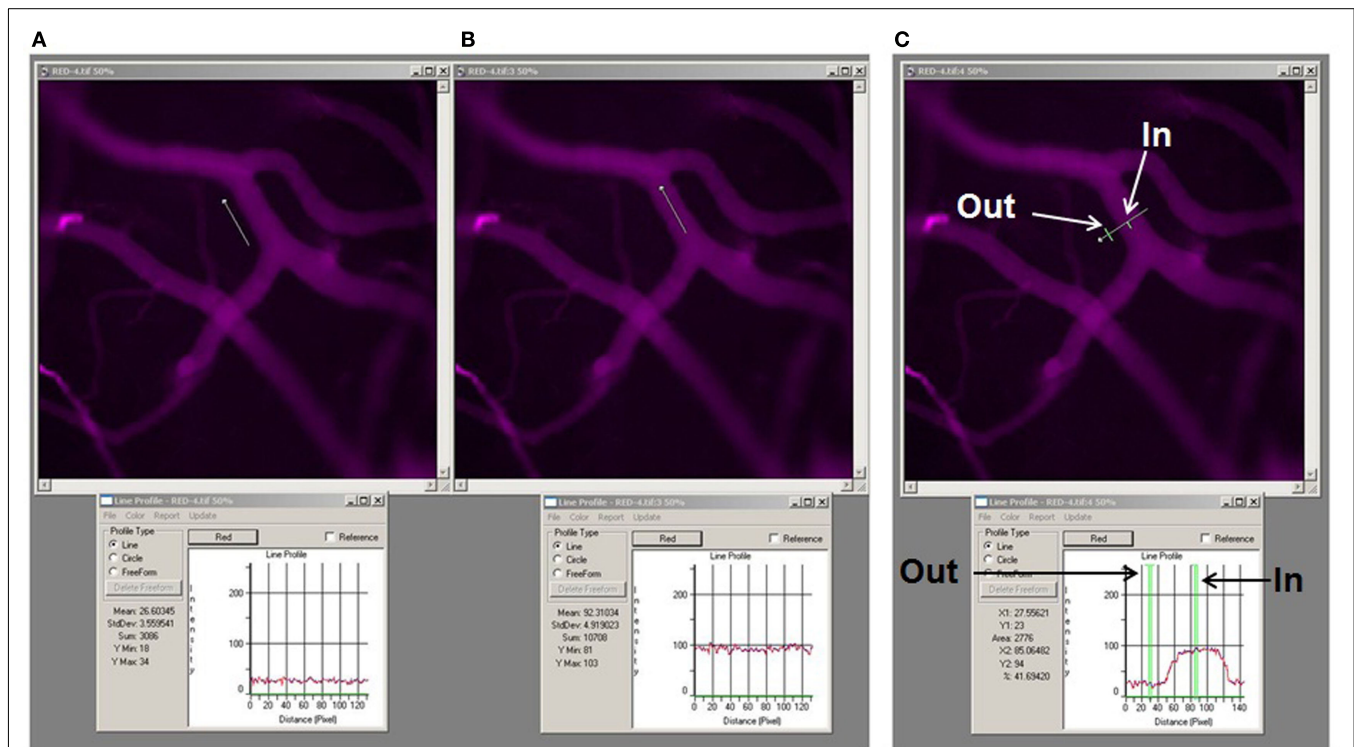


FIGURE 2 | Image analysis of microvascular leakage using Image-Pro Plus software. Examples of pial microvascular bed images (with circulating BSA-647) with a digital Line Profile probe (LPP) placed in the area of interest (upper row) and corresponding results of fluorescent light intensity readings shown in respective Line profile boxes (lower row). About thirty micrometer long LPP was first placed in interstitium adjacent to the venular segment (**A**) and then inside the venular segment (**B**). To perform quantitative analysis of fluorescence intensity along a LPP the following steps were followed: <Measure>, <Line profile> (this led to appearance of the Line profile box. The size and the place of the LPP on the image were adjusted manually), <Report> in the Line profile box, then “statistics.” For assessment of fluorescence intensity of BSA-647 <red> was chosen in the Line profile box, while <green> was chosen for FITC intensity measurement. Values of the fluorescence intensities were given as “Mean” and “Standard deviation” in the Line profile box (see lower row). Fluorescence intensity profile along the LPP for each image is shown in the Line profile box below the respective image. Mean values averaged along the LPP are also shown in the Line profile box. Note that

mean fluorescence intensity inside the venule is 92.3 fluorescence intensity units (FIU) and in the adjacent interstitium is 26.6 FIU. Thus ratio of fluorescence intensity in interstitium to that in the venule is 0.29. This value was expressed as a percent of baseline values calculated for images obtained immediately after infusion of the dual-tracer probe. Example of the LPP placed across the venular segment and over the adjacent interstitium (upper image) with the fluorescence intensity profile along the LPP (below) is shown (**C**). Arrows indicate precise locations of where the fluorescence intensities were measured along the LPP. Note that fluorescence intensity inside the venule (In) is 85.1 FIU and in interstitium (Out) is 23. Thus ratio of fluorescence intensity in interstitium to that in the venule in the marked places along the LPP is 0.27. However, to obtain reliable data the LPP should be moved along the vessel and several measurements performed to calculate an average of these results. Since the same data, with better precision, can be obtained using the method described above (**A,B**), we placed the LPP across the vessel to define the vascular wall and the distance from the vessel where the LPP should have been placed (parallel to the vessel) in interstitium.

with polycarbonate membranes (Nuclepore Track-Etch, 6.5 mm in diameter, 0.4 μm pore size, and pore density of $10^8/\text{cm}^2$) coated with fibronectin were seeded with MBECs and grown in DMEM until they formed a complete monolayer. Cell confluence and the presence of an intact monolayer on the membranes were confirmed in each series of experiments (Tyagi et al., 2008; Patibandla et al., 2009). To inhibit the effect of thrombin's activity, hirudin (0.1 U/ml) was added to each well in all experiments. The surface levels of solutions in the luminal (200 μl) and abluminal (600 μl) compartments of the Transwells were the same.

For the permeability assay, cells were washed with PBS and treated with 4 mg/ml of Fg or with medium alone in the presence of Lucifer yellow (0.3 mg/ml) and BSA-647 (0.2 mg/ml). After 10, 20, 40, 60, and 120 min media samples (50 μl) were collected from lower chambers of the Transwell system and the same volume of the sample was added to the each appropriate upper well. Fluorescence intensity of each dye in samples were measured by a microplate reader (SpectraMax M2e, Molecular Devices Corporation, Sunnyvale, CA) with excitation at 488 nm and emission at 520 nm (cutoff 515 nm) for Lucifer Yellow and with excitation at 650 nm and emission at 668 nm (cutoff 665 nm) for BSA-647. Results are expressed as a ratio of fluorescence intensity of each dye in the bottom chamber (of each experimental group) to fluorescence intensity of the respective dye in the original sample (of the respective group) at the end of the experiment. Experiments were performed eight times for each treatment.

DATA ANALYSIS

All data are expressed as mean \pm SEM. The experimental groups were compared by one-way ANOVA with repeated measures. If ANOVA indicated a significant difference ($p < 0.05$), Tukey's multiple comparison test was used to compare group means. Differences were considered significant if $p < 0.05$.

RESULTS AND DISCUSSION

Genotyping of experimental animals using appropriate primers and PCR positively identified HFg transgenic mice (Figure 1). Body weight of animals used in the study varied from 29 to 32 g. Mean arterial blood pressure did not change in WT (-1 ± 0.5 mmHg) or in HFg (-3 ± 0.5 mmHg) mice after FITC and BSA-647 infusion. During the observation period venular diameters (38 ± 6 μm) in WT animals changed insignificantly less ($+1 \pm 0.2$ μm) than venular diameters (40 ± 5 μm) in HFg mice ($+2 \pm 0.6$ μm).

We found that HFg caused greater leakage of plasma components through both transcellular and paracellular pathways (Figure 3). While the leakage of BSA-647 from pial venules was greater in HFg mice than that in WT mice starting from 20 min (Figure 3B), leakage of FITC was more in HFg mice than in WT mice only at 20 and 40 min (Figure 3A). Similarly, while at higher levels of Fg the leakage of BSA-647 through EC layer was greater starting from 20 min (Figure 3C), leakage of Lucifer Yellow through Fg-treated cells was more than that in control group only at 20 and 40 min (Figure 3D).

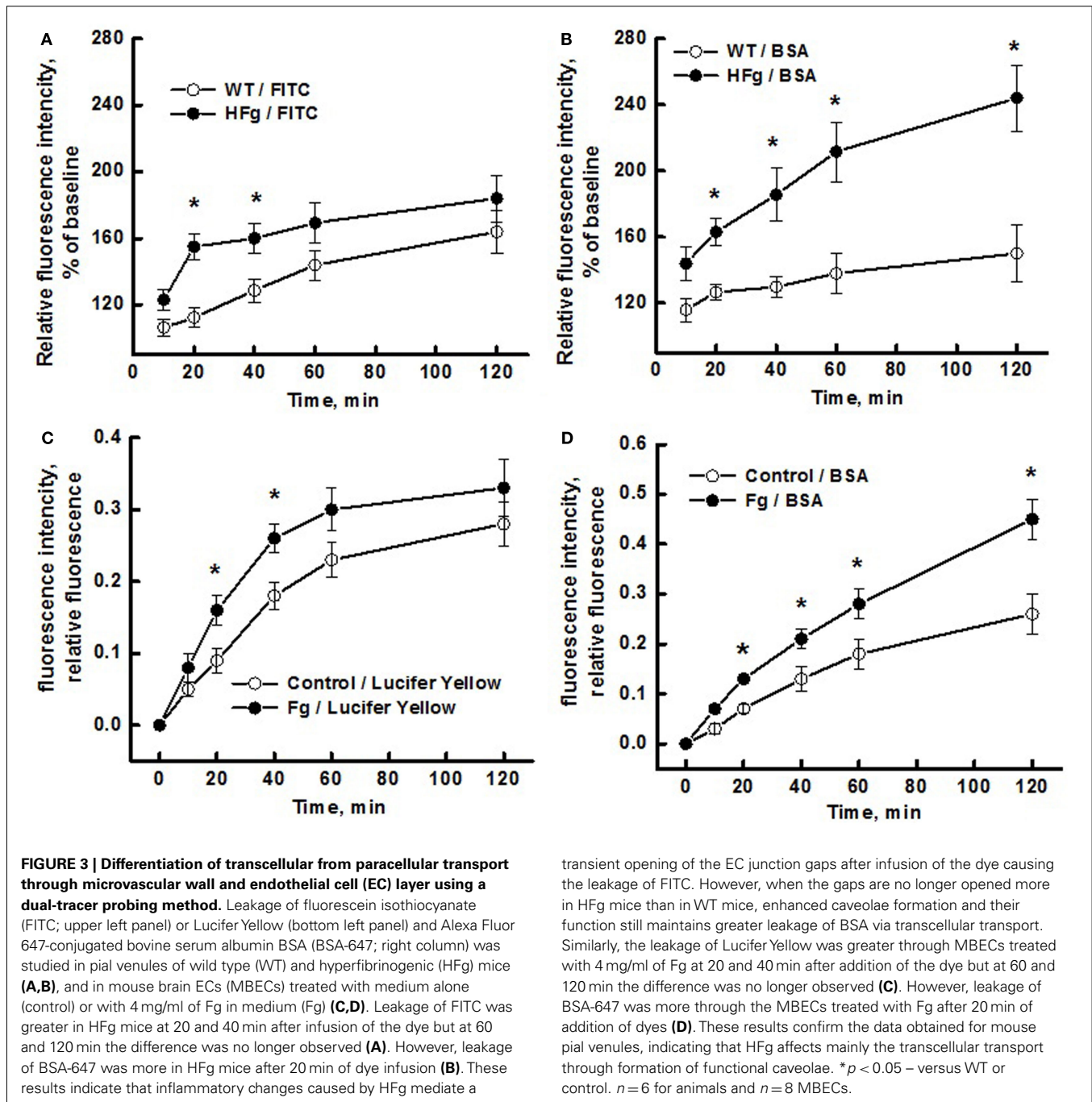
Stokes–Einstein radii of Lucifer Yellow (~ 0.49 nm; Heyman and Burt, 2008) and FITC (~ 0.45 nm; Fu and Shen, 2003) are significantly less than that (3.5 nm) of BSA (Fu and Shen, 2003).

Therefore, in case of increased level of Fg that affects EC junctions and caveolae formation (Tyagi et al., 2008; Patibandla et al., 2009; Muradashvili et al., 2011, 2012), Lucifer Yellow (and FITC) may leak mainly through the cell junctions (Little et al., 1995), while BSA would leak through the cell junctions, when they are opened wide enough and traverse via the transcellular route, when caveolae-mediated transport is stimulated: more caveolae are formed and become functional (with enhanced mobility and ability of albumin endocytosis).

Thus, leakage of Lucifer Yellow through EC layer (*in vitro*) or leakage of FITC through pial venules (*in vivo*) induced by high level of Fg was greater than that in respective control groups starting from 20 min but was no longer different from the control groups at 60 and 120 min (Figure 3). This data may indicate that after 40 min Fg no longer had an effect on EC gap formation. However, leakage of BSA-647 *in vitro* and *in vivo* induced by high level of Fg was greater than that in respective control groups from 40 min and continued to rise with time (Figure 3). These results suggest that Fg affects junction proteins (JPs) and leads to a transient opening of gaps between cells enhancing the leakage of LMWMs (Lucifer Yellow or FITC). This notion is supported by our data showing that Fg can cause translocation of JPs (Patibandla et al., 2009). As the effect of Fg on JPs subsides, the difference in Lucifer Yellow or FITC leakage between the HFg and the control groups vanish. However, high level Fg-induced leakage of HMWM (BSA) increases even after the paracellular pathway is no longer stimulated by Fg (Figures 3A,C). Thus BSA may move through MBEC layer and through pial venular wall first through both transport pathways and later (after relative closure of the junctional gaps) by mostly transcytosis.

The complicated nature of microvascular permeability was defined long ago using intravital microscopy and light absorbing dyes (Landis, 1927). Nakamura and Wayland (1975) tested leakage of fluorescently tagged BSA and various molecular weight dextrans. The leakage of these tracers was tested one at a time (Nakamura and Wayland, 1975). Even earlier, Witte (1965) used fluorescent tracers in qualitative studies on extravascular circulation in both normal and pathological conditions in mammals. Since then there were numerous reports related to microvascular or EC layer permeability using fluorescent dyes. However, none of them compared leakage kinetics of two different size tracers occurring at relatively the same time course in normal and pathological conditions.

Use of fluorescent and radioactive tracers to better define mechanisms of endothelial or vascular permeability continued. Vogel et al. (2001) define their method as a “single-sample” technique of Kern et al. (1983). Later John et al. (2003) presented quantitative analysis of albumin uptake and transport in ECs *in vitro* using ^{125}I -albumin. Its leakage through the EC layer was compared to that of unlabeled albumin. The authors showed that transcellular uptake and transport of ^{125}I -albumin can be blocked by excess of native albumin, and that any remaining leakage in these Transwell assays was via gaps in the monolayer. The results also indicated that albumin internalized and transported via caveolae can be distinguished in overall transendothelial albumin transport through the EC barrier *in vitro*. This method, which defines internalization of albumin in caveolae, was also used to demonstrate



that by interacting with the actin crosslinking protein filamin A, caveolin-1 phosphorylation plays a critical role in the mechanism of caveolae-mediated transcytosis and thereby stimulates transcellular permeability (Sverdlov et al., 2009).

Kovar et al. (1997) compared low and high molecular weight tracers to investigate perfusion rate in rodent tumors. Use of two tracers, sodium fluorescein and Texas red-dextran (70 kD), has been reported by Russ et al. (2001). The first tracer was used to indicate vessel leak and the second to indicate vessel filling. Again, this study did not differentiate transcellular and paracellular transport. Hu et al. (2008) demonstrated a novel

role of caveolae-mediated albumin transport in microvascular inflammatory hyperpermeability. They showed that intercellular adhesion molecule-1 activation-dependent caveolin-1 phosphorylation stimulated transcytosis of albumin in the pulmonary vasculature and that this increase in inflammatory transcellular albumin hyperpermeability (^{125}I -albumin permeability surface area product) as well as the increase in capillary filtration coefficient (fluid permeability) was abolished in caveolin-1 knockout mouse lungs. Leakage of ^{125}I -albumin through ECs was compared to that of ^3H -mannitol, a low-molecular-weight (182-Da) tracer that traverses the endothelium via the paracellular pathway. However,

authors did not record time-dependent changes in leakage of these tracers. Therefore, the method did not show if albumin leaked more via the paracellular or transcellular pathway. In addition, this was not the aim of the study.

A two-tracer isotope method using albumin labeled with ^{131}I and ^{125}I was used previously to define accumulation of albumin in vascular and extravascular space of various tissue (Tucker et al., 1992). Although it has been emphasized that the advantages of the two-tracer isotope methods to investigate transvascular macromolecule transport are becoming more widely recognized (Nagy et al., 2008), their use with transgenic mouse models has been limited. Lately this method has been used with better success to define the effects of atrial natriuretic peptide in microvascular permeability (Curry et al., 2010). However, as the two-tracer isotope method uses the same molecule with two different tracers, the method may not differentiate between the involvement of transcellular or paracellular transport pathways in total microvascular permeability. In another study, alterations in blood brain barrier permeability were studied using Evans blue and ^{125}I -tagged albumin (Nag, 1991). However, the probes were infused at separate times and no time-dependent observation of the vascular leakage was performed (Nag, 1991).

Our data indicate that using the newly developed dual-tracer probing method allows differentiation of the relative involvement of transcellular and paracellular transport pathways in inflammation-induced vascular and EC layer permeability. Since the method is based on comparison of leakage of LMWM and HMWM during pathology, we conclude that it can be used during various pathologies to differentiate the role of transcellular versus paracellular transport in overall vascular or EC layer permeability. In addition, by assessing the rate (kinetics) of leakage of small and larger molecules the method may also allow the assessment of the difference in response time between paracellular and transcellular protein transport.

LIMITATIONS OF THE METHOD

It has been shown that the addition of fluorescent dyes can alter the physicochemical characteristics of water-soluble macromolecules (Bingaman et al., 2003). It was found that the greatest changes were observed for BSA when it was conjugated with FITC (Bingaman et al., 2003). Therefore, in our study we used BSA that was conjugated with Alexa-647. However, properties of BSA still may have been different from that of unconjugated BSA. This may have less significance as we compared leakage of the dye alone or dye-conjugated BSA in the same type of vessels (venules) between the animals (or ECs).

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Since we measured only the relative fluorescence intensity (in the interstitial space adjacent to a pial venule over the fluorescence intensity inside the vessel) and did not evaluate hydrostatic pressure in the venule, we could not assess the venular permeability to LMWM (FITC) as required by Starling's concept. We made an assumption that leakage of LMWM (FITC) through the vascular wall occurs via the paracellular pathway and any changes in this process may occur due to pathology (HFg in our case) causing alterations in this pathway. Presented data indicate an accumulation of BSA-647 in interstitium, which can be considered an adequate measure for venular permeability to proteins. In addition, we did not find a difference in vascular diameters and MABPs in response to dual-tracer probe infusion in both groups of mice.

Thus, the precision of the presented approach is based on the ability to make a pairwise comparison of simultaneously assessed leakage kinetics of small and large molecules during normal and pathological conditions. Therefore, this method does not provide quantitative assessment for one or the other transport pathway in overall protein leakage. It defines if one or the other pathway prevails in total protein leakage.

There are several methods for quantitative analysis of endothelial permeability, which are discussed by Mehta and Malik (2006). It seems that the most adequate technique for quantitative assessment of microvascular permeability can be the method that uses an isolated vessel (He et al., 2006). This method is based on the modified Landis technique (Curry et al., 1976). Quantitative assessment of EC layer permeability can be best performed with the methods discussed above and presented elsewhere (John et al., 2003; Hu et al., 2008).

In addition, due to competition with endogenous albumin the sensitivity of fluorescently labeled BSA (infused in small quantities into the circulation) in detecting transcytosis is limited. Possible use of dextrans (instead of albumin) may exclude receptor-mediated specificity typically involved in caveolae-mediated albumin transcytosis (Tiruppathi et al., 1997).

Since the Stokes–Einstein radius of Lucifer Yellow is slightly greater than that of FITC, we used the Lucifer Yellow as a LMWM *in vitro*. In preliminary experiments, we found that 100 μl of Lucifer Yellow (3 mg/ml) did not produce detectable fluorescent light *in vivo*.

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