



Microbial Adhesion on Circular Obstacles: An Optimization Study

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Microbial filtration is an important process with applications in environmental, mining, and sanitary engineering. Here, we study the interplay between the motility of microswimmers and the imposed flow to determine the adhesion of bacteria at the surface of the solid obstacle. For that, we perform numerical simulations of active Brownian particles interacting with a single cylindrical obstacle when an imposed laminar flow is present. Highly and weakly persistent swimmers are studied, representing extreme cases of bacteria used in experiments and we vary the swimmers' velocity u_0 , the imposed flow velocity U_∞ , and the obstacle radius R . Starting with no swimmers close to the cylinder, we inject them steadily until a constant number of swimmers are adhered to the obstacle surface. The deposition/erosion process is characterized by the number of bacteria in contact with the obstacle, quantified by the average coverage of the cylinder surface λ_{trap} , and the relaxation time to reach the steady state τ_{trap} . Two regimes are found. The Brownian deposition is attained when swimmer velocities are smaller than the imposed flow. In this case, the particles can diffuse across the streamlines and settle around the obstacle covering the whole perimeter, forming multiple layers. The direct interception is obtained when the particle's velocities are larger, reaching the obstacle by direct swimming, in which case they form approximately one layer on the obstacle surface. It is found that λ_{trap} decreases with u_0 and R , but the dependence with the imposed flow U_∞ is non-monotonic, with an optimum coverage for intermediate flows, given by the crossover of the two regimes. The relaxation rate τ_{trap} decreases with u_0 and increases with R . The dependence of τ_{trap} with U_∞ is more complex, depending on the persistence of the swimmers. The existence of an optimum value of the flow velocity to reach maximum values of the number of deposited swimmers is an important design information for different applications that use microbial filtration. Finally, in general, it is found that optimal adhesion that has larger values of λ_{trap} and smaller values of τ_{trap} is obtained for more-persistent swimmers moving at small velocities interacting with small obstacles.

Keywords: ABP, biofilm, filtration, motility, bacterial accumulation, microswimmers

1 INTRODUCTION

The interaction of microorganisms with surfaces has been extensively studied in the last years [1–5], showing that active particles, in general, spend long times exploring surfaces, enhancing microbes' first adhesion or attachment to them [6–9]. This seed or precursor of biofilm formation might be optimized if, for instance, bacteria self-organize forming stains or clusters in the space producing density gradients or, in very dense systems, orientation gradients [10, 11]. In this last case, the bacteria produce attractive fluxes on the fluid that can replenish nutrients or oxygen to the biofilm.

On the other hand, one of the principle benefits of active particle's attraction to surfaces is microbes filtration [12]. This has been studied theoretically in the first works of Rubenstein *et al.* [13] and later with the work of Shimeta *et al.* [14]. In both cases, they analyzed the problem of microbes passing through a circular obstacle moving in a Stokes flow. By performing a dimensional analysis among different filtration parameters such as microbes activity, relative size, and relative density, they could give glances of how microbes filtration, depending on this parameters, experience different regimes where microbes' adhesion to the surface is mediated by different physical mechanisms.

In Nature and industry, motile and non-motile microorganisms are often constricted to move on micro-channels or through porous media in the presence of external flows such as sperm in the female reproductive tract, microbes on the urine tract, soil bacteria through roots, bacteria on phytoremediation treatment, plants and bacteria on mining bioflotations [7, 15–17]. Microorganisms in all these cases are constricted to move through a series of obstacles that, recently, has been reproduced under novel laboratory conditions. It has been observed that the transport and particle's dispersion across obstacles are strongly dependent on the external flow, obstacle radius, and bacterial strains or motility [18–21]. In this aspect, Alonso-Matilla *et al.* [22] studied theoretically the transport of active agents through an array of obstacles of different shapes, showing that the external flow might span different dispersion mechanisms. Recently, Secchi *et al.* [20] performed experiments using different strains of bacteria, whereby measuring the capture efficiency, they found that depending on their motility, the external flow, and obstacle size, the bacteria attachment was located at specific regions of the collecting surface. In recent works, the role of hydrodynamic interactions (HI) and activity, in microbe adhesion on complex surfaces, has been studied either numerically [23–27], theoretically [28–31], and experimentally [19, 20, 32–35], showing that motility define a sharp difference in particle adhesion with non-motile particles. In the case of flagellated microswimmers, their hydrodynamic interactions with the surface are crucial to understand the contact angle for particle-obstacle interactions, and therefore determine the contact time with the surface, which is a key to prop the first adhesion [6]. HI are also important to enhance predation opportunity by microbe's entrainment on convex surfaces [28, 33] and relevant in the accumulation of active particles in the rear of an obstacle, under the effect of an external flow and due to the effect of upstream swimming for elongated microswimmers [23].

Surprisingly, the artificial microswimmers such as active colloids also explore pillar's surfaces for long time, revealing that varying microswimmer's activity effectively changes microswimmer's accumulation on surfaces [32]. Sipos *et al.* [35] explored the role of obstacle curvature on bacterial adhesion finding that there is a characteristic radius of 140 μm , where entrapment is reduced.

Here, we present a simple model for active Brownian particles [36] to study microbe's adhesion on convex surfaces under the effect of an external flow. The particle-obstacle hydrodynamic interactions are modeled with a short-range attractive interaction to the obstacle's surface. Two types of active particles are studied, with different swimming persistences (low and large persistence). By adding a short-range repulsive interaction between microswimmers, we can reproduce bacterial attachment over circular obstacles of different radii [35] and the bacterial attachment on specific regions of the obstacle, depending on the relation between microswimmer's activity and external flow [20]. Furthermore, by varying the microbe's activity, we found a narrow velocity screen where microswimmer's adhesion strongly changes and might determine microbes first adhesion to the surface by changing the contact time with the surface. We find that more-persistent microswimmers with low activity moving close to small obstacles, rather than big ones, in the presence of intermediate external flows optimize microbe's adhesion on the surfaces, where the number of microswimmers attached to the surface increases and the system reaches faster the steady state. We expect that this detail study might help to improve *in vitro* fertilization, bio-inspired chemical treatments in industry to optimize biofilm formation, and other processes where the accumulation in surfaces is relevant.

1.1 Numerical Model

To describe the microbe's motion, we model microswimmers as active Brownian particles (ABP) in two dimensions [37]. Here, each swimmer moves at constant speed u_0 with a persistent orientation $\hat{e}(t)$ that undergoes rotational diffusion. That is, the orientation changes smoothly on time as compared to run-and-tumble particles (RTP), for which the director changes abruptly at discrete events. Although different, it has been shown that at large times, both models present similar dynamics and there is a direct mapping of the tumbling rate to rotational diffusion coefficient D_R [38]. The microswimmers are circular particles with diameter $2a$ that interact between them by excluded volume only, and no mutual alignment takes place. The ABP model, despite its simplicity, is known to reproduce many of the observed properties of microswimmers, in particular the accumulation near walls, regime where it has also been shown that the key features are equivalent to other models of active particles [39]. On the other hand, the simplicity of the ABP model, characterized by a few parameters, allows for systematic analysis and to unveil the key features of relevant phenomena for a wide range of microswimmers, without needing to model specific details of each microswimmer under study. Finally, we restrict to spherical swimmers as it has been shown that considering the ellipticity only changes quantitatively the results, with the same phenomenology as for spherical particles for the study of accumulation in surfaces [23]. The

use of this model here shows how different accumulation regimes appear as a function of the self-propulsion speed compared to the imposed flow.

There is a single circular obstacle of radius R , which is impenetrable by the swimmers. At short distances, due to hydrodynamic interactions, pusher swimmers, like bacteria, are attracted to solid surfaces and they are aligned to swim parallel to them [2]. To correctly describe this interaction, for example, to get finite-induced velocities, near field hydrodynamics should be considered [40, 41], which are specific for each microbe. Instead, to mimic this effect in a more general way, without introducing hydrodynamic interactions, which are also computationally expensive, we introduce a short-range attractive force that exerts the obstacle on the swimmers and a torque that aligns them. The whole system is subject to an imposed external flow. We assume that the swimmer concentration is low enough such that the induced flow generated by them can be neglected. Hence, the form of this velocity profile is simply the one that results from the interaction of the external flow with the obstacle. Finally, the modeling is done in two spatial dimensions; the extension to three dimensions is direct.

The swimmers' motion is completely described by the low Reynolds dynamics, i.e., inertia can be completely neglected. Hence, instead of forces and torques, it is more convenient to describe interactions by the induced linear and angular velocities they generate. Thus, the equations of motion for the position \vec{r}_i of swimmer i are

$$\frac{d\vec{r}_i}{dt} = u_0\hat{e}_i + u(\vec{r}_i) + \vec{u}_O(\vec{r}_i) + \sum_{i \neq j} \vec{u}_S(|\vec{r}_i - \vec{r}_j|), \quad (1)$$

where the first term is the self-propulsion along the director, the second term is the drift produced by the external flow, and the last two terms are the induced velocities produced by the interaction with the obstacle and other swimmers, respectively. Similarly, for the director \hat{e}_i ,

$$\frac{d\hat{e}_i}{dt} = \left[\frac{1}{2} \nabla \times \vec{u}(\vec{r}_i) + \vec{\Omega}_O(\vec{r}_i, \hat{e}_i) + \sqrt{2D_R} \vec{\xi} \right] \times \hat{e}_i, \quad (2)$$

where the first term describes the rotation induced by the flow vorticity, that for a spherical swimmer adopts this simple form [42, 43], the second one accounts for the reorientation of the swimmer by the interaction with the obstacle, and the last one is a stochastic term, with ξ a white noise, that produces rotational diffusion with a diffusion coefficient D_R . The cross product with the director guarantees that remains unitary. No swimmer-swimmer torques are considered.

For an ambient fluid with density ρ , viscosity η , and a small imposed flow $U_\infty \hat{x}$ far from the obstacle, the presence of the obstacle centered at the origin of the coordinate system results in the velocity profile $\vec{u}(\vec{r}) = U_\infty [(1 + \frac{R^3}{2r^3} - \frac{3R}{2r}) \cos \theta \hat{r} - (1 - \frac{R^3}{4r^3} - \frac{3R}{4r}) \sin \theta \hat{\theta}]$. Here, $r = |\vec{r}|$ is the distance to the origin, θ is measured with respect to the \hat{x} axis and $(\hat{r}, \hat{\theta})$ is the pair of polar unit vectors.

The obstacle has radius R and the interaction is modeled with a potential U_O , such that $\vec{u}_O(\vec{r}) = -\nabla U_O(\vec{r})$. The potential is attractive in the adhesion region, $R < r_i < \epsilon_0 + R$, and is repulsive for $r < R$, describing the rigidity of the surface (see

Figure 1A). This interaction mimics, in a simple way, electrostatic, hydrodynamic, or substrate effects on surfaces [16, 32, 33, 35], and allows for reversible adhesion to the surface. For simplicity, we use a Morse potential to have a simple expression valid for all distances:

$$U_O(\vec{r}_i) = U_O [e^{-2\beta_M(r_i - R_M)} - 2e^{-\beta_M(r_i - R_M)}]. \quad (3)$$

When the microswimmer is close to the surface of the obstacle, there is also a torque that aligns the swimmer with the surface. For simplicity, we consider that the induced angular velocity is

$$\vec{\Omega}_O(\vec{r}_i, \hat{e}_i) = \begin{cases} \Omega_O \hat{r}_i \times \hat{e}_i & , \text{if } |\vec{r}_i| < R + \epsilon_0 \\ 0 & , \text{otherwise} \end{cases}, \quad (4)$$

with the same range as the interaction potential.

For the swimmer-swimmer interaction, we use a simple repulsive Yukawa potential

$$\vec{U}_S(\vec{r}) = U_S e^{-r/(2a)} / r, \quad (5)$$

which gives the induced velocity $\vec{u}_S(\vec{r}) = -\nabla U_S(\vec{r})$.

The simulation is performed in a stripe of size $L_y = 4R$ in the vertical direction and unbounded in the x direction. Periodic boundary conditions are used in the y direction. To generate a continuous injection of microswimmers that approach the obstacle, particles are released periodically, every τ_{wave} , at a distance $d_0 = 3R$, randomly distributed along L_y . Each wave is composed of $N = 100$ microswimmers, uniformly distributed in the chamber all pointing initially in the positive \hat{x} direction (see **Figure 1A**). The distance to the obstacle is sufficient for the swimmers to randomize and in the different observables that quantify the accumulation of swimmers in the obstacle, and there is no signature of the periodicity τ_{wave} .

1.2 Model Parameters and Numerical Implementation

The model has several parameters, characterizing the motion of the swimmers, their mutual interaction, and the interaction with the wall, as well as the properties of the imposed flow and obstacle size. In this study, we focus on varying the swimmer's speed u_0 , the imposed flow U_∞ , and the obstacle radius R . The rest of the parameters are fixed to represent typical experimental and natural conditions.

We set the microswimmer's diameter $2a = 1 \mu\text{m}$ in the Yukawa potential, as the length scale of the problem. The time scale of the problem is set by the rate of particle injections $\tau_{\text{wave}} = 1 \text{ s}$. Hence, in what follows, all lengths and times, and the derived units, are expressed as dimensionless quantities.

We define the obstacle adhesion region in $\epsilon_0 = 7$, which accounts for the typical hydrodynamic effects in the vicinity of the obstacle [19, 20, 28]. The intensity of the interactions is rather arbitrary as it is only needed that excluded volume is accurately achieved. We use $U_S = 2$, $U_O = 3.2$, $\beta_M = 1.44$, and $\Omega_O = 0.28$, which are sufficient to enforce the excluded volume with the integration time step $\Delta t / \tau_{\text{wave}} = 1 \times 10^{-3}$ and a rapid

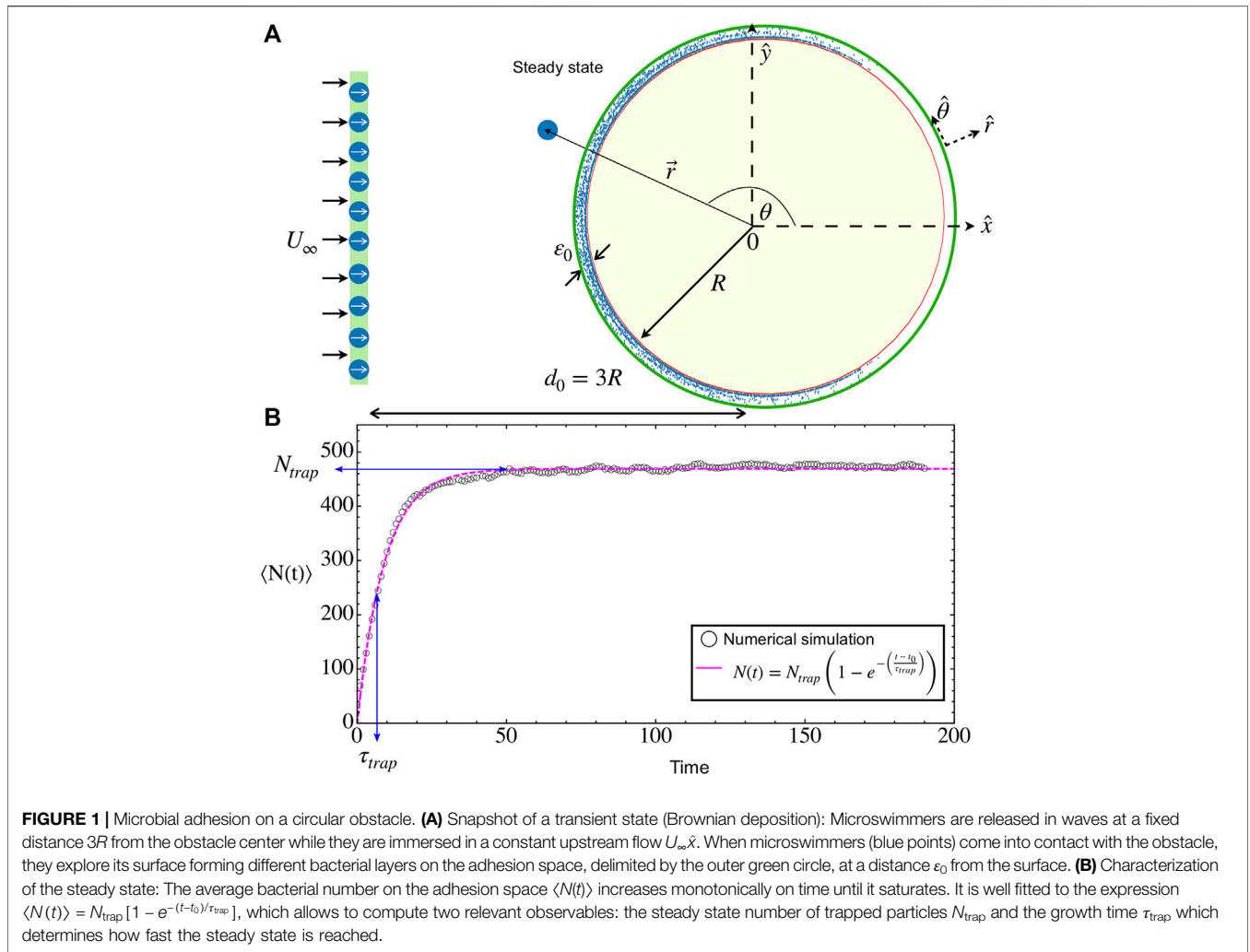


FIGURE 1 | Microbial adhesion on a circular obstacle. **(A)** Snapshot of a transient state (Brownian deposition): Microswimmers are released in waves at a fixed distance $3R$ from the obstacle center while they are immersed in a constant upstream flow $U_\infty \hat{x}$. When microswimmers (blue points) come into contact with the obstacle, they explore its surface forming different bacterial layers on the adhesion space, delimited by the outer green circle, at a distance ϵ_0 from the surface. **(B)** Characterization of the steady state: The average bacterial number on the adhesion space $\langle N(t) \rangle$ increases monotonically on time until it saturates. It is well fitted to the expression $\langle N(t) \rangle = N_{\text{trap}} [1 - e^{-(t-t_0)/\tau_{\text{trap}}}]$, which allows to compute two relevant observables: the steady state number of trapped particles N_{trap} and the growth time τ_{trap} which determines how fast the steady state is reached.

alignment with the obstacle. We consider two microswimmer types, with very different persistences, characterized by their rotational diffusion coefficient: *more-persistent* microswimmers with $D_R = 0.16$ [44, 45], and *less-persistent* ones with $D_R = 0.6$ [46]. This classification is related with different bacterial strains modified and used for medical or experimental tasks [17].

We solve the equations of motion (1) and (2) using molecular dynamics simulations with the Euler-Maruyama integration method, for a total time of 200 s. To improve the computational efficiency, we implemented *cell lists* for the particle-particle interactions and an effective *cut-off* for the particle-obstacle interaction in order to avoid unnecessary interactions when their distance is large [47].

To study how the activity u_0 , obstacle radius R , and external flow U_∞ affect the first adhesion of microbes, we performed three different studies varying different parameters, for both microswimmer's types.

- i. Microswimmer activity: in this case, we will fix the obstacle radius $R = 100$ and the external flow $U_\infty = 40$, unless otherwise

indicated. We study bacterial activity in the range $u_0 = 14, \dots, 65$.

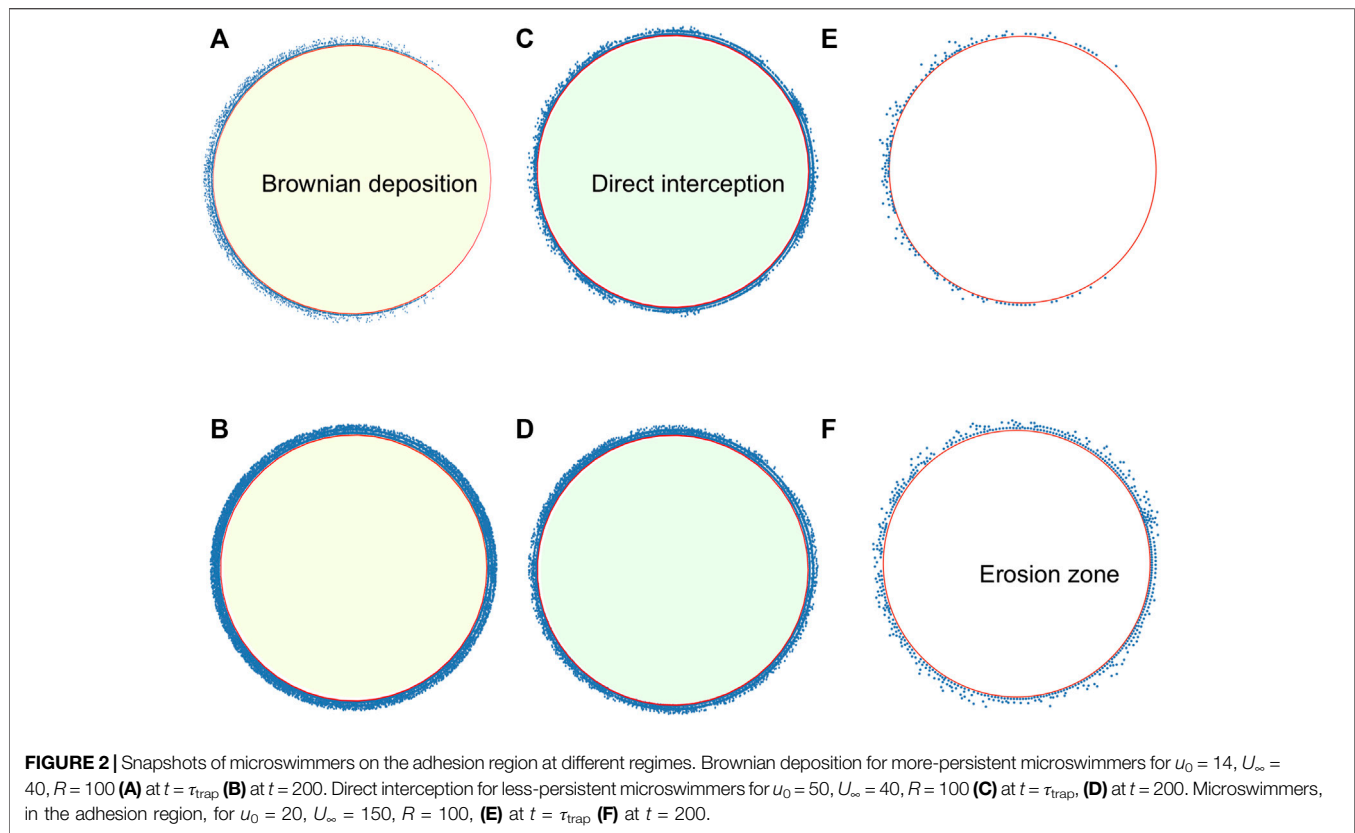
- ii. Obstacle radius: in this case, we will fix $u_0 = 20$ and $U_\infty = 40$, while varying R in the range $10, \dots, 350$.
- iii. External flow: in this case, we fix the obstacle radius $R = 100$ and the microswimmer activity $u_0 = 20$, while varying $U_\infty = 10, \dots, 200$.

With these set of parameters, the concentration of swimmers in the bulk of the system is dilute. Yet, still accounts a considerable accumulation of microswimmers on the obstacle surface. We performed 24 different simulations for each studied parameter combination and, for all cases, we show the average results.

2 RESULTS

2.1 General Features and Observables

For all considered cases of velocities and obstacle radii, the temporal dynamics is rather similar. First, it takes a time $t_0 \sim$



$3R/(u_0 + U_\infty)$ for the first swimmers that were injected into the system to reach the obstacle. After this time, there is a continuous income of swimmers to the obstacle. Some of them will reach the adhesion region and remain there while swimming and being advected by the flow. Interactions between swimmers create crowded environments that enhance the residence time in this zone but, also, it is possible to scatter bacteria from the surface after an encounter, helping their erosion by the external flow. As a whole, the total number of particles in the adhesion zone $N(t)$ starts to increase steadily after t_0 until it saturates to the steady value N_{trap} (see **Figure 1B** and the **Supplementary Video S1**). In all cases, the average growth curves can be well fitted to the model

$$\langle N(t) \rangle = N_{\text{trap}} \left[1 - e^{-(t-t_0)/\tau_{\text{trap}}} \right], \quad (6)$$

where τ_{trap} gives the relaxation time to reach the steady state, similar to the probability of successful interaction presented in Refs. [28, 48]. Considering that the incoming rate is constant, having **Eq. 6** as solution of the balance equation implies that the desorption rate is proportional to the actual number of particles in the adhesion layer. In the steady state, the obstacle is saturated and ready for microbes to form the first adhesion [6, 8]. From the simulations, we will obtain τ_{trap} and N_{trap} , which are important parameters to characterize and optimize the microbe's adhesion in convex surfaces.

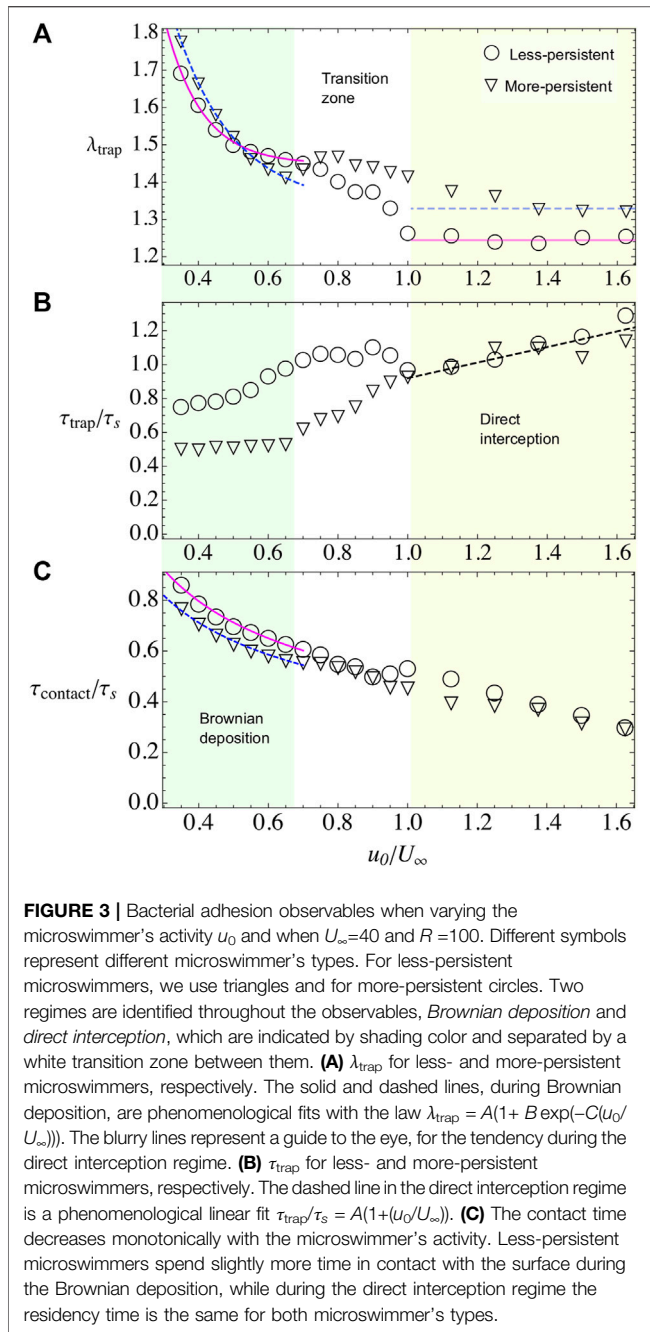
Figure 2 presents snapshots of the system in the three regimes that are described in the text for the transient at $t = \tau_{\text{trap}}$ and in the steady state. In the transient, the distribution is not uniform with

particles still being transported along the perimeter, except for the direct interception regime, where the distribution is uniform, although with less particles than in the steady state. In all cases, it is seen that the steady-state distribution is rather uniform in the circle, contrary to other studies where there is a larger accumulation in the back [20, 23]. The three regimes differ notably on the number of accumulated particles.

Another relevant observable is the contact time of microswimmers with obstacle's surface, τ_{contact} . This parameter gives the average residency time of microbes on the surface and therefore the time available to realize an irreversible adhesion to prompt a biofilm. It is measured, for each set of parameters, as the mode considering 24 realizations of the time that particles spend inside the adhesion region.

The number of trapped particles can be compared to the maximum occupation in a monolayer, $N_{\text{max}} \equiv 2\pi R/(2a)$, which allows us to define the dimensionless average number of deposited layers $\lambda_{\text{trap}} = N_{\text{trap}}/N_{\text{max}}$. Similarly, the relaxation time and the contact time can be compared to the time it takes a swimmer to travel the obstacle by its own, $\tau_s \equiv \pi R/u_0$.

Using dimensional analysis, we expect that the microbial behavior depends on the Péclet number which compares advective transport with diffusion $Pe = u_0/(RD_R)$. Then, in the limit of $Pe \rightarrow 0$, we expect that Brownian diffusivity dominates microswimmer's exploration of the medium, the phenomenon is known as "Brownian deposition." While in the other limit $Pe \rightarrow \infty$, the advection dominates and particles encounter the obstacle surface by "direct interception" [13, 14]. When varying the



microswimmer’s activity, in a biological range of velocities [8], we are changing the Péclet number in a narrow window for each microswimmer’s type, and the two limiting cases are not always achieved. Furthermore, the external velocity allows to define new dimensionless parameters. Therefore, for simplicity, we present the results in terms of the control parameters, where the transition between both regimes can also be appreciated.

2.2 Varying Swimmer’s Activity

Here we keep the obstacle radius constant to $R = 100$ and vary the swimmer’s speed u_0 . For the imposed flow, we consider three

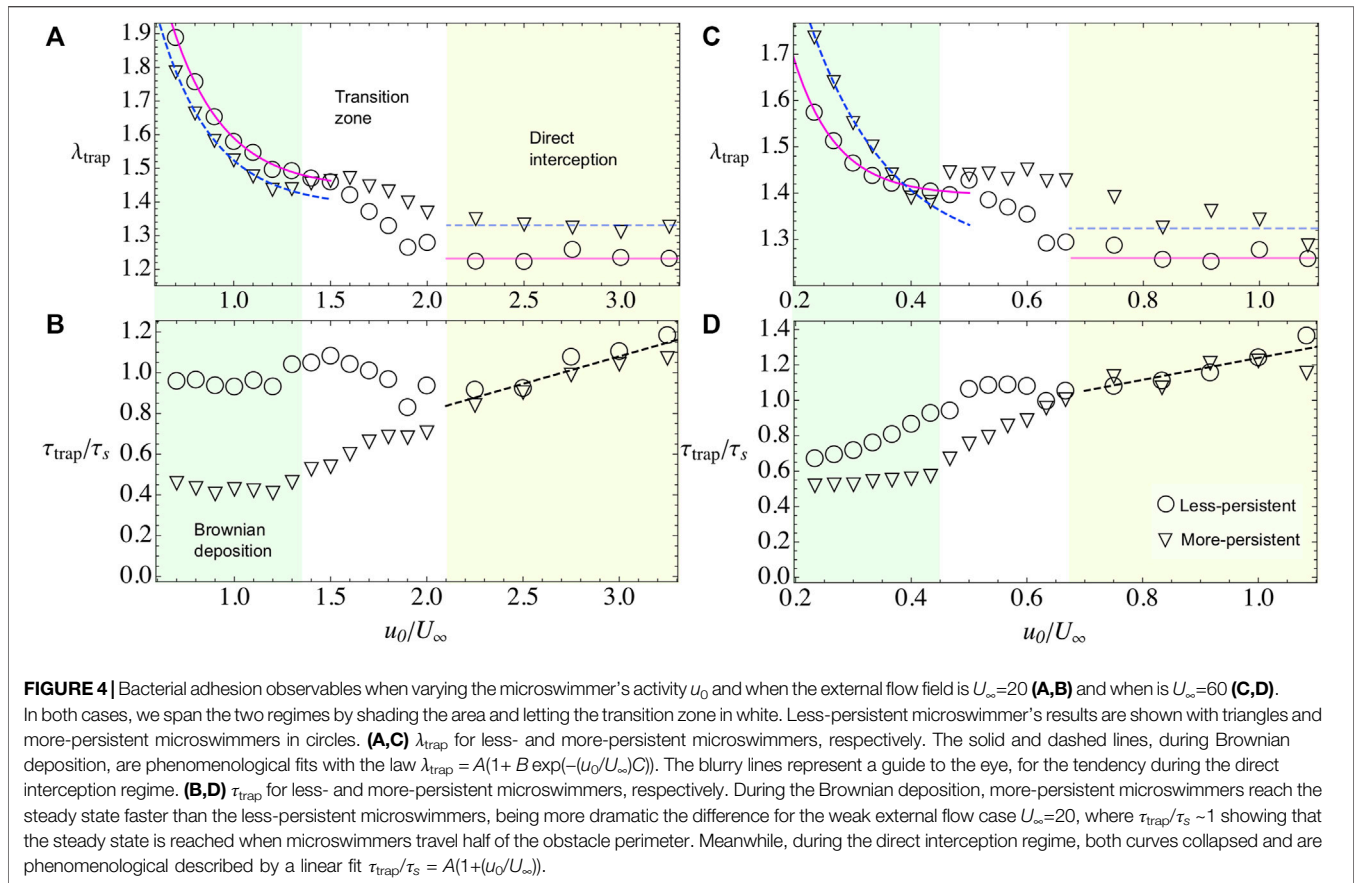
different values: $U_\infty = 20, 40$, and 60 . We found that depending on the microswimmer’s activity and external flow there are, basically, two different regimes. In one of them, the microswimmer’s velocity is smaller compared with external flow, yet particles diffuse across the streamlines and settle around the obstacle covering the whole perimeter and forming multiple layers, this regime is known as *Brownian deposition* [13, 14]. In the second regime, when particle’s activity is larger than the external flow, particles scatter faster forming approximately one layer on the obstacle surface. The particle’s capture now depends only on the *direct interception* with the obstacle. In **Figure 3**, we show λ_{trap} , τ_{trap} , and the contact time τ_{contact} for the case $U_\infty = 40$, for both values of persistence. These three observables decrease with the parameter u_0/U_∞ . Naturally, as the swim speed increases, the relaxation and contact times decrease accordingly. Also, the thickness of the deposited layer decreases as particles can escape more easily due to excluded volume interactions with other microswimmers.

2.2.1 First Regime: Brownian deposition

In this regime, microswimmers move slowly than the external flow. Nevertheless, the particles are not purely advected by the flow, on the contrary, they perform an exploration of the space crossing the streamlines and diffusing across the simulation area (see **Supplementary Video S1**). At contact with the obstacle, the flow velocity vanishes and it remains small in the adhesion region, defined as a ring of width $\epsilon_0 = 7$ across the obstacle’s surface. Hence, the attractive potential becomes a dominant factor, increasing the contact time between microswimmers and the obstacle (**Figure 3C**), and also increasing the number of microbes in the adhesion region λ_{trap} (**Figure 3A, Figure 4A,C**). Moreover, the microswimmers also present a transition zone (see **Figures 3,4**), at $u_0^* \sim 30$ for all external flow’s values, where particle capture slightly increases before entering in the *direct interception* regime.

We find that λ_{trap} depends on the external flow. In general, when the external flow is slower than particle’s velocity, the microswimmers can stay around the adhesion space increasing the number of trapped particles while, for stronger flows, the capture decreases. In the case of, less-persistent microswimmers (circles in **Figures 3,4**). For weak flows $U_\infty = 20, 40$ (**Figures 3A,4A**), respectively, the microswimmer’s disperse more enhancing the adhesion [21] and exploring for longer times the obstacle’s surface (**Figure 3C**), while for strong flows $U_\infty = 60$ (**Figure 4C**), since the particle trajectories are very noisy, it is highly probable to encounter another particle. As a result of the interaction, the particle can be easily kicked out from the adhesion area and dragged by the external flow, decreasing the fraction of microbes adhered to the obstacle, for all cases, with $\lambda_{\text{trap}}(u_0/U_\infty) = A + B \exp(-(u_0/U_\infty)C)$, finding that the rate of decay C for less-persistent microswimmers increases with U_∞ being $C(U_\infty = 20) = 3.68$, $C(U_\infty = 40) = 9.47$, and $C(U_\infty = 60) = 13.53$ with $A \approx 1.4$ and $B \approx 4$.

More-persistent microswimmers are less affected by the external flow, in this regime (inverted triangles in **Figures 3,4**), we found a less dramatic rate of decay C with $C(U_\infty =$



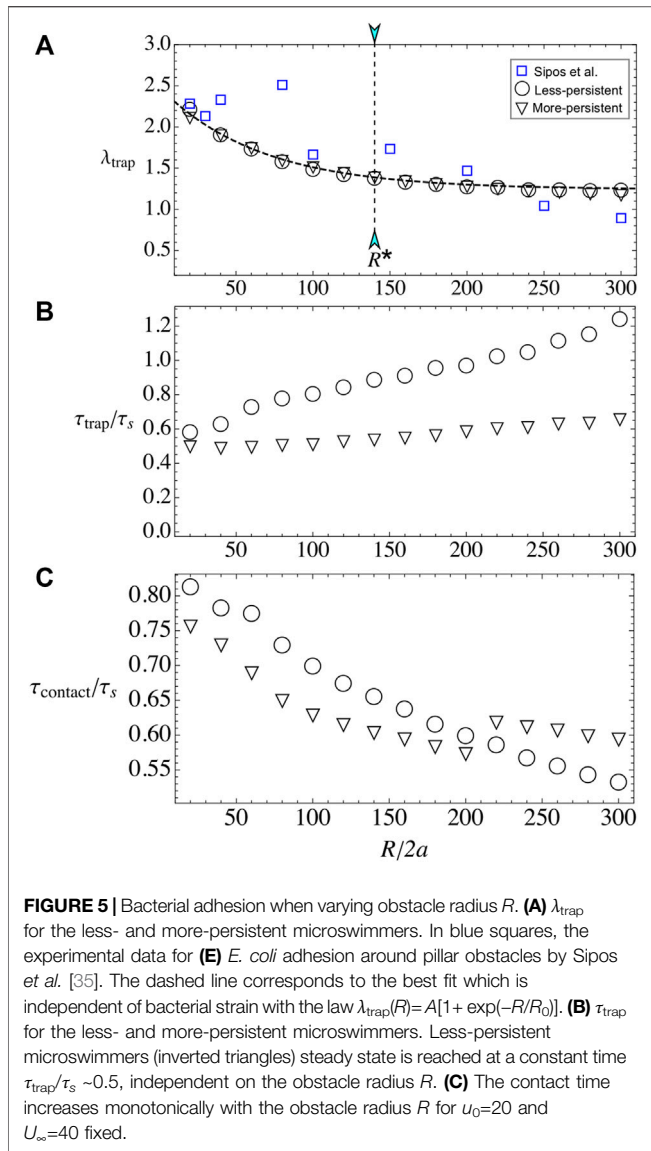
20) = 3.57, $C(U_\infty = 40) = 5.91$, and $C(U_\infty = 60) = 7.15$, respectively, and $A \approx 1.3$, $B \approx 3$. Then, since the microswimmers perform less reorientations, microbe's capture is faster as we can observe in **Figure 3B**, **Figure 4B,D** for different external flows. The relaxation time τ_{trap} has a similar behavior for all U_∞ . We found that during this regime, more-persistent microswimmers reach the steady state before a single microswimmer performs an exploration around the obstacle's perimeter with $\tau_{\text{trap}}/\tau_s \sim 0.5$ in all cases, while less-persistent microswimmers take longer times depending on the external flow.

The contact time that in average microswimmers spent on the adhesion region decays as $\tau_{\text{contact}} = (AU_\infty/u_0)^{1/2}$, with $A = 0.25$ and $A = 0.2$ for the less- and more-persistent microswimmers, respectively (**Figure 6A**), following a power law as [25]. According to Secchi *et al.* [20], non-motile particles distribute uniformly around the obstacle's surface while motile microswimmers accumulate on the back of the obstacle [19, 20]. Here, since microswimmers are slow, we observe something similar to the case of non-motile microswimmers since they spent more time close to the surface while they diffuse around the adhesion space.

2.2.2 Second Regime: Direct Interception

In this regime, the self-propulsion is higher than the external flow, thus microswimmers move freely around the obstacle's

surface. They are scattered out from this region when they meet another microswimmer and, due to excluded volume interactions, they are deviated from their trajectory, or when they change their orientation due to rotation diffusion. Then, particle's capture decreases as they move faster and the steady state is also reached faster (see **Figure 3B**, **Figures 4B,D**). The number of captured particles is roughly independent of U_∞ for both the more- and less-persistent microswimmers, being the number of more-persistent microswimmers in the adhesion region higher than the less-persistent. The steady state is reached at the same time for all microswimmer's type, and varying slightly with the external flow. In **Figure 3B**, **Figure 4B,D**, the dashed line shows the best fit, which follows $\tau_{\text{trap}}(u_0/U_\infty)/\tau_s = A(1 + u_0/U_\infty)$, with $A(U_\infty = 20) = 0.27$, $A(U_\infty = 40) = 0.46$, and $A(U_\infty = 60) = 0.62$. In average, the steady state is reached after one particle travels half of the obstacle's perimeter, that is, $\tau_{\text{trap}} \approx \tau_s$ for both microswimmer's persistences and the same happens for the contact time (see **Figure 3C**). Thus, since microswimmers are fast, the steady state is reached after there is a constant number of microswimmers exploring the back of the obstacle's adhesion space [19, 20]. In this regime, the microbe's adhesion is optimized for the more-persistent microswimmers since the obstacle captures the same number of particles, and they spent the same amount of time on the surface, yet the steady state is reached faster.



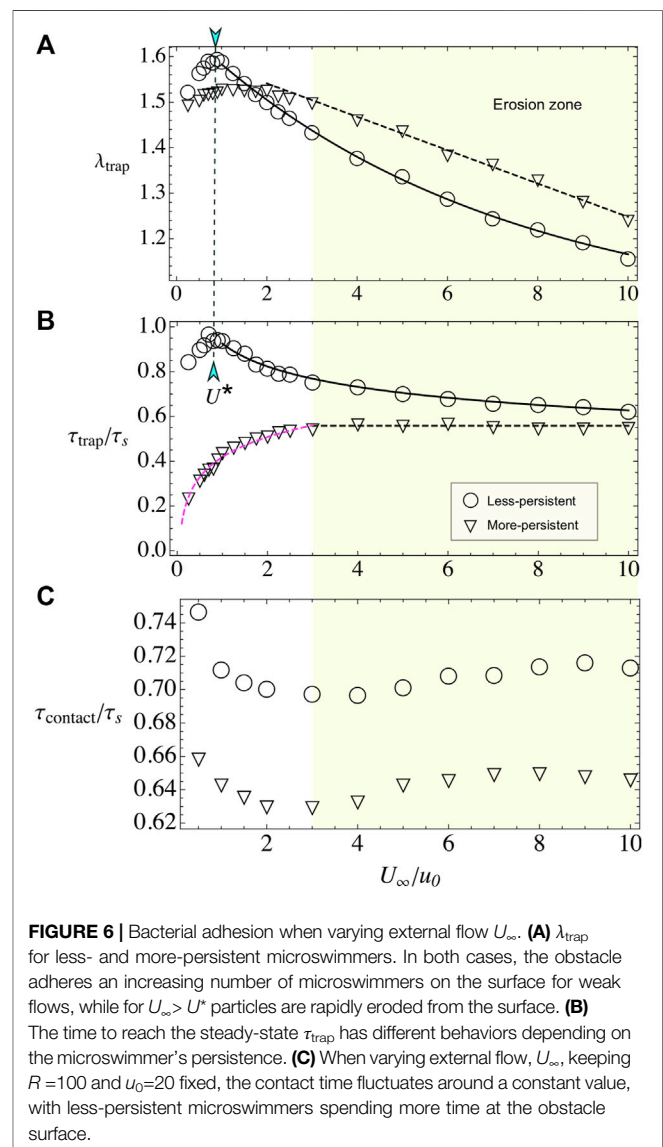
2.3 Varying the Obstacle Radius

Now, we vary the obstacle radius R , while keeping fixed the microswimmer’s activity to $u_0 = 20$ and the external flow to $U_\infty = 40$, unless otherwise indicated. The number of layers λ_{trap} decreases with R (**Figure 5A**). Small pillars are capable to adhere more than two layers of microbes and for large radii, the number of layers saturates to a value slightly larger than one. The results are well fitted to the expression $\lambda_{\text{trap}}(R) = A[1 + \exp(-R/R_0)]$, with $A = 1.24$ and $R_0 = 65.2$, independent of microswimmer’s type and external flow. With this, the total number of accumulated particles increases monotonically with R . Microbe’s capture is in agreement with some experimental results in cylindrical pillars, either for biological microswimmers such as bacteria or algae [33, 34] or artificial microswimmers [35], where there is a critical radius for constant particle’s capture located at $R^* \approx 140$.

Regarding the relaxation time, the more-persistent microswimmers reach the steady state faster than the less-persistent ones, and in both cases τ_{trap} grows with the radius. The results show that for more-persistent microswimmers follows $\tau_{\text{trap}}/\tau_s \sim 0.5$ for all R (see **Figure 5B**), while for less-persistent microswimmers the steady state increases linearly with the obstacle radius. The time that particles remain in contact with the surface τ_{contact} increases also with obstacle’s radius, similar to Refs. [32, 35], but it does not follow the simple law $\tau_{\text{contact}}(R) \approx \tau_s$ (see **Figure 5C**). Instead, the contact time increases with R for both microswimmer’s types, yet there is not linear dependence on its growth. Thus, the microbe’s adhesion is enhanced with small pillar radius and less-persistent microswimmers.

2.4 Varying External Flow

Here, we vary the external flow U_∞ , while we keep fixed the bacterial activity to $u_0 = 20$ and the obstacle radius to $R = 100$. The



number of captured layers presents a non-monotonic behavior, with a pronounced maximum for the less-persistent swimmers at $U^* \approx 1$, where the microswimmer and the flow velocities are similar. For the more-persistent swimmers, the maximum is less pronounced and it is located at $U^* \approx 2$ (see **Figure 6A**). For larger external velocities, microbe's adhesion decreases due to erosion by the flow [19, 20, 49]. For the less-persistent swimmers, the erosion is well fitted to the expression $\lambda_{\text{trap}}(U_\infty/u_0) = 1 + 0.66 \exp(-0.15U_\infty/u_0)$, according with microbe's erosion of the surface [20, 49]. For the more-persistent microswimmers, the decrease of λ_{trap} is slower and well fitted to $\lambda_{\text{trap}}(U_\infty/u_0) = 1.62 - 0.037(U_\infty/u_0)$, similar to the experimental limit for erosion observed by Miño *et al.* [19].

In the case of relaxation time, we observe a very different behavior for the two analyzed persistences. For the less-persistent microswimmers, τ_{trap} is non-monotonic, with a maximum at U^* and larger values than for the more-persistent swimmers (see **Figure 6B**). In the erosion phase, the time that takes to reach the steady state, for less-persistent microswimmers, decays as $\tau_{\text{trap}}(U_\infty/u_0)/\tau_s = 0.9(u_0/U_\infty)^{1/6}$. For more-persistent microswimmers, the τ_{trap} time increases following a law $\tau_{\text{trap}}(U_\infty/u_0)/\tau_s = 0.13 \log(25.7U_\infty/u_0)$ in the first phase for $U_\infty/u_0 < 3$ and then, in the erosion zone, it is constant with $\tau_{\text{trap}}/\tau_s \approx 0.56$.

Surprisingly, the contact time is constant (see **Figure 6C**), even in the erosion zone, with small variations around $\tau_{\text{contact}}/\tau_s \approx 0.63$ for the more-persistent swimmers and $\tau_{\text{contact}}/\tau_s \approx 0.71$ for the less-persistent ones. We state that the existence of this almost constant value in the contact time is related with the accumulation of microswimmers in the front and in the back of the obstacle, where there are stagnation points. The particles are expelled from these regions then by their own activity but not on by the flow [20]. Consistent with this hypothesis, the less-persistent swimmers present larger contact times. Also, in the transport of the swimmers along the adhesion zone, the imposed flow almost vanishes there, resulting in that the contact time is dominated by the travel time τ_s .

3 DISCUSSION

We showed, with a simple ABP model, that optimizing microorganism attachment to surfaces is possible by using the right set of mechanical and biological parameters for a given problem. Our simple model proves to be in agreement with the previous quantitative and qualitative theoretical and experimental results for biological and artificial microswimmers [19, 20, 32, 35]. We found that particle's capture around the adhesion region of a circular obstacle diminishes with the particle's activity in all the regimes and for both studied microswimmer's types, namely less- and more-persistent ones. In the case of active Janus particles, Simmchen *et al.* [32] found that increasing hydrogen peroxide concentration or activity in their experiments results in a particle's fluorescence increase around the pillars. However, in that case, there was no external flow, and the same applies to the

theoretical works for filters [13, 14]. In our model, we considered particle-particle interactions. Therefore, the scattering between particles is now very sensitive to the applied external flow showing that the limiting streamline around the obstacle determines particle's capture [24].

We also observed that the net accumulation is larger for the more-persistent swimmers. Also, although for both microswimmer's types the contact time increases with obstacle radius, more-persistent microswimmer's tend to reach the steady state faster, showing that again they are good candidates for the optimization in biofilm formation. Then, by choosing the right nutrient or fuel source for microswimmers and the right microswimmer strain (less or more noisy), it is possible to enhance the chances in bacterial encounter with the obstacle's surface. This might be also relevant for medical applications such as *in vitro* fertilization.

In the case of varying obstacle's radius, we found that small obstacles can capture more particle's layers. Larger obstacles, even though have more space to capture swimmers, are less efficient. We also found that for a limiting radius, particle's capture becomes constant in agreement to previous results by Sipos *et al.* [35]. Finally, we explored the case when we vary the external flow which in the last years has been one of the most revisited problems in microswimmer's filtration [21, 22, 27], particle hydrodynamic entrainment [28–30, 33, 34], and obstacle adhesion [19, 20]. We found a non-explored behavior for more-persistent microswimmers with a slower decay in particle's capture in the erosion region and lower times for the system to reach the steady state in this case. We also could predict the velocity for the external flow passing through a circular obstacle [19] at which the erosion of the surface starts.

Our model can be straightforward applied in 3D obstacles, dense systems, porous media, or in different external flow conditions. It is also possible to extend the simple ABP model to include aligning interactions for elongated microswimmers, far-field interactions to study complex microbes, tumbling, polydispersity, or other effects. Also, different experiments show that the microbe-wall interaction is more complex than the simple attraction and alignment that we incorporated in the model, including rheotaxis [50], upstream swim [51], circular motion [52], and changes in the tumbling rate [53]. The influence of these and other effects, as well as the extension to the ABP model, must be studied in detail for quantitative predictions for specific microbes. Finally, choosing the right set of mechanical parameters such as external flow and obstacle's radius could open new avenues in the control of bacterial deposition on roots in hydroponic crops or in mining bioflotations, opening new environmentally friendly alternatives in engineering and industrial applications.

DATA AVAILABILITY STATEMENT

All simulation codes and raw data used for this paper are available from the corresponding authors upon request.

AUTHOR CONTRIBUTIONS

FG-L and RS designed and planned research collaboratively and wrote the paper. BE and TF developed the theoretical model, and performed the numerical simulations.

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SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: <https://www.frontiersin.org/articles/10.3389/fphy.2022.865937/full#supplementary-material>

Supplementary Video S1 | Simulation for less-persistent microswimmers for an obstacle of radius $R = 100$, External flow $U_\infty = 40$ and microswimmer's activity $u_0 = 20$.

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