Check for updates

OPEN ACCESS

EDITED BY Enis Ozyar, Acıbadem University, Türkiye

REVIEWED BY Rei Umezawa, Tohoku University Hospital, Japan Alessio G. Morganti, University of Bologna, Italy

*CORRESPONDENCE Masato Tsuneda Masato.tsune@gmail.com

[†]These authors have contributed equally to this work and share first authorship

RECEIVED 09 November 2023 ACCEPTED 15 April 2024 PUBLISHED 10 May 2024

CITATION

Kurokawa M, Tsuneda M, Abe K, Ikeda Y, Kanazawa A, Saito M, Kodate A, Harada R, Yokota H, Watanabe M and Uno T (2024) A pilot study on interobserver variability in organ-at-risk contours in magnetic resonance imaging-guided online adaptive radiotherapy for pancreatic cancer. *Front. Oncol.* 14:1335623. doi: 10.3389/fonc.2024.1335623

COPYRIGHT

© 2024 Kurokawa, Tsuneda, Abe, Ikeda, Kanazawa, Saito, Kodate, Harada, Yokota, Watanabe and Uno. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.

A pilot study on interobserver variability in organ-at-risk contours in magnetic resonance imaging-guided online adaptive radiotherapy for pancreatic cancer

Marie Kurokawa^{1†}, Masato Tsuneda^{2*†}, Kota Abe², Yohei Ikeda³, Aki Kanazawa³, Makoto Saito³, Asuka Kodate³, Rintaro Harada³, Hajime Yokota¹, Miho Watanabe¹ and Takashi Uno¹

¹Diagnostic Radiology and Radiation Oncology, Graduate School of Medicine, Chiba University, Chuo-ku, Chiba, Japan, ²Department of Radiation Oncology, MR Linac ART Division, Graduate School of Medicine, Chiba University, Chuo-ku, Chiba, Japan, ³Department of Radiology, Chiba University Hospital, Chuo-ku, Chiba, Japan

Purpose: Differences in the contours created during magnetic resonance imaging-guided online adaptive radiotherapy (MRgOART) affect dose distribution. This study evaluated the interobserver error in delineating the organs at risk (OARs) in patients with pancreatic cancer treated with MRgOART. Moreover, we explored the effectiveness of drugs that could suppress peristalsis in restraining intra-fractional motion by evaluating OAR visualization in multiple patients.

Methods: This study enrolled three patients who underwent MRgOART for pancreatic cancer. The study cohort was classified into three conditions based on the MRI sequence and butylscopolamine administration (Buscopan): 1, T2 imaging without butylscopolamine administration; 2, T2 imaging with butylscopolamine administration; and 3, multi-contrast imaging with butylscopolamine administration. Four blinded observers visualized the OARs (stomach, duodenum, small intestine, and large intestine) on MR images acquired during the initial and final MRgOART sessions. The contour was delineated on a slice area of ± 2 cm surrounding the planning target volume. The dice similarity coefficient (DSC) was used to evaluate the contour. Moreover, the OARs were visualized on both MR images acquired before and after the contour delineation process during MRgOART to evaluate whether peristalsis could be suppressed. The DSC was calculated for each OAR.

Results: Interobserver errors in the OARs (stomach, duodenum, small intestine, large intestine) for the three conditions were 0.636, 0.418, 0.676, and 0.806; 0.725, 0.635, 0.762, and 0.821; and 0.841, 0.677, 0.762, and 0.807, respectively. The DSC was higher in all conditions with butylscopolamine administration compared with those without it, except for the stomach in condition 2, as observed in the last session of MR image. The DSCs for OARs (stomach, duodenum, small intestine, large intestine) extracted before and after

contouring were 0.86, 0.78, 0.88, and 0.87; 0.97, 0.94, 0.90, and 0.94; and 0.94, 0.86, 0.89, and 0.91 for conditions 1, 2, and 3, respectively.

Conclusion: Butylscopolamine effectively reduced interobserver error and intrafractional motion during the MRgOART treatment.

KEYWORDS

MRgOART, pancreatic cancer, organs-at-risk, butylscopolamine, contouring, interobserver variability

1 Introduction

In patients with unresectable locally advanced pancreatic cancer, conventional radiation therapy confers a slight survival advantage compared with chemotherapy alone, necessitating the discovery of more effective local approaches (1-3). Dose escalation is essential to achieve local tumor control and improve overall survival. However, dose cannot be escalated due to restrictions on the tolerable dose of healthy organs surrounding the pancreas. Advances in irradiation techniques, such as intensity-modulated radiation therapy, facilitate the administration of high doses while minimizing the dose to the organs at risk (OAR). Treatment of unresectable pancreatic cancer using a general linear accelerator is performed in 15 or 25 fractions, while meeting the dose limit to the surrounding normal organs, using countermeasures against respiratory migration and image-guided technology (4, 5). Recently, magnetic resonance imaging-guided Online Adaptive Radiation Therapy (MRgOART), which fully uses MR imageguided and online adaptive technology for pancreatic cancer, has enabled more effective dose prescription (6-9).

Recommendations for precise delineation of tumors and OARs in abdominal regions with respiratory movements and intestinal peristalsis have been reported (10). Motion artifacts occur due to the movement of internal organs during MRI, reducing visibility. Mostafaei et al. investigated body movements induced by breathing and peristalsis on computed tomography (CT) and MRI scans acquired during free breathing and breath-holding. They concluded that evaluating both respiratory movement and peristalsis is essential (11). Breath-holding and abdominal compression have been reported as countermeasures for respiratory movement (7-9). The pre-treatment images can directly correct the current gastrointestinal position and movement in an online adaptive radiotherapy plan. Some drugs can also inhibit peristalsis (12). No study has investigated whether it is possible to accurately defininig the contours of normal organs on images affected by motion artifacts could be possible.

This study aimed to evaluate interobserver error while delineating OARs in patients with pancreatic cancer treated with MRgOART. Furthermore, we also aimed to demonstrate the utility of drugs that suppress peristalsis by evaluating OAR visualization in multiple patients.

2 Methods

2.1 Patient data and MRI

This study was approved by the Ethics Committee of Chiba University Hospital (HK202304-07). The study enrolled three patients who underwent MRgOART for pancreatic cancer using Elekta Unity MR-linac (Elekta, Stockholm, Sweden). The patient details are presented in Table 1. At our hospital, MRIs are performed using a T2 navigator echo sequence under abdominal compression to measure respiratory movement. Patients 2 and 3 (conditions 2 and 3) who could be treated with butylscopolamine bromide (Buscopan®Injection, Paris, France) were administered the drug to suppress intestinal peristalsis. Butylscopolamine was deemed contraindicated in Patient 1 (condition 1) owing to a history of valvular heart disease. Moreover, our hospital incorporates contour delineation on images captured in multiple sequences into the workflow using the treatment planning support device MIM Maestro (MIM Software, 7.1.5, Cleveland, OH, USA) (condition 3) (9, 13). The imaging sequences provided by the vendor were used for MRI acquisition, except for one sequence, T1-eTHRIVE. Table 2 presents the parameters of the imaging sequence. Figure 1 shows an example of a treatment image captured using the T2 3D Tra Navi sequence and provides an overview of our delineation study.

2.2 Evaluation of contouring

The observers were three radiation oncologists (RO1, RO2, and RO3) and one resident physician (T1); the other observers were blinded to the contours during contour delineation. RO1, RO2, RO3, and T1 had treatment experiences of 14, 15, 13, and 3 years, respectively. In this study, MR images from the initial and final MRgOART sessions were used to delineate the contours of OAR for

TABLE 1 Patient overview.

Patient No.	1	II	ш
Condition No.	1	2	3
Age (years)	78	59	51
Sex	F	М	М
Tumor location	Head of the pancreas	Uncinate process of the pancreas	Head of the pancreas
Prior chemotherapy	GEM+nabPTX	GEM+nabPTX→mFOLFIRINOX	GEM+nabPTX→mFOLFIRINOX
KPS at the start of ablative radiotherapy	90	90	100
Imaging sequence	T2 3D Tra Navi	T2 3D Tra Navi	T2 3D Tra Navi with optional imaging
Abdominal compression	+	+	+
Butylscopolamine (20 mg/ampule)	_	+	+

GEM, gemcitabine; nabPTX, nanoparticle albumin-bound paclitaxel; FOLFIRINOX, oxaliplatin, irinotecan, fluorouracil, and leucovorin; KPS, Karnofsky Performance Status.

each condition. Each observer created an outline of the stomach, duodenum, small intestine, and large intestine on this MR image. The range for delineating the contour was an area extending ± 2 cm in the craniocaudal direction from the slice coordinates of the planning target volume (PTV). The primary outcome measure was the agreement between observers for each contour. The dice similarity coefficient (DSC) was used to assess interobserver agreement for each contour in each patient (14). DSC has been used broadly in the field of segmentation as a measure of spatial overlap ranging between 0 and 1, where 0 indicates no overlap and 1 indicates exact overlap. The OARs were depicted using the MIM software and exported after anonymization. DSC values were calculated using an in-house program developed in Python and subsequently averaged.

2.3 Peristaltic motion

Two MR images obtained before and after contouring were used to evaluate intestinal peristalsis. In the MRgOART workflow, MR images (pre-treatment MR images) were acquired before the treatment planning. The contouring, optimization, and dose

TABLE 2 Overview of imaging sequences.

calculation were performed immediately using this image. Since this process was time-consuming, position verification MR images could be acquired immediately before irradiation to assess patient misalignment (15, 16). These two images were compared, and the process proceeded to irradiation if no positional shift was found. The contours to be evaluated were the duodenum, stomach, small intestine, and large intestine, as described above. One observer (RO1) compared the contours using the DSC.

2.4 Evaluation of contouring (distance and area of overlapping)

Figure 2 depicts a conceptual diagram of the distance and area of overlap between the PTV and OARs. We determined the presence or absence of overlap between the PTV and OAR in each slice containing the PTV (range, 0–n). Regarding overlapping region for each observer, the area of overlap was calculated and accumulated, representing the overlap volume. In cases wherein no overlap occurred, the shortest distance between the PTV and each OAR contour was calculated. The average value of the shortest distances for each observer was evaluated.

Name	T2 3D Tra Navi	b3D VaneXD	T1 3D VaneXD	eTHRIVE*
Scan technique	T2-TSE	B-FFE	T1-FFE	T1-FFE
Scan time	2:21	6:51	6:01	2:29
Voxel size	$0.79\times0.79\times1.2$	$0.78\times0.78\times1.5$	$0.78\times0.78\times1.5$	$0.78\times0.78\times2.4$
Field-of-view	360 × 455	500 × 500	500 × 500	360 × 438
TR/TE	2100/102	3.3/1.31	3.9/1.18	4.6/2.3
ETL	167	94	_	15
FA	90	40	15	10
NEX	2	1	1	5
Fat suppression	-	_	_	+

*These sequences are developed at our facility.

TR/TE, repetition time/echo time; ETL, echo train length; NEX, number of excitations; FA, flip angle.





FIGURE 2

Evaluation of the positional relationship between the PTV and OARs. (A, B) Calculation of the overlap area for RO1 and T1 when the PTV and OARs overlap; (C, D) Determination of the shortest distance *d* for RO1 and T1 when there is no overlap between the PTV and OAR. Evaluation is conducted on slices containing the PTV. PTV, planning target volume; OAR, organ-at-risk.

MR images of two sessions were analyzed. These indicators were calculated using an in-house program developed in Python. In all OARs, the values of overlap volume and averaged shortest distance were calculated for each combination of condition and observers. The values for all observers were averaged. We calculated the standard deviation (SD) and coefficient of variation (CV) as a measure of interobserver error. Larger CVs indicated greater interobserver differences among observers in these indicators.

3 Results

3.1 Treatment time

Treatment was completed within 100 min for the treatment fractions included in our analysis. Figure 3 shows the duration of

treatment for each process, including administration time. Subcutaneous, intravenous, and mixed injections of butylscopolamine bromide are denoted by plus, cross, and triangular marks, respectively.

3.2 DSC comparison for each contour

Figure 1 shows T2 Navi images of condition1 without butylscopolamine bromide administration and of conditions 2 and 3 with butylscopolamine bromide administration. The visibility of the image obtained without butylscopolamine bromide administration was poor (Figure 1 upper row). Figure 4 shows the DSC results for each patient. DSC values were higher for all conditions involving butylscopolamine bromide administration compared to condition 1, where butylscopolamine bromide was not administered.





3.3 Shortest distance and area of overlap between the PTV and OARs

Table 3 summarizes the results of the shortest distance from the PTV to the OARs and CV for each condition, while Table 4 lists the results of the overlap volume between the PTV and OARs and CV for each condition. The overlap volumes of the stomach and large intestine could only be calculated under one condition. Therefore, the volume of these structures was not evaluated (Table 4). Although SD is a measure of dispersion of population, comparing dispersion of multiple ones, it may not be an effective in analysis. In a population wherein the average value is larger, SD is likely to be larger. In such cases, the comparison takes into account the population size by dividing SD by the average value to calculate CV. In some conditions

and fractions, administration resulted in lower CV values. However, no trend was found depending on whether butylscopolamine bromide was administered or not. We consider that this is because the anatomical position of OARs differs among patients and positions of OARs change between inter-fractions.

3.4 Peristaltic motion

Figure 5 shows the pre-treatment, and position verification MR images for conditions 1, 2, and 3. The outline created by observer RO1 in the pre-treatment image is depicted in both MR images. It is a solid line on the pre-treatment MR image and a dotted line on the position verification MR image. Furthermore, yellow lines indicate the

TABLE 3 Average values of the shortest distance between the planning target volume and organ-at-risk in each slice.

Average distance [mm]	Condition	Average		Coefficient of variation (\downarrow)	
Average distance [mm]		Initial fraction	Final fraction	Initial fraction	Final fraction
	1	19.53 ± 6.67	18.56 ± 8.19	0.34	0.44
Average distance [mm] Stomach Duodenum Small intestine	2	N/A	N/A	N/A	N/A
	3	4.55 ± 2.96	5.70 ± 1.91	0.65	0.34
Duodenum	1	12.41 ± 3.02	2.52 ± 1.03	0.24	0.41
	2	13.44 ± 0.98	14.59 ± 5.30	0.07	0.36
	3	N/A	N/A	N/A	N/A
	1	9.03 ± 2.77	11.10 ± 5.36	0.31	0.48
Small intestine	2	26.20 ± 6.65	28.90 ± 3.90	0.25	0.14
	3	12.01 ± 4.00	24.97 ± 4.08	0.33	0.16
Large intestine	1	34.50 ± 7.74	23.24 ± 0.70	0.22	0.03
	2	62.33 ± 3.52	30.53 ± 3.55	0.06	0.12
	3	26.24 ± 1.89	33.48 ± 2.87	0.08	0.08

"N/A" indicates that the OAR does not exist on all evaluated slices and the distance is not calculated.

Area [cc]	Condition	Average		Coefficient of variation (\downarrow)		
	Condition	Initial fraction	Final fraction	Initial fraction	Final fraction	
Duodenum	1	1.04 ± 0.91	0.77 ± 0.43	0.87	0.56	
	2	1.05 ± 0.53	0.66 ± 0.48	0.50	0.72	
	3	16.85 ± 2.94	11.34 ± 0.55	0.17	0.05	
Small intestine 2 3	1	6.12 ± 4.34	0.02 ± 0.03	0.71	1.34	
	2	1.66 ± 2.96	N/A	1.78	N/A	
	3	1.89 ± 3.05	0.07 ± 0.07	1.62	1.04	

TABLE 4 Area of overlap between the planning target volume and organ-at-risk.

"N/A" indicates that the PTV and OAR do not overlap and the volume cannot be calculated.

duodenum, pink lines indicate the small intestine, and light blue lines indicate the large intestine. In the conditions with butylscopolamine, although the movement of gas and water within the intestinal tract was observed, there were no major positional changes. Conversely, positional fluctuations were observed in condition 1. Table 5 shows the results of the DSC. For all OARs, conditions 2 and 3 had higher DSC values than condition 1. Therefore, it can be inferred that butylscopolamine helps suppress peristalsis during the OART workflow.

4 Discussion

In our study, we evaluated three patients with pancreatic cancer who underwent treatment with MRgOART. Normal organ contours were visualized for each observer on MR images acquired during both the initial and final MRgOART sessions. These patients were categorized into three conditions based on the MRI sequence and butylscopolamine administration. We examined the contour delineation accuracy and investigated the conditions suitable for contour delineation. The DSC was used to verify the accuracy of contour delineation among observers and to evaluate peristaltic motion. Evaluating DSC using the same threshold for multiple organs due to its sensitivity to contour delineation volume is challenging. Therefore, we compared the results for conditions 1, 2, and 3 within the same OAR. The average DSC value was higher in conditions wherein butylscopolamine was administered compared with those wherein it was not used. This suggests that butylscopolamine administration could contribute to the improved accuracy of OARs contour delineation. Thus, using butylscopolamine may be effective in reducing interobserver error.

Regarding the MRgOART workflow, contours are drawn using MRI. There is a concern that artifacts due to respiratory movement or peristalsis may occur during imaging. These movements may reduce the image quality and make identifying lesion challenging. Heerkens et al. evaluated respiratory migration in patients with pancreatic cancer. Respiratory migration of tumor was verified on sagittal and coronal MRI using in-house software. Their results indicated that the body moves by an average of 15 mm in the craniocaudal direction and that the deep expiration (end-expiration position) phase is the most stable (10). In this study, we adopted the T2 navigator echo imaging method, which acquires images in time with deep exhalation, which helps mitigate the effects of respiratory movement. Additionally, abdominal compression suppresses the





Comparison of the pre- and verification MR images for conditions 1, 2, and 3. The contour created in the pre-image is depicted on both MR images. MR, magnetic resonance.

		Condition No		
		1	2	3
DSC	Stomach	0.86	0.97	0.94
	Duodenum	0.78	0.94	0.86

0.88

0.87

0.90

0.94

0.89

0.91

Small intestine

Large intestine

TABLE 5 DSCs for organ-at-risk delineations extracted from pretreatment and verification magnetic resonance imaging.

DSC, dice similarity coefficient.

amount of movement. Mostafaei et al. (11) concluded that peristalsis must also be assessed in addition to respiratory movement. Therefore, we used the DSC in this study to determine whether the contour changed between the pretreatment and verification MR images to evaluate peristalsis. We found that the DSC was high when butylscopolamine was used.

Wagner et al. reported that butylscopolamine administration before MRI improves the diagnostic accuracy of lesions in the pancreatic head and body during interobserver evaluation (17). In their study, patients received an intramuscular injection of 40 mg of butylscopolamine immediately before undergoing MR imaging. It was reported that repeat imaging after 29 min (mean) did not result in a significant deterioration in image quality. MR imaging of the abdominal region following butylscopolamine administration are of significantly superior quality (18, 19). Additionally, Martí-Bonmatí et al. demonstrated the effectiveness of suppressing peristalsis using medication for MR imaging of pancreatic cancer (12). Our results also could support previous findings; hence we conclude that butylscopolamine contributes to improved contouring accuracy and reduces intra-fractional motion.

The limitations of this study are that it was conducted within a single institution; the number of conditions and observers was small. Due to the small number of cases, discussing the duration of effectiveness of butylscopolamine might be impossible. However, the evaluation of DSC between the pre- and verification-MR images confirmed the suppression of peristaltic movement in the presence of drugs. Our assessment was limited to two specific periods during the MRgOART process -before treatment planning and before irradiation- and we did not extensively evaluate intra-fractional motion. Therefore, we suggest that the following two studies will be needed: 1) an examination of interobserver error with a large number of cases and 2) an evaluation of peristaltic motion during treatment. The number of cases and observers will be increased to assure our result of interobserver error. An analysis of cine 2D MR images (5 frames/second) acquired during irradiation will be required to evaluate the effect of peristaltic suppression.

5 Conclusion

We used DSC to evaluate the interobserver errors in OAR delineation in patients with pancreatic cancer treated with MRgOART at our hospital. Using butylscopolamine resulted in high DSC values in all organs, suggesting that it reduces

interobserver error. Furthermore, it helped reduce intra-fractional motion, in addition to improving the accuracy of contour delineation.

Data availability statement

The raw data supporting the conclusions of this article will be made available by the authors, without undue reservation.

Ethics statement

The studies involving humans were approved by Chiba University Clinical Research Center, Chiba University Hospital. The studies were conducted in accordance with the local legislation and institutional requirements. Written informed consent for participation was not required from the participants or the participants' legal guardians/next of kin in accordance with the national legislation and institutional requirements.

Author contributions

MK: Writing – original draft, Conceptualization, Funding acquisition, Project administration, Visualization. MT: Conceptualization, Data curation, Formal analysis, Project administration, Software, Visualization, Writing – original draft. KA: Formal analysis, Software, Writing – review & editing. YI: Resources, Software, Writing – review & editing. AKa: Resources, Writing – review & editing. MS: Resources, Writing – review & editing. AKo: Resources, Writing – review & editing. RH: Writing – review & editing. HY: Writing – review & editing. MW: Writing – review & editing. TU: Writing – review & editing.

Funding

The author(s) declare financial support was received for the research, authorship, and/or publication of this article. This work was supported by JSPS KAKENHI (grant number 21K15822).

Acknowledgments

We borrowed a radiation treatment planning system for this research from Elekta K.K. We thank Mr. Yoshio Iwai of the same company. We thank Editage (www.editage.com) for the English language editing.

Conflict of interest

MT and KA received endowed chairs funded by Elekta K.K.

The remaining authors declare that the research was conducted in the absence of any commercial or financial relationships that could be constructed as a potential conflict of interest.

Publisher's note

All claims expressed in this article are solely those of the authors and do not necessarily represent those of their affiliated

References

1. Crane CH. Hypofractionated ablative radiotherapy for locally advanced pancreatic cancer. J Radiat Res. (2016) 57 Suppl 1:i53-7. doi: 10.1093/jrr/rrw016

2. Hammel P, Huguet F, van Laethem JL, Goldstein D, Glimelius B, Artru P, et al. Effect of chemoradiotherapy vs chemotherapy on survival in patients with locally advanced pancreatic cancer controlled after 4 months of gemcitabine with or without erlotinib: the LAP07 Randomized Clinical Trial. *JAMA*. (2016) 315:1844–53. doi: 10.1001/jama.2016.4324

3. Loehrer PJ, Feng Y, Cardenes H, Wagner L, Brell JM, Cella D, et al. Gemcitabine alone versus gemcitabine plus radiotherapy in patients with locally advanced pancreatic cancer: an Eastern Cooperative Oncology Group trial. *J Clin Oncol.* (2011) 29:4105–12. doi: 10.1200/JCO.2011.34.8904

4. Reyngold M, Parikh P, Crane CH. Ablative radiation therapy for locally advanced pancreatic cancer: techniques and results. *Radiat Oncol.* (2019) 14:95. doi: 10.1186/s13014-019-1309-x

5. Krishnan S, Chadha AS, Suh Y, Chen HC, Rao A, Das P, et al. Focal radiation therapy dose escalation improves overall survival in locally advanced pancreatic cancer patients receiving induction chemotherapy and consolidative chemoradiation. *Int J Radiat Oncol Biol Phys.* (2016) 94:755–65. doi: 10.1016/j.ijrobp.2015.12.003

6. Bohoudi O, Bruynzeel AME, Senan S, Cuijpers JP, Slotman BJ, Lagerwaard FJ, et al. Fast and robust online adaptive planning in stereotactic MR-guided adaptive radiation therapy (SMART) for pancreatic cancer. *Radiother Oncol.* (2017) 125:439–44. doi: 10.1016/j.radonc.2017.07.028

7. Chuong MD, Bryant J, Mittauer KE, Hall M, Kotecha R, Alvarez D, et al. Ablative 5-fraction stereotactic magnetic resonance-guided radiation therapy with on-table adaptive replanning and elective nodal irradiation for inoperable pancreas cancer. *Pract Radiat Oncol.* (2021) 11:134–47. doi: 10.1016/j.prro.2020.09.005

8. Hassanzadeh C, Rudra S, Bommireddy A, Hawkins WG, Wang-Gillam A, Fields RC, et al. Ablative five-fraction stereotactic body radiation therapy for inoperable pancreatic cancer using online MR-guided adaptation. *Adv Radiat Oncol.* (2021) 6:100506. doi: 10.1016/j.adro.2020.06.010

9. Tyagi N, Liang J, Burleson S, Subashi E, Godoy Scripes P, Tringale KR, et al. Feasibility of ablative stereotactic body radiation therapy of pancreas cancer patients on a 1.5 Tesla magnetic resonance-linac system using abdominal compression. *Phys Imaging Radiat Oncol.* (2021) 19:53–9. doi: 10.1016/j.phro.2021.07.006 organizations, or those of the publisher, the editors and the reviewers. Any product that may be evaluated in this article, or claim that may be made by its manufacturer, is not guaranteed or endorsed by the publisher.

10. Heerkens HD, Hall WA, Li XA, Knechtges P, Dalah E, Paulson ES, et al. Recommendations for MRI-based contouring of gross tumor volume and organs at risk for radiation therapy of pancreatic cancer. *Pract Radiat Oncol.* (2017) 7:126–36. doi: 10.1016/j.prro.2016.10.006

11. Mostafaei F, Tai A, Omari E, Song Y, Christian J, Paulson E, et al. Variations of MRI-assessed peristaltic motions during radiation therapy. *PloS One.* (2018) 13: e0205917. doi: 10.1371/journal.pone.0205917

12. Martí-Bonmatí L, Graells M, Ronchera-Oms CL. Reduction of peristaltic artifacts on magnetic resonance imaging of the abdomen: a comparative evaluation of three drugs. *Abdom Imaging*. (1996) 21:309–13. doi: 10.1007/s002619900070

13. Tringale KR, Tyagi N, Reyngold M, Romesser PB, Wu A, O'Reilly EM, et al. Stereotactic ablative radiation for pancreatic cancer on a 1.5 Telsa magnetic resonance-linac system. *Phys Imaging Radiat Oncol.* (2022) 24:88–94. doi: 10.1016/j.phro.2022.10.003

14. Dice LR. Measures of the amount of ecologic association between species. *Ecology*. (1945) 26:297–302. doi: 10.2307/1932409

15. Uno T, Tsuneda M, Abe K, Fujita Y, Harada R, Saito M, et al. A new workflow of the on-line 1.5-T MR-guided adaptive radiation therapy. *Jpn J Radiol.* (2023) 41:1316–22. doi: 10.1007/s11604-023-01457-4

16. Werensteijn-Honingh AM, Kroon PS, Winkel D, Aalbers EM, van Asselen B, Bol GH, et al. Feasibility of stereotactic radiotherapy using a 1.5 T MR-linac: Multi-fraction treatment of pelvic lymph node oligometastases. *Radiother Oncol.* (2019) 134:50–4. doi: 10.1016/j.radonc.2019.01.024

17. Wagner M, Klessen C, Rief M, Elgeti T, Taupitz M, Hamm B, et al. Highresolution T2-weighted abdominal magnetic resonance imaging using respiratory triggering: impact of butylscopolamine on image quality. *Acta Radiol.* (2008) 49:376– 82. doi: 10.1080/02841850801894806

 Dosdá R, Martí-Bonmatí L, Ronchera-Oms CL, Mollá E, Arana E. Effect of subcutaneous butylscopolamine administration in the reduction of peristaltic artifacts in 1.5-T MR fast abdominal examinations. *Eur Radiol.* (2003) 13:294–8. doi: 10.1007/ s00330-002-1500-5

19. Tanaka O, Komeda H, Tamaki M, Seike K, Fujimoto S, Yama E, et al. Efficacy of butylscopolamine in obtaining clear MR image for intensity-modulated radiotherapy for prostate cancer. *Tech Innov Patient Support Radiat Oncol.* (2017) 3–4:19–22. doi: 10.1016/j.tipsro.2017.08.001