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Predicting of axillary lymph node metastasis in invasive breast cancer using multiparametric MRI dataset based on CNN model

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Purpose: To develop a multiparametric MRI model for predicting axillary lymph node metastasis in invasive breast cancer.

Methods: Clinical data and T2WI, DWI, and DCE-MRI images of 252 patients with invasive breast cancer were retrospectively analyzed and divided into the axillary lymph node metastasis (ALNM) group and non-ALNM group using biopsy results as a reference standard. The regions of interest (ROI) in T2WI, DWI, and DCE-MRI images were segmented using MATLAB software, and the ROI was unified into 224 \times 224 sizes, followed by image normalization as input to T2WI, DWI, and DCE-MRI models, all of which were based on ResNet 50 networks. The idea of a weighted voting method in ensemble learning was employed, and then T2WI, DWI, and DCE-MRI models were used as the base models to construct a multiparametric MRI model. The entire dataset was randomly divided into training sets and testing sets (the training set 202 cases, including 78 ALNM, 124 non-ALNM; the testing set 50 cases, including 20 ALNM, 30 non-ALNM). Accuracy, sensitivity, specificity, positive predictive value, and negative predictive value of models were calculated. The receiver operating characteristic (ROC) curve and area under the curve (AUC) were used to evaluate the diagnostic performance of each model for axillary lymph node metastasis, and the DeLong test was performed, P< 0.05 statistically significant.

Results: For the assessment of axillary lymph node status in invasive breast cancer on the test set, multiparametric MRI models yielded an AUC of 0.913 (95% CI, 0.799-0.974); T2WI-based model yielded an AUC of 0.908 (95% CI, 0.792-0.971); DWI-based model achieved an AUC of 0.702 (95% CI, 0.556-0.823); and the AUC of the DCE-MRI-based model was 0.572 (95% CI, 0.424-0.711). The improvement in the diagnostic performance of the multiparametric MRI model compared with the DWI and DCE-MRI-based models were

significant (P< 0.01 for both). However, the increase was not meaningful compared with the T2WI-based model (P = 0.917).

Conclusion: Multiparametric MRI image analysis based on an ensemble CNN model with deep learning is of practical application and extension for preoperative prediction of axillary lymph node metastasis in invasive breast cancer.

KEYWORDS

breast cancer, magnetic resonance imaging, axillary lymph node, metastasis, convolutional neural network

Introduction

Global cancer statistics for 2020 show that breast cancer has surpassed lung cancer as the most common cancer in women and the leading cause of cancer deaths in women (1). Lymphatic metastasis is the most common route for breast cancer, and the status of axillary lymph nodes becomes an important indicator to determine the clinical stage, treatment method, and prognosis (2, 3). Axillary lymph node dissection (ALND) and sentinel lymph node biopsy (SLNB) are the clinical standards for the evaluation of axillary lymph node metastasis (ALNM). Since postoperative complications after ALND are challenging to recover from, such as narrow shoulder and upper arm movement, lymphedema, Etc., ALND is now gradually being replaced by SLNB (4-7). Although SLNB has become the primary means of evaluating the status of axillary lymph nodes, the negative rate of SLNB reaches 70% (8), and the incidence of postoperative complications of SLNB reaches 41% (7), which still has a significant impact on the prognosis of breast cancer patients. Therefore, preoperative non-invasive and accurate axillary lymph node status evaluation is of clinical importance.

Currently, the main non-invasive methods for preoperative assessment of axillary lymph node status are imaging examinations, including mammography, ultrasound, magnetic resonance imaging (MRI), and PET/CT (9–13). However, mammography cannot show the entire axilla, and only the anterior and inferior portions of the axilla can be observed. Ultrasound is not only limited to superficial lymph nodes, but is also determined by the diagnostic experience of the doctor. PET/CT is expensive and may expose the patient to ionizing radiation. Nevertheless, MRI has excellent tissue resolution and is the best imaging examination to evaluate breast cancer and axillary lymph nodes (14, 15). Radiologists usually observe axillary lymph node morphology, size, fat hilum, and cortical

thickness in MR images to diagnose the occurrence of metastasis (16, 17). However, when axillary lymph nodes are small and have poor contrast with surrounding tissues, radiologists have difficulty interpreting them. As a result, the sensitivity of conventional breast MRI for detecting axillary lymph node metastasis is still moderate (18). Therefore, it cannot be a definitive evaluation method for axillary lymph node metastasis. In addition, previous studies have shown an intrinsic connection between preoperative MRI images of the breast cancer tumor and axillary lymph node metastasis, including anatomical and functional sequences (19–22). However, this inherent connection is difficult for radiologists to observe.

In the past few years, deep learning methods have been increasingly used for medical image processing and are evolving into a new field of medical imaging. Deep learning (23) differs from radiomics, an end-to-end learning model that automatically learns and extracts the intrinsic features of medical images and then completes the corresponding tasks, avoiding the human factor and omitting the traditional complex operational steps. The deep learning using the MRI dataset applied to axillary lymph node metastasis in breast cancer mainly focuses on axillary lymph nodes and breast cancer tumors. Convolutional neural networks (CNN) are commonly used as a conventional deep learning model in breast image analysis. Ha, et al. (24) and Ren et al. (25) used MR images of axillary lymph nodes to build CNN models for their studies, and the studies by Luo et al. (26) and Wang et al. (27)used anatomical and functional MR images of breast cancer tumors. All of their deep-learning models achieved good prediction results.

This study aims to develop an innovative prediction model that can differentiate between ALNM and non-ALNM in breast cancer using multiparametric MRI datasets based on the CNN model.

Materials and methods

Population

We retrospectively studied 465 breast cancer patients from January 2016 to June 2022. The study was approved by the ethics committee and institutional review and waived the requirement for informed consent. Inclusion criteria for this study: (1) invasive breast cancer confirmed by surgical pathology and axillary lymph node status also confirmed by postoperative pathology; (2) pathological stage ≥ pN1a was selected for the ALNM group and pN0 for the non-ALNM group; (3) all preoperative breast MRI scan and enhancement examinations were done. Exclusion criteria: (1) pathological findings showing the presence of isolated tumor cells in axillary lymph nodes or the occurrence of micrometastases; (2) receiving tissue aspiration biopsy or neoadjuvant chemotherapy before MRI examination; (3) the presence of artifacts in MRI images. The specific inclusion and exclusion process is illustrated in Figure 1. 252 patients with invasive breast cancer, including 98 with ALNM and 154 with non-ALNM, were finally included in our study, and the clinical characteristics of these people are shown in Table 1.

MR imaging parameters

Breast MRI was performed using a 3.0T MRI scanner (Magnetom Skyra, Siemens, Germany) and a 1.5T MRI scanner (Signa Explorer, GE, USA) with dedicated breast coils. Both scanners acquired the following sequences: axial T2-weighted imaging (T2WI), axial diffusion-weighted imaging

(DWI), and axial dynamic contrast-enhanced magnetic resonance imaging (DCE-MRI) images, and DCE-MRI sequences were imaged by injecting 15 ml of gadolinium contrast medium (Magnevist, Bayer Schering, Germany) at a rate of 3.0 ml/s, and a total of 7 phases were performed. Only the phase with the most significant enhancement, determined by the time-intensity curve (TIC), was used in the DCE-MRI images. The specific parameters are shown in Table 2.

Image processing and base model building

The clipping of the lesion region of interest (ROI) included the breast tumor and peritumoral area in this study, not the axillary lymph nodes. Two doctors with three years of breast imaging experience determined the tumor's location, size, and borders. When a dispute arose, a senior doctor with fifteen years of experience decided it independently. We later used Matlab-R2018b (Math works, Massachusetts, USA) software to crop out the ROI from T2WI, DWI, and DCE-MRI raw images of 252 breast cancer, and the ROI segmentation example is in Figure 2. First, boundary boxes were formed around each axial 2D ROI for layer-by-layer ROI segmentation. Then, all segmented 2D ROI images were unified into 224×224. Finally, image normalization was performed by equation (1) so that the pixel values fall in the [0,1] interval.

$$Norm = \frac{xi - min(x)}{max(x) - min(x)} \tag{1}$$

Where xi represents the image pixel value, max(x), min(x) represent the maximum and minimum values of the image pixels, respectively. All datasets were randomly divided into

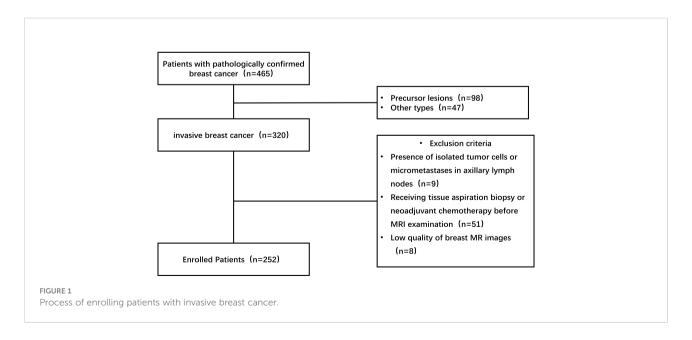


TABLE 1 Population characteristics.

	Characteristics number	Total n=252	ALNM n=98	Non-ALNM n=154	P
All patients	Age (mean ± SD), years old	51.3 ± 11.24	51.0 ± 11.05	51.6 ± 11.40	0.698
	Tumor size (mean ± SD), cm	2.1 ± 0.97	2.4 ± 1.15	1.9 ± 0.78	< 0.01
	Tumor margin				0.079
	Regular	102 (40.5)	33 (33.7)	69 (44.8))	
	Irregular	150 (59.5)	65 (66.3)	85 (55.2)	
	TIC curve type				0.201
	II	168 (66.7)	70 (71.4)	98 (63.6)	
	III	84 (33.3)	28 (28.6)	56 (36.4)	
	Number	n=50	n=20	n=30	
Testing dataset	Age (mean ± SD), years old	50.7 ± 10.74	49.1 ± 11.77	51.7 ± 10.06	0.394
	Tumor size (mean ± SD), cm	2.0 ± 0.80	2.3 ± 0.92	1.9 ± 0.67	0.086
	Tumor margin			0.387	
	Regular	22 (44.0)	7 (35.0)	15 (50.0)	
	Irregular	28 (56.0)	13 (65.0)	15 (50.0)	
	TIC curve type				0.243
	II	29 (58.0)	14 (70.0)	15 (50.0)	
	III	21 (42.0)	6 (30.0)	15 (50.0)	

ALNM, axillary lymph node metastasis; SD, standard deviation; TIC, time-intensity curve.

TABLE 2 Magnetic Resonance Imaging Scanner Parameters.

MRI parameters	1.5T			3.0T		
	T2WI	DWI	DCE-MRI	T2WI	DWI	DCE-MRI
TR (ms)	7210	5030	5.6	4300	6650	3.6
TE (ms)	102	56	1.7	75	65	1.8
Flip angle	160°	180°	15°	120°	180°	10°
Slice gap (mm)	1	1	0.5	0.8	1.1	0.5
Slice thickness(mm)	4	5	1.5	4	4	2
FOV (mm²)	320×320	320×320	320×320	351×351	340×340	340×340
Matrix	288×224	110×170	114×224	576×576	224×224	512×512
b value (s/mm²)	_	50,800	_	_	50,1000	_

TR, repetition time; TE, echo time; FOV, the field of view; T2WI, T2-weighted imaging; DWI, diffusion weighting imaging; DCE-MRI, dynamic contrast-enhanced magnetic resonance imaging.

training and test sets, with 202 cases in the training set, including 78 cases of ALNM and 124 cases of non-ALNM; 50 cases in the test set, including 20 cases of ALNM and 30 cases of non-ALNM.

For the outstanding image feature extraction ability and classification accuracy of residual network (ResNet), the base model in this study is constructed based on ResNet50. The ResNet50 architecture is shown in Figure 3. In this study, T2WI, DWI, and DCE-MRI of breast cancer tumors were used as input, and the feature classifier Softmax score threshold 0.5 was used for classification. Three base models of T2WI, DWI, and DCE-MRI were constructed to distinguish between ALNM and non-

ALNM. ResNet50 models were trained and tested on a Windows image workstation using Python, the open-source deep learning library torch, and math architecture with an NVIDIA GeForce GTX 2080ti GPU graphics processor. In our study, we used the training set data for training and fine-tuning the parameters of ResNet50, initially we set the learning rate interval to 0.001-0.000001 and the batch size to 16, by gradually adjusting the batch size (16-32-64) and learning rate to make ResNet50 more suitable for our research task. Finally, during the training process, we determined the learning rate be 0.00005, the batch size to be 64, and the number of training epochs was set to 300.

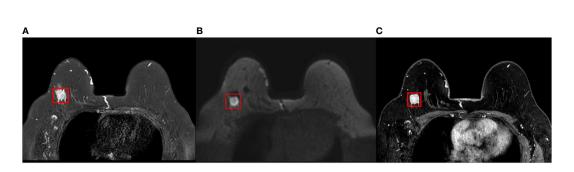
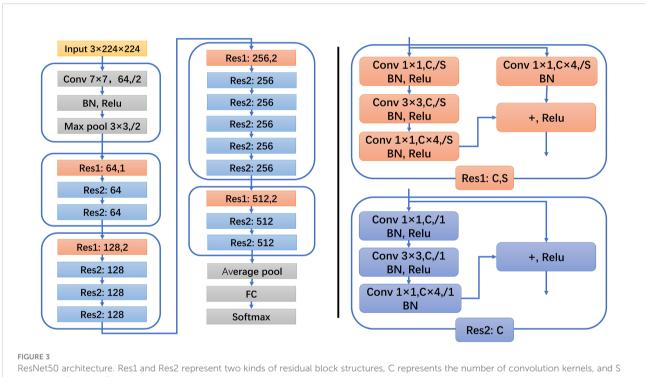


FIGURE 2
Cropping of ROI in raw MRI images of invasive breast cancer. (A) T2WI of the breast; (B) DWI of the breast; (C) Period with the most significant enhancement in DCE-MRI of the breast. ROI, region of interest; T2WI, T2-weighted imaging; DWI, diffusion weighting imaging; DCE-MRI, dynamic contrast-enhanced magnetic resonance imaging.



ResNet50 architecture. Res1 and Res2 represent two kinds of residual block structures, C represents the number of convolution kernels, and represents the step distance.

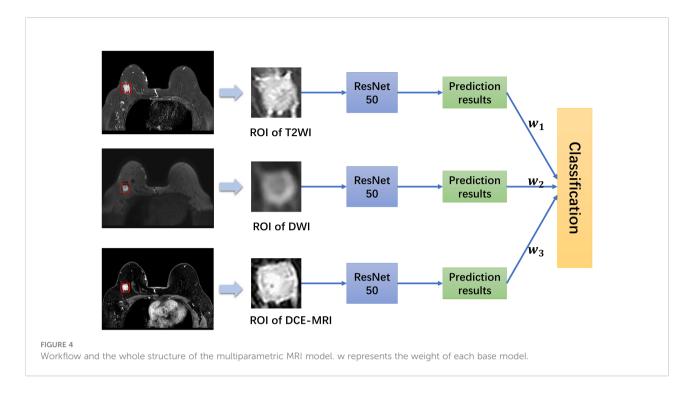
Multiparametric MRI combined with an ensemble learning model

Ensemble learning is a machine learning model that accomplishes the learning task by constructing and combining multiple base models so that multiple weak classification models can be turned into a single robust model (28). In this study, the idea of a weighted voting method in ensemble learning was adopted, and three base models, T2WI, DWI, and DCE-MRI, were applied as part of the novel prediction model we studied. The workflow of the integrated model is shown in Figure 4.

In this work, the trained three base models of T2WI, DWI, and DCE-MRI were tested, the weight value of each base model was calculated according to equation (2), and then a comprehensive decision was made by equation (3). Finally, half of the sum of the weights of the three base models were used as the threshold to make the final classification.

$$w_i = \frac{\sum_{i=1}^3 ACC_i}{3} \tag{2}$$

Where ACC_i represents the accuracy of each base model on the test set, and w_i refers to the classification weight of each base



model.

$$H(x) = \sum_{i=1}^{3} w_i h_i(x)$$
 (3)

Where $h_i(x)$ represents the probability value of the output of each base model for the same case in the test set, and H(x) refers to the final probability value of the output of the multiparameter combined integrated learning model. The multiparametric MRI model combined the information from the three base models of T2WI, DWI, and DCE-MRI to predict the status of axillary lymph nodes, which was more consistent with the clinical diagnostic environment.

Statistical analysis

SPSS 22.0 and MedCalc 20.0 were used for statistical analysis, the Kolmogorov–Smirnov test was used for normality, and quantitative data conforming to a normal distribution were expressed using the mean \pm standard deviation. Independent samples t-test was used for continuous data between ALNM and Non-ALNM groups, and χ^2 test or Fisher's exact test was used for categorical data. P< 0.05 was statistically significant. Model assessment indexes were used to evaluate the diagnostic performance of the base models and multiparametric model for axillary lymph node metastasis, including accuracy, sensitivity, specificity, positive predictive value, negative predictive value, receiver operating characteristic (ROC) curve, and area under the curve (AUC).

The DeLong test evaluated the ROC curves between different models, and P< 0.05 was considered statistically significant.

Results

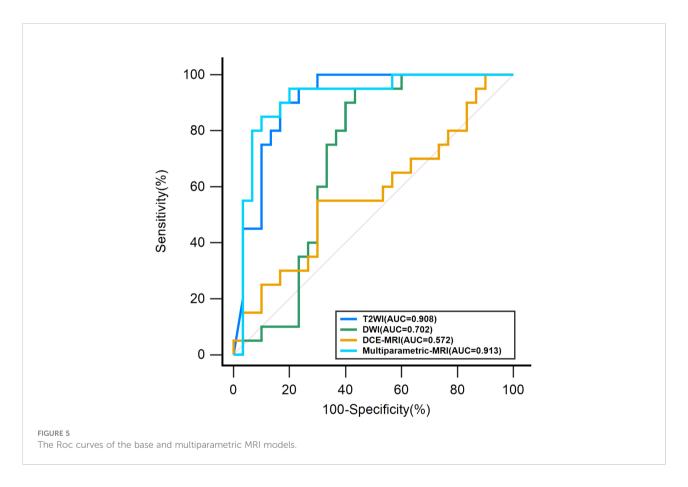
The mean age of all patients was 51.3 ± 11.24 years old, the mean age of the ALNM group was 51.0 ± 11.05 years old, and the mean age of the non-ALNM group was 51.6 ± 11.40 years old. There was no significant difference in age, tumor margin, and TIC curve type between the two groups of ALNM and non-ALNM, except for tumor size. This statistic is consistent with previous studies (29, 30) but not affecting our deep-learning experiment. In the testing set, the mean age of the ALNM group was 49.1 ± 11.77 years, and the mean tumor size was 2.3 ± 0.92 cm, the mean age of the non-ALNM group was 51.7 ± 10.06 years, and the mean tumor size was 1.9 ± 0.67 cm. There were no significant differences between the ALNM and non-ALNM groups regarding age, tumor size, tumor margin, or the type of TIC curve.

The model indicators are presented in Table 3. The Roc curves of the base and multiparametric MRI models are shown in Figure 5. The AUC of the T2WI-based model was 0.908 (95% CI, 0.792-0.971), with an accuracy of 0.840, a sensitivity of 0.750, a specificity of 0.900, a PPV of 0.833, and an NPV of 0.844. The AUC of the DWI-based model was 0.702 (95% CI, 0.556-0.823), with an accuracy of 0.640, a sensitivity of 0.550, a specificity of 0.700, a PPV of 0.550, and an NPV of 0.700. The AUC of the DCE-MRI-based model was 0.572 (95% CI, 0.424-0.711), with an accuracy of 0.540, a sensitivity of 0.550, a specificity of 0.533,

TABLE 3 Performance characteristics of the base and multiparametric MRI models.

Model	ACC	SEN	SPE	PPV	NPV	AUC (95%CI)
T2WI	0.840	0.750	0.900	0.833	0.844	0.908 (0.792-0.971)
DWI	0.640	0.550	0.700	0.550	0.700	0.702 (0.556-0.823)
DCE-MRI	0.540	0.550	0.533	0.440	0.640	0.572 (0.424-0.711)
Multiparametric MRI	0.880	0.850	0.900	0.850	0.900	0.913 (0.799-0.974)

T2WI, T2-weighted imaging; DWI, diffusion weighting imaging; DCE-MRI, dynamic contrast-enhanced magnetic resonance imaging; ACC, accuracy; SEN, sensitivity; SPE, specificity; PPV, positive predictive value; NPV, negative predictive value; AUC, area under the receiver operating characteristic curve; CI, confidence interval.



a PPV of 0.440, and an NPV of 0.640. The AUC of the multiparametric MRI model was 0.913 (95% CI, 0.799-0.974), with an accuracy of 0.880, a sensitivity of 0.850, a specificity of 0.900, a PPV of 0.850, and an NPV of 0.900. Comparing the three base models, the T2WI-based model best predicted axillary lymph node metastasis with an AUC of 0.908 (95% CI, 0.792-0.971). As a combination, the multiparametric MRI model was the best model for predicting axillary lymph node metastasis, and its AUC was 0.913 (95% CI, 0.799-0.974). The improvement compared with the AUC of the DWI base model and the DCE-MRI base model was significant (P< 0.01 for both). However, the

increase was insignificant compared with the T2WI-based model (P=0.917).

Discussion

This study developed a multiparametric MRI model incorporating ensemble learning to explore the performance of predicting axillary lymph node metastasis in invasive breast cancer before operation. To fully utilize the information from breast MRI, T2WI, DWI, and DCE-MRI were independent

inputs to CNN model, and the predictions of the three base models were weighted and fused by ensemble learning based on weighted voting to achieve the final classification of axillary lymph nodes.

Deep learning is a method of feature learning in machine learning. It can automatically learn deep abstract features in the input data by simulating the mechanism of the human brain neural network processing information, reducing the dependence of human factors on crucial features and achieving an end-to-end learning effect, thus improving the extension ability of the model. Deep learning has been widely used in breast imaging, including segmentation (31, 32), differentiation of benign and malignant tumors (33, 34), and preoperative prediction related to breast cancer (35, 36).

There are only five studies on the preoperative evaluation of axillary lymph node status in breast cancer. Ha, et al. (24)and Ren et al. (25) studied only T1WI images of axillary lymph nodes using CNN models, and the accuracy of the CNN models in diagnosing axillary lymph node metastasis reached 0.843 and 0.848, respectively. Ren et al. (37) further analyzed T1WI, T2WI, and DCE-MRI of axillary lymph nodes, and the accuracy and AUC values of the three fused CNN models for assessing the status of axillary lymph nodes reached 0.885 and 0.882, respectively. Wang et al. (27)also investigated T1WI, T2WI, and DWI images, and their traditional CNN+SVM model was used for the deep-learning analysis of breast cancer tumors. The T1WI+T2WI+DWI model had the best diagnostic efficacy for axillary lymph node metastasis, with accuracy and AUC values of 0.970 and 0.996. Luo et al. (26)developed a CNN+SVM model to extract deep features from DWI images of different orientations of the breast cancer tumor by using the CNN model and SVM as a classifier. They then evaluated the status of axillary lymph nodes, and the AUC value of this model was 0.852. These studies suggest that deep learning analysis of MRI images of the breast cancer tumor and axillary lymph nodes would be useful for predicting axillary lymph node status in breast cancer patients.

In this study, axial T2WI, DWI, and DCE-MRI images of breast cancer tumors of the same resolution size were used for deep learning analysis to ensure consistency of image input. The efficacy of the T2WI-based model for diagnosing axillary lymph node metastasis remained superior to that of the DWI and DCE-MRI-based models. The results were consistent with those of Wang et al (27). The possible reasons are mainly in two aspects. First, the T2WI-based model may extract richer features than the DWI and DCE-MRI base models in our study. ResNets are widely used in image classification tasks, such like ResNet18, ResNet50, ResNet101, but the number of extracted features varies with the number of layers of the ResNet. The feature

extraction process is generally simple to complex and low-level to high-level. The ResNet50 model may be too shallow for DWI and DCE-MRI images in terms of the number of layers to extract relevant deep features. Second, for axillary lymph node metastasis, T2WI raw images of invasive breast cancer have more meaningful features than DWI and DCE-MRI raw images. The ROI in this study included the breast tumor itself and peritumoral edema. Previous studies (38)showed that the presence of perineural edema in breast cancer and axillary lymph node metastasis were closely related, and T2WI was the best sequence to show perineural edema.

Our study has some limitations. First, this study is a retrospective analysis and lacks multicenter data, which needs to be further validated by prospective studies. Second, the sample size is small, and the data distribution is unbalanced between ALNM and Non-ALNM groups, which needs a more extensive data set for further study. Third, the MR images acquired in this study are from two types of MR scanners, which may have some influence on the accuracy of the final results. However, based on the idea of multicenter validation, we believe that the model in our study could achieve similar accuracy in different medical centers and has the value of clinical replication.

In conclusion, we developed a novel model for preoperative prediction of axillary lymph node metastasis in breast cancer using multi-parametric MRI datasets. Our results showed that T2WI outperformed DWI and DCE-MRI for predicting axillary lymph node metastasis in breast cancer for a single MRI sequence, but the multiparametric MRI model combined with ensemble learning improved the predictive performance. This model may give clinicians more information about breast cancer axillary lymph nodes preoperatively and assist in clinical decision-making.

Data availability statement

The original contributions presented in the study are included in the article/supplementary material. Further inquiries can be directed to the corresponding author.

Ethics statement

The studies involving human participants were reviewed and approved by the ethics committee and institutional review of The First Affiliated Hospital of Shandong First Medical University. The ethics committee waived the requirement of written informed consent for participation. Written informed consent was not obtained from the individual(s) for the

publication of any potentially identifiable images or data included in this article.

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Author contributions

XZ: Data investigation, experiment design, manuscript writing; ML: Experiment guidance and statistical method selection; WR and JS: Data collection and analysis; KW and XX: Data processing and analysis; GZ: Experiment Design, Supervision, Writing – Review. All authors contributed to the article and approved the submitted version.

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Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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