



Blood-Brain Barrier Disruption in Neuro-Oncology: Strategies, Failures, and Challenges to Overcome

Brij S. Karmur^{1†}, Justine Philteos^{1†}, Aram Abbasian^{1,2†}, Brad E. Zacharia³, Nir Lipsman⁴, Victor Levin⁵, Stuart Grossman⁶ and Alireza Mansouri^{3*}

¹ Faculty of Medicine, University of Toronto, Toronto, ON, Canada, ² Department of Physiology, University of Toronto, Toronto, ON, Canada, ³ Penn State Health Neurosurgery, College of Medicine, Penn State University, Hershey, PA, United States, ⁴ Division of Neurosurgery, University of Toronto, Toronto, ON, Canada, ⁵ Department of Neurosurgery, Medical School, University of California, San Francisco, San Francisco, CA, United States, ⁶ Department of Oncology, Johns Hopkins Medicine, Baltimore, MD, United States

OPEN ACCESS

Edited by:

Olaf Van Tellingen,
The Netherlands Cancer Institute
(NKI), Netherlands

Reviewed by:

David Fortin,
Université de Sherbrooke, Canada
Matthew Tate,
Northwestern University, United States

*Correspondence:

Alireza Mansouri
amansouri@pennstatehealth.psu.edu

[†]These authors have contributed
equally to this work

Specialty section:

This article was submitted to
Neuro-Oncology and Neurosurgical
Oncology,
a section of the journal
Frontiers in Oncology

Received: 19 May 2020

Accepted: 13 August 2020

Published: 18 September 2020

Citation:

Karmur BS, Philteos J, Abbasian A,
Zacharia BE, Lipsman N, Levin V,
Grossman S and Mansouri A (2020)
Blood-Brain Barrier Disruption in
Neuro-Oncology: Strategies, Failures,
and Challenges to Overcome.
Front. Oncol. 10:563840.
doi: 10.3389/fonc.2020.563840

The blood-brain barrier (BBB) presents a formidable challenge in the development of effective therapeutics in neuro-oncology. This has fueled several decades of efforts to develop strategies for disrupting the BBB, but progress has not been satisfactory. As such, numerous drug- and device-based methods are currently being investigated in humans. Through a focused assessment of completed, active, and pending clinical trials, our first aim in this review is to outline the scientific foundation, successes, and limitations of the BBBD strategies developed to date. Among 35 registered trials relevant to BBBD in neuro-oncology in the ClinicalTrials.gov database, mannitol was the most common drug-based method, followed by RMP-7 and regadenoson. MR-guided focused ultrasound was the most common device-based method, followed by MR-guided laser ablation, ultrasound, and transcranial magnetic stimulation. While most early-phase studies focusing on safety and tolerability have met stated objectives, advanced-phase studies focusing on survival differences and objective tumor response have been limited by heterogeneous populations and tumors, along with a lack of control arms. Based on shared challenges among all methods, our second objective is to discuss strategies for confirmation of BBBD, choice of systemic agent and drug design, alignment of BBBD method with real-world clinical workflow, and consideration of inadvertent toxicity associated with disrupting an evolutionarily-refined barrier. Finally, we conclude with a strategic proposal to approach future studies assessing BBBD.

Keywords: blood-brain barrier, neuro-oncology, neurosurgical oncology, clinical trial, drug delivery, glioma

INTRODUCTION

The vertebrate blood-brain barrier (BBB) is a multi-faceted entity comprising metabolic, transport, and structural elements (1–6). Through strict regulation of the cerebral microenvironment, the BBB ensures optimal neuronal function (7). Because of this high-fidelity control mechanism, however, the BBB also presents a significant challenge in the management of brain tumors.

THE BBB CHALLENGE IN NEURO-ONCOLOGY

As one of the “success stories” in glioblastoma (GBM) treatment, one of the most common and fatal adult brain tumors, the highest tumor-to-blood concentration ratio achieved for temozolomide (TMZ) is <20%, largely due to the BBB (8–10). Although there is evidence of regional BBB disruption (BBBD) in all gliomas, much of the infiltrative component of the tumor is protected by intact BBB and this impermeability has been a key barrier to treatment success (11). Similar challenges have significantly impeded the pace of therapeutic advances for brain metastases, compared to the range of options available for systemic primaries, where immunotherapy-based regimens have had limited comparative success in advanced-phase clinical trials (12–16).

Attempts at overcoming the BBB, broadly categorizable into bypass or disruption methods, have spanned decades. Examples of the former include convection-enhanced drug delivery and direct implantation of carmustine-loaded polymers into the resection cavity, which have been comprehensively reviewed elsewhere (17–21). Another bypass strategy, ANG1005, is outlined in **Supplementary Table 2** because it was developed more recently and is currently being investigated in multiple trials. In this review, however, we focus exclusively on BBBD strategies.

A search of the ClinicalTrials.gov database was conducted on June 2nd, 2019 for interventional studies assessing BBBD for brain tumors. Linked publications were assessed for detailed trial outcomes. We identified 35 total trials (25 completed, seven active, one terminated, one suspended, and one withdrawn; **Supplementary Table 1**). Twenty-six were drug-based and nine were device-based.

Our objective in this review is three-fold. First, we provide an overview of key trials pertinent to each drug- and device-based strategy, summarized below and outlined in more detail in **Table 1**. Subsequently, through a careful analysis of the methodologies used, we highlight several factors that we believe have hindered progress in this field thus far. These include definitive confirmation of BBBD, rationale for concomitant systemic drug choice, optimal integration into real-world clinical workflow, and the long-term toxicity associated with repeated BBBD. Finally, possible solutions to these issues and ways to increase chances of success in future trials are discussed.

DRUG-BASED STRATEGIES

Mannitol

The BBBD potential of hyperosmotic agents such as mannitol was first demonstrated in rodents in the 1970's (**Table 1**) (22–25). While numerous agents were initially tested, mannitol became the preferred choice owing to its already-established use in patients, and its ability to enhance survival in animal models led to the beginning of clinical investigations in the 1980's. Since then, mannitol-BBBD in patients has been reported in numerous trials (**Table 1**) (26–29, 54–62). Overall, Phase I and II testing has produced potentially encouraging results, with clinical safety well demonstrated and possible indications of effects

on survival. However, control arms are lacking in all studies. Furthermore, proposals for overcoming the significant logistical challenges associated with mannitol administration in a clinical setting are scarce. Both of these issues need to be addressed in future investigations. Trials assessing mannitol combined with chemotherapeutic agents are continuing in one Phase I, four Phase I/II, and one Phase II trial as of the writing of this review, all of which are focused on high grade gliomas (HGGs) except one investigating primary CNS lymphoma. Five are single-arm and one is a non-randomized two-arm trial.

RMP-7

Bradykinin is an endogenous compound that reversibly disrupts the BBB via endothelial B₂ receptors and structural changes in tight junctions (63). RMP-7, a synthetic analog of bradykinin, induces similar changes but has a longer half-life and greater B₂ receptor selectivity, and has been shown to increase drug delivery and survival in rodent models (**Table 1**) (30–32). Both intraarterial (IA) and intravenous (IV) administration of RMP-7 in combination with IV chemotherapy have been tested (33–37, 64–66). Early-phase testing of RMP-7 + carboplatin in HGG established clinical safety and showed potential efficacy, but these studies lacked control arms (33, 35). In contrast, a controlled Phase II trial reported no significant benefit of combining RMP-7 with carboplatin; dosing and timing of RMP-7 should be considered as possible issues (37). In the pediatric setting, a Phase I trial showed no dose-limiting toxicity (DLT) for RMP-7 + carboplatin but a subsequent Phase II trial was terminated for commercial reasons before the majority of first stage accrual goals could be met (**Table 1**) (34). RMP-7 is not currently being investigated for BBBD purposes.

Regadenoson

Regadenoson is an adenosine A_{2A} receptor agonist FDA-approved for pharmacologic cardiac stress testing (67). Investigations into its BBBD potential began on the basis that adenosine is known to mediate BBB permeability, and regadenoson was shown to increase brain concentrations of various agents including TMZ in rats (**Table 1**), an effect likely mediated by decreased expression of tight junction proteins and vasodilation (38, 39). In two pilot studies, however, investigators failed to detect an increase in BBB permeability or evidence of enhanced TMZ delivery after regadenoson administration (**Table 1**) (40, 41). Dosing, timing, and method of BBBD detection are all potential reasons for this discrepancy. Although future studies employing different protocols may yield better results, there are currently no registered pending trials investigating this.

DEVICE-BASED STRATEGIES

MR-gLA

Magnetic resonance-guided laser ablation (MRgLA) employs laser interstitial thermal therapy (LITT) to achieve cytoreduction and BBBD (42, 43). With a rational evaluation of LITT for BBBD, using brain-specific enolase (BSE) and K^{trans}, a completed Phase II trial provides promising evidence in GBM patients with BBBD

TABLE 1 | Overview of drug-based and device-based strategies for BBBB.

Strategy	Type	BBBD duration	Systemic agent	Time to steady state	Molecular weight	Biological Rationale	Clinical Evidence
Mannitol	Drug-based	15–18 min	Temozolomide	9 h	194.1 (g/mol)	- Osmotic BBBB shown to increase diffusion and bulk flow via endothelial cell shrinkage, widening of tight junctions, and vasodilation in rodents (22–25)	- Two Phase I studies; recurrent GBM; IA mannitol + bevacizumab or cetuximab: <ul style="list-style-type: none"> o No DLTs (26, 27) o Median PFS in those receiving bevacizumab was 10 months, longer than historical controls (28). - Phase II; brain metastases; methotrexate or carboplatin, IA mannitol (30-s infusion): median OS of 13.5 months compared with the historical survival of 2.3–4.2 months for the corresponding RPA classes of 2 and 3 (29).
RMP-7	Drug-based	2–20 min	Carboplatin	30 h (post-distribution)	371.2 (g/mol)	- Enhanced delivery of methotrexate and carboplatin and increased survival in tumor-bearing rats (30–32)	- Phase I; children with brainstem glioma, HGG, medulloblastoma/PNET, and ependymoma; IV carboplatin + RMP-7 (administered for 10 min beginning 5 min before the end of carboplatin infusion): <ul style="list-style-type: none"> o No DLT (33) o Subsequent Phase II: no objective response in patients with brainstem gliomas and HGGs; study was terminated for commercial reasons before first stage accrual goals could be met for other tumor strata (34). - Phase I; carboplatin + IV RMP-7 (given during the last 5 min of 15-min carboplatin infusion or as 10-min infusion starting 10 min after the completion of carboplatin): transient side effects related to carboplatin (35). <ul style="list-style-type: none"> o Two multicenter Phase II trials; adult HGG; IV RMP-7 + carboplatin: stable disease or partial or complete response (36). o Randomized double-blind placebo-controlled Phase II study; recurrent HGG: no difference between IV carboplatin + RMP-7 and carboplatin + placebo (37). - Pilot: Adults with no intracranial disease undergoing regadenoson cardiac stress tests; FDA-approved dose of 400 µg: no BBBB observed using brain SPECT and CT imaging (40).
Regadenoson	Drug-based	30–180 min	Methotrexate	40–75 h	454.4 (g/mol)	- IV administration in rodents led to detection of 10 kDa dextrans that peaked at 30 min and lasted for 180 min. It also led to 60% higher brain TMZ levels in non-tumor-bearing rats (38, 39).	- Pilot; recurrent GBM; IV regadenoson administered one hour after oral TMZ: no significant increase in TMZ levels as measured by microdialysis catheters (41).

(Continued)

TABLE 1 | Continued

Strategy	Type	BBBD duration	Systemic agent	Time to steady state	Molecular weight	Biological Rationale	Clinical Evidence
MRgLA	Device	3–45 days	Bevacizumab	100 days	149a	<ul style="list-style-type: none"> - Thin laser probe (1.65–3.3 mm) stereotactically guided to target via diffusing tip (3–25 mm diameter) (42–44) - Hyperthermic ablation temperature of tumor core to 60–70°C; peritumoral region to 40–45°C 	<ul style="list-style-type: none"> - NCT01851733 (Phase II): recurrent GBM patients; early (1-week post-LITT) or late (6-weeks post-LITT) IV doxorubicin injections (44) - K^{trans} peaked immediately post-LITT followed by a decline over 4 weeks. Serum BSE levels peaked 1–3 weeks post-LITT and decreased to baseline by 6 weeks (44)
Cranial-implantable ultrasound (SonoCloud)	Device	<8 h	Cetuximab	114 h	146 kDa	<ul style="list-style-type: none"> - Small (11.5 mm diameter) implantable ultrasound transducer which introduces unfocused low-intensity sonication (1-MHz frequency) to area of interest (45–47). - Gas microbubbles (sulfur hexafluoride) facilitate BBBD for up to 8 h 	<ul style="list-style-type: none"> - NCT02253212 (Phase I): recurrent GBM patients; dose-escalating carboplatin infusion; no permanent severe neurologic AEs occurred (48) - Adequate BBBD (11; 58%) patients vs. no/poor BBBD (PFS: 2.73 vs. 4.11 months, 95% CI, 0.11–0.94, $p = 0.03$; OS: 8.64 vs. 12.94 months, 95% CI, 0.16–1.14, $p = 0.09$) (48)
MRgFUS	Device	<4 h	Etoposide Doxorubicin	100–240 h 20–55 h	588.6 g/mol 543.5 g/mol	<ul style="list-style-type: none"> - Non-invasive ultrasound-based strategy used in conjunction with perfluorocarbon microbubbles. - Stable cavitation (oscillating without bursting) of microbubbles, followed by microstreaming (jet fluid around oscillating microbubbles) and extravasation of microbubbles across vessel walls due to tight junction disruption (49–52) 	<ul style="list-style-type: none"> - NCT02343991 (Phase I): five patients with HGG; doxorubicin (one patient) or TMZ (four patients); no serious AEs were noted; 10–15% immediate increase in gadolinium enhancement with resolution ~20 h (53). - NCT03551249 (USA) and NCT03712293 (Korea): HGG patients - NCT03322813 (USA): Suspected infiltrative glioma on pre-operative brain imaging scans - NCT03714243 (Canada): Her2 positive breast metastasis

AEs, adverse events; BBBD, blood-brain barrier disruption; CI, confidence interval; CT, computed tomography; DLT, dose-limiting toxicity; FDA, Food and Drug Administration; GBM, glioblastoma; HGG, high grade glioma; IA, intraarterial; IV, intravenous; LITT, laser interstitial thermal therapy; NCT, ClinicalTrials.gov identifier number; OS, overall survival; PNET, primitive neuroectodermal tumor; PFS, progression-free survival; RPA, recursive partitioning analysis; SPECT, single-photon emission computed tomography; TMZ, temozolamide.

for 1–3 weeks (**Table 1**) (44). However, the capital and procedural cost of LITT, and the invasive nature of this procedure could be potential deterrents to widespread use (68). Furthermore, 1–3 weeks of BBBD may result in an unnecessarily prolonged exposure of healthy brain tissue to the external environment, which may reduce drug residence time by promoting leakage of drug back into the bloodstream. Although more Phase II testing can offer great insight into the efficacy of LITT for BBBD, only one ongoing Phase I trial, in pediatric glioma, is underway.

Cranial Implantable Ultrasound

SonoCloud is an implantable transducer device which introduces unfocused low-intensity sonication to the area of interest, and has demonstrated BBBD in multiple preclinical studies (45–47). The safety and efficacy of SonoCloud is established in a Phase I trial, with a moderate increase in PFS and OS (**Table 1**) (48). However, despite being more amenable to repetitive sonication, implanting a permanent device increases the theoretical risk of infection. Another limitation involves the linear beam of the transducer and lack of beam focusing, making it difficult to assess the specificity of sonication in the region of interest. At this time, there are no active clinical trials investigating SonoCloud for BBBD.

MRgFUS

MR-guided focused ultrasound (MRgFUS) is a non-invasive ultrasound-based strategy for BBBD (49–52). A single-arm Phase I trial demonstrated BBBD by dynamic contrast-enhanced MRI (DCE-MRI) using MRgFUS in high-grade glioma (HGG) patients (53). Although BBBD was demonstrated in the completed Phase I trial by gadolinium enhancement seen on DCE-MRI, the extravasation of chemotherapy can only be accurately measured through serum biomarkers. However, one of the major advantages of MRgFUS is its precision, and that BBBD can be directly visualized to enable refinements in real-time rather than relying on a delayed assessment (**Figure 1**). From a safety standpoint, it eliminates the risks associated with implantation. In order to be successful for larger and/or diffusely infiltrating lesions, larger volumes of sonication and/or repeated sonication sessions would likely be required, necessitating repetitive shaving of the head and frame application, higher doses of microbubble administration, longer imaging time, or additional sessions, all with inherently increased risk to patients. MRgFUS is the most widely studied device based BBBD strategies with multiple non-randomized ongoing trials in Canada, USA, and Korea (**Table 1**).

CHALLENGES AND FUTURE DIRECTIONS

The tremendous difficulty in overcoming the BBB for optimal delivery of therapeutics is reflected in the limited success of the decades of effort dedicated to this topic, and this remains a fundamental gap in research pertaining to the treatment of primary and secondary brain neoplasms. Consequently, one must approach testing BBBD methods in a stepwise manner to increase probability of ruling in or out the therapeutic utility of specific strategies.

One such approach involves go/no-go decision-making, in which specific criteria are used to make early decisions regarding continuing or stopping a drug development process (69). Simply put, the go/no-go system is a binary decision-aid in which two factors are required for a pass—“go” conditions must be met and “no go” criteria must fail—and can be used to make clinical investigations of BBBD strategies as efficient as possible.

Moving forward, the standardized go/no-go approach can help investigators identify which BBBD strategies should proceed with more thorough testing and which should be halted at earlier phases. Key challenges and considerations which need to be taken into account, and which we believe have received inadequate attention so far, are outlined below.

Trial Design

One of the common limitations among studies published so far is the lack of control arms, applying equally to the drug- and device-based investigations reviewed here. Achieving balanced control arms in this setting is of course difficult and part of the broader challenge of designing effective randomized controlled trials (RCTs) in neurosurgery (70). Notwithstanding, simply incorporating arms without BBBD would enable investigators to make firmer conclusions early on regarding the potential of a given strategy. As an example, a controlled Phase II trial of RMP-7 + carboplatin produced conflicting results relative to preceding studies (37). Looking forward, very few of the pending trials include control arms, and improving on this front would expedite progress.

Confirmation of BBBD

Serum and CSF markers of BBBD are potentially viable strategies for direct assessment of the success of BBBD methods. Brain-related proteins, such as S100B, monomeric transthyretin (TTR), and BSE, can be detected in the peripheral circulation in pathologies affecting BBB integrity (71). Assessment of CSF albumin is another potential method of assessing BBBD. Albumin is synthesized peripherally, is not catabolized within the CNS, and does not readily diffuse across an intact BBB (72). Aside from the invasive nature of this method, disruption of the blood-CSF barrier is not necessarily an accurate reflection of the status of the BBB.

In addition to serum and CSF biomarkers, there are also several imaging techniques used in assessing BBBD, including cerebral angiography, single-photon emission computed tomography (SPECT), static contrast-enhanced MRI, and DCE-MRI. Cerebral angiography is one of the oldest imaging techniques in neurosurgery. Assessment of changes in the blush pattern following administration of contrast can be used in assessing changes in BBB permeability; however, this is a relatively invasive technique. Another invasive technique is SPECT, a nuclear imaging scan that integrates computed tomography and a radioactive tracer. Challenges with SPECT imaging include the use of radiolabeled material and the time-sensitive nature of the results. Furthermore, the molecular size of the radiolabeled material, typically iodine or technetium, does not compare with most systemic therapeutic agents—the

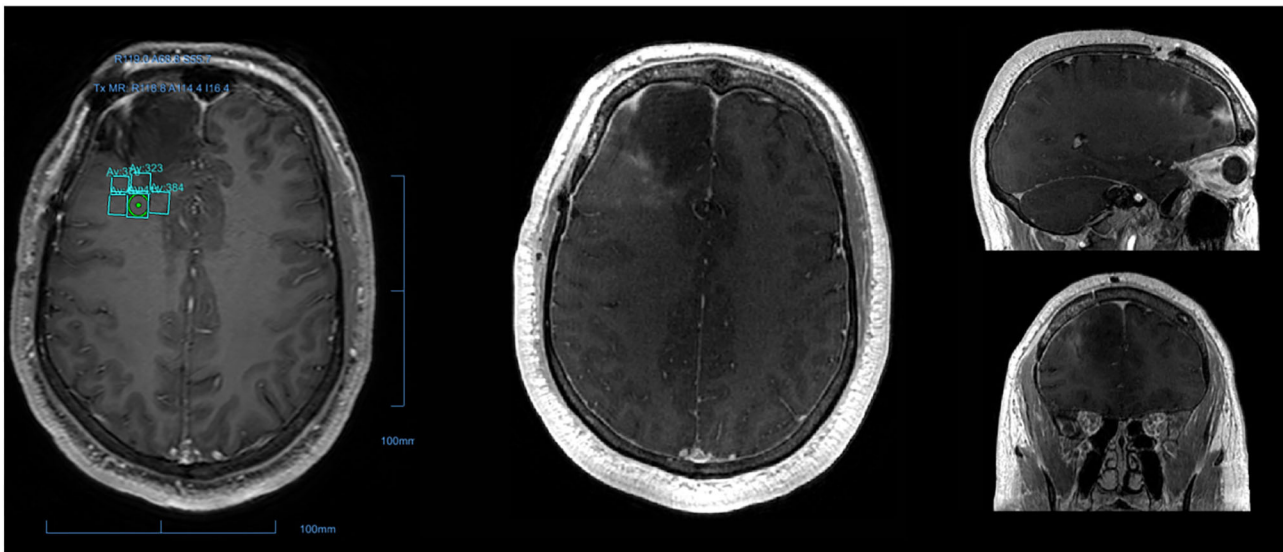


FIGURE 1 | Post-operative peritumoral BBB disruption via MR-guided focused ultrasound. T1-weighted MRI from a patient who underwent surgery for glioblastoma followed by sonication of the resection boundary. The sonication field encompassed the 1×1 cm grid demonstrated, with nine sonication spots in each. Gadolinium, administered immediately after sonication was complete, was used to confirm precise disruption of the blood-brain barrier as indicated by the nine small areas of gadolinium leakage.

ultimate target of interest. Contrastingly, static contrast-enhanced MRI based on changes of gadolinium enhancement is relatively non-invasive in comparison to angiography and SPECT has often been used to assess BBB permeability in the modern imaging era. However, we advocate for DCE-MRI, in which several images are acquired in rapid succession enabling dynamic assessment of changes in contrast while also providing parameters pertinent to perfusion and permeability (73). Limitations of DCE-MRI, as stated in the MRgFUS discussion, include the spatial resolution and the ability to correlate dynamic variations in contrast enhancement with pharmacokinetic properties of test agents. Optimal sonication power has been established in previous studies (74, 75).

The timing of BBB disruption must align well with the pharmacokinetics of the agent. Furthermore, direct confirmation of drug accumulation and maintenance in the target tissue is critical. Direct drug measurement through microdialysis catheters is one option, though invasive. Alternatively, advances in drug development have facilitated the generation of radiolabeled agents for investigational use (76). This enables the possibility of assessing BBB disruption through non-invasive detection of the concentration of systemic agents of interest. However, this once again raises the need for pharmacological studies and complication of the regulatory process as the original identity of the compound has been altered—further illustrating the challenges involved in confirming BBB disruption.

Choice of Systemic Agent

In-depth knowledge regarding the pharmacokinetic parameters of systemic agents, such as time to steady-state, is critical in optimizing the timing and duration of systemic agent delivery

in relation to BBB disruption. Indeed, the time to steady-state of most systemic agents used in the reviewed trials was notably higher than the duration of BBB disruption. The success of cancer chemotherapy typically hinges upon circumventing dose-limited toxicity. In addition, pharmacokinetic properties of the drug must also be considered. Recent literature has proven that in order to improve brain exposure, polarity, and/or hydrogen-bonding capacity of the agent must be decreased (77). At the most basic level, these include interactions with drug-resistance factors such as extracellular receptors and intra-cellular DNA repair enzymes. At a deeper level, drug-related (e.g., tumor-binding specificity, low plasma clearance and lipophilicity) and tumor-related (e.g., size and mass effect exerted on surrounding brain) factors are also critical (78). Indeed, brain tumors influence their surrounding microenvironment, such that the established dynamics for an intact BBB are altered. Based on analyses of pharmacological properties of various compounds, it has been demonstrated that the distribution of high molecular weight compounds (such as monoclonal antibodies) is greater and faster in tumor tissue than normal brain, despite this being diffusion-limited (79). As such, it would be erroneous to assume uniform tumor cell vulnerability to drugs, as there are regional differences in BBB permeability and drug diffusion parameters.

These pharmacological considerations also put forth a predicament when designing a trial. The standard of care at the time of study initiation may not be the most effective drug against the target disease. Alternatively, a drug with suitable activity against the target disease may be unable to penetrate the BBB or the doses required for adequate tissue accumulation would be too toxic. This dilemma is readily applicable to the BBB disruption studies for GBM. For example, demonstration of increased

permeability to carboplatin—a hydrophilic agent that does not readily penetrate the BBB—would in theory represent successful BBBB; however, the inferior effectiveness of this agent against malignant gliomas diminishes the relevance of the findings to the GBM population. Alternatively, increasing the concentration of TMZ—the current standard of care for GBM—in tumor tissue through an investigational BBBB method could be marked as a success.

Applicability to Real-World Setting

In designing a BBBB strategy, unless the technique and its scheduling aligns with reasonable clinical care pathways and minimizes undue risk to patients, the uptake for the technique may be limited, even if shown to be successful.

One criticism of CNS drug development is that molecular targets have been the focus of research and the pharmaceutical industry without significant therapeutic advancements. The aim of early “go-no go” decisions is that investment in studies is targeted toward therapeutic potential, quickly ruling out ineffective mechanisms. The “go-no go” approach hinges on the approach that efficacious processes for data interpretation require frontload data interpretation. This requires that decision criteria is established during the design phase, and adoption of standard methodology (80). Thus, in the absence of measurability of drug function in the human brain an early decision is made not to pursue clinical efficacy trials (81). However, even after establishing the successful target molecular interaction, the researcher is faced with an additive layer of “go-no go” decision-making: is the demonstration of desired target molecular interaction sufficient to justify an efficacy trial? Or must one also require demonstration of functional brain effect? (82).

In the case of brain metastases, the optimal timing of BBBB in relation to treatments for the systemic primary must also be considered: should BBBB be included upfront and in conjunction with systemic therapies of established effectiveness (e.g., Herceptin for Her2 positive breast cancer), in the absence of evidence of metastases, or should this be isolated to patients with established metastases only? The case for upfront treatment is based on the rationale that if tumor metastasis is inevitable given the stage of the disease, systemic treatment with BBBB may be of utility in preventing or decreasing CNS burden. In such a case, drug-based strategies may offer benefit over more focused device-based ones. Alternatively, in the case of established brain metastases, a device-based strategy may enable focused therapeutic delivery to targets, in the brain-tumor interphase.

For diffusely infiltrating gliomas, the target of sonication would be the FLAIR hyperintense regions where there is likely a high degree of tumor infiltration but an intact BBB. Also potentially necessitating targeted BBBB are cases in which a global increase in the systemic agent would introduce unacceptable toxicity, as has been demonstrated for TMZ in animal glioma models (83). Ultimately, both device- and drug-based strategies, once established, will likely have complementary roles.

Toxicity

Although safety and tolerability within an early phase clinical trial setting has been shown for most BBBB methods, long-term analyses, and the effect of other concomitant medications on the neuronal environment when exposed to a more permeable BBB has not been studied in detail. The latter in particular is a concern that must be taken into consideration as we strive to incorporate BBBB from the research realm into the clinical sphere. Therefore, a comprehensive evaluation of the safety profile of many of the drugs currently in use for other disorders may be needed prior to wide-spread clinical implementation of a successful BBBB method.

CONCLUSION

In this review of the landscape of BBBB, a variety of methods were discussed, with device-based strategies predominating the most recent time period. Early-phase trials have yielded encouraging results overall, but the lack of efficacy in later phase testing and termination of several lines of investigation indicate the urgent need for a more systematic, standardized approach to trial design in this space. The points raised here aim to generate an in-depth collaborative discussion in order to expedite progress in the development of effective BBBB strategies. The field of neuro-oncology is in need of a breakthrough.

AUTHOR CONTRIBUTIONS

All authors have contributed, read, and approved the final manuscript.

SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: <https://www.frontiersin.org/articles/10.3389/fonc.2020.563840/full#supplementary-material>

REFERENCES

- Abbott NJ, Ronnback L, Hansson E. Astrocyte-endothelial interactions at the blood-brain barrier. *Nat Rev Neurosci.* (2006) 7:41–53. doi: 10.1038/nrn1824
- Rubin LL, Hall DE, Porter S, Barbu K, Cannon C, Horner HC, et al. A cell culture model of the blood-brain barrier. *J Cell Biol.* (1991) 115:1725–35. doi: 10.1083/jcb.115.6.1725
- Obermeier B, Daneman R, Ransohoff RM. Development, maintenance and disruption of the blood-brain barrier. *Nat Med.* (2013) 19:1584–96. doi: 10.1038/nm.3407
- Carvey PM, Hendey B, Monahan AJ. The blood-brain barrier in neurodegenerative disease: a rhetorical perspective. *J Neurochem.* (2009) 111:291–314. doi: 10.1111/j.1471-4159.2009.06319.x
- Schinkel AH. P-Glycoprotein, a gatekeeper in the blood-brain barrier. *Adv Drug Deliv Rev.* (1999) 36:179–94. doi: 10.1016/S0169-409X(98)00085-4
- Marchetti S, Mazzanti R, Beijnen JH, Schellens JH. Concise review: clinical relevance of drug drug and herb drug interactions mediated by the ABC transporter ABCB1 (MDR1, P-glycoprotein). *Oncologist.* (2007) 12:927–41. doi: 10.1634/theoncologist.12-8-927

7. Abbott NJ, Hughes CC, Revest PA, Greenwood J. Development and characterisation of a rat brain capillary endothelial culture: towards an *in vitro* blood-brain barrier. *J Cell Sci.* (1992) 103 (Pt 1):23–37.
8. Ostermann S, Csajka C, Buclin T, Leyvraz S, Lejeune F, Decosterd LA, et al. Plasma and cerebrospinal fluid population pharmacokinetics of temozolomide in malignant glioma patients. *Clin Cancer Res.* (2004) 10:3728–36. doi: 10.1158/1078-0432.CCR-03-0807
9. Portnow J, Badie B, Chen M, Liu A, Blanchard S, Synold TW. The neuropharmacokinetics of temozolomide in patients with resectable brain tumors: potential implications for the current approach to chemoradiation. *Clin Cancer Res.* (2009) 15:7092–8. doi: 10.1158/1078-0432.CCR-09-1349
10. Stupp R, Mason WP, van den Bent MJ, Weller M, Fisher B, Taphoorn MJ, et al. Radiotherapy plus concomitant and adjuvant temozolomide for glioblastoma. *N Engl J Med.* (2005) 352:987–96. doi: 10.1056/NEJMoa043330
11. Sarkaria JN, Hu LS, Parney IF, Pafundi DH, Brinkmann DH, Laack NN, et al. Is the blood-brain barrier really disrupted in all glioblastomas? A critical assessment of existing clinical data. *Neuro Oncol.* (2018) 20:184–91. doi: 10.1093/neuonc/nox175
12. Pestalozzi BC, Brignoli S. Trastuzumab in CSF. *J Clin Oncol.* (2000) 18:2349–51. doi: 10.1200/JCO.2000.18.11.2349
13. Nayak L, Lee EQ, Wen PY. Epidemiology of brain metastases. *Curr Oncol Rep.* (2012) 14:48–54. doi: 10.1007/s11912-011-0203-y
14. Reck M, Rodriguez-Abreu D, Robinson AG, Hui R, Czoszi T, Fulop A, et al. Pembrolizumab versus chemotherapy for PD-L1-positive non-small-cell lung cancer. *N Engl J Med.* (2016) 375:1823–33. doi: 10.1056/NEJMoa1606774
15. Motzer RJ, Escudier B, McDermott DF, George S, Hammers HJ, Srinivas S, et al. Nivolumab versus everolimus in advanced renal-cell carcinoma. *N Engl J Med.* (2015) 373:1803–13. doi: 10.1056/NEJMoa1510665
16. Robert C, Schachter J, Long GV, Arance A, Grob JJ, Mortier L, et al. Pembrolizumab versus ipilimumab in advanced melanoma. *N Engl J Med.* (2015) 372:2521–32. doi: 10.1056/NEJMoa1503093
17. Brem H, Piantadosi S, Burger PC, Walker M, Selker R, Vick NA, et al. Placebo-controlled trial of safety and efficacy of intraoperative controlled delivery by biodegradable polymers of chemotherapy for recurrent gliomas. The Polymer-brain Tumor Treatment Group. *Lancet.* (1995) 345:1008–12. doi: 10.1016/S0140-6736(95)90755-6
18. Westphal M, Hilt DC, Bortey E, Delavault P, Olivares R, Warnke PC, et al. A phase 3 trial of local chemotherapy with biodegradable carmustine (BCNU) wafers (Gliadel wafers) in patients with primary malignant glioma. *Neuro Oncol.* (2003) 5:79–88. doi: 10.1093/neuonc/5.2.79
19. Westphal M, Ram Z, Riddle V, Hilt D, Bortey E, Executive Committee of the Gliadel Study G. Gliadel wafer in initial surgery for malignant glioma: long-term follow-up of a multicenter controlled trial. *Acta Neurochir (Wien).* (2006) 148:269–75; discussion 75. doi: 10.1007/s00701-005-0707-z
20. Bruce JN, Fine RL, Canoll P, Yun J, Kennedy BC, Rosenfeld SS, et al. Regression of recurrent malignant gliomas with convection-enhanced delivery of topotecan. *Neurosurgery.* (2011) 69:1272–9; discussion 9–80. doi: 10.1227/NEU.0b013e3182233e24
21. Vogelbaum MA, Aghi MK. Convection-enhanced delivery for the treatment of glioblastoma. *Neuro Oncol.* (2015) 17(Suppl 2):ii3–ii8. doi: 10.1093/neuonc/nou354
22. Rapoport SI. Advances in osmotic opening of the blood-brain barrier to enhance CNS chemotherapy. *Expert Opin Investig Drugs.* (2001) 10:1809–18. doi: 10.1517/13543784.10.10.1809
23. Rapoport SI. Effect of concentrated solutions on blood-brain barrier. *Am J Physiol.* (1970) 219:270–4. doi: 10.1152/ajplegacy.1970.219.1.270
24. Brightman MW, Hori M, Rapoport SI, Reese TS, Westergaard E. Osmotic opening of tight junctions in cerebral endothelium. *J Comp Neurol.* (1973) 152:317–25. doi: 10.1002/cne.901520402
25. Rapoport SI, Hori M, Klatzo I. Testing of a hypothesis for osmotic opening of the blood-brain barrier. *Am J Physiol.* (1972) 223:323–31. doi: 10.1152/ajplegacy.1972.223.2.323
26. Boockvar JA, Tsiouris AJ, Hofstetter CP, Kovanlikaya I, Fralin S, Kesavabhotla K, et al. Safety and maximum tolerated dose of superselective intraarterial cerebral infusion of bevacizumab after osmotic blood-brain barrier disruption for recurrent malignant glioma. *Clinical article. J Neurosurg.* (2011) 114:624–32. doi: 10.3171/2010.9.JNS101223
27. Shin BJ, Burkhardt JK, Riina HA, Boockvar JA. Superselective intra-arterial cerebral infusion of novel agents after blood-brain barrier disruption for the treatment of recurrent glioblastoma multiforme: a technical case series. *Neurosurg Clin N Am.* (2012) 23:323–9, ix–x. doi: 10.1016/j.nec.2012.01.008
28. Burkhardt JK, Riina H, Shin BJ, Christos P, Kesavabhotla K, Hofstetter CP, et al. Intra-arterial delivery of bevacizumab after blood-brain barrier disruption for the treatment of recurrent glioblastoma: progression-free survival and overall survival. *World Neurosurg.* (2012) 77:130–4. doi: 10.1016/j.wneu.2011.05.056
29. Fortin D, Desjardins A, Benko A, Niyonsega T, Boudrias M. Enhanced chemotherapy delivery by intraarterial infusion and blood-brain barrier disruption in malignant brain tumors: the Sherbrooke experience. *Cancer.* (2005) 103:2606–15. doi: 10.1002/cncr.21112
30. Inamura T, Nomura T, Bartus RT, Black KL. Intracarotid infusion of RMP-7, a bradykinin analog: a method for selective drug delivery to brain tumors. *J Neurosurg.* (1994) 81:752–8. doi: 10.3171/jns.1994.81.5.0752
31. Bartus RT, Elliott PJ, Dean RL, Hayward NJ, Nagle TL, Huff MR, et al. Controlled modulation of BBB permeability using the bradykinin agonist, RMP-7. *Exp Neurol.* (1996) 142:14–28. doi: 10.1006/exnr.1996.0175
32. Elliott PJ, Hayward NJ, Dean RL, Blunt DG, Bartus RT. Intravenous RMP-7 selectively increases uptake of carboplatin into rat brain tumors. *Cancer Res.* (1996) 56:3998–4005.
33. Warren KE, Patel MC, Aikin AA, Widemann B, Libucha M, Adamson PC, et al. Phase I trial of lobaradimil (RMP-7) and carboplatin in children with brain tumors. *Cancer Chemother Pharmacol.* (2001) 48:275–82. doi: 10.1007/s002800100356
34. Warren K, Jakacki R, Widemann B, Aikin A, Libucha M, Packer R, et al. Phase II trial of intravenous lobaradimil and carboplatin in childhood brain tumors: a report from the Children's Oncology Group. *Cancer Chemother Pharmacol.* (2006) 58:343–7. doi: 10.1007/s00280-005-0172-7
35. Ford J, Osborn C, Barton T, Bleehe NM. A phase I study of intravenous RMP-7 with carboplatin in patients with progression of malignant glioma. *Eur J Cancer.* (1998) 34:1807–11. doi: 10.1016/S0959-8049(98)00155-5
36. Gregor A, Lind M, Newman H, Grant R, Hadley DM, Barton T, et al. Phase II studies of RMP-7 and carboplatin in the treatment of recurrent high grade glioma. RMP-7 European Study Group. *J Neurooncol.* (1999) 44:137–45.
37. Prados MD, Schold SC Jr, Fine HA, Jaeckle K, Hochberg F, et al. A randomized, double-blind, placebo-controlled, phase 2 study of RMP-7 in combination with carboplatin administered intravenously for the treatment of recurrent malignant glioma. *Neuro Oncol.* (2003) 5:96–103. doi: 10.1093/neuonc/5.2.96
38. Carman AJ, Mills JH, Krenz A, Kim DG, Bynoe MS. Adenosine receptor signaling modulates permeability of the blood-brain barrier. *J Neurosci.* (2011) 31:13272–80. doi: 10.1523/JNEUROSCI.3337-11.2011
39. Jackson S, Anders NM, Mangraviti A, Wanjiku TM, Sankey EW, Liu A, et al. The effect of regadenoson-induced transient disruption of the blood-brain barrier on temozolomide delivery to normal rat brain. *J Neurooncol.* (2016) 126:433–9. doi: 10.1007/s11060-015-1998-4
40. Jackson S, George RT, Lodge MA, Piotrowski A, Wahl RL, Gujar SK, et al. The effect of regadenoson on the integrity of the human blood-brain barrier, a pilot study. *J Neurooncol.* (2017) 132:513–9. doi: 10.1007/s11060-017-2404-1
41. Jackson S, Weingart J, Nduom EK, Harfi TT, George RT, McAreavey D, et al. The effect of an adenosine A2A agonist on intra-tumoral concentrations of temozolomide in patients with recurrent glioblastoma. *Fluids Barriers CNS.* (2018) 15:2. doi: 10.1186/s12987-017-0088-8
42. Patel NV, Mian M, Stafford RJ, Nahed BV, Willie JT, Gross RE, et al. Laser interstitial thermal therapy technology, physics of magnetic resonance imaging thermometry, and technical considerations for proper catheter placement during magnetic resonance imaging-guided laser interstitial thermal therapy. *Neurosurgery.* (2016) 79(Suppl 1):S8–S16. doi: 10.1227/NEU.0000000000001440
43. Hawasli AH, Bandt SK, Hogan RE, Werner N, Leuthardt EC. Laser ablation as treatment refractory for medically refractory dominant insular epilepsy: therapeutic and functional considerations. *Stereotact Funct Neurosurg.* (2014) 92:397–404. doi: 10.1159/000366001
44. Leuthardt EC, Duan C, Kim MJ, Campian JL, Kim AH, Miller-Thomas MM, et al. Hyperthermic laser ablation of recurrent glioblastoma leads to temporary disruption of the peritumoral blood brain barrier. *PLoS One.* (2016) 11:e0148613. doi: 10.1371/journal.pone.0148613

45. Beccaria K, Canney M, Goldwirt L, Fernandez C, Adam C, Piquet J, et al. Opening of the blood-brain barrier with an unfocused ultrasound device in rabbits. *J Neurosurg.* (2013) 119:887–98. doi: 10.3171/2013.5.JNS122374
46. Beccaria K, Canney M, Goldwirt L, Fernandez C, Piquet J, Perier MC, et al. Ultrasound-induced opening of the blood-brain barrier to enhance temozolomide and irinotecan delivery: an experimental study in rabbits. *J Neurosurg.* (2016) 124:1602–10. doi: 10.3171/2015.4.JNS142893
47. Horodyckid C, Canney M, Vignot A, Boisgard R, Drier A, Huberfeld G, et al. Safe long-term repeated disruption of the blood-brain barrier using an implantable ultrasound device: a multiparametric study in a primate model. *J Neurosurg.* (2017) 126:1351–61. doi: 10.3171/2016.3.JNS151635
48. Idbah A, Canney M, Belin L, Desseaux C, Vignot A, Bouchoux G, et al. Safety and feasibility of repeated and transient blood-brain barrier disruption by pulsed ultrasound in patients with recurrent glioblastoma. *Clin Cancer Res.* (2019) 25:3793–801. doi: 10.1158/1078-0432.CCR-18-3643
49. Kinoshita M, McDannold N, Jolesz FA, Hynynen K. Targeted delivery of antibodies through the blood-brain barrier by MRI-guided focused ultrasound. *Biochem Biophys Res Commun.* (2006) 340:1085–90. doi: 10.1016/j.bbrc.2005.12.112
50. Sheikov N, McDannold N, Jolesz F, Zhang YZ, Tam K, Hynynen K. Brain arterioles show more active vesicular transport of blood-borne tracer molecules than capillaries and venules after focused ultrasound-evoked opening of the blood-brain barrier. *Ultrasound Med Biol.* (2006) 32:1399–409. doi: 10.1016/j.ultrasmedbio.2006.05.015
51. Suzuki R, Oda Y, Utoguchi N, Maruyama K. Progress in the development of ultrasound-mediated gene delivery systems utilizing nano- and microbubbles. *J Control Release.* (2011) 149:36–41. doi: 10.1016/j.jconrel.2010.05.009
52. Etame AB, Diaz RJ, Smith CA, Mainprize TG, Hynynen K, Rutka JT. Focused ultrasound disruption of the blood-brain barrier: a new frontier for therapeutic delivery in molecular neurooncology. *Neurosurg Focus.* (2012) 32:E3. doi: 10.3171/2011.10.FOCUS11252
53. Mainprize T, Lipsman N, Huang Y, Meng Y, Bethune A, Ironside S, et al. Blood-brain barrier opening in primary brain tumors with non-invasive mr-guided focused ultrasound: a clinical safety and feasibility study. *Sci Rep.* (2019) 9:321. doi: 10.1038/s41598-018-36340-0
54. Chakraborty S, Filippi CG, Wong T, Ray A, Fralin S, Tsiouris AJ, et al. Superselective intraarterial cerebral infusion of cetuximab after osmotic blood/brain barrier disruption for recurrent malignant glioma: phase I study. *J Neurooncol.* (2016) 128:405–15. doi: 10.1007/s11060-016-2099-8
55. Fortin D, Gendron C, Boudrias M, Garant MP. Enhanced chemotherapy delivery by intraarterial infusion and blood-brain barrier disruption in the treatment of cerebral metastasis. *Cancer.* (2007) 109:751–60. doi: 10.1002/cncr.22450
56. Jahnke K, Kraemer DF, Knight KR, Fortin D, Bell S, Doolittle ND, et al. Intraarterial chemotherapy and osmotic blood-brain barrier disruption for patients with embryonal and germ cell tumors of the central nervous system. *Cancer.* (2008) 112:581–8. doi: 10.1002/cncr.23221
57. Hall WA, Doolittle ND, Daman M, Bruns PK, Muldoon L, Fortin D, et al. Osmotic blood-brain barrier disruption chemotherapy for diffuse pontine gliomas. *J Neurooncol.* (2006) 77:279–84. doi: 10.1007/s11060-005-9038-4
58. Doolittle ND, Miner ME, Hall WA, Siegal T, Jerome E, Osztie E, et al. Safety and efficacy of a multicenter study using intraarterial chemotherapy in conjunction with osmotic opening of the blood-brain barrier for the treatment of patients with malignant brain tumors. *Cancer.* (2000) 88:637–47. doi: 10.1002/(SICI)1097-0142(20000201)88:3<637::AID-CNCR22>3.0.CO;2-Y
59. Miyagami M, Tsubokawa T, Tazoe M, Kagawa Y. Intra-arterial ACNU chemotherapy employing 20% mannitol osmotic blood-brain barrier disruption for malignant brain tumors. *Neurol Med Chir (Tokyo).* (1990) 30:582–90. doi: 10.2176/nmc.30.582
60. Macnealy MW, Newton HB, McGregor JM, Bell SD, Ray Chaudhury A, Slone HW, et al. Primary meningeal CNS lymphoma treated with intra-arterial chemotherapy and blood-brain barrier disruption. *J Neurooncol.* (2008) 90:329–33. doi: 10.1007/s11060-008-9667-5
61. Angelov L, Doolittle ND, Kraemer DF, Siegal T, Barnett GH, Peereboom DM, et al. Blood-brain barrier disruption and intra-arterial methotrexate-based therapy for newly diagnosed primary CNS lymphoma: a multi-institutional experience. *J Clin Oncol.* (2009) 27:3503–9. doi: 10.1200/JCO.2008.19.3789
62. Guillaume DJ, Doolittle ND, Gahramanov S, Hedrick NA, Delashaw JB, Neuwelt EA. Intra-arterial chemotherapy with osmotic blood-brain barrier disruption for aggressive oligodendroglial tumors: results of a phase I study. *Neurosurgery.* (2010) 66:48–58; discussion 58. doi: 10.1227/01
63. Regoli D, Barabe J. Pharmacology of bradykinins and related kinins. *Pharmacol Rev.* (1980) 32:1–46.
64. Packer RJ, Krailo M, Mehta M, Warren K, Allen J, Jakacki R, et al. Phase I study of concurrent RMP-7 and carboplatin with radiotherapy for children with newly diagnosed brainstem gliomas. *Cancer.* (2005) 104:1281–7. doi: 10.1002/cncr.21301
65. Kurzrock R, Gabrail N, Chandhasin C, Moulder S, Smith C, Brenner A, et al. Safety, pharmacokinetics, and activity of GRN1005, a novel conjugate of angiopep-2, a peptide facilitating brain penetration, and paclitaxel, in patients with advanced solid tumors. *Mol Cancer Ther.* (2012) 11:308–16. doi: 10.1158/1535-7163.MCT-11-0566
66. Cloughesy TF, Black KL, Gobin YP, Farahani K, Nelson G, Villablanca P, et al. Intra-arterial Cereport (RMP-7) and carboplatin: a dose escalation study for recurrent malignant gliomas. *Neurosurgery.* (1999) 44:270–8; discussion 8–9. doi: 10.1097/00006123-199902000-00015
67. Zoghbi GJ, Iskandrian AE. Selective adenosine agonists and myocardial perfusion imaging. *J Nucl Cardiol.* (2012) 19:126–41. doi: 10.1007/s12350-011-9474-9
68. Ashraf O, Patel NV, Hanft S, Danish SF. Laser-induced thermal therapy in neuro-Oncology: a review. *World Neurosurg.* (2018) 112:166–77. doi: 10.1016/j.wneu.2018.01.123
69. Chuang-Stein C, Kirby S, French J, Kowalski K, Marshall S, Smith MK, et al. A quantitative approach for making go/no-go decisions in drug development. *Drug Inform J.* (2011) 45:187–202. doi: 10.1177/009286151104500213
70. Mansouri A, Cooper B, Shin SM, Kondziolka D. Randomized controlled trials and neurosurgery: the ideal fit or should alternative methodologies be considered? *J Neurosurg.* (2016) 124:558–68. doi: 10.3171/2014.12.JNS142465
71. Blyth BJ, Farhavar A, Gee C, Hawthorn B, He H, Nayak A, et al. Validation of serum markers for blood-brain barrier disruption in traumatic brain injury. *J Neurotrauma.* (2009) 26:1497–507. doi: 10.1089/neu.2008.0738
72. Reiber H, Peter JB. Cerebrospinal fluid analysis: disease-related data patterns and evaluation programs. *J Neurol Sci.* (2001) 184:101–22. doi: 10.1016/S0022-510X(00)00501-3
73. Varatharaj A, Liljeroth M, Darekar A, Larsson HBW, Galea I, Cramer SP. Blood-brain barrier permeability measured using dynamic contrast-enhanced magnetic resonance imaging: a validation study. *J Physiol.* (2019) 597:699–709. doi: 10.1113/jp276887
74. Huang Y, Alkins R, Schwartz ML, Hynynen K. Opening the blood-brain barrier with MR imaging-guided focused ultrasound: preclinical testing on a trans-human skull porcine model. *Radiology.* (2017) 282:123–30. doi: 10.1148/radiol.2016152154
75. O'Reilly MA, Hynynen K. Blood-brain barrier: real-time feedback-controlled focused ultrasound disruption by using an acoustic emissions-based controller. *Radiology.* (2012) 263:96–106. doi: 10.1148/radiol.11111417
76. Woo SK, Jang SJ, Seo MJ, Park JH, Kim BS, Kim EJ, et al. Development of (64)Cu-NOTA-trastuzumab for HER2 targeting: a radiopharmaceutical with improved pharmacokinetics for human studies. *J Nucl Med.* (2019) 60:26–33. doi: 10.2967/jnumed.118.210294
77. Loryan I, Sinha V, Mackie C, Van Peer A, Drinkenburg WH, Vermeulen A, et al. Molecular properties determining unbound intracellular and extracellular brain exposure of CNS drug candidates. *Mol Pharm.* (2015) 12:520–32. doi: 10.1021/mp5005965
78. Levin VA, Ellingson BM. Understanding brain penetrance of anticancer drugs. *Neuro Oncol.* (2018) 20:589–96. doi: 10.1093/neuonc/nyo018
79. Levin VA, Tonge PJ, Gallo JM, Birtwistle MR, Dar AC, Iavarone A, et al. CNS anticancer drug discovery and development conference white paper. *Neuro Oncol.* (2015) 17(Suppl 6):vi1–26. doi: 10.1093/neuonc/nov169
80. Frewer P, Mitchell P, Watkins C, Matcham J. Decision-making in early clinical drug development. *Pharm Stat.* (2016) 15:255–63. doi: 10.1002/pst.1746

81. Ganju J. Improving the operational efficiency of Phase 2 and 3 trials. *Trials*. (2016) 17:332. doi: 10.1186/s13063-016-1465-3
82. Potter WZ. Optimizing early Go/No Go decisions in CNS drug development. *Expert Rev Clin Pharmacol*. (2015) 8:155–7. doi: 10.1586/17512433.2015.991715
83. Drapeau AI, Poirier MB, Madugundu GS, Wagner JR, Fortin D. Intra-arterial temozolomide, osmotic blood-brain barrier disruption and radiotherapy in a rat F89-glioma model. *Clin Cancer Drugs*. (2017) 4:135–44. doi: 10.2174/2212697X04666170727152212

Conflict of Interest: The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

Copyright © 2020 Karmur, Philteos, Abbasian, Zacharia, Lipsman, Levin, Grossman and Mansouri. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.