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Preclinical antibody-PET imaging of PD-L1

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Programmed cell death protein-1/ligand-1 (PD-1/PD-L1) blockade, including antibody therapeutics, has transformed cancer treatment. However, a major challenge in the field relates to selecting patients who are likely to respond to immune checkpoint inhibitors. Indeed, biopsy-based diagnostic tests to determine immune checkpoint protein levels do not accurately capture the inherent spatial and temporal heterogeneity of PD-L1 tumor expression. As a result, not all PD-L1-positive tumors respond to immunotherapies, and some patients with PD-L1-negative tumors have shown clinical benefits. In 2018, a first-in-human study of the clinically-approved anti-PD-L1 antibody Atezolizumab labeled with the positron emitter zirconium-89 validated the ability of positron emission tomography (PET) to visualize PD-L1 expression in vivo and predict tumor response to immunotherapy. These studies have triggered the expansion of PD-L1-targeted immunoPET to assess PD-L1 protein levels and PD-L1 expression heterogeneity in real time and across the whole tumor. First, this mini-review introduces new PD-L1 PET imaging studies of the last 4 years, focusing on the expansion of preclinical tumor models and anti-PD-L1 antibodies/antibody fragments in development. Then, the review discusses how these preclinical models and targeting agents can be utilized to study spatial and temporal heterogeneity of PD-L1 expression.

KEYWORDS

antibody-PET, PD-L1, immune checkpoint inhibition, preclinical PET imaging, heterogeneity

Introduction

Immune checkpoint inhibition is a mainstay in cancer treatment (1). The regulatory checkpoint pathway involving the programmed cell death protein 1 (PD-1) and its ligand programmed cell death ligand 1 (PD-L1) is a major mechanism for cancers to escape immune attack. This pathway includes PD-1 on T cells and PD-L1 on cancer cells and antigen-presenting cells. Cancer cells upregulate cell-surface PD-L1 levels to increase PD-1-mediated inhibitory signaling, and antibodies that target PD-L1 have shown impressive clinical outcomes for multiple cancers (1). At the time of this review, there are three clinically-approved antibodies specific for PD-L1: Atezolizumab, Avelumab, and Durvalumab (2, 3). In addition to being used as therapeutics, anti-PD-L1 antibodies labeled with positron emitters can be employed as companion diagnostics and allow

assessment of PD-L1 protein levels and therapeutic response in patients with cancer (4). For this mini-review, we focus on preclinical PD-L1-targeted immuno-positron emission tomography (PET) imaging reported in the last 4 years.

The expansion in PD-L1 immunoPET has been triggered by the ability of this non-invasive technology to provide information complementary to conventional methods of immunohistochemistry (IHC) used to identify patients that will likely benefit from PD-L1 immunotherapies. Indeed, the extensive heterogeneity of PD-L1 expression across the entire tumor volume results in inaccurate patient stratification when using minimal tissue biopsies for IHC (5–7). Immuno-PET has demonstrated great promise in determining protein levels and heterogeneity of immune checkpoint PD-L1 (2), which allows patient stratification, prediction and monitoring response to immune checkpoint inhibitors non-invasively across a patient's therapy regime.

In 2018, two landmark publications showed the feasibility and safety of radiolabelled agents targeted toward PD-L1 (8, 9) to non-invasively image its expression in human tumors and healthy tissues. For information on considerations for the development and use of PD-L1 tracers in the clinic and early preliminary work conducted prior to 2018, we refer the reader to other reviews (2, 3). Here, we concisely review preclinical PD-L1 PET imaging research, which has followed the landmark publications of 2018. We first discuss the expansion of preclinical PD-L1 imaging antibody and antibody-fragment based imaging agents, where an increasing number of models and targeting agents are being developed. We then describe studies illustrating the potential of preclinical molecular PD-L1 imaging to reveal PD-L1 biology, specifically discussing the use of preclinical imaging to monitor spatial and temporal heterogeneity of PD-L1 expression throughout tumor development and treatment regimes.

Expansion of preclinical PD-L1 molecular imaging

Since the first-in-human trials utilizing radiolabeled antibodies targeted toward PD-L1/PD-1 were reported (8, 9), clinical imaging [recently reviewed by Hegi-Johnson et al. (3)] of PD-L1 expression in human cancer has expanded. In the preclinical setting, the number of targeting agents and models used is increasing, demonstrating excellent specificity and imaging capabilities, and illustrating the potential of non-invasive *in vivo* PD-L1 molecular imaging across multiple cancer types. These preclinical studies are concisely outlined below and reported in Table 1.

Clinically-approved anti-PD-L1 antibodies

The combination of antibodies' specificity with the sensitivity of PET allows measurements of *in vivo* PD-L1 expression in both the laboratory and clinical settings. Since the publication of the first-in-human zirconium-89 (⁸⁹Zr)-labeled Atezolizumab study in 2018, radiolabeled Atezolizumab and Avelumab, which bind both human and mouse PD-L1, have been explored preclinically in different tumor models (Table 1).

Atezolizumab, an anti-PD-L1 antibody with a mutant Fc, showed accumulation in two independent clear cell renal carcinoma xenografts derived from the same patient (10) (4.2 \pm 0.6%ID/g and 5.2 \pm 0.4%ID/g, Table 1), which mimicked uptake values in a human lung cancer model (11) (3.97 \pm 1%ID/g, Table 1). In a syngeneic mouse model, melanoma tumors with high PD-L1 expression showed correspondingly higher Atezolizumab uptake in the tumor, compared to the aforementioned models (13.92 \pm 1.0%ID/g, Table 1).

Avelumab has been investigated in multiple independent breast cancer xenograft cohorts, showing tracer uptake of 6.1 \pm 1%ID/g (12) and 2.93 \pm 0.54%ID/g (13) (Table 1). In a dose escalation study by Jagoda et al. (13) co-injection of unlabeled Avelumab led to higher tumor uptake values with decreased uptake in other organs such as spleen. Blocking with unlabeled or "cold" antibodies is a method often used to limit off-target interactions with healthy organs that express PD-L1 and Fcgamma receptors. The importance of optimizing dose and timepoints of admnistration, the specific activity of radiolabeled antibodies, and the amount of labeled and unlabeled antibody to be injected to reduce off-target uptake while preserving tumor targeting are reviewed elsewhere (14, 15).

Studies using radiolabeled Durvalumab as an imaging agent have only recently begun, with the first clinical study published in 2022 (16) and others underway (14). Preclinical studies using Durvalumab as a PD-L1 imaging agent are limited (17) probably due to the fact that Durvalumab interacts exclusively with human PD-L1 and mouse models may be unable to recapitulate human biodistribution of the antibody.

Novel full-length anti-PD-L1 antibodies

In addition to the preclinical expansion of currently approved antibodies, novel full-length antibodies are being developed. In a comparative study of Atezolizumab and a newly developed C4 anti-PD-L1 antibody, Moroz et al. found that C4 distinguishes PD-L1 positive tumors while maintaining lower background in healthy organs than Atezolizumab in immunocompetent mice (tumor: 13.83 ± 0.5 C4 vs. 13.92 ± 1 Atezolizumab; liver: 7.33 ± 1.1 C4 vs. 6.79 ± 1.6 Atezolizumab;

	Antibody/label	Mice strain/cell line	Tumor accumulation (%ID/g)	Biodistribution	Reference
Full-Length	⁸⁹ Zr-DFO-C4	Athymic nu/nu,	⁸⁹ Zr-C4	⁸⁹ Zr-C4 in C57BL/6J	(11)
Antibodies	⁸⁹ Zr-DFO-	C57BL/6J.	B16 F10: 13.83 \pm 0.50	Liver: 7.33 ± 1.1	
	Atezolizumab	B16 F10 PD-L1 ^{high}	H1975: 7.08 \pm 0.8	Spleen: 6.05 ± 0.2	
		H1975 PD-L1 ^{moderate}	⁸⁹ Zr-Atezolizumab	Kidney: 2.76 \pm 0.8	
			B16 F10: 13.92 \pm 1.0	⁸⁹ Zr-atezolizumab in C57BL/6J	
			H1975: 3.97 ± 1.0	Liver: 6.79 ± 1.6	
				Spleen: 19.95 ± 1.5	
				Kidney: 6.71 ± 0.3	
	⁶⁴ Cu-NOTA-MX001	C57BL/6,	C57BL/6 mice bearing MC38	C57BL/6 mice bearing MC38	(24)
		BALB/c,	tumors, 48 h	tumors, 48 h	
		Nu/Nu.	15.06 ± 4.52	Liver: 12.35 ± 1.27	
		MC38 PD-L1 ^{high}		Spleen: 6.37 ± 0.48	
		BGC823 PD-L1 ^{high}		Kidney: 4.39 ± 1.13	
		4T1 PD-L1 ^{low}			
		U87MG PD-L1 ^{low}			
		[expression confirmed by FACs			
		and IHC]			
	⁸⁹ 7r-DEO-	NOD/SCID and	Day 6 post-injection	Tumor/muscle ratio: 4.4 ± 0.4	(10)
	Aterolizumah	notiont derived venograft of clear	Independent cohort 1:		(10)
	Atezolizulilab	coll ropol corringma (coPCC)	4.2 ± 0.6		
		[PD 11 arpressed in > 20% tumor	4.2 ± 0.0		
		[FD-LI expressed iii > 50% tuilioi			
	897a DEO Analumah	Nu (mu	5.2 ± 0.4	Limm D1 20.08 2.25	(12)
	21-DFO-Avelumad	NDA MB 221	Day 1 (D1) post-injection: 2.79	Liver: $D1-20.08 \pm 5.25$	(15)
		MDA-MB-231 xenografis	± 0.3	$D/-10.93 \pm 3.04$	
		[PD-L1 moderate by <i>in vitro</i>	D3 : 2.93 ± 0.54	Spleen: D1- 60.41 \pm 6.23	
		binding study]	D7: 2.44 ± 0.58	$D/-29.90\% \pm 7.58$	
				Kidney: D1-10.26 \pm 1	
				$D/-5.06 \pm 0.81$	
				Lymph nodes: D1-18.64 \pm 1.6	
	64			$D7-27.03 \pm 5.38$	()
	⁶⁴ Cu-NOTA-Anti-PD-	C57BL/6;	24 h post-injection >10%1D/g	Highest to lowest %ID/g at 24 h	(22)
	L1	murine pancreatic cells with		post-injection: Lymph node,	
		KRAS ^{G12D} mutation injected		spleen, liver, kidney	
		orthopically.			
	⁸⁹ Zr-CX-072	C57BL/6, BALB/c.	BALB/c mice bearing	BALB/c mice bearing	(19)
		MC38 PD-L1 ^{low} ,	MDA-MB-231 tumors,	MDA-MB-231 tumors,	
		MDA-MB-231 PD-L1 ^{high} .	accumulation in spleen at 6 days	accumulation in spleen at 6 days	
		[expression confirmed by flow	post-injection	post-injection:	
		cytometry]	10 µg	10 μg labeled: 25.8 \pm 4.1	
			labeled: 8.7 \pm 1;	$10~\mu g$ labeled $+~40~\mu g$	
			10 µg	unlabeled: 10.8 ± 2.8	
			$labeled + 40\mu g$	$10~\mu g$ labeled $+~240~\mu g$	
			unlabeled: 6.0 ± 1.3 ;	unlabeled: 5.3 ± 2.6	
			10 µg		
			labeled + 240 μ g		
			unlabeled: 4.3 ± 0.7		

TABLE 1 Preclinical imaging studies of antibody/fragment PET imaging agents for PD-L1 that have been reported in the last 4 years.

(Continued)

TABLE 1 Continued

Antibody/label	Mice strain/cell line	Tumor accumulation (%ID/g)	Biodistribution	Reference
⁸⁹ Zr-DFO-Avelumab	Nu/Nu MDA-MB-231 xenografts [PD-L1 expression validated by immunofluorescence and FACs]	48 h post-injection Targeting group: 6.1 ± 1.0 Pre-blocked group: 5.2 ± 1.0	At 48 h (unblocked) Spleen: 10.2 ± 0.7 Lymph nodes: 6.9 ± 1.0 At 48 h (blocking study) Spleen: 4.9 ± 0.5 Lymph nodes: 5.8 ± 1.1	(12)
⁸⁹ Zr-DFO-6E11	NMRI nude, BALB/c, C56BL/6. NSCLC lines (H1703- PD-L1 ^{low} , H1993- PD-L1 ^{moderate} , HCC827- PD-L1 ^{high}), CT26.WT- PD-L1 ^{high} , and B16F10- PD-L1 ^{high} [FACs, confirmed by IHC]	Mean tumor uptake, 72 h H1703: 1.35 ± 0.1 ; H1993: 2.32 ± 0.2 ; HCC827: 5.1 ± 0.6 ; CT26: 8.26 ± 0.6 ; B16F10: 10.78 ± 0.9 .	HCC827 in NMRI nude mice, HCC827 in NMRI nude mice, 144 h (unblocked) Liver: 7.99 ± 0.03 Spleen: 14.44 ± 3.1 Kidney: 2.11 ± 0.28 Tumor: 0.35 ± 0.04 Tumor/blood ratio: 9.01 ± 1.82 Tumor/muscle ratio: 1.25 ± 0.05	(21)
⁸⁹ Zr-DFO-anti-6E11	C57/BL6J KPC cells injected orthotopically into pancreas	At 72 h, vehicle: <5%ID/g At 72 h, ERKi: ~10%ID/g	Vehicle cohort (highest to lowest %ID/g): spleen, liver, lungs, blood/kidney, bone ERK inhibition cohort (highest to lowest %ID/g): spleen, liver, lungs, blood/kidney, bone	(20)
⁸⁹ Zr-DFO-REGN3504	SCID PD-1/PD-L1 humanized mice NCI-H441, MDA-MB-231, HCC827 [moderate PD-L1 expression by FACs and low by IHC)] MC-38 with CRISPR KO of mPD-L1 and engineered to express hPD-L1. All lines implanted into flank of mouse Primate model: cynomolgus monkey	NCI-H441: 52.3%ID/g HCC827: 38.7%ID/g MDA-MB231: 38.8%ID/g	Humanized mice, MC-38/hPD-L1 tumors, Vehicle cohort Spleen: 29.3 ± 1.8 Inguinal lymph nodes: 4.5 ± 8.0 Brachial lymph nodes: $28.8\% \pm$ 7.4 Clodronate treated Spleen: 8.9 ± 4.5 Inguinal lymph nodes: 24.5 ± 8.0 Brachial lymph nodes: 18.7 ± 3.9	(23)
¹²⁴ I -Durvalumab	Male SPF Balb/c nude A549 (PD-L1 ^{low}) and H460 (PD-L1 ^{high}) [PD-L1 expression validated by qPCR, western blot, flow cytometry, IHC]	48 h post-injection: 5.18 ± 0.73% ID/g	12 h post-injection:Blood: $22.01 \pm 1.34\%$ ID/gKidneys: $4.68 \pm 0.48\%$ ID/g48 h post-injection:Blood: $17.84 \pm 0.82\%$ ID/g72 h post-injection:Blood: $16.34\pm1.08\%$ ID/gTumor-to-liver ratio (after 12 h post-injection): >2	(17)

(Continued)

	Antibody/label	Mice strain/cell line	Tumor accumulation (%ID/g)	Biodistribution	Reference
Antibody	⁸⁹ Zr-DFO-KN035	BALB/c nude	24 h post-injection: 18.08 ± 2.34	In LN229 tumor bearing mice	(29)
Fragments		LN229 (PD-L1 ^{high} by IHC), A375	120 h post-injection: 4.66 ± 0.93	24 h post-injection	
		(engineered to express PD-L1)		Kidneys: 8.16 \pm 1.84	
				Liver: 7.36 ± 0.32	
				Spleen: 2.83 ± 0.41	
				Blood: 13.21 ± 1.86	
				Tumor:blood- 0.5 ± 0.05	
				Tumor:muscle- 5.64 ± 0.65	
				120 h post-injection	
				Kidney: 6.69 \pm 0.94	
				Liver: 5.69 ± 0.58	
				Spleen: 2.84 ± 0.76	
				Blood: 4.2 ± 0.36	
				Tumor/blood: 1.1 ± 0.12	
				Tumor/muscle: 7.7 \pm 1.37	
	⁶⁴ Cu-NOTA-anti-PD-	Athymic nude	n/a	Nude mice, in vivo 45 min	(26)
	L1 (Fab	C57BL/6		post-injection	
	conjugate)			BAT: 6.1 ± 2.1	
				Spleen: 12.0 ± 1.9	
				C57BL/6 mice, ex vivo 90 min	
				post-injection	
				Kidneys: 157 \pm 27	
				BAT: 4.5 ± 1.5	
				Spleen: 9.4 ± 3.9	
	⁶⁸ Ga-NOTA-Nb109	BALB/c nude	1 h post-injection	A375-hPD-L1 tumor bearing	(27)
		A375 (PD-L1 ^{low}), A375-hPD-L1	A375-hPD-L1:	mice, 1 h post-injection	
		(transfected, hPD-L1 ^{high}), MCF-7	5.0 ± 0.35	Kidneys: 33.66 ± 3.26	
		(PD-L1 ^{low})	MCF-7: 1.7 \pm 0.36	Liver: 1.11 ± 0.41	
			2 h post-injection	Remaining organs: <1.5%ID/g	
			A375-hPD-L1:	Tumor/blood: 5.48 \pm 0.12	
			4.05 ± 0.31	Tumor/muscle: 9.33 \pm 0.82	
			MCF-7: 1.46 \pm 0.34	2 h post-injection	
				Tumor/blood: 7.07 \pm 0.11	
				Tumor/muscle: 6.76 \pm 0.41	
	⁸⁹ Zr-Df-F(ab') ₂	C57BL/6	From graph, 2 h post-injection:	2 h post-injection:	(28)
		B16F10 PD-L1 ^{high} by flow	$\sim 4\%$ ID/g	Kidney: ~12%ID/g	
		cytometry		Liver: ~8%ID/g	
	¹²⁴ I -Durvalumab-	Male SPF Balb/c nude	12 h post-injection:	12 h post-injection:	(17)
	F(ab') ₂	A549 (PD-L1 ^{low}) and H460	$5.29\pm0.42\%~\text{ID/g}$	Blood: 15.41 \pm 1.49%ID/g	
		(PD-L1 ^{high})		Kidneys: 7.60 \pm 0.59% ID/g	
		[PD-L1 expression validated by		48 h post-injection:	
		qPCR, western blot, flow		Blood: 6.01 \pm 0.62% ID/g	
		cytometry, IHC]		72 h post-injection:	
				Blood: 5.07 \pm 0.29% ID/g	
				Tumor-to-liver ratio (after 4 h	
				post-injection): >2	

TABLE 1 Continued

⁸⁹Zr, Zirconium-89; ⁶⁴Cu, Copper-64; ⁶⁸Ga, Gallium-68; PD-L1, Programmed death-ligand 1; NOTA, 1,4,7-triazacyclononane-1,4,7-triacetic acid; DFO, Deferoxamine; ID, injected dose; BAT, brown adipose tissue.

spleen: 6.05 ± 0.2 C4 *vs.* 19.95 ± 1.5 Atezolizumab; kidney: 2.76 ± 0.8 C4 *vs.* 6.71 ± 0.3 %ID/g Atezolizumab, Table 1) (11, 18).

In other works, a protease-activatable antibody, CX-072, showed specific tumor targeting once activated by proteases in the tumor microenvironment (TME) (19). Here, uptake in breast tumor xenografts and spleen was 2.1-fold higher and 5.3-fold lower, respectively, when using the activatable antibody *vs.* control (non-activatable) antibody. The validation of CX-072 as an imaging agent for patients with solid tumors or lymphomas was further explored in the PROCLAIM-CX-072 clinical trial (NCT03013491) (19).

Other antibodies in development include the antibody clone 6E11 (Genentech), which has been investigated in mouse models of non-small cell lung cancer and pancreatic ductal adenocarcinoma (20, 21). In the pancreatic tumor model, high uptake was noted in the spleen and liver (\sim 3–4 fold higher *vs.* tumor), as well as blood and lungs (20) (Table 1). For abdominal tumors such as pancreatic tumors, co-injecting unlabeled antibody at a dose that reduces radiolabeled antibody accumulation in the spleen may facilitate tumor visualization (22). In the non-small cell lung cancer model, Christensen et al. (21) observed similar uptake of 6E11 in spleen, liver, and lungs, with notably lower 6E11 levels in blood. Co-injection of unlabeled 6E11 showed a decrease in 6E11 uptake in spleen and liver with an overall tumor uptake of 3.07 ± 0.15% ID/g.

Another antibody in development, REGN3504 (Regeneron), has been examined in breast and lung cancers, showing high tumor uptake (up to 50%ID/g, depending on tumor type, Table 1) as well as binding to spleen and lymph nodes (29.3 \pm 1.8%ID/g in spleen, 24.5 \pm 8.0%ID/g in inguinal lymph nodes, 28.8 \pm 7.4%ID/g in brachial lymph nodes, Table 1) (23). These novel antibodies demonstrate potential to monitor PD-L1 expression with high specificity across multiple tumor types (11, 19–24).

Anti-PD-L1 antibody fragments

In addition to full-length antibodies, smaller antibody fragments (~15-80 kDa) allow for accelerated targeting and clearance while retaining high PD-L1 specificity (25). To this point, several of the antibody fragments presented in Table 1 show tumor uptake within 2 h after antibody administration (26-28). High uptake is also observed in the kidneys (26-28), owing to the faster renal clearance of these small molecules compared to full-length antibodies. Furthermore, PET images of the single-domain antibody KN035 at 24 h post-injection demonstrated high tumor uptake in a human glioma murine model and lower accumulation in the kidneys compared to fragments imaged closer to the time of injection (Table 1) (29). KN035 is currently being investigated in numerous clinical trials from phase 1 to 3 and may be a promising fragment for clinical imaging setting (NCT04977128 and NCT03638804). Beyond

targeting the primary tumor region, a very recent study demonstrated the potential of iodine-124 labeled anti-PD-L1 fragments to offer good tumor-to-background contrast for visualizing metastases, with minimal radionuclide shedding to bone and tumor-to-liver ratios of 2 in non-small cell lung cancer (17).

Preclinical models of PD-L1 expressing tumors

In order to investigate the ability of PD-L1 antibodies and fragments to interact with human PD-L1 on human tumor cells, preclinical studies include PD-L1 overexpressing cell lines (27, 29). It should be noted that these overexpression models may not reflect clinical PD-L1 heterogeneity and protein levels and may overestimate the uptake of the anti-PD-L1 imaging agents in human tumors. To address this, Table 1 describes studies that have used multiple models in addition to those which overexpress PD-L1 to affirm the possibility of translatable imaging (29).

Preclinical research has also relied heavily on subcutaneous injection of human cancer cell lines into immunocompromised mice. While immunocompromised mice demonstrate tumorbinding ability and specificity, it is important to recognize that PD-L1 is also expressed on host cells, as well as in other murine tissues (30, 31). Additionally, PD-1, the co-inhibitory receptor to PD-L1, is highly expressed on T-cells which are absent in many of these immunocompromised models. Thus, the binding of PD-L1 antibodies/fragments to local and circulating immune cells, or other cells in the body, will need to be investigated further to ensure tumor targeting without excessive host background. In fact, PD-L1 expression is high in tumorassociated macrophages, and uptake of PD-L1 targeting agents by macrophages will also influence biodistribution and should be thoroughly characterized (32). To study the possible uptake of anti-PD-L1 antibody by murine macrophages, Kelly et al. (23) performed biodistribution studies in mice upon chemical depletion of macrophages. Clodronate-induced macrophage depletion decreased splenic and lymph node uptake, although uptake was still relatively high in these organs (8.9 \pm 4.5%ID/g in spleen and ~18.7–19%ID/g in lymph nodes, Table 1) without impacting tumor uptake. The same group demonstrated that anti-PD-L1 antibody accumulates in the spleen, lymph nodes, thymus, and liver of mice genetically humanized to express human PD-L1 and PD-1 (23). Interestingly, localization to spleen and lymph nodes occurs across immunocompromised and immunocompetent models used in the studies discussed here (Table 1), suggesting that immunocompromised models may still serve as useful tools when initially investigating PD-L1 imaging agents, perhaps due to a degree of functioning innate immunity. Nevertheless, the use of transgenic or syngeneic models alongside immunocompromised models where possible

may provide more realistic and clinically applicable settings for antibody/fragment analysis.

Revealing PD-L1 spatial and temporal heterogeneity with molecular imaging

The studies described thus far in this review demonstrate the ability to target PD-L1 with molecular imaging agents. Having shown that this is possible across multiple cancer types, animal models and with multiple radiolabeled targeting agents now available, this section draws on how non-invasive information of PD-L1 status can be utilized to reveal aspects of PD-L1 biology, particularly its inherent spatial and temporal heterogeneity.

Antibody-PET of PD-L1 heterogeneity

Heterogeneity of PD-L1 expression is widely observed in tumor specimens and is of clinical concern when considering PD-L1 protein levels as a biomarker to stratify patients for checkpoint inhibitor therapy (5-7). This heterogeneity is 2fold: spatial and temporal. Spatial heterogeneity of PD-L1 expression causes sampling bias in the clinic, as a small patient biopsy will not necessarily represent expression across the entire tumor tissue (33). Temporal heterogeneity of PD-L1 expression across disease progression and therapy regimes is also reported, with some tumors initially negative and then becoming positive for PD-L1 (34), which represents another clinical challenge as acquiring numerous patient biopsies is not always possible. Molecular imaging of PD-L1 across entire tumor volumes may provide a complementary tool to a clinical oncologist to non-invasively monitor both spatial and temporal heterogeneity. Importantly, the molecular mechanisms which give rise to this heterogeneity are not well described and are largely unknown. Additionally, while mechanisms of spatial and temporal heterogeneity are uncovered, visualizing and monitoring them accurately is limited with the current clinical standard of IHC and assays conducted on minimal tissue biopsies.

PD-L1 spatial heterogeneity

In the landmark Bensch et al. study, PD-L1 on IHC co-registered with autoradiography of radiolabeled antibody uptake, as these patients had previously undergone ⁸⁹Zr-Atezolizumab PET imaging (8). Similar studies were conducted preclinically in human breast tumor xenografts with the novel protease-activatable ⁸⁹Zr-CX-072 (19). In both studies, areas of high and low PD-L1 expression on IHC spatially correlated with uptake of radiolabeled antibody on autoradiography, helping to validate the molecular imaging agent.

A current challenge for mouse models of human cancer is accurate recapitulation of the TME, which may impede antibody delivery to the tumor. Cells within the TME, particularly other immune cells and stromal cells, as well as physical barriers such as fibrosis and vascular perfusion, may impact the ability of PD-L1 targeting agents to bind their antigen. Of the studies presented in Table 1, two utilized an immune-competent orthotopic pancreatic ductal adenocarcinoma (PDAC) LSL-Kras^{G12D/+};LSL-Trp53^{R172H/+};Pdx-1-Cre (KPC) model, to more accurately recapitulate the pancreatic TME (20, 22). In this model, the addition of an Erk inhibitor to increase PD-L1 levels significantly increased tumor uptake of the full-length antibody 6E11 (compared to vehicle treated control), suggesting Erk inhibition can prime the TME for PD-L1 targeted therapies (20). Additionally, a hypoxic TME is known to increase the expression of PD-L1 (35). Indeed, oncogenic pathways such as epidermal growth factor receptor signaling regulate PD-L1 expression (33), while chemo-, radio- and antibody-therapeutic regimes are reported to increase PD-L1 expression (34, 36). While many of the studies in Table 1 displayed inter-model heterogeneity in PD-L1 expression, they also showed intratumoral spatial heterogeneity across the entire tumor volumes in PET imaging (Figures 1A,B) (12, 21, 27, 29), and recent progress in computational approaches will be helpful to understand this complex heterogeneity of PD-L1 (37). While investigating PD-L1 heterogeneity preclinically, PD-L1 PET images could be spatially colocalized to large tissue areas processed ex vivo in IHC or similar methods, to co-register areas of high uptake with molecular expression.

While not discussed in this mini-review, PD1, the coinhibitory receptor of PD-L1, expressed on T-cells, is also a target of checkpoint inhibition and shows extreme spatial heterogeneity on IHC and in molecular imaging (9, 38). As the two are so heavily related, monitoring the expression of both PD1 and its ligand PD-L1 may prove useful in a clinical setting. We therefore direct the reader to the other reviews for further information on PD1 imaging (2, 14).

PD-L1 temporal heterogeneity

Temporal heterogeneity of PD-L1 expression could be explored with PD-L1 molecular imaging, particularly in preclinical studies that mimic clinical treatment regimes, with a view to translate these findings to clinical applications. So far, preclinical studies have largely focused on monitoring response to standard therapies, showing an increase in PD-L1 uptake and immune activation in response to radiotherapy and immunotherapy (21, 39, 40), corroborated by *ex vivo* IHC. The predictive value of PD-L1 PET imaging is also demonstrated by Christensen et al. (21) in a study showing that PD-L1 PET signal (expressed as maximum tumor to muscle ratios) following radiotherapy treatments negatively correlated with tumor volume increase. Where along the treatment pathway



PD-L1 PET would be most predictive or provide accurate measurement of response is currently unclear and could be explored in preclinical treatment regimes. Additionally, utilizing the non-invasive nature of molecular imaging to include multiple imaging time-points longitudinally would help to characterize temporal heterogeneity. Here, the potential role of antibody fragments labeled with short half-life radionuclides comes to the forefront, as their fast clearance and decay would enable multiple imaging time-points for the same tumor within a treatment period of a few months (Figure 1C) (25). Additionally, there are multiple small peptide fragments in development for PD-L1 imaging (14), a discussion of which was largely beyond the scope of this review. In this context, the fragment DK222 was able to determine PD-L1 availability at the cell surface, which could then be targeted with anti-PD-L1 antibody therapy. Target availability was shown to relate to tumor volume increase across the treatment period in breast and melanoma models (40). Both the predictive power and ability to monitor response to therapy of PD-L1 PET imaging will likely continue to be explored in the coming years (Figure 1C).

Discussion

Checkpoint inhibitor therapy has been heralded as a gamechanger to treat multiple solid tumors (1). While durable responses can be seen in many patients, response rate can be as low as 15% (1). Therefore, monitoring the expression of checkpoint inhibitor ligands such as PD-L1 is essential to stratify patients that will respond to these therapies as well as monitor response to treatment. Currently, PD-L1 protein levels are monitored by IHC in minimal *ex vivo* tissue biopsies. A disadvantage of measuring PD-L1 expression in tumor samples *via* IHC is that this can only be conducted on a small section of the tumor tissue taken during a single biopsy, disregarding the extensive spatial and temporal heterogeneity of PD-L1 that exists (33). Additionally, PD-L1 IHC diagnostic tests are often discordant, and range in their threshold of PD-L1 positivity (>1% or >50%) (41, 42). Indeed, many of the publications quoted in Table 1 are discordant in their classification of PD-L1 high and low tumors by IHC or *ex vivo* methods.

Molecular imaging of PD-L1 using radiolabeled antibodies or antibody fragments presents a non-invasive approach to visualize expression of PD-L1 across the entire tumor volume. Since the first-in-human studies of molecular imaging of PD-L1 were published in 2018 (8, 9), there has been an expansion in the number of targeting agents proposed and tested across multiple cancer types (Table 1). In this review, we outlined how novel agents and models have been tested preclinically, focusing on both antibodies and antibody fragments that are under development (Table 1). These studies demonstrated a range of tumor uptake values, as well as uptake in other lymphatic organs including the spleen and lymph nodes. Having demonstrated the ability to target PD-L1 expression in these models, these studies can inform human dosimetry as these imaging agents move toward the clinic. However, caution should be taken with the heavy-reliance thus far on immunocompromised models and PD-L1 overexpressing cell lines, and the use of syngeneic and transgenic models alongside these will provide more accurate modeling of biodistribution and the TME. We believe the current landscape of preclinical PD-L1 molecular imaging presents a useful platform for translational studies, with many targeting agents and animal models available for research.

We discussed how these preclinical models could be utilized to further explore PD-L1 spatial and temporal heterogeneity. Owing to the fact that molecular imaging captures the entire tumor volume and is non-invasive, we present PD-L1 molecular imaging as a possible complementary tool for a clinical oncologist to determine patient PD-L1 expression. From a preclinical perspective, molecular imaging would be utilized in determining the origins of spatial and temporal heterogeneity of PD-L1 expression. Imaging can be spatially colocalized with IHC (37) to determine whether origins are molecular, cellular or due to chemical/physical processes within the TME, while preclinical models can also be manipulated genetically or pharmacologically to determine how this changes the spatial and temporal expression of PD-L1 (20, 34). Overall, PD-L1 molecular imaging is expanding and holds immense potential to reveal multiple aspects of PD-L1 spatial and temporal heterogeneity, both preclinically and in patient imaging.

Author contributions

ELB collected and reviewed the literature, prepared Figure 1, assisted with compiling Table 1, and contributed to the writing of the manuscript. RAD and AZ contributed to writing parts of this mini-review, and compiled Table 1. PMRP conceived and structured the mini-review, assisted with collecting literature, and drafted the final version of the manuscript. All authors contributed to the article and approved the submitted version.

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Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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