



# Brain state-dependent abnormal LFP activity in the auditory cortex of a schizophrenia mouse model

Kazuhiro Nakao<sup>1,2</sup> and Kazu Nakazawa<sup>1,2\*</sup>

<sup>1</sup> Department of Psychiatry and Behavioral Neurobiology, University of Alabama at Birmingham, Birmingham, AL, USA

<sup>2</sup> Unit on Genetics of Cognition and Behavior, Department of Health and Human Services, National Institute of Mental Health, National Institutes of Health, Bethesda, MD, USA

## Edited by:

Yukiko Kikuchi, Newcastle University Medical School, UK

## Reviewed by:

Piia Astikainen, University of Jyväskylä, Finland

Huan Luo, Chinese Academy of Sciences, China

## \*Correspondence:

Kazu Nakazawa, Department of Psychiatry and Behavioral Neurobiology, University of Alabama at Birmingham, Shelby Building 1105, 1825 University Boulevard, Birmingham, AL 35294, USA  
e-mail: nakazawk@uab.edu

In schizophrenia, evoked 40-Hz auditory steady-state responses (ASSRs) are impaired, which reflects the sensory deficits in this disorder, and baseline spontaneous oscillatory activity also appears to be abnormal. It has been debated whether the evoked ASSR impairments are due to the possible increase in baseline power. GABAergic interneuron-specific NMDA receptor (NMDAR) hypofunction mutant mice mimic some behavioral and pathophysiological aspects of schizophrenia. To determine the presence and extent of sensory deficits in these mutant mice, we recorded spontaneous local field potential (LFP) activity and its click-train evoked ASSRs from primary auditory cortex of awake, head-restrained mice. Baseline spontaneous LFP power in the pre-stimulus period before application of the first click trains was augmented at a wide range of frequencies. However, when repetitive ASSR stimuli were presented every 20 s, averaged spontaneous LFP power amplitudes during the inter-ASSR stimulus intervals in the mutant mice became indistinguishable from the levels of control mice. Nonetheless, the evoked 40-Hz ASSR power and their phase locking to click trains were robustly impaired in the mutants, although the evoked 20-Hz ASSRs were also somewhat diminished. These results suggested that NMDAR hypofunction in cortical GABAergic neurons confers two brain state-dependent LFP abnormalities in the auditory cortex; (1) a broadband increase in spontaneous LFP power in the absence of external inputs, and (2) a robust deficit in the evoked ASSR power and its phase-locking despite of normal baseline LFP power magnitude during the repetitive auditory stimuli. The “paradoxically” high spontaneous LFP activity of the primary auditory cortex in the absence of external stimuli may possibly contribute to the emergence of schizophrenia-related aberrant auditory perception.

**Keywords:** auditory steady-state responses, GABAergic interneurons, gamma oscillation, local field potentials, NMDA receptors, parvalbumin, schizophrenia, mouse models

## INTRODUCTION

Neural oscillation and synchronization abnormalities have been suggested to play a role in the information and sensory processing deficits commonly seen in schizophrenia (Ford and Mathalon, 2008; Uhlhaas and Singer, 2010; Gandal et al., 2012a). Periodic auditory stimulation entrains the electro-encephalogram (EEG) to a specific phase and frequency, often referred to as the auditory steady-state response (ASSR). In both human and animal models, the ASSR has been used to assess the functional integrity of neural circuits that support synchronization (Picton et al., 2003; Brenner et al., 2009; O'Donnell et al., 2013). In schizophrenia, reduced ASSR power (magnitude) and phase locking (phase consistency across trials), particularly at 40 Hz, are observed in EEG (Kwon et al., 1999; Brenner et al., 2003; Light et al., 2006; Spencer et al., 2008, 2009; Vierling-Claassen et al., 2008; Krishnan et al., 2009) as well as in magneto-encephalogram (MEG) (Teale et al., 2008; Maharajh et al., 2010; Tsuchimoto et al., 2011) studies. Since cortical parvalbumin (PV)-positive fast-spiking interneurons have an intrinsic resonance near this range (Tateno et al., 2004; Golomb et al., 2007), the reduction in 40-Hz ASSRs

may reflect functional deficits of these fast-spiking neurons in schizophrenia.

Earlier studies of gamma synchrony deficits in schizophrenia reported the *relative* changes in gamma band activity in response to task stimuli, by assessing stimulus-evoked responses in synchrony compared with a pre-stimulus baseline (Kwon et al., 1999; Haig et al., 2000; Lee et al., 2003). Thus, in these studies *relatively* less evoked gamma synchrony could be a reflection of greater baseline spontaneous gamma phase synchrony under pre-stimulus conditions. However, in schizophrenia the evidence regarding baseline gamma activity abnormalities is inconsistent. Both increases (Jalili et al., 2007; Venables et al., 2009; Kikuchi et al., 2011; Spencer, 2012) and decreases (Yeragani et al., 2006; Rutter et al., 2009) in *baseline* spontaneous gamma power during pre-stimulus period or “resting state” have been reported. The reason for these contradictory results has yet to be clarified.

To measure the baseline spontaneous gamma band power with high precision, it would be useful to directly record local field potentials (LFPs), necessitating the use of animal models. To that end, we recorded LFPs directly from the primary auditory

(A1) cortex of GABAergic interneuron-specific NMDA receptor (NMDAR) hypofunction mice (*Ppp1r2-cre/fGluN1* KO mice). Previous studies using this mutant mouse revealed that the selective deletion of GluN1, an indispensable subunit of NMDARs, in cortical and hippocampal interneurons during early postnatal development recapitulates several schizophrenia-like behavioral and pathophysiological phenotypes (Belforte et al., 2010; Jiang et al., 2013). In the present study, we subjected these mutant mice to the ASSR paradigm, similar to the one used in human studies (Krishnan et al., 2009). We assessed the auditory click train-evoked ASSRs and baseline LFP fluctuations in pre/post-stimulus period and at baseline (i.e., between stimulus presentations).

## MATERIALS AND METHODS

All experimental procedures were in accordance with National Research Council guidelines for the care and use of laboratory animals, and were approved by the National Institute of Mental Health Animal Care and Use Committee. Data analysis was conducted at the University of Alabama at Birmingham.

### ANIMAL

*Ppp1r2-cre*<sup>(+/-)</sup>/*fGluN1*<sup>(f/f)</sup> mice (henceforth referred to as KO mice or mutants) were generated as previously described (Belforte et al., 2010). Briefly, the protein phosphatase 1, regulatory subunit 2 (*Ppp1r2*)-*cre* line and a floxed-GluN1 (*fGluN1*) line were used to delete exons 9 and 10 of GluN1 gene from the postnatal second week in a subset of cortical and hippocampal *Ppp1r2-cre* positive interneurons, the majority of which are PV-positive. Female mutant mice were bred to homozygously *fGluN1* male mice to generate the same mutant and *fGluN1* control mice with a 50% probability. In the present study, 65 male mice received chronic survival surgery for the microwire array implantation. After successful detection of the auditory-evoked potentials 1 week after the surgery, 7 *fGluN1* control (13–16 week-old,  $30.6 \pm 0.65$  g body weight) and 6 mutant (12–14 week-old,  $28.1 \pm 0.8$  g) mice were subjected to in-depth analysis of ASSRs, as described in Result section.

### SURGICAL PROCEDURES

Animals were anesthetized with isoflurane to surgical levels and were mounted in a stereotaxic instrument with non-rupture ear bars (Zygonia ear cups, David Kopf Instruments). A custom-made plastic headpost was secured to the occipital bone at the midline with superglue and dental acrylic, and was used to fix the animal's skull to the stereotaxic instrument. This was done to prevent physical occlusion of the external ear canals by stereotaxic ear bars in order to obtain tone-evoked LFP responses. A unilateral craniotomy was made over the right temporal bone from 1.5 to 3.5 mm posterior to bregma and from 3.5 to 4.5 mm lateral to midline. The vasculature was inspected. The microwire multi-electrode array consisted of six tetrodes, which were custom-configured in a  $2 \times 3$  matrix with inter-electrode distance of  $\sim 200 \mu\text{m}$ , covering  $0.6 \times 0.8 \text{ mm}^2$ . The impedance of each electrode was between 0.2 and 0.3 M $\Omega$ . The microwire array was inserted into the superficial layers of A1 cortex with the aid of cortical vascular patterns, and two stainless steel screws in the frontal cortex which served as ground and reference electrodes. After the

dosage of isoflurane was reduced to 1%, a single white noise pulse (1 ms, duration; 80 dB, SPL) was applied to activate the A1 cortical area. In order to allow for the tone-evoked responses it is critical to maintain the isoflurane concentration at 1% (Santarelli et al., 2003). The animal was held in place with adhesive tape to prevent head twitching or grooming. An analgesia (buprenorphine, 0.1 mg/kg *s.c.*) was given to diminish pain sensation during the surgery. If single-tone evoked potentials (over 0.1 mV magnitude) were detected in at least one electrode of the microwire array, the electrodes were inserted further until maximal responses were obtained. The anesthetic dose was then returned back to surgical levels, and the microwire array was fixed to the skull with dental acrylic.

### IN VIVO RECORDING

Seven days after surgery, LFP recording was performed from A1 cortex of awake, head-restrained mice. The mice were briefly anesthetized with 1% isoflurane to hold the animal head fixed to the stereotaxic instrument using the headpost, and the body was covered with adhesive paper tape to limit body movements. The micro-array electrodes were directly connected, via an EIB-27-Micro headstage pre-amplifier, to a Cheetah-64 recording system (Neuralynx Inc.), where LFP signals were filtered (bandwidth from 0.1 to 475 Hz), digitized, and acquired at a sampling rate of 1.56 kHz per channel. Thirty minutes after the cessation of anesthesia, LFP recording began from A1 cortex of awake, head-restrained mice in a custom-made auditory isolation chamber (background sound level, 40 dB SPL).

In the first session, spontaneous LFP activity during a pre-stimulus period was recorded from A1 cortex for 2–25 min. Subsequently, in the second session, 500-ms long click trains consisting of 80 dB white-noise pulses presented at 40 Hz (40-Hz ASSR stimuli) were applied 50 times with an inter-stimulus interval of 20 s, which mimics the ASSR protocol used in human studies (Krishnan et al., 2009). Auditory click stimuli, consisting of white noise pulses (1 ms, duration; 80 dB, SPL), were generated in Labview (National Instruments Inc.), and presented using a speaker with a 35 Hz–20 kHz frequency response (Z3, Logitech Inc.) placed 30 cm above the mouse head. In the third session, which began 10 min after cessation of the second session, 1000-ms long click trains consisting of 80 dB white-noise presented at 20 Hz (20-Hz ASSR stimuli) were applied 50 times with an inter-stimulus interval of 20 s. In the last session, spontaneous LFP activity was recorded for 25 min as a post-stimulus period. When no auditory evoked LFP responses were detected in any channels during the second session, the experiment was terminated and the animal was euthanized.

### LFP ANALYSIS

Only the channel data in which the amplitude of initial N1 response in the 40 Hz-ASSRs was more than 0.1 mV ( $\sim 4$  times the standard deviation), were used for subsequent analyses. Neuralynx LFP files were first converted to Spike2 format to visually inspect the raw data. Next, LFP voltage values in the Neuralynx files were converted to Matlab (Mathworks) files, and these values were normalized to the z-scores by subtracting the mean and dividing by the standard deviation of the LFP

voltages during entire recording epoch (~20 min). The Matlab files with the z-scores were then converted to NeuroExplorer (Nex Technologies) files to calculate the power.

In order to assess the oscillatory component of evoked ASSRs, z-score normalized LFPs during the last 200-ms of each ASSR were analyzed with a fast Fourier transform (FFT) algorithm in the range of 0–100 Hz using 256 frequency bins and presented as total ASSR power (e.g., **Figure 1C**). Relative power amplitudes were calculated by subtracting a baseline spontaneous power, which was from the 200-ms inter-stimulus segment 10 s prior to each click-train onset, from the total ASSR power (see **Figure 1E**).

For spontaneous LFP power during a pre-stimulus period, LFP data (200-ms bin) during the last 10 s prior to the first click-train administration were analyzed with FFT algorithm in the range of 0–200 Hz using 256 frequency bins (**Figure 3**). To compare the baseline power magnitudes in-between ASSR sessions with the spontaneous power during the pre- or post-stimulus period, z-score normalized LFP from 5 to 15 s (200-ms bin) after 1st stimuli, 25th stimuli, and 50th stimuli were analyzed with FFT algorithm in the range of 0–100 Hz using 256 frequency bins. For the pre-stimulus period, the baseline spontaneous power during last 10 s before click train onset was analyzed in the range of 0–100 Hz using 256 frequency bins. For power spectral analysis during the post-stimulus period, LFP data obtained from a 10-s period (200-ms bin) 20 min after the cessation of all ASSR stimuli were analyzed with FFT algorithm in the range of 0–100 Hz using 256 frequency bins (see **Figure 4A**).

To calculate phase locking to auditory click- trains, phase locking was performed in a frequency range 0–100 Hz with a 60% overlapping window after applying Hanning tapering of normalized LFP data, which was further analyzed with FFT algorithm. To plot a scalogram (wavelet spectrogram), Matlab z-score files of LFP were wavelet transformed using a Complex Gaussian wavelet from Matlab wavelet toolbox.

## STATISTICS

Given that between-animal variability may be larger than within-animal variability in per-channel (i.e., per electrode) design, we mainly presented the data with per-animal design in the Figures and some data with per-channel design in the Supplemental Figures (see Lasic and Essioux, 2013). Differences between groups were assessed for normally distributed data using a Student's *t*-test (Statcel 2nd ed., OMS, Tokyo, Japan). The effect size was assessed as Cohen's *d*. For the graph data in **Figures 4, 5**, differences were assessed by repeated measures of ANOVAs followed by Bonferroni *post-hoc* analysis (SPSS, IBM). Data were presented as mean ± s.e.m.

## RESULTS

### ROBUST REDUCTION OF 40-Hz AUDITORY STEADY-STATE RESPONSES (ASSRs)

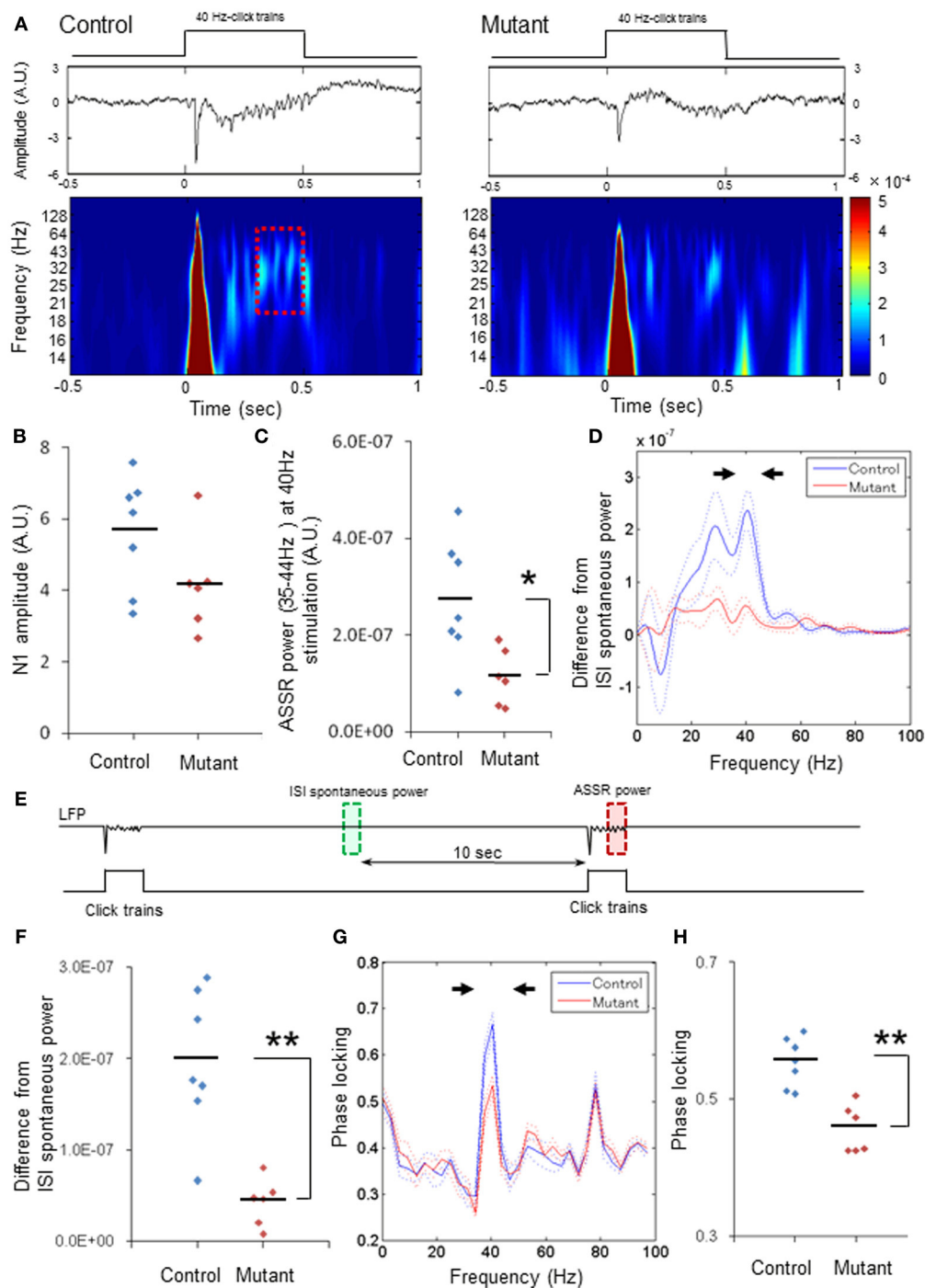
Seven days after surgery, 40-Hz click train-evoked initial N1 responses (i.e., the transient auditory evoked potentials to click train onset, more than 0.1 mV) were detected in A1 cortex from 13 mice (7 fGluN1 control and 6 mutant mice), out of a total of 65 animals in which the click-train-evoked responses had been detected during the electrode implantation surgery. The relative

high number of animals that displayed no evoked LFPs was mostly likely to be due to a shift of or damage to the electrode microarray placed on the temporal bone. Thirty-one LFP recordings from 7 control mice [animal #1: 2 (number of recording sites to be analyzed)/6 (total channel number), #2: 6/6, #3: 3/6, #4: 6/6, #5: 6/6, #6: 3/6, #7: 5/6], and 26 LFP recordings from 6 mutant mice (animal #1: 5/6, #2: 4/6, #3: 6/6, #4: 5/6, #5: 3/6, #6: 3/6) were subjected to subsequent LFP in-depth analysis.

Fifty 40-Hz click trains (duration, 500 ms) were delivered to click train-naïve animals with an inter-stimulus interval of 20 s. **Figure 1A** depicts representative examples of the averaged ASSRs (middle) and scalogram (wavelet spectrogram, bottom) evoked by 40 Hz stimulation (upper) in the floxed-control (left) and mutant mouse (right). Robust click train-evoked N1 potentials were elicited within the first 100 ms after click-train onset in both genotypes, and there were no differences in the averaged N1 amplitudes between genotypes per animal (**Figure 1B**). However, the N1 amplitudes averaged per channel were lower in the mutants compared to the floxed-control mice ( $p < 0.05$ , Student's *t*-test, Supplemental Figure 1A). To assess the subsequent ASSRs coherent to the 40-Hz click trains without any impact of evoked N1 potentials on the steady-state responses, LFP data (z-score) during last 200 ms before click-train cessation (a dashed line period in **Figure 1A**) were analyzed with an FFT algorithm. We found that the amplitudes of 40-Hz ASSRs were smaller in the mutants compared to the controls per animal [**Figure 1C**,  $t_{(11)} = 2.8$ ,  $p < 0.05$ , Cohen's  $d = 1.60$  (large effect size)] and per channel [Supplemental Figure 1B,  $t_{(55)} = 5.23$ ,  $p < 0.01$ ,  $d = 1.43$  (large effect size)]. Difference in evoked ASSR power from baseline spontaneous power during inter-stimulus intervals, which were obtained by subtracting the spontaneous power amplitudes in-between ASSR stimuli from total ASSR power (**Figure 1E**), also peaked at 40 Hz and, to the lesser degree, at 30 Hz in the controls. Conversely, only small differences were detected in the mutant mice (**Figure 1D** and Supplemental Figure 1C). **Figure 1F** and Supplemental Figure 1D showed power spectrum density difference from the baseline at 35–44 Hz for each animal [ $n = 7$  controls,  $n = 6$  mutants,  $t_{(11)} = 4.57$ ,  $p < 0.01$ ,  $d = 2.64$  (large effect size)] and for each channel [ $n = 31$  sites from 7 controls,  $n = 26$  sites from 6 mutants,  $t_{(55)} = 7.79$ ,  $p < 0.01$ ,  $d = 2.14$  (large effect size)], indicating that average low gamma power for the evoked ASSRs was lower in the mutants compared to the controls. In addition, phase locking analysis of the 40-Hz ASSRs (z-score) revealed two peaks at 40 Hz (35–44 Hz) and at 80 Hz (75–84 Hz) for both controls and mutants (**Figure 1G**), but only phase locking at 40 Hz in the mutants was lower in comparison to controls for each animal [**Figure 1H**,  $t_{(11)} = 4.93$ ,  $p < 0.01$ ,  $d = 2.75$  (large effect size)] and for each channel [Supplemental Figure 1E,  $t_{(55)} = 9.42$ ,  $p < 0.01$ ,  $d = 2.47$  (large effect size)]. These findings suggest that mutants are severely impaired in 40-Hz ASSR for both amplitude and phase locking, both of which are reminiscent of ASSR deficits in schizophrenia patients.

### DIMINISHED 20-Hz ASSR POWER AND PHASE-LOCKING

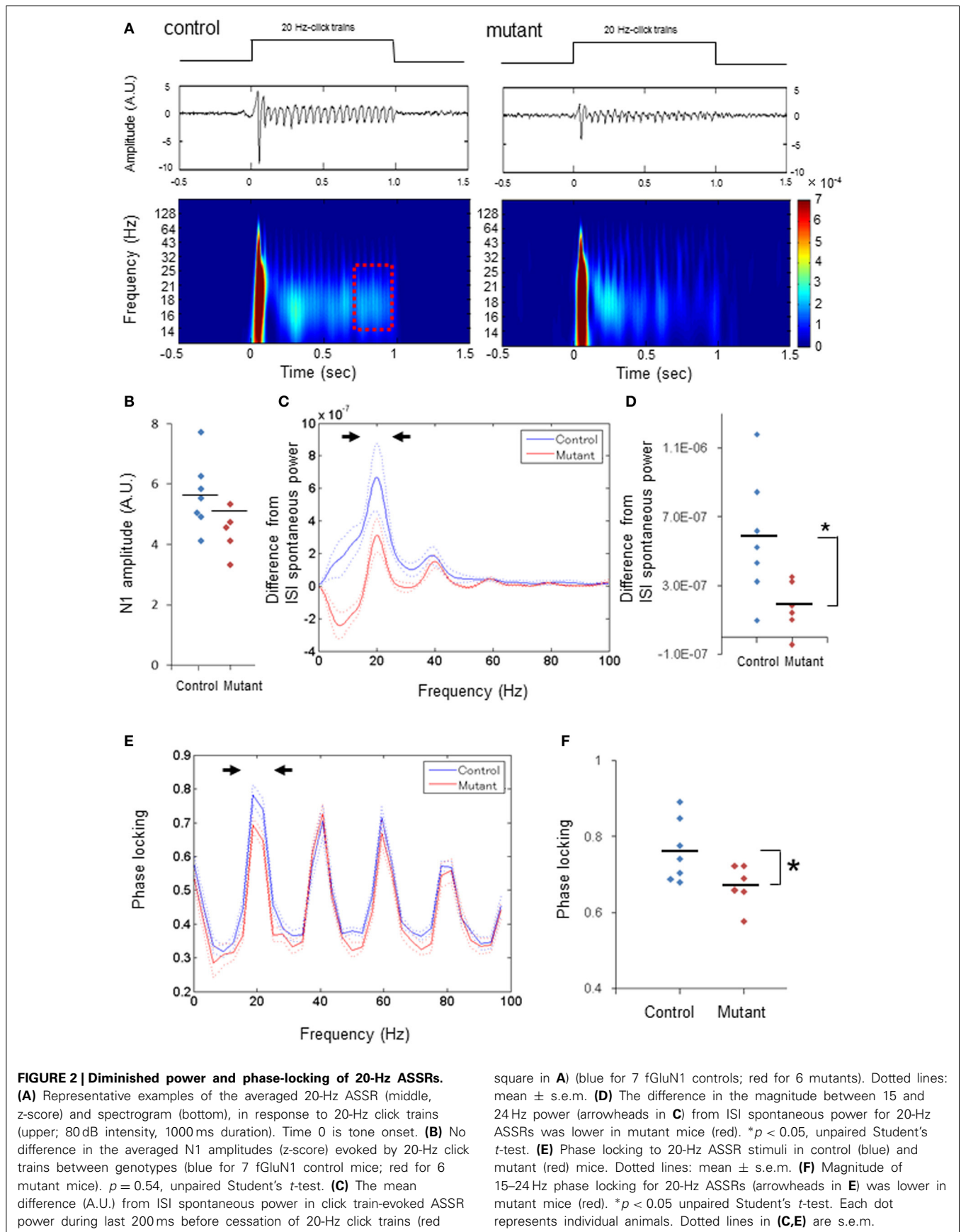
We next examined 20-Hz ASSRs (duration, 1000 ms) to explore whether ASSR deficits are specific to 40-Hz stimuli. **Figure 2A**



**FIGURE 1 | Robust reduction in power and phase-locking of 40-Hz ASSRs.**

(A) Representative examples of the averaged 40-Hz ASSR (middle, z-score) and spectrogram (bottom) in response to 40-Hz click trains (upper; 80 dB intensity, 500 ms duration). Time 0 is tone onset. (B) No difference in the averaged N1 amplitudes (z-score) evoked by 40-Hz click trains between genotypes (blue for 7 fGluN1 control mice; red for 6 mutant mice).  $p = 0.11$ , unpaired Student's  $t$ -test (C) Evoked ASSR power (z-score) at 35–44 Hz frequency range during 40-Hz click train stimulation in mutants (red) was lower than controls (blue).  $*p < 0.05$ , unpaired Student's  $t$ -test. (D) The mean difference (A.U.) from baseline spontaneous power during inter-stimulus interval (ISIs; green square in Panel E) in click train-evoked ASSR power during last 200 ms before cessation of 40-Hz click trains (red square in Panels A, E). Dotted lines: mean  $\pm$  s.e.m. (E)

Schematic diagram indicates the analysis periods of baseline LFP power (green, ISI spontaneous power) and the evoked ASSR power (red). Relative ASSR power amplitudes shown in Panel (D) were calculated by subtracting an ISI power (in green) from the evoked ASSR power (in red) for each channel, and averaged per animal. (F) The difference in the magnitude between 35 and 44 Hz spectral power (arrowheads in Panel D) and the baseline for 40-Hz ASSRs in mutants (red) was lower than controls (blue).  $**p < 0.01$ , unpaired Student's  $t$ -test. (G) Phase locking to 40-Hz steady-state tone stimuli in control (blue) and mutant (red) mice. Dotted lines: mean  $\pm$  s.e.m. (H) Magnitude of 35–44 Hz phase locking for 40-Hz ASSRs (arrowheads in Panel G) in mutants (red) was lower than controls (blue).  $**p < 0.01$ , unpaired Student's  $t$ -test. Each dot represents individual animals. Dotted lines in Panels (D, G) are s.e.m.



**FIGURE 2 | Diminished power and phase-locking of 20-Hz ASSRs.**

**(A)** Representative examples of the averaged 20-Hz ASSR (middle, z-score) and spectrogram (bottom), in response to 20-Hz click trains (upper; 80 dB intensity, 1000 ms duration). Time 0 is tone onset. **(B)** No difference in the averaged N1 amplitudes (z-score) evoked by 20-Hz click trains between genotypes (blue for 7 fGluN1 control mice; red for 6 mutant mice).  $p = 0.54$ , unpaired Student's  $t$ -test. **(C)** The mean difference (A.U.) from ISI spontaneous power in click train-evoked ASSR power during last 200 ms before cessation of 20-Hz click trains (red

square in **A**) (blue for 7 fGluN1 controls; red for 6 mutants). Dotted lines: mean  $\pm$  s.e.m. **(D)** The difference in the magnitude between 15 and 24 Hz power (arrowheads in **C**) from ISI spontaneous power for 20-Hz ASSRs was lower in mutant mice (red).  $*p < 0.05$ , unpaired Student's  $t$ -test. **(E)** Phase locking to 20-Hz ASSR stimuli in control (blue) and mutant (red) mice. Dotted lines: mean  $\pm$  s.e.m. **(F)** Magnitude of 15–24 Hz phase locking for 20-Hz ASSRs (arrowheads in **E**) was lower in mutant mice (red).  $*p < 0.05$  unpaired Student's  $t$ -test. Each dot represents individual animals. Dotted lines in **(C,E)** are s.e.m.

depicts a representative example of the averaged evoked potentials (middle) and spectrogram (bottom) evoked by 20-Hz click trains (upper) in control (left) and mutant mice (right). First, we found no difference in the averaged N1 amplitudes between genotypes analyzed per animal (**Figure 2B**) or analyzed per channel (Supplemental Figure 2A). The difference in the evoked ASSR power, which were obtained by subtracting the spontaneous power amplitudes in between ASSR stimuli from the total ASSR power during last 200 ms before cessation of click-trains (dashed period in **Figure 2A**), also peaked at 20 Hz with a smaller peak at the 40 Hz harmonic in both genotypes (**Figure 2C** and Supplemental Figure 2B). However, the relative power of the dominant peak at 20 Hz (15–24 Hz) was lower in the mutants compared to controls per animal [**Figure 2D**,  $t_{(11)} = 2.59$ ,  $p < 0.05$ ,  $d = 1.47$  (large effect size)] and in per-channel design [Supplemental Figure 2C,  $t_{(55)} = 4.58$ ,  $p < 0.01$ ,  $d = 1.25$  (large effect size)]. Furthermore, phase locking of the 20-Hz ASSR consisted of a dominant peak at 20 Hz with several spectral peaks at harmonics of 20 Hz (**Figure 2E** and Supplemental Figure 2D). The dominant peak of phase locking factor at 15–24 Hz in the mutants was lower than the controls analyzed per animal [**Figure 2F**,  $t_{(11)} = 2.29$ ,  $p < 0.05$ ,  $d = 1.3$  (large effect size)] and analyzed per channel [Supplemental Figure 2E,  $t_{(55)} = 3.77$ ,  $p < 0.01$ ,  $d = 1.01$  (large effect size)], but other spectral peaks in the mutants were similar to those in controls per animal ( $p = 0.63$  for 35–44 Hz,  $p = 0.37$  for 55–64 Hz,  $p = 0.40$  for 75–84 Hz, unpaired Student's *t*-test) and per channel ( $p = 0.44$  for 35–44 Hz,  $p = 0.27$  for 55–64 Hz,  $p = 0.50$  for 75–84 Hz, unpaired Student's *t*-test). These results indicate both ASSR and phase-locking evoked by 20-Hz ASSR stimuli are also diminished in the mutant mice, while the magnitudes of auditory-evoked potentials triggered by 20-Hz stimuli are largely unaffected.

### ENHANCED SPONTANEOUS LFP POWER IN AWAKE QUIESCENT PERIOD

To systematically explore the levels of spontaneous power throughout the periods of inter-ASSR stimulus intervals and the post-ASSR period, we further assessed the transition of spontaneous LFP power (z-score) from the pre-stimulus period to the inter-stimulus periods post to the first, 25th and 50th 40-Hz click-train administration, and the post-stimulus period 20 min after the cessation of last (50th) 40-Hz click-train (**Figure 3A**). First, we assessed the power spectra of z-score normalized LFPs during the pre-stimulus period from awake head-restrained animals. We found that baseline spontaneous power during the last 10-s pre-stimulus period prior to the first click-train administration was augmented in the mutants compared to the controls regardless of the spectral frequency found in both per-animal (**Figure 3B**) and per-channel (Supplemental Figure 3A) design. The intensities of averaged power for baseline LFPs at low gamma (30–50 Hz) and high gamma (50–100 Hz) range were both higher in the mutant mice compared to the controls per animal [**Figure 3C**,  $t_{(11)} = 3.00$ ,  $p < 0.01$ ,  $d = 1.67$  for low gamma;  $t_{(11)} = 3.13$ ,  $p < 0.01$ ,  $d = 1.74$  for high gamma] and per channel [Supplemental Figure 3B,  $t_{(55)} = 6.41$ ,  $p < 0.01$ ,  $d = 1.66$  for low gamma;  $t_{(55)} = 5.56$ ,  $p < 0.01$ ,  $d = 1.46$  for high gamma]. This elevation of LFP fluctuation continued even at super gamma frequency (100–120 Hz) per animal [ $t_{(11)} = 2.41$ ,  $p < 0.05$ ,  $d = 1.33$  (large effect size)]

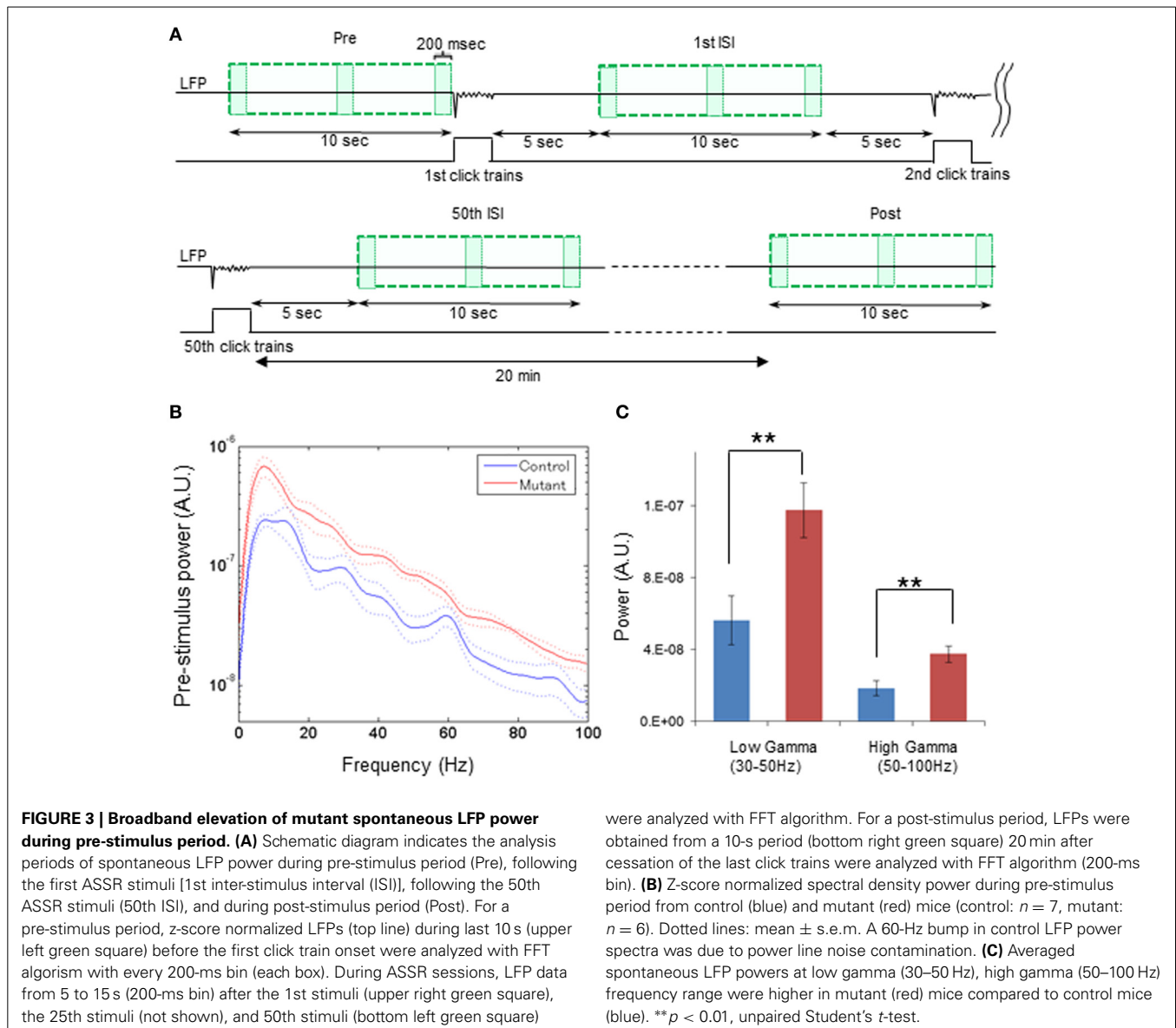
and per channel [ $t_{(55)} = 4.68$ ,  $p < 0.01$ ,  $d = 1.24$  (large effect size)], suggesting a broadband LFP power increase in the mutant animals during the awake quiescent period.

### SPONTANEOUS LFP POWER RETURNS BACK TO NORMAL UPON ASSR STIMULI

After the 40-Hz ASSR session began, we found a clear trend of a gradual reduction in mutant spontaneous LFP power amplitudes during inter-stimulus intervals with the increasing number of ASSR stimuli (**Figures 4A–C**, **5A–C**). For example, spontaneous LFP power per animal was reduced in the inter-stimulus period following the 25th ASSRs, compared to the pre-ASSR period at 35–44 Hz [**Figure 4B**,  $F_{(1, 11)} = 1.389$ ,  $p = 0.263$  for genotype, Bonferroni *post-hoc* test,  $p < 0.05$ ]. In per-channel design, spontaneous LFP power at 21–30 Hz [**Figure 5A**,  $F_{(1, 54)} = 1.326$ ,  $p = 0.255$  for genotype, Bonferroni *post-hoc* test,  $p < 0.05$ ], 35–44 Hz [**Figure 5B**,  $F_{(1, 54)} = 6.392$ ,  $p = 0.014$  for genotype, Bonferroni *post-hoc* test,  $p < 0.05$ ], and 71–80 Hz [**Figure 5C**,  $F_{(1, 54)} = 2.707$ ,  $p = 0.106$  for genotype, Bonferroni *post-hoc* test,  $p < 0.05$ ], were all decreased by the 25th ISI in the mutants. On the other hand, the spontaneous LFP power in the control mice tended to increase after the 1st ASSR stimuli, particularly in beta frequency range (**Figure 4A**). This power increase upon ASSR stimuli in the control mice was prominent in the per-channel design (**Figures 5A,B**,  $p < 0.05$ , respectively). Consequently, no genotypic difference was detected in spontaneous LFP power magnitudes during 10-s inter-stimulus intervals (combined data of first, 25th and 50th ISIs) at any power spectra examined per animal (**Figure 4D**) and per channel (**Figure 5D**). Interestingly, 20-min after the last ASSR, the spontaneous LFP power in the mutants was significantly augmented [**Figure 4A**,  $F_{(1, 11)} = 1.104$ ,  $p = 0.335$  for genotype, Bonferroni *post-hoc* test,  $p < 0.05$ ] to the level of pre-stimulus period. The elevation of LFP power amplitudes was more prominent in per channel analysis (**Figures 5A–C**,  $p < 0.05$ ). These results suggest a brain state-dependent abnormality of baseline spontaneous LFP power in the mutant mice, i.e., an abnormally high spontaneous LFP power in an awake quiescent period, which disappears upon receiving external auditory stimuli. Our findings also strongly suggests that the evoked ASSR deficit found in our mutants is not due to greater baseline spontaneous gamma power, rather it is simply caused by the deficits in evoking responses by external stimuli.

### DISCUSSION

We demonstrated abnormal oscillatory LFP power and impaired auditory-evoked LFP responses from the auditory cortex of awake, head-restrained GABA neuron-specific NMDAR hypofunction mice. Specifically, we found (1) a profound reduction of ASSR power and phase locking at 40-Hz, and to lesser degree, at 20-Hz, and (2) a broadband increase in spontaneous LFP power during the pre-stimulus period, but not during the inter-ASSR stimulus intervals. Interestingly, abnormal elevation of baseline spontaneous LFP power during the pre-stimulus period disappeared after the ASSR stimuli were presented. These findings suggest that NMDAR hypofunction in cortical GABAergic interneurons leads to two temporally distinct, brain state-dependent LFP deficits in A1 cortex; (1) the evoked ASSR deficits with normal level of spontaneous LFP

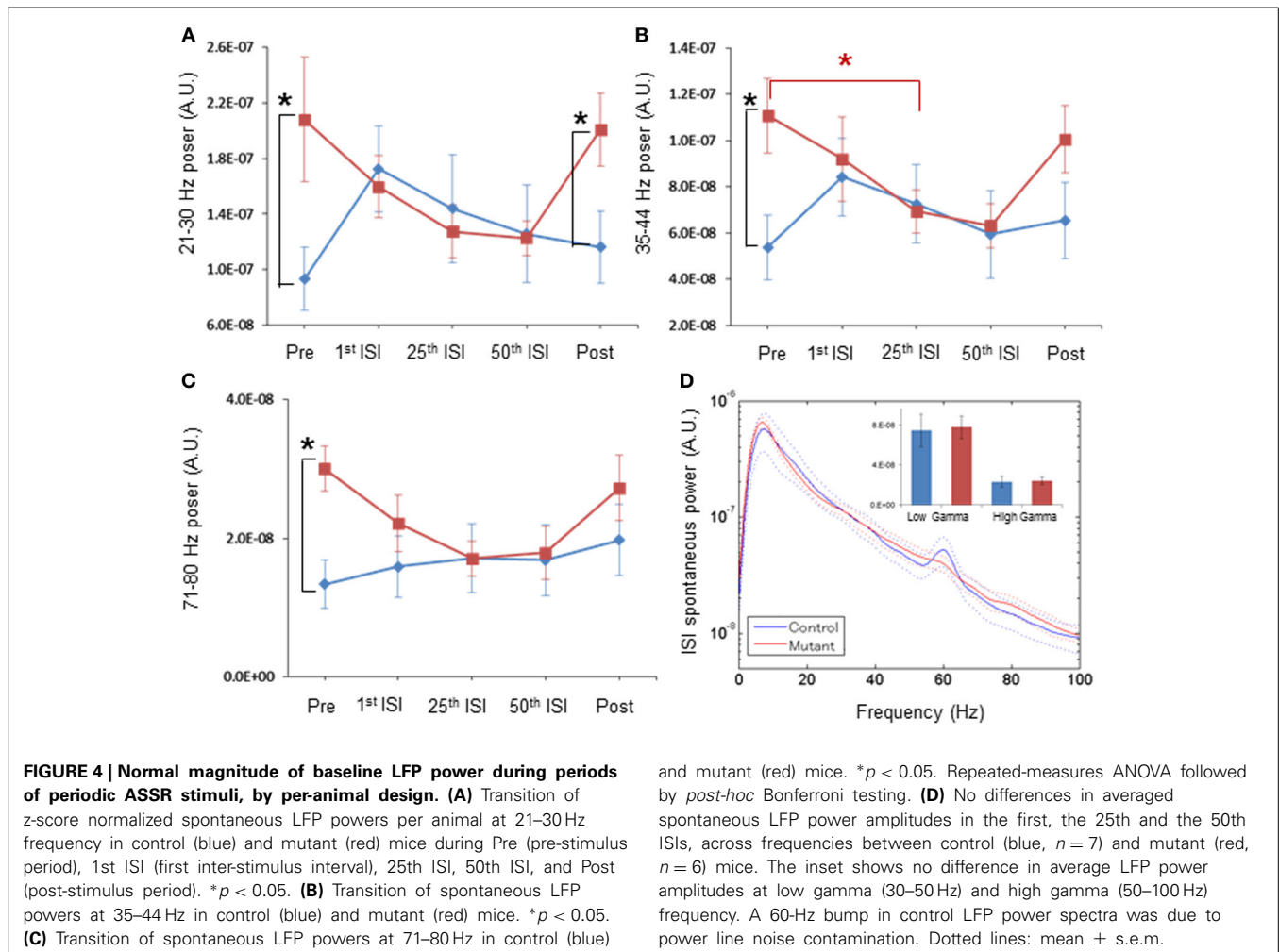


power and (2) abnormal broadband elevation of spontaneous LFP power when no auditory stimuli are presented. Our study also showed no obvious contribution to the evoked ASSR deficits of augmented spontaneous LFP fluctuation following NMDAR hypofunction in GABAergic interneurons.

#### POTENTIAL MECHANISMS UNDERLYING EVOKED ASSR DEFICITS

We demonstrated robust ASSR deficits in the mutant mice in which NMDARs were selectively eliminated from 75 to 84% of PV-containing interneurons in neocortex (Belforte et al., 2010). This suggests that NMDARs in the PV-positive fast-spiking neurons are crucial for emergence of ASSRs. Optogenetically evoked-gamma oscillations have also been shown to be defective in mice in which NMDARs are genetically ablated from all PV-positive neurons (Carlén et al., 2012). The mechanism by which NMDAR deletion from PV neurons results in the ASSR deficits is not fully known. However, activation of cortical PV-positive interneurons

in the thalamorecipient circuit is known to enhance acoustic information flow by feed-forward inhibition, which contributes to improved signal-to-noise ratio (Hamilton et al., 2013). In particular, the firing rate of fast-spiking neurons, likely PV-positive, appears to increase with increasing attention to external stimuli (Mitchell et al., 2007; Chen et al., 2008). It is noted that although selective genetic GluN1 deletion also occurs in  $\sim 30\%$  of Reelin-positive interneurons in the mutant cortex, Reelin-positive neurons are located mostly in the supra-granular layers. Therefore, the most likely mechanism for our observation is a functional deficit in the NMDAR-deleted PV neurons that receive thalamocortical afferents. Presumed impairment in their feed-forward inhibition in response to acoustic stimuli may attenuate the generation of auditory evoked potentials followed by gamma oscillations. Further research exploring whether NMDAR hypofunction in cortical PV-neurons disturbs feedforward information flow elicited by auditory stimuli in A1 cortex is warranted.

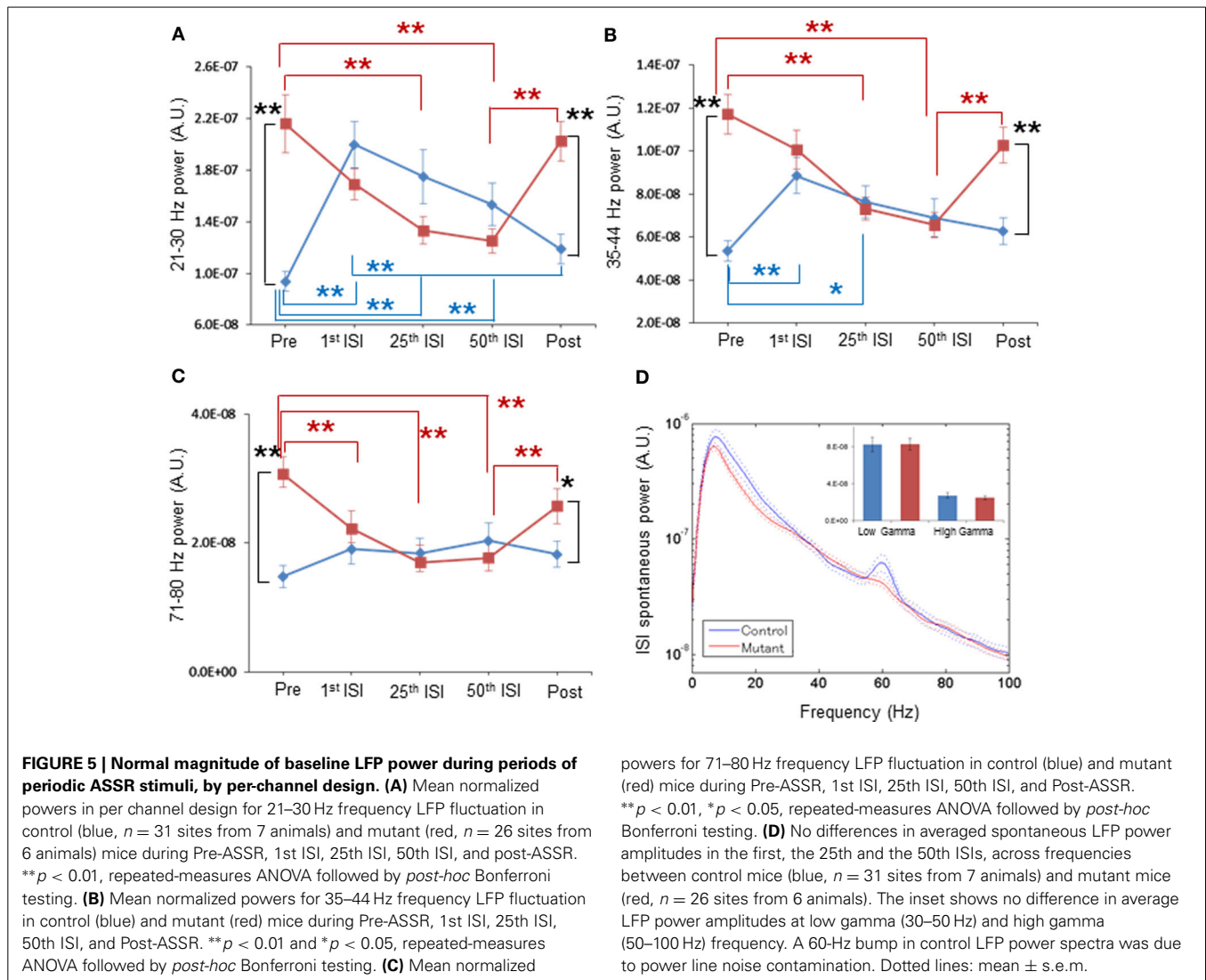


#### POTENTIAL MECHANISMS UNDERLYING THE ENHANCED BASELINE LFP FLUCTUATION

We also observed elevated spontaneous LFP oscillatory power in the pre-stimulus period before the animal attends to the auditory stimuli. Since genetic ablation of NMDARs selectively from PV neurons in awake mice also results in increased baseline power (Korotkova et al., 2010; Carlén et al., 2012), this finding is most likely due to NMDAR hypofunction in PV neurons. Similar results were also obtained from GluN1 hypomorph mice (Dzirasa et al., 2009; Gandal et al., 2012b) and from the acute administration of NMDAR antagonists (phencyclidine, ketamine, or MK-801) to rodents (Leung, 1985; Ma and Leung, 2000, 2007; Pinault, 2008; Ehrlichman et al., 2009; Hakami et al., 2009; Páleníček et al., 2011; Kulikova et al., 2012; Wood et al., 2012; Caixeta et al., 2013; Molina et al., 2014), to humans (Maksimow et al., 2006; Hong et al., 2010), and in *in vitro* slice preparation (McNally et al., 2011). The most likely mechanistic explanation for these effects is that cortical disinhibition elicited by NMDAR deletion from local PV neurons render the cortical glutamatergic neurons hyperexcitable (Olney and Farber, 1995; Homayoun and Moghaddam, 2007; Lisman et al., 2008; Nakazawa et al., 2012). However, the NMDAR hypofunction-induced baseline power increase is

unlikely to be caused by hyper-synchrony of spiking activity. A recent *in vivo* unit/LFP recording study revealed that cortical disinhibition elicited by MK-801, a NMDAR antagonist, evoked an increase in the number of random spike trains of individual units and consequently a reduced synchronized firing of action potentials in mPFC of free-moving rats, despite a robust increase in LFP power at gamma frequency (Molina et al., 2014). This finding suggests a decoupling of gamma band LFP power from neuronal spiking synchrony. Similarly, we also previously reported in the same mutant mice used in this study there was a disruption in *in vivo* spike synchrony among pyramidal neurons in somatosensory cortex (Belforte et al., 2010). Therefore, the spontaneous LFP power increase following cortical NMDAR hypofunction may simply reflect a robust increase in synaptic inputs with aberrant or “noisy” spike firing. It is also plausible that NMDAR antagonism on GABAergic neurons in the basal ganglia and/or thalamic reticular nucleus causes disinhibition of thalamocortical neurons, leading to massive stimulation of cortical neurons at gamma frequency (Llinás and Ribary, 1993; Santana et al., 2011). However, this is unlikely in our model because the genetic manipulation is largely confined to the cortex and hippocampus.





### BRAIN STATE-DEPENDENT ELEVATION OF SPONTANEOUS LFP POWER

Unexpectedly, we found that spontaneous LFP power amplitudes tends to decrease during the repeated ASSR stimuli; a phenomenon which was more robust in per-channel design (Figure 5). Accordingly, the broadband elevation of spontaneous LFP power in the pre-stimulus period (Figure 3B) disappeared during the inter-ASSR stimulus periods (Figure 4D). The structure of cortical spontaneous activity is known to vary with cortical state or behavioral state (Steriade et al., 2001; Harris and Thiele, 2011). During the slow-wave sleep period and awake quiescent period, auditory cortex exhibits fluctuations of global activity between “synchronized” states of larger low frequency waves known as up and down state (Steriade et al., 1993; Harris and Thiele, 2011). In active wakefulness during tone presentation, these fluctuations are replaced by the “desynchronized” state characterized by low amplitude, high frequency LFPs (Castro-Alamancos, 2004). It has been reported that superficial pyramidal cells and putative fast-spiking neurons in rat A1 cortex dominate in awake quiescent period, and their activity was largely suppressed during auditory stimuli-induced cortical

desynchronization (Sakata and Harris, 2012). The firing of fast-spiking neurons in rat somatosensory cortex, which is highly active during quiet wakefulness, is also dramatically suppressed during active whisking behavior (Gentet et al., 2010). Considering that the majority of cell-types in which NMDAR elimination occurred in our mutant mice are PV-positive fast-spiking neurons, it is conceivable that the state-dependent elevation of spontaneous LFP power reflects the dysfunction of mutant A1 cortex fast-spiking neurons during awake quiescent period. However, a recent study showed a dramatic increase in the putative fast-spiking neurons in visual cortex by the active running in a head-restrained condition that may elicit desynchronized state (Niell and Stryker, 2010). Further study is necessary to clarify the mechanisms of the state-dependent elevation of spontaneous LFP power observed in our mutant mice.

### COMPARISON TO CLINICAL DATA

Overall, the present results were consistent with the clinical EEG data showing reductions in the onset of auditory evoked responses (P50, N100) and of 40-Hz ASSR power and

phase-locking in the cortex of individuals with schizophrenia, supporting the face validity of our mouse model. Furthermore, our findings argue against the possibility that 40-Hz ASSR deficits in patients with schizophrenia may reflect antipsychotic effects (Woo et al., 2010). However, we also found several findings inconsistent with the human data. First, in human adult subjects 40-Hz click trains induce the maximal ASSR at 40 Hz and the effects of 40-Hz stimuli at 20 and 30 Hz are smaller compared to 40 Hz (Galambos et al., 1981; Pastor et al., 2002; Picton et al., 2003). Since the optimal input frequency of fast-spiking neurons for action potential generation is known to be 30–50 Hz in rats (Pike et al., 2000), the ASSR impairment selectively at 40 Hz stimulation may suggest unequivocal deficits of fast-spiking neurons in patients with schizophrenia. In our study, however, 40-Hz stimuli induced a resonance peak at 30 Hz in addition to the 40-Hz peak (Figure 1D) whereas the phase locking spectrum showed a peak only at 40 Hz (Figure 1G). This may suggest that the murine A1 cortex exhibits a broader resonance frequency (30 Hz as well as 40 Hz) than in humans; although no power peak at 30 Hz was detected when stimulated at 20 Hz (Figure 2B). Further study is warranted to determine whether the resonant frequency to auditory stimuli is varied depending on the species.

Second, 20-Hz ASSRs are usually unaffected in schizophrenia (Kwon et al., 1999; Light et al., 2006; Vierling-Claassen et al., 2008); however some human ASSR studies also showed attenuation in 20-Hz ASSRs (Krishnan et al., 2009). In contrast, in our model 20 Hz ASSRs are reduced in power and phase locking (Figure 2). Nonetheless, the mutant ASSR peak at 20 Hz was still visible (Figure 2B) and attenuation of phase locking at 20 Hz was modest (Figure 2E), compared to robustness of 40-Hz ASSR deficits. Furthermore, the initial N1 responses triggered by 20-Hz ASSR stimuli were normal in the mutant mice. Therefore, the degree of evoked ASSR deficits appears to be more robust at 40-Hz than at 20-Hz in our mutant mice. It is conceivable that LFP recording directly from A1 cortex is more sensitive to detect ASSR impairment, compared to clinical skull-EEG recording.

Third, broadband enhancement of baseline EEG may not be characteristic of studies of resting EEG in patients with schizophrenia (Winterer et al., 2004; Kikuchi et al., 2011; Silverstein et al., 2012). However, Spencer (2012) re-analyzed their previous data which showed deficits in auditory evoked gamma oscillations and found that the pre-stimulus baseline gamma power was increased in the left auditory cortex of chronic patients. Interestingly, in his study, the baseline power increased across a wide frequency band (15–100 Hz) and this broadband increase was marginally significant, which is consistent with our finding.

Finally, this study involved relatively small sample sizes under per-animal analysis design (7 control and 6 mutant mice), which could be a confounding factor. However, nearly the same results were obtained by per-channel analysis (for example, Figure 4 vs. Figure 5), which further supports our conclusion.

#### CLINICAL MANIFESTATION OF BASELINE LFP POWER INCREASE

Given that sensory-evoked gamma oscillation deficits are presumably linked to the cognitive deficits (Spencer et al., 2004; Cho et al., 2006), there are several possible clinical manifestation

of baseline power increase. Increased baseline gamma oscillations have been reported in patients during psychotic episodes, including visual and auditory hallucinations (Baldeweg et al., 1998; Ropohl et al., 2004; Lee et al., 2006; Becker et al., 2009). Other studies suggest a link between baseline gamma oscillations and negative symptoms (Suazo et al., 2012), working memory (Winterer et al., 2004; Suazo et al., 2012), or synaptic plasticity (Bikbaev et al., 2008; Kulikova et al., 2012). A recent meta-analysis of functional neuroimaging in schizophrenia patients with auditory hallucinations revealed “paradoxical” engagement of A1 cortex, such that left A1 cortex displayed increased activation in the absence of external auditory stimuli (but with auditory verbal hallucinations), and decreased activation when an external stimulus was actually present (Kompus et al., 2011). Consistent with this, our mutant mice also exhibited an increase in baseline spontaneous LFP increase in the absence of external stimuli, which tended to decrease during repetitive ASSR stimuli and to return back to the elevated level 20 min after the last ASSR stimuli. This remarkable similarity between human patient studies and the finding in the present study may suggest that baseline LFP power increase is a signature of “paradoxical” A1 cortex activation in the absence of external stimuli. Further studies are warranted to assess the clinical and neurobiological significance of oscillations and synchrony deficits in schizophrenia.

#### AUTHOR CONTRIBUTIONS

Kazuhiro Nakao conceived and designed the study, performed the experiments, assembled, analyzed and interpreted the data, and wrote manuscript. Kazu Nakazawa conceived and designed the study, interpreted the data, and wrote the manuscript.

#### ACKNOWLEDGMENTS

This work was supported by an NIH grant K22MH099164 (Kazu Nakazawa) and by NIH Intramural Research Program. We thank Stefan Kolata and Kentaroh Takagaki for their advice on the earlier version of manuscript.

#### SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: <http://www.frontiersin.org/journal/10.3389/fnins.2014.00168/abstract>

#### REFERENCES

- Baldeweg, T., Spence, S., and Hirsch, S. R. (1998). Gamma-band electroencephalographic oscillations in a patient with somatic hallucinations. *Lancet* 352, 620–621. doi: 10.1016/S0140-6736(05)79575-1
- Becker, C., Gramann, K., Müller, H. J., and Elliott, M. A. (2009). Electrophysiological correlates of flicker-induced color hallucinations. *Conscious. Cogn.* 18, 266–276. doi: 10.1016/j.concog.2008.05.001
- Belforte, J. E., Zsiros, V., Sklar, E. R., Jiang, Z., Yu, G., Li, Y., et al. (2010). Postnatal NMDA receptor ablation in corticolimbic interneurons confers schizophrenia-like phenotypes. *Nat. Neurosci.* 13, 76–83. doi: 10.1038/nn.2447
- Bikbaev, A., Manahan-vaghaan, D., and Sandi, C. (2008). Relationship of hippocampal theta and gamma oscillations to potentiation of synaptic transmission. *Front. Neurosci.* 2:1. doi: 10.3389/neuro.01.010.2008
- Brenner, C. A., Krishnan, G. P., Vohs, J. L., Ahn, W.-Y., Hetrick, W. P., Morzorati, S. L., et al. (2009). Steady state responses: electrophysiological assessment of sensory function in schizophrenia. *Schizophr. Bull.* 35, 1065–1077. doi: 10.1093/schbul/sbp091

- Brenner, C. A., Sporns, O., Lysaker, P. H., and O'Donnell, B. F. (2003). EEG synchronization to modulated auditory tones in schizophrenia, schizoaffective disorder, and schizotypal personality disorder. *Am. J. Psychiatry* 160, 2238–2240. doi: 10.1176/appi.ajp.160.12.2238
- Caixeta, F. V., Cornélio, A. M., Scheffer-Teixeira, R., Ribeiro, S., and Tort, A. B. L. (2013). Ketamine alters oscillatory coupling in the hippocampus. *Sci. Rep.* 3:2348. doi: 10.1038/srep02348
- Carlén, M., Meletis, K., Siegle, J. H., Cardin, J. A., Futai, K., Vierling-Claassen, D., et al. (2012). A critical role for NMDA receptors in parvalbumin interneurons for gamma rhythm induction and behavior. *Mol. Psychiatry* 17, 537–548. doi: 10.1038/mp.2011.31
- Castro-Alamancos, M. A. (2004). Absence of rapid sensory adaptation in neocortex during information processing states. *Neuron* 41, 455–464. doi: 10.1016/S0896-6273(03)00853-5
- Chen, Y., Martinez-Conde, S., Macknik, S. L., Bereshpolova, Y., Swadlow, H. A., and Alonso, J.-M. (2008). Task difficulty modulates the activity of specific neuronal populations in primary visual cortex. *Nat. Neurosci.* 11, 974–982. doi: 10.1038/nn.2147
- Cho, R. Y., Konecky, R. O., and Carter, C. S. (2006). Impairments in frontal cortical gamma synchrony and cognitive control in schizophrenia. *Proc. Natl. Acad. Sci. U.S.A.* 103, 19878–19883. doi: 10.1073/pnas.0609440103
- Dzirasa, K., Ramsey, A. J., Takahashi, D. Y., Stapleton, J., Potes, J. M., Williams, J. K., et al. (2009). Hyperdopaminergia and NMDA receptor hypofunction disrupt neural phase signaling. *J. Neurosci.* 29, 8215–8224. doi: 10.1523/JNEUROSCI.1773-09.2009
- Ehrlichman, R. S., Gandal, M. J., Maxwell, C. R., Lazarewicz, M. T., Finkel, L. H., Contreras, D., et al. (2009). N-methyl-D-aspartic acid receptor antagonist-induced frequency oscillations in mice recreate pattern of electrophysiological deficits in schizophrenia. *Neuroscience* 158, 705–712. doi: 10.1016/j.neuroscience.2008.10.031
- Ford, J. M., and Mathalon, D. H. (2008). Neural synchrony in schizophrenia. *Schizophr. Bull.* 34, 904–906. doi: 10.1093/schbul/sbn090
- Galambos, R., Makeig, S., and Talmachoff, P. J. (1981). A 40-Hz auditory potential recorded from the human scalp. *Proc. Natl. Acad. Sci. U.S.A.* 78, 2643–2647. doi: 10.1073/pnas.78.4.2643
- Gandal, M. J., Edgar, J. C., Klook, K., and Siegel, S. J. (2012a). Gamma synchrony: towards a translational biomarker for the treatment-resistant symptoms of schizophrenia. *Neuropharmacology* 62, 1504–1518. doi: 10.1016/j.neuropharm.2011.02.007
- Gandal, M. J., Sisti, J., Klook, K., Ortinski, P. I., Leitman, V., Liang, Y., et al. (2012b). GABAB-mediated rescue of altered excitatory-inhibitory balance, gamma synchrony and behavioral deficits following constitutive NMDAR-hypofunction. *Transl. Psychiatry* 2, e142. doi: 10.1038/tp.2012.69
- Gentet, L. J., Avermann, M., Matyas, F., Staiger, J. F., and Petersen, C. C. H. (2010). Membrane potential dynamics of GABAergic neurons in the barrel cortex of behaving mice. *Neuron* 65, 422–435. doi: 10.1016/j.neuron.2010.01.006
- Golomb, D., Donner, K., Shacham, L., Shlосberg, D., Amitai, Y., and Hansel, D. (2007). Mechanisms of firing patterns in fast-spiking cortical interneurons. *PLoS Comput. Biol.* 3:e156. doi: 10.1371/journal.pcbi.0030156
- Haig, A. R., Gordon, E., De Pascalis, V., Meares, R. A., Bahramali, H., and Harris, A. (2000). Gamma activity in schizophrenia: evidence of impaired network binding? *Clin. Neurophysiol.* 111, 1461–1468. doi: 10.1016/S1388-2457(00)00347-3
- Hakami, T., Jones, N. C., Tolmacheva, E. A., Gaudias, J., Chaumont, J., Salzberg, M., et al. (2009). NMDA receptor hypofunction leads to generalized and persistent aberrant gamma oscillations independent of hyperlocomotion and the state of consciousness. *PLoS ONE* 4:e6755. doi: 10.1371/journal.pone.0006755
- Hamilton, L. S., Sohl-Dickstein, J., Huth, A. G., Carels, V. M., Deisseroth, K., and Bao, S. (2013). Optogenetic activation of an inhibitory network enhances feed-forward functional connectivity in auditory cortex. *Neuron* 80, 1066–1076. doi: 10.1016/j.neuron.2013.08.017
- Harris, K. D., and Thiele, A. (2011). Cortical state and attention. *Nat. Rev. Neurosci.* 12, 509–523. doi: 10.1038/nrn3084
- Homayoun, H., and Moghaddam, B. (2007). NMDA receptor hypofunction produces opposite effects on prefrontal cortex interneurons and pyramidal neurons. *J. Neurosci.* 27, 11496–11500. doi: 10.1523/JNEUROSCI.2213-07.2007
- Hong, L. E., Summerfelt, A., Buchanan, R. W., O'Donnell, P., Thaker, G. K., Weiler, M. A., et al. (2010). Gamma and delta neural oscillations and association with clinical symptoms under subanesthetic ketamine. *Neuropsychopharmacology* 35, 632–640. doi: 10.1038/npp.2009.168
- Jalili, M., Lavoie, S., Deppen, P., Meuli, R., Do, K. Q., Cuénod, M., et al. (2007). Dysconnection topography in schizophrenia revealed with state-space analysis of EEG. *PLoS ONE* 2:e1059. doi: 10.1371/journal.pone.0001059
- Jiang, Z., Rompala, G. R., Zhang, S., Cowell, R. M., and Nakazawa, K. (2013). Social isolation exacerbates schizophrenia-like phenotypes via oxidative stress in cortical interneurons. *Biol. Psychiatry* 73, 1024–1034. doi: 10.1016/j.biopsych.2012.12.004
- Kikuchi, M., Hashimoto, T., Nagasawa, T., Hirose, T., Minabe, Y., Yoshimura, M., et al. (2011). Frontal areas contribute to reduced global coordination of resting-state gamma activities in drug-naïve patients with schizophrenia. *Schizophr. Res.* 130, 187–194. doi: 10.1016/j.schres.2011.06.003
- Kompus, K., Westerhausen, R., and Hugdahl, K. (2011). The “paradoxical” engagement of the primary auditory cortex in patients with auditory verbal hallucinations: a meta-analysis of functional neuroimaging studies. *Neuropsychologia* 49, 3361–3369. doi: 10.1016/j.neuropsychologia.2011.08.010
- Korotkova, T., Fuchs, E. C., Ponomarenko, A., von Engelhardt, J., and Monyer, H. (2010). NMDA receptor ablation on parvalbumin-positive interneurons impairs hippocampal synchrony, spatial representations, and working memory. *Neuron* 68, 557–569. doi: 10.1016/j.neuron.2010.09.017
- Krishnan, G. P., Hetrick, W. P., Brenner, C. A., Shekhar, A., Steffen, A. N., and O'Donnell, B. F. (2009). Steady state and induced auditory gamma deficits in schizophrenia. *Neuroimage* 47, 1711–1719. doi: 10.1016/j.neuroimage.2009.03.085
- Kulikova, S. P., Tolmacheva, E. A., Anderson, P., Gaudias, J., Adams, B. E., Zheng, T., et al. (2012). Opposite effects of ketamine and deep brain stimulation on rat thalamocortical information processing. *Eur. J. Neurosci.* 36, 3407–3419. doi: 10.1111/j.1460-9568.2012.08263.x
- Kwon, J. S., O'Donnell, B. F., Wallenstein, G. V., Greene, R. W., Hirayasu, Y., Nestor, P. G., et al. (1999). Gamma frequency-range abnormalities to auditory stimulation in schizophrenia. *Arch. Gen. Psychiatry* 56, 1001–1005. doi: 10.1001/archpsyc.56.11.1001
- Lazic, S. E., and Essioux, L. (2013). Improving basic and translational science by accounting for litter-to-litter variation in animal models. *BMC Neurosci.* 14:37. doi: 10.1186/1471-2202-14-37
- Lee, K.-H., Williams, L. M., Breakspear, M., and Gordon, E. (2003). Synchronous gamma activity: a review and contribution to an integrative neuroscience model of schizophrenia. *Brain Res. Rev.* 41, 57–78. doi: 10.1016/S0165-0173(02)00220-5
- Lee, S.-H., Wynn, J. K., Green, M. F., Kim, H., Lee, K.-J., Nam, M., et al. (2006). Quantitative EEG and low resolution electromagnetic tomography (LORETA) imaging of patients with persistent auditory hallucinations. *Schizophr. Res.* 83, 111–119. doi: 10.1016/j.schres.2005.11.025
- Leung, L. W. (1985). Spectral analysis of hippocampal EEG in the freely moving rat: effects of centrally active drugs and relations to evoked potentials. *Electroencephalogr. Clin. Neurophysiol.* 60, 65–77. doi: 10.1016/0013-4694(85)90952-6
- Light, G. A., Hsu, J. L., Hsieh, M. H., Meyer-Gomes, K., Sprack, J., Swerdlow, N. R., et al. (2006). Gamma band oscillations reveal neural network cortical coherence dysfunction in schizophrenia patients. *Biol. Psychiatry* 60, 1231–1240. doi: 10.1016/j.biopsych.2006.03.055
- Lisman, J. E., Coyle, J. T., Green, R. W., Javitt, D. C., Benes, F. M., Heckers, S., et al. (2008). Circuit-based framework for understanding neurotransmitter and risk gene interactions in schizophrenia. *Trends Neurosci.* 31, 234–242. doi: 10.1016/j.tins.2008.02.005
- Llinás, R., and Ribary, U. (1993). Coherent 40-Hz oscillation characterizes dream state in humans. *Proc. Natl. Acad. Sci. U.S.A.* 90, 2078–2081. doi: 10.1073/pnas.90.5.2078
- Ma, J., and Leung, L. S. (2000). Relation between hippocampal gamma waves and behavioral disturbances induced by phencyclidine and methamphetamine. *Behav. Brain Res.* 111, 1–11. doi: 10.1016/S0166-4328(00)00138-8
- Ma, J., and Leung, L. S. (2007). The supramammillo-septal-hippocampal pathway mediates sensorimotor gating impairment and hyperlocomotion induced by MK-801 and ketamine in rats. *Psychopharmacology (Berl.)* 191, 961–974. doi: 10.1007/s00213-006-0667-x
- Maharajh, K., Teale, P., Rojas, D. C., and Reite, M. L. (2010). Fluctuation of gamma-band phase synchronization within the auditory cortex in schizophrenia. *Clin. Neurophysiol.* 121, 542–548. doi: 10.1016/j.clinph.2009.12.010
- Maksimov, A., Särkelä, M., Långsjö, J. W., Salmi, E., Kaisti, K. K., Yli-Hankala, A., et al. (2006). Increase in high frequency EEG activity explains the poor

- performance of EEG spectral entropy monitor during S-ketamine anesthesia. *Clin. Neurophysiol.* 117, 1660–1668. doi: 10.1016/j.clinph.2006.05.011
- McNally, J. M., McCarley, R. W., McKenna, J. T., Yanagawa, Y., and Brown, R. E. (2011). Complex receptor mediation of acute ketamine application on *in vitro* gamma oscillations in mouse prefrontal cortex: modeling gamma band oscillation abnormalities in schizophrenia. *Neuroscience* 199, 51–63. doi: 10.1016/j.neuroscience.2011.10.015
- Mitchell, J. F., Sundberg, K. A., and Reynolds, J. H. (2007). Differential attention-dependent response modulation across cell classes in macaque visual area V4. *Neuron* 55, 131–141. doi: 10.1016/j.neuron.2007.06.018
- Molina, L. A., Skelin, I., and Gruber, A. J. (2014). Acute NMDA receptor antagonism disrupts synchronization of action potential firing in rat prefrontal cortex. *PLoS ONE* 9:e85842. doi: 10.1371/journal.pone.0085842
- Nakazawa, K., Zsiros, V., Jiang, Z., Nakao, K., Kolata, S., Zhang, S., et al. (2012). GABAergic interneuron origin of schizophrenia pathophysiology. *Neuropharmacology* 62, 1574–1583. doi: 10.1016/j.neuropharm.2011.01.022
- Niell, C. M., and Stryker, M. P. (2010). Modulation of visual responses by behavioral state in mouse visual cortex. *Neuron* 65, 472–479. doi: 10.1016/j.neuron.2010.01.033
- O'Donnell, B. F., Vohs, J. L., Krishnan, G. P., Rass, O., Hetrick, W. P., and Morzorati, S. L. (2013). The auditory steady-state response (ASSR): a translational biomarker for schizophrenia. *Suppl. Clin. Neurophysiol.* 62, 101–112. doi: 10.1016/B978-0-7020-5307-8.00006-5
- Olney, J. W., and Farber, N. B. (1995). Glutamate receptor dysfunction and schizophrenia. *Arch. Gen. Psychiatry* 52, 998–1007. doi: 10.1001/archpsyc.1995.03950240016004
- Páleníček, T., Fujáková, M., Brunovski, M., Balíková, M., Horáček, J., Gorman, I., et al. (2011). Electroencephalographic spectral and coherence analysis of ketamine in rats: correlation with behavioral effects and pharmacokinetics. *Neuropsychobiology* 63, 202–218. doi: 10.1159/000321803
- Pastor, M. A., Artieda, J., Arbizu, J., Marti-Climent, J. M., Peñuelas, I., and Masdeu, J. C. (2002). Activation of human cerebral and cerebellar cortex by auditory stimulation at 40 Hz. *J. Neurosci.* 22, 10501–10506.
- Picton, T. W., John, M. S., Dimitrijevic, A., and Purcell, D. (2003). Human auditory steady-state responses. *Int. J. Audiol.* 42, 177–219. doi: 10.3109/14992020309101316
- Pike, F. G., Goddard, R. S., Suckling, J. M., Ganter, P., Kasthuri, N., and Paulsen, O. (2000). Distinct frequency preferences of different types of rat hippocampal neurons in response to oscillatory input currents. *J. Physiol.* 529, 205–213. doi: 10.1111/j.1469-7793.2000.00205.x
- Pinault, D. (2008). N-methyl D-aspartate receptor antagonists ketamine and MK-801 induce wake-related aberrant gamma oscillations in the rat neocortex. *Biol. Psychiatry* 63, 730–735. doi: 10.1016/j.biopsych.2007.10.006
- Ropohl, A., Sperling, C. A. W., Elstner, S., Tomandl, B., Reulbach, U., Kaltenhüser, M., et al. (2004). Cortical activity associated with auditory hallucinations. *Neuroreport* 15, 3–6. doi: 10.1097/00001756-200403010-00028
- Rutter, L., Carver, F. W., Holroyd, T., Nadar, S. R., Mitchell-Francis, J., Apud, J., et al. (2009). Magnetoencephalographic gamma power reduction in patients with schizophrenia during resting condition. *Hum. Brain Mapp.* 30, 3254–3264. doi: 10.1002/hbm.20746
- Sakata, S., and Harris, K. D. (2012). Laminar-dependent effects of cortical state on auditory cortical spontaneous activity. *Front. Neural Circuits* 6:109. doi: 10.3389/fncir.2012.00109
- Santana, N., Troyano-Rodríguez, E., Mengod, G., Celada, P., and Artigas, F. (2011). Activation of thalamocortical networks by the N-methyl-D-aspartate receptor antagonist phencyclidine: reversal by clozapine. *Biol. Psychiatry* 69, 918–927. doi: 10.1016/j.biopsych.2010.10.030
- Santarelli, R., Carraro, L., Conti, G., Capello, M., Plourde, G., and Arslan, E. (2003). Effects of isoflurane on auditory middle latency (MLRs) and steady-state (SSRs) responses recorded from the temporal cortex of the rat. *Brain Res.* 973, 240–251. doi: 10.1016/S0006-8993(03)02520-4
- Silverstein, S. M., All, S. D., Thompson, J. L., Williams, L. M., Whitford, T. J., Nagy, M., et al. (2012). Absolute level of gamma synchrony is increased in first-episode schizophrenia during face processing. *J. Exp. Psychopathol.* 3, 702–723. doi: 10.5127/jep.023311
- Spencer, K. M. (2012). Baseline gamma power during auditory steady-state stimulation in schizophrenia. *Front. Hum. Neurosci.* 5:190. doi: 10.3389/fnhum.2011.00190
- Spencer, K. M., Nestor, P. G., Perlmutter, R., Niznikiewicz, M. A., Klump, M. C., Frumin, M., et al. (2004). Neural synchrony indexes disordered perception and cognition in schizophrenia. *Proc. Natl. Acad. Sci. U.S.A.* 101, 17288–17293. doi: 10.1073/pnas.0406074101
- Spencer, K. M., Niznikiewicz, M. A., Nestor, P. G., Shenton, M. E., and McCarley, R. W. (2009). Left auditory cortex gamma synchronization and auditory hallucination symptoms in schizophrenia. *BMC Neurosci.* 10:85. doi: 10.1186/1471-2202-10-85
- Spencer, K. M., Salisbury, D. F., Shenton, M. E., and McCarley, R. W. (2008). Gamma-band auditory steady-state responses are impaired in first episode psychosis. *Biol. Psychiatry* 64, 369–375. doi: 10.1016/j.biopsych.2008.02.021
- Steriade, M., Nuñez, A., and Amzica, F. (1993). A novel slow (< 1 Hz) oscillation of neocortical neurons *in vivo*: depolarizing and hyperpolarizing components. *J. Neurosci.* 13, 3252–3265.
- Steriade, M., Timofeev, I., and Grenier, F. (2001). Natural waking and sleep states: a view from inside neocortical neurons. *J. Neurophysiol.* 85, 1969–1985.
- Suazo, V., Díez, Á., Martín, C., Ballesteros, A., Casado, P., Martín-Loeches, M., et al. (2012). Elevated noise power in gamma band related to negative symptoms and memory deficit in schizophrenia. *Prog. Neuropsychopharmacol. Biol. Psychiatry* 38, 270–275. doi: 10.1016/j.pnpbp.2012.04.010
- Tateno, T., Harsch, A., and Robinson, H. P. C. (2004). Threshold firing frequency-current relationships of neurons in rat somatosensory cortex: type 1 and type 2 dynamics. *J. Neurophysiol.* 92, 2283–2294. doi: 10.1152/jn.00109.2004
- Teale, P., Collins, D., Maharajh, K., Rojas, D. C., Kronberg, E., and Reite, M. (2008). Cortical source estimates of gamma band amplitude and phase are different in schizophrenia. *Neuroimage* 42, 1481–1489. doi: 10.1016/j.neuroimage.2008.06.020
- Tsuchimoto, R., Kanba, S., Hirano, S., Oribe, N., Ueno, T., Hirano, Y., et al. (2011). Reduced high and low frequency gamma synchronization in patients with chronic schizophrenia. *Schizophr. Res.* 133, 99–105. doi: 10.1016/j.schres.2011.07.020
- Uhlhaas, P. J., and Singer, W. (2010). Abnormal neural oscillations and synchrony in schizophrenia. *Nat. Rev. Neurosci.* 11, 100–113. doi: 10.1038/nrn2774
- Venables, N. C., Bernat, E. M., and Sponheim, S. R. (2009). Genetic and disorder-specific aspects of resting state EEG abnormalities in schizophrenia. *Schizophr. Bull.* 35, 826–839. doi: 10.1093/schbul/sbn021
- Vierling-Claassen, D., Siekmeier, P., Stufflebeam, S., and Kopell, N. (2008). Modeling GABA alterations in schizophrenia: a link between impaired inhibition and altered gamma and beta range auditory entrainment. *J. Neurophysiol.* 99, 2656–2671. doi: 10.1152/jn.00870.2007
- Winterer, G., Coppola, R., Sc, D., Goldberg, T. E., Ph, D., Egan, M. F., et al. (2004). Prefrontal broadband noise, working memory, and genetic risk for schizophrenia. *Am. J. Psychiatry* 161, 490–500. doi: 10.1176/appi.ajp.161.3.490
- Woo, T.-U. W., Spencer, K., and McCarley, R. W. (2010). Gamma oscillation deficits and the onset and early progression of schizophrenia. *Harv. Rev. Psychiatry* 18, 173–189. doi: 10.3109/10673221003747609
- Wood, J., Kim, Y., and Moghaddam, B. (2012). Disruption of prefrontal cortex large scale neuronal activity by different classes of psychotomimetic drugs. *J. Neurosci.* 32, 3022–3031. doi: 10.1523/JNEUROSCI.6377-11.2012
- Yeragani, V. K., Cashmere, D., Miewald, J., Tancer, M., and Keshavan, M. S. (2006). Decreased coherence in higher frequency ranges (beta and gamma) between central and frontal EEG in patients with schizophrenia: a preliminary report. *Psychiatry Res.* 141, 53–60. doi: 10.1016/j.psychres.2005.07.016

**Conflict of Interest Statement:** The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

Received: 26 April 2014; accepted: 02 June 2014; published online: 01 July 2014.

Citation: Nakao K and Nakazawa K (2014) Brain state-dependent abnormal LFP activity in the auditory cortex of a schizophrenia mouse model. *Front. Neurosci.* 8:168. doi: 10.3389/fnins.2014.00168

This article was submitted to *Auditory Cognitive Neuroscience*, a section of the journal *Frontiers in Neuroscience*.

Copyright © 2014 Nakao and Nakazawa. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) or licensor are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.