



Diffusion Kurtosis Imaging of Microstructural Changes in Gray Matter Nucleus in Parkinson Disease

Gao Bingbing^{††}, Zhou Yujing^{††}, Miao Yanwei^{1*}, Dong Chunbo^{1*}, Wang Weiwei¹, Tian Shiyun¹, Liu Yangyingqiu¹, Shang Jin¹, Song Qingwei¹, Liu Ailian¹ and Xie Lizhi²

¹ Department of Radiology, First Affiliated Hospital of Dalian Medical University, Dalian, China, ² GE Healthcare, MR Research, Beijing, China

OPEN ACCESS

Edited by:

Yu Zhang,
VA Palo Alto Health Care System,
United States

Reviewed by:

Masaaki Hori,
Toho University, Japan
Brian Hansen,
Aarhus University, Denmark

*Correspondence:

Miao Yanwei
ywmiao716@163.com
Dong Chunbo
dcb101@sina.com

^{††}These authors have contributed
equally to this work

Specialty section:

This article was submitted to
Applied Neuroimaging,
a section of the journal
Frontiers in Neurology

Received: 07 November 2019

Accepted: 17 March 2020

Published: 17 April 2020

Citation:

Bingbing G, Yujing Z, Yanwei M,
Chunbo D, Weiwei W, Shiyun T,
Yangyingqiu L, Jin S, Qingwei S,
Ailian L and Lizhi X (2020) Diffusion
Kurtosis Imaging of Microstructural
Changes in Gray Matter Nucleus in
Parkinson Disease.
Front. Neurol. 11:252.
doi: 10.3389/fneur.2020.00252

Objective: To explore the microstructural damage of extrapyramidal system gray matter nuclei in Parkinson disease (PD) using diffusion kurtosis imaging (DKI).

Materials and Methods: We enrolled 35 clinically confirmed PD patients and 23 healthy volunteers. All patients underwent MR examination with conventional MRI scan sequences and an additional DKI sequence. We subsequently reconstructed the DKI raw images and analyzed the data. A radiologist in our hospital collected the Mini-Mental State Examination (MMSE) score of all subjects.

Results: In the PD group, the mean kurtosis and axial kurtosis level decreased in the red nucleus (RN) and thalamus; the radial kurtosis increased in the substantia nigra (SN) and globus pallidus (GP). Fractional anisotropy decreased in the putamen. The largest area under the ROC curve of mean diffusion in GP was 0.811. Most kurtosis parameters demonstrated a positive correlation with the MMSE score, while several diffusion parameters showed a negative correlation with the same.

Conclusion: DKI can qualitatively distinguish PD from healthy controls; furthermore, DKI-derived parameters can quantitatively evaluate the modifications of microstructures in extrapyramidal system gray matter nucleus in PD.

Keywords: parkinson disease, diffusion magnetic resonance imaging, gray matter, extrapyramidal tracts, neurodegenerative diseases

INTRODUCTION

Parkinson disease (PD) is the second most common neurodegenerative disease. Clinical diagnosis of PD is based on motor symptoms and signs including rest tremor, bradykinesia, rigidity and postural instability, and several variations of clinical scales. However, these symptoms are not particularly exclusive to PD, considering the fact that a number of other diseases have similar symptoms or atypical parkinsonian disorders. Due to this, the early diagnosis of PD is particularly difficult in clinical settings. This issue can be addressed by radiologists, by exploring the structural and functional changes in the brain of PD patients via various MR protocols. A previous study reported that neurons projecting from lateral nigra to posterior dorsal putamen were most severely affected by Lewy body pathology in PD (1). Volumetric analysis of basal ganglia nuclei and SN in patients with PD revealed tissue atrophy at the cortical, basal ganglia, and brainstem (particularly the SN and red nucleus, RN) levels (2); furthermore, the motor nerve conduction

among these were divided into the pyramidal and extrapyramidal systems. Pathophysiology and pathology of PD demonstrated that the diminution of the brainstem is attributed to the neurotic breakdown and necrosis in SN, which indicated the existence of microstructural changes inside the nucleus. Pathological studies also reported the presence of neurotic changes at levels of the cortex and basal ganglia (2). We hypothesized that there must be a connection inside the nuclei of the extrapyramidal system. Diffusion kurtosis imaging (DKI) offers improved sensitivity to tissue microstructure (3), which may be considered as an advantage over diffusion tensor imaging (DTI) (4). The basal ganglia and brainstem can be visualized in the DKI images (5). We aimed to investigate microstructural changes of extrapyramidal system nuclei in PD patients and its association with the disease progression, and to explore the connection of nuclei exchange between the levels of the basal ganglia and brainstem.

MATERIALS AND METHODS

Subjects

The prospective study was approved by local ethics committee, and each participant provided written consent. We enrolled 35 clinical diagnosed PD patients hospitalized in our hospital, along with 23 sex- and age-matched healthy controls (HC). PD was diagnosed based on the criteria provided by UK Parkinson Disease Society Brain Bank. The criteria also included the absolute exclusion criteria of PD, resulting in the exclusion of patients with hypertension and diabetes. The exclusion criteria for those in the HC group were history of surgery, cardiovascular disease, hypertension, diabetes, and other chronic diseases. The demographic and clinical data of the two groups are presented in **Table 1**. All patients and HC were right-handed. We assessed the Mini-Mental State Examination (MMSE) of all subjects; the MMSE score of all HC was above 27. Moreover, subjects with none or mild T2WI or T2 FLAIR high signal (Fazekas, grade 1) were considered normal. All subjects had no trauma, tumor, or a history of surgeries involving the central nervous system.

Images

Each subject underwent a GE Revolution CT scan of whole brain to exclude physiological or pathological calcification. All subjects underwent MR examination on a GE Signa HDxT 3.0 T MR scanner with a dedicated eight-channel head coil. The

protocols included routine axial T1-, T2-, and diffusion kurtosis weighted images. DKI was obtained using an echo-planar imaging technique with b values of 0, 1,000, and 2,000 s/mm^2 in 15 directions. Parameters of each protocol are described in **Table 2**. Scan baseline was parallel to the line running through the anterior commissure and the posterior commissure. Scan area ranged from the foramen magnum to the cranial vault.

DKI Interpretation

Quantitative Assessment

Initial DKI images of all subjects were reconstructed on ADW4.4 workstation with Functool 2 software using all b values. The reconstructive images included mean kurtosis image (MK), axial kurtosis image (Ka), radial kurtosis image (Kr), mean diffusivity image (MD), axial diffusivity image (Da), radial diffusivity image (Dr), and fractional anisotropy image (FA), and the parameters were recorded as MK, Ka, Kr, MD, Da, Dr, and FA, respectively (**Supplementary Table 2**). Small round region of interest (ROI) was drawn with a diameter of 3 mm at the center of the maximum level of target nucleus (**Supplementary Figure 1**), which included RN, SN, thalamus (T), putamen (P), globus pallidus (GP), and the head of caudate nuclei (HCN). The ROIs were manually drawn by two neuroradiologists in the same manner. To improve intra-observer reliability, the neuroradiologists performed the same measurements for all subjects three times and average the results. To evaluate interobserver reliability, the intraclass correlation coefficients (ICCs) were calculated.

Statistical Analysis

Demographic variables and MMSE scores were compared using two-tailed t tests and chi-squared tests. ICC test was calculated to evaluate interobserver reliability prior to data analysis. The consequent analysis would be performed if ICC test returned a consistent result (i.e., $ICC \geq 0.75$). The diffusion and kurtosis parameters of right and left deep gray matter structures were compared using two-sided Satterthwaite T test. Two independent-samples T tests or two-sample Mann-Whitney U tests were used to compare the parameters of six nuclei between two groups. We performed the receiver operating characteristic (ROC) test to assess the ability of distinguishing two groups for each DKI parameter of every nucleus. The correlations between DKI parameters and MMSE score were tested using Spearman's correlation test. All measurement data were presented as mean value and standard deviation. $P < 0.05$ was set to be statistically significant.

TABLE 1 | Clinical data of PD and HC groups.

	PD	HC
n	35	23
Age (years), mean \pm SD	67.00 \pm 8.76	66.48 \pm 5.20
Sex (M/F)	18/17	12/11
MMSE (score), mean \pm SD	22.91 \pm 4.27	29.91 \pm 0.42
Course (years)	3–10	—

All patients had been treated with dopamine agonists.

TABLE 2 | MRI protocol parameters.

Protocol	TR (ms)	TE (ms)	TI (ms)	Thick slices (mm)	Intersection (mm)	FOV (cm \times cm)	Matrix size
T1WI	2,500	25	/	6	1	22.0 \times 19.8	320 \times 256
T2WI	5,000	118	/	6	1	22.0 \times 19.8	320 \times 256
T2 Flair	9,000	172	2250	6	1	22.0 \times 22.0	256 \times 192
DKI	10,000	107	/	4	0	24.0 \times 24.0	128 \times 128

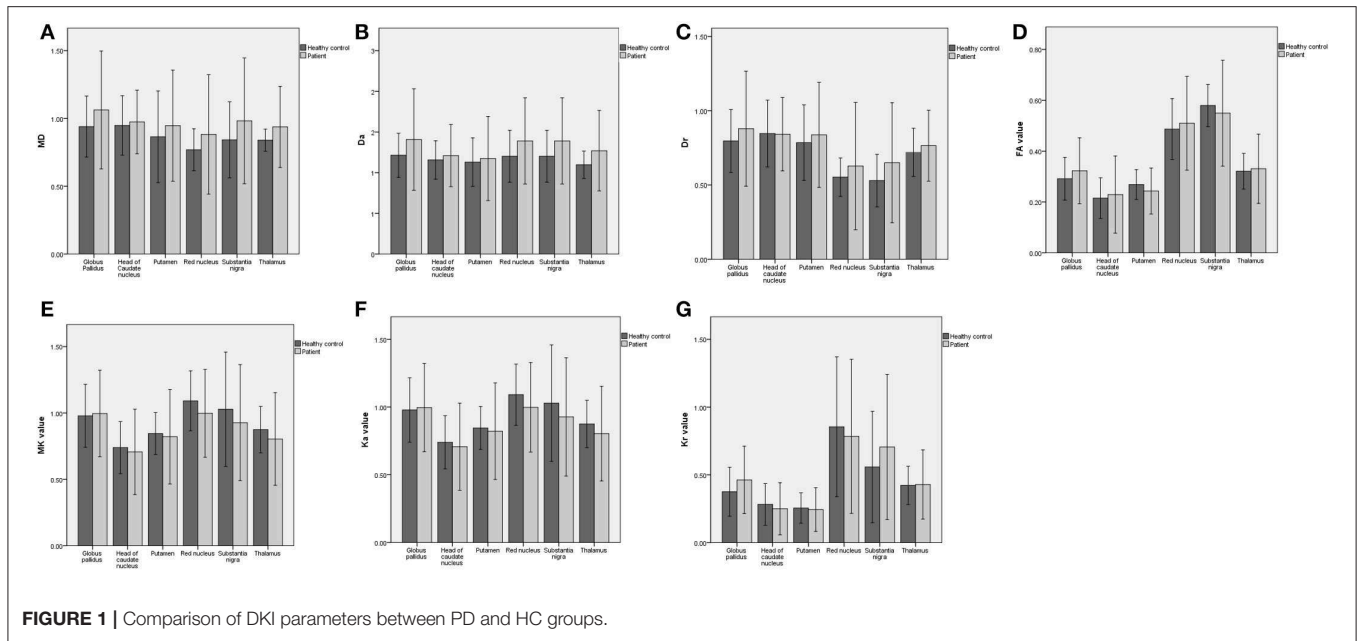


FIGURE 1 | Comparison of DKI parameters between PD and HC groups.

TABLE 3 | ROI analysis of DKI parameters of nuclei.

Nucleus	Parameter	Accuracy	Cutoff	Sensitivity	Specificity
GP	MD	0.811	0.979	0.657	0.870
RN	Da	0.796	1.285	0.686	0.783
SN	MD	0.775	0.900	0.714	0.826
GP	Da	0.763	1.450	0.457	1.000
SN	Da	0.742	1.560	0.714	0.826
SN	Dr	0.724	0.576	0.600	0.913
Putamen	MD	0.701	0.890	0.571	0.783

The bold values are statistically significant results.

RESULTS

Clinical Data

There were no observed significant differences between patient’s age ($t = 0.284, P = 0.777$) and sex ($\chi^2 = 0.069, P = 0.793$) between the two groups. However, there was a significant intergroup difference in the MMSE score ($t = 7.807, P = 0.000$).

DKI Data

The ICC values of all ROIs were >0.75 (shown in **Supplementary Table 1**). The results did not show any lateral difference in any of MK, Ka, Kr, MD, Da, Dr, and FA of each nucleus for all subjects ($P > 0.05$). Comparison of all the derived parameters between groups is presented in **Figure 1**.

ROC Analysis

The largest area under ROC curve (AUC) value of 0.811 was observed for MD in GP. MD of GP had a sensitivity, specificity, and accuracy of 65.7% (23 out of 35), 87% (30 out of 35), and

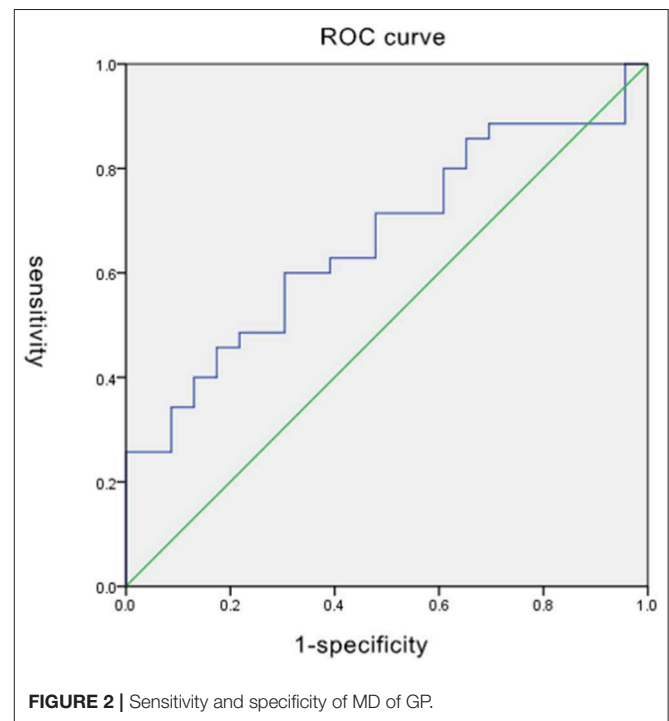


FIGURE 2 | Sensitivity and specificity of MD of GP.

81.1% (28 out of 35) when using a cutoff of 0.979 (shown in **Table 3** and **Figure 2**).

MMSE Score

The majority of the diffusion kurtosis parameters (MK, Ka, and Kr) demonstrated positive correlations with MMSE scores while the diffusion parameters exhibited several negative correlations (shown in **Tables 4, 5** and **Figure 3**).

TABLE 4 | The positive correlation of kurtosis parameters and MMSE scores.

Score	Nucleus		MK value	Ka value	Kr value
MMSE	Substantia nigra	<i>r</i>	0.284	0.389	0.130
		<i>P</i>	0.098	0.021	0.456
	Globus pallidus	<i>r</i>	0.428	0.458	0.340
		<i>P</i>	0.010	0.006	0.046
	Red nucleus	<i>r</i>	0.353	0.337	0.210
		<i>P</i>	0.038	0.048	0.226

r refers to the correlation coefficient, *P* is 95% confidence (two-tailed). The bold values are statistically significant results.

TABLE 5 | The negative correlation of diffusion parameters and MMSE scores.

Scores	Nucleus		MD value	Da value	Dr value
MMSE	Thalamus	<i>r</i>	-0.408	-0.384	-0.241
		<i>P</i>	0.015	0.023	0.163
	Head of caudate nucleus	<i>r</i>	-0.369	-0.280	-0.340
		<i>P</i>	0.029	0.104	0.045
	Red nucleus	<i>r</i>	-0.091	-0.354	-0.043
		<i>P</i>	0.602	0.037	0.805

r refers to the correlation coefficient, *P* is 95% confidence (two-tailed). The bold values are statistically significant results.

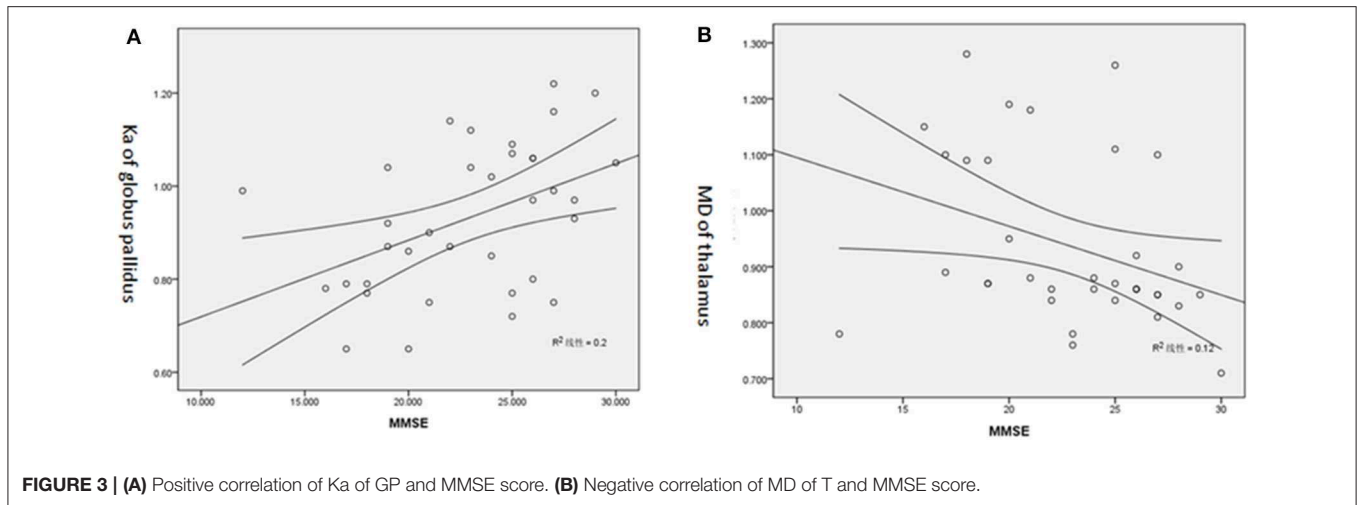
DISCUSSION

DKI parameters provide a quantitative analysis of PD, and certain derived parameters offer novel diagnostic perspectives. A previous report revealed that DKI was highly sensitive to microstructural changes in tissue, which is not typically highlighted by the diffusion coefficient value (6). We observed statistical differences of DKI parameters between PD patients and HC, among which MD of GP was the best biomarker for diagnosis. It is well-recognized that DKI is sensitive to capture the “complexity” of tissue microstructure; thus, it has already been extensively used to probe microstructural changes in normal aging. The FA and MK of frontal lobe, temporal lobe, corpus callosum (knee and splenium), thalamus, posterior limb of internal capsule, and head of the caudate nucleus decreased with aging; however, there was an increase in the MD levels (7, 8). Another study by Latt, which focused on healthy adults across different age groups, observed that MK of thalamus, white matter of frontal lobe, knee of corpus callosum, and centrum semiovale were negatively linearly correlated with aging (9). Overall, a pattern of increased MD and radial and axial diffusivity, together with decreased FA, MK, and radial and axial kurtosis in GM, was found in normal aging (9–12). These age-related alterations may possibly be driven by mixed effects of axonal disintegration, cell loss, and iron accumulation. In our research, MD, Da, and Dr in some deep GM of PD group appeared to be higher than that of the HC group. However, a specific pattern of increased Kr in SN and GP was found in PD, which has the highest iron concentration in the brain in PD (13). Therefore, one probable interpretation of our result is excessive deposition of iron, neuronal degeneration, and apoptosis in SN and GP in PD patients, especially along the “radial” direction. We speculate that the alterations in diffusion metrics in PD may reflect both iron-related and age-related microstructure changes, with a leading factor by the former. This idea is supported by earlier research about effect of cocaine addiction and age on the microstructure of striatum and thalamus using DKI (14). Pathological studies of PD patients suggested that microstructural changes occur from brainstem at an early stage and subsequently spread to the limbic system and the cortices (15, 16). Therefore, the goal of this present study was to assess the microstructural changes in extrapyramidal system and to elucidate its associations.

Diffusion and Kurtosis Parameters

Here, three diffusion parameters of the PD group appeared to be higher than that of the HC group. Studies have reported the presence of heterogeneous pathological encephalatrophy of brain in PD patients; additionally, the earliest onset was demonstrated in the SN and was considered as the most vulnerable structure (16). It was proposed that the dilated intercellular space caused by neuronal degeneration and apoptosis could enhance water molecule movement. Furthermore, the remaining areas of gray matter in PD patients may also experience a similar degree of modification. Damage in the neurons of the brainstem will lead to an accumulation of the materials in synapses of the nerve fibers transporting nutrients from cerebrum downward to the brainstem, resulting in the deficiency of nutritious materials in fibers from the brainstem downward to the spine. Both consequences will lead to secondary damage to adjacent structures and increase membrane permeability to facilitate the diffusion of water molecules.

Diffusion kurtosis parameters were associated with the complexity of structures, which varied across the diverse brain structures in healthy adults. The observed decline in the diffusion kurtosis parameters and FA may be due to neuronal degeneration and apoptosis combined with secondary damage of adjacent structures. Microglial cells are the most significant immune cells of brain. They distribute heterogeneously in brain, with their highest intensity being in the SN. In the resting (physiological) state, microglial cells provide a certain extent of protection to the central nervous system. While in the activated (pathological) state, they may cause damage to central nervous system by secreting varieties of interleukins and cytokines that are closely related to inflammatory reactions and neuronal repair (17, 18). The pathological examination of PD demonstrated a large number of activated microglial cells in the SN, with an even higher intensity in the areas of neuronal degeneration (19, 20). In addition to neuronal damage in the brain of PD patients, the formation of Lewy body, accumulation of microglial cells, and repair of neurons enhanced the complexity of tissue structures and resulted in the increase of diffusion kurtosis parameters. Here, PD patients were not categorized into subtypes according to an early or late clinical period or in consideration of shorter or longer disease duration. The decrease observed in MK, Ka, and FA of deep GM may be attributed to neuronal damage. The



increase of Kr in SN and GP may be due to the dominating effect of neuronal repair in the region.

DKI is an extension of DTI, which could reflect microstructural complexity, particularly in isotropic tissues such as gray matter (10). Some research focused on gray matter seemed more concerned with the overall diffusional metrics of MK, FA, and MD, rather than directional metrics such as axial diffusivity and radial kurtosis. This is because the GM microstructure lacks evident directionality that the radial and axial directions will be random and highly influenced by noise (21). However, a variety of changed Kr, Dr, Ka, and Kr in GM continue to be reported in normal aging (9–12, 22), in Moyamoya Disease (23), in Bipolar Disorders (24), and in various neurodegenerative processes including Alzheimer's disease (25, 26) and Parkinson's disease (27, 28). In fact, some of the deep GMs are composed of both gray matter and white matter (10, 29). The caudate nucleus includes the associative fibers projecting to the prefrontal cortex. The putamen contains projecting fibers from the primary motor and premotor cortices. Different from the caudate nucleus and putamen, the globus pallidus is rich in long, smooth, and sparsely branched neuronal dendrites that are well-protected by myelin. The red nucleus consists of densely packed cells and small myelinated axons (12, 30). These findings may suggest that varying proportion of white matter in the deep GM make motion of water restricted and directional. Actually, anisotropic water diffusion depends on oriented barriers. The deep GM is composed primarily of neurons and glia, which also have the highest iron deposits in the brain (12, 31). The myelinated axons, large cells, and ferritin protein constitute a complex microstructure that imposed extensive hindrance to free diffusion of water molecules. Thus, diffusion metrics in the deep GM appears to be different and more complicated than that in white matter. The degeneration of nigrostriatal dopaminergic neurons in the substantia nigra (SN) is the neuropathologic hallmark of PD (28). One previous study using the PD mouse model indicates that Dr in the SN is related with the numbers of SN dopaminergic neurons (32). As interesting findings in directional diffusion metrics

were observed in deep GM, we speculate that they are of potential significance in deep GM. However, their underlying pathophysiological meaning should be examined in further studies. In our study, all diffusion parameters including the directional ones were presented to provide a comprehensive view with potentially intriguing findings.

Diagnostic Efficiency of DKI Parameters

In our study, ROC analysis revealed that the MD for the globus pallidus had the best diagnostic performance. It is worth noting that, although the loss of dopaminergic neurons in the SN is the neuropathological hallmark in PD, the diffusion metric for the globus pallidus is the best biomarker to differentiate PD patients from HC. Globus pallidus is the most important relayed nucleus between striatum and subthalamic nuclei (STN) and plays an important role in the integration between inhibition from striatum and excitation from neocortex, thalamus, and STN (33). Changes in activity of neurotransmitters and related receptors along with abnormal synchronized oscillatory activity in the globus pallidus are associated with PD symptoms, such as bradykinesia, rigidity, and tremor, which reflects that globus pallidus plays an important role in the process of PD (34, 35). DBS researches have confirmed that stimulation of the globus pallidus is effective in reducing parkinsonian motor signs (36, 37). Among all the deep gray matter structures, globus pallidus has the relatively complex microstructural compositions and has the highest iron concentration in the brain (31). In summary, these results suggested that changed MD for the globus pallidus may reflect distinct pathological changes in PD. Future studies are needed to shed more light on the mechanisms underlying the changes in globus pallidus of patients with PD. Diffusivity parameters of RN and SN were useful; however, their sensitivity was not sufficiently high for clinical purposes. Alternatively, the diagnostic confidence was promoted with an accurate final diagnosis, considering that it is possible to employ these diagnostic parameters and that they may be applied in the form of assisted methods.

MMSE Score

The correlation between DKI parameters and MMSE in our subjects suggested that the changes in the microstructure detected by DKI corresponded to the psycho-neural state; therefore, further investigation of DKI may benefit PD patients with dementia. As discussed previously, when the neuron repair dominated a particular region, the damage to the central neural system was restrained. This indicated that the psycho-neural state would be better in cases with a higher MMSE score. Diffusivity parameters represent the severity of damage that occurs to the brain, with higher levels indicating greater damage and a lower MMSE score. Therefore, both diffusivity and kurtosis parameters work as independent biomarkers to assess the psycho-neural state of PD patients. It was of great importance to note that the kurtosis parameters correlating with MMSE was focused on GP, RN, and SN, which had the most complicated microstructural compositions (12). We speculate that microstructural “complexity” in GP, RN, and SN may be the basis of psycho-neural state in PD. Meanwhile, negative correlations with MMSE score were observed for axial, radial, and mean diffusivity of the thalamus and HCN in our study. The caudate nucleus and thalamus had a relatively simple microstructure, which were mostly constituted by neurons and glia (12). The diffusion parameters of these regions likely reflect the distribution of neuron cell bodies, synapses, and dendrites. This may suggest that the integrity of thalamus and HCN had potential correlation with the psycho-neural state in PD.

CONCLUSION

DKI can qualitatively distinguish PD from HC; furthermore, DKI-derived parameters can quantitatively evaluate the modifications of microstructures in extrapyramidal system gray matter nucleus in PD.

LIMITATIONS

One limitation of our study is that the spatial resolution is $1.875 \times 1.875 \times 4 \text{ mm}^3$. This may yield imperfect reference values and is thus biased. Another limitation is that treatment medication is not taken into account, the impact of which may lead to distorted brain structure. This needs to be explored in a future study.

REFERENCES

- Hughes AJ, Ben-Shlomo Y, Daniel SE, Lees AJ. What features improve the accuracy of clinical diagnosis in Parkinson's disease: a clinicopathologic study. *Neurology*. (1992) (2001) 57:S34–8.
- Geng DY, Li YX, Zee CS. Magnetic resonance imaging-based volumetric analysis of basal ganglia nuclei and substantia nigra in patients with Parkinson's disease. *Neurosurgery*. (2006) 58:256–62; discussion 256–62. doi: 10.1227/01.NEU.0000194845.19462.7B
- Hansen B, Jespersen SN. Recent developments in fast kurtosis imaging. *Front Phys*. (2017) 5:40. doi: 10.3389/fphy.2017.00040
- Kamagata K, Tomiyama H, Motoi Y, Kano M, Abe O, Ito K, et al. Diffusional kurtosis imaging of cingulate fibers in Parkinson disease: comparison with conventional diffusion tensor imaging. *Magnet Resonance Imaging*. (2013) 31:1501–6. doi: 10.1016/j.mri.2013.06.009
- Kamagata K, Tomiyama K, Hatano T, Motoi Y, Abe O, Shimoji K, et al. A preliminary diffusional kurtosis imaging study of Parkinson disease: comparison with conventional diffusion tensor imaging. *Neuroradiology*. (2014) 56:251–8. doi: 10.1007/s00234-014-1327-1
- Gloria C, Nie SD. Diffusion kurtosis imaging for diagnosis of Parkinson's disease: a novel software tool proposal. *J Xray Sci Technol*. (2017) 25:561–71.
- Coutu JP, Chen JJ, Rosas HD, Salat DH. Non-Gaussian water diffusion in aging white matter. *Neurobiol Aging*. (2014) 35:1412–21. doi: 10.1016/j.neurobiolaging.2013.12.001

DATA AVAILABILITY STATEMENT

The raw data supporting the conclusions of this article will be made available by the authors, without undue reservation, to any qualified researcher.

ETHICS STATEMENT

The studies involving human participants were reviewed and approved by Ethics Committee of First Affiliated Hospital of Dalian Medical University. The patients/participants provided their written informed consent to participate in this study.

AUTHOR CONTRIBUTIONS

GB, MY, and LA conceived the study and participated in its design, data collection. TS, LY, and WW participated in statistical analysis, sketching ROI and drafting of the manuscript. SJ, SQ, and XL participated in image reconstruction and data analysis. ZY and DC participated in the manuscript revise, including statistical analysis. The authors read and approved the final manuscript.

FUNDING

This study was supported by the National Natural Science Foundation of China (81671646, 81801657).

ACKNOWLEDGMENTS

The authors are grateful to the Department of Radiology, First Affiliated Hospital of Dalian Medical University, for supporting this study. The authors thank all patients and healthy control volunteers who participated in this study.

SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at: <https://www.frontiersin.org/articles/10.3389/fneur.2020.00252/full#supplementary-material>

8. Billiet T, Vandenbulcke M, Mädler B, Peeters R, Dhollander T, Zhang H, et al. Age-related microstructural differences quantified using myelin water imaging and advanced diffusion MRI. *Neurobiol Aging*. (2015) 36:2107–21. doi: 10.1016/j.neurobiolaging.2015.02.029
9. Lätt J, Nilsson M, Wirestam R, Ståhlberg F, Karlsson N, Johansson M, et al. Regional values of diffusional kurtosis estimates in the healthy brain. *J Magnet Resonan Imaging*. (2013) 37:610–8. doi: 10.1002/jmri.23857
10. Wang Q, Xu X, Zhang M. Normal aging in the basal ganglia evaluated by eigenvalues of diffusion tensor imaging. *AJNR*. (2010) 31:516–20. doi: 10.3174/ajnr.A1862
11. Vaillancourt DE, Spraker MB, Prodoehl J, Zhou XJ, Little DM. Effects of aging on the ventral and dorsal substantia nigra using diffusion tensor imaging. *Neurobiol Aging*. (2012) 33:35–42. doi: 10.1016/j.neurobiolaging.2010.02.006
12. Gong NJ, Wong CS, Chan CC, Leung LM, Chu YC. Aging in deep gray matter and white matter revealed by diffusional kurtosis imaging. *Neurobiol Aging*. (2014) 35:2203–16. doi: 10.1016/j.neurobiolaging.2014.03.011
13. McDonald C, Gordon G, Hand A, Walker RW, Fisher JM. 200 years of parkinson's disease: what have we learnt from James Parkinson? *Age Ageing*. (2018) 47:209–14. doi: 10.1093/ageing/afx196
14. Garza-Villarreal EA, Chakravarty MM, Hansen B, Eskildsen SF, Devenyi GA, Castillo-Padilla D, et al. The effect of crack cocaine addiction and age on the microstructure and morphology of the human striatum and thalamus using shape analysis and fast diffusion kurtosis imaging. *Transl Psychiatr*. (2017) 7:e1122. doi: 10.1038/tp.2017.92
15. Hughes AJ, Daniel SE, Kilford L, Lees AJ. Accuracy of clinical diagnosis of idiopathic Parkinson's disease: a clinico-pathological study of 100 cases. *J Neurol Neurosurg Psychiatr*. (1992) 55:181–4. doi: 10.1136/jnnp.55.3.181
16. Goedert M, Spillantini MG, Del Tredici K, Braak H. 100 years of lewy pathology. *Nat Rev Neurol*. (2013) 9:13–24. doi: 10.1038/nrneurol.2012.242
17. Shimura H, Hattori N, Kubo S, Mizuno Y, Asakawa S, Minoshima S, et al. Familial parkinson disease gene product, parkin, is a ubiquitin-protein ligase. *Nat Genet*. (2000) 25:302–5. doi: 10.1038/77060
18. Gorell JM, Ordridge RJ, Brown GG, Deniau JC, Buderer NM, Helpner JA. Increased iron-related MRI contrast in the substantia nigra in Parkinson's disease. *Neurology*. (1995) 45:1138–43. doi: 10.1212/WNL.45.6.1138
19. Koshimori Y, Ko JH, Mizrahi R, Rusjan P, Mabrouk R, Jacobs MF, et al. Imaging striatal microglial activation in patients with parkinson's disease. *PLoS ONE*. (2015) 10:e0138721. doi: 10.1371/journal.pone.0138721
20. Fan Z, Aman Y, Ahmed I, Chetelat G, Landeau B, Ray Chaudhuri K, et al. Influence of microglial activation on neuronal function in Alzheimer's and Parkinson's disease dementia. *Alzheim Dement*. (2015) 11:608–21.e7. doi: 10.1016/j.jalz.2014.06.016
21. Hansen B, Shemesh N, Jespersen SN. Fast imaging of mean, axial and radial diffusion kurtosis. *Neuroimage*. (2016) 142:381–93. doi: 10.1016/j.neuroimage.2016.08.022
22. Das SK, Wang JL, Bing L, Bhetuwal A, Yang HF. Regional values of diffusional kurtosis estimates in the healthy brain during normal aging. *Clin Neuroradiol*. (2017) 27:283–98. doi: 10.1007/s00062-015-0490-z
23. Qiao PG, Cheng X, Li GJ, Song P, Han C, Yang ZH. MR Diffusional kurtosis imaging-based assessment of brain microstructural changes in patients with moyamoya disease before and after revascularization. *AJNR*. (2020) 41:246–54. doi: 10.3174/ajnr.A6392
24. Zhao L, Wang Y, Jia Y, Zhong S, Sun Y, Zhou Z, et al. Microstructural abnormalities of basal ganglia and thalamus in bipolar and unipolar disorders: a diffusion kurtosis and perfusion imaging study. *Psychiatr Invest*. (2017) 14:471–82. doi: 10.4306/pi.2017.14.4.471
25. Falangola MF, Jensen JH, Tabesh A, Hu C, Deardorff RL, Babb JS, et al. Non-gaussian diffusion MRI assessment of brain microstructure in mild cognitive impairment and Alzheimer's disease. *Magnet Resonan Imag*. (2013) 31:840–6. doi: 10.1016/j.mri.2013.02.008
26. Gong NJ, Wong CS, Chan CC, Leung LM, Chu YC. Correlations between microstructural alterations and severity of cognitive deficiency in Alzheimer's disease and mild cognitive impairment: a diffusional kurtosis imaging study. *Magnet Resonan Imaging*. (2013) 31:688–94. doi: 10.1016/j.mri.2012.10.027
27. Nagae LM, Honce JM, Tanabe J, Shelton E, Sillau SH, Berman BD. Microstructural changes within the basal ganglia differ between parkinson disease subtypes. *Front Neuroanat*. (2016) 17:10. doi: 10.3389/fnana.2016.00017
28. Kamagata K, Zalesky A, Hatano T, Ueda R, Di Biase MA, Okuzumi A, et al. Gray matter abnormalities in idiopathic parkinson's disease: evaluation by diffusional kurtosis imaging and neurite orientation dispersion and density imaging. *Human Brain Mapp*. (2017) 38:3704–22. doi: 10.1002/hbm.23628
29. Si J, Chang L, Wang J, Zhang S, Yao Y, Zhang S, et al. Initial application of diffusional kurtosis imaging in evaluating brain development of healthy preterm infants. *PLoS ONE*. (2016) 11:e0154146. doi: 10.1371/journal.pone.0154146
30. Onodera S, Hicks TP. A comparative neuroanatomical study of the red nucleus of the cat, macaque and human. *PLoS ONE*. (2009) 4:e6623. doi: 10.1371/journal.pone.0006623
31. Haacke EM, Cheng NY, House MJ, Liu Q, Neelavalli J, Ogg RJ, et al. Imaging iron stores in the brain using magnetic resonance imaging. *Magnet Resonance Imaging*. (2005) 23:1–25. doi: 10.1016/j.mri.2004.10.001
32. Boska MD, Hasan KM, Kibuule D, Banerjee R, McIntyre E, Nelson JA, et al. Quantitative diffusion tensor imaging detects dopaminergic neuronal degeneration in a murine model of Parkinson's disease. *Neurobiol Dis*. (2007) 26:590–6. doi: 10.1016/j.nbd.2007.02.010
33. Langenecker SA, Briceno EM, Hamid NM, Nielson KA. An evaluation of distinct volumetric and functional MRI contributions toward understanding age and task performance: a study in the basal ganglia. *Brain Res*. (2007) 1135:58–68. doi: 10.1016/j.brainres.2006.11.068
34. Eusebio A, Brown P. Oscillatory activity in the basal ganglia. *Parkinson Related Disord*. (2007) S434–6. doi: 10.1016/S1353-8020(08)70044-0
35. Milosevic L, Gramer R, Kim TH, Algarni M, Fasano A, Kalia SK, et al. Modulation of inhibitory plasticity in basal ganglia output nuclei of patients with Parkinson's disease. *Neurobiol Dis*. (2019) 124:46–56. doi: 10.1016/j.nbd.2018.10.020
36. Follett KA, Weaver FM, Stern M, Hur K, Harris CL, Luo PM, et al. Pallidal versus subthalamic deep-brain stimulation for Parkinson's disease. *N Engl J Med*. (2010) 362:2077–91. doi: 10.1056/NEJMoa0907083
37. Fan SY, Wang KL, Hu W, Eisinger RS, Han A, Han CL, et al. Pallidal versus subthalamic nucleus deep brain stimulation for levodopa-induced dyskinesia. *Annals Clin Transl Neurol*. (2020) 7:59–68. doi: 10.1002/acn3.50961

Conflict of Interest: The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

Copyright © 2020 Bingbing, Yujing, Yanwei, Chunbo, Weiwei, Shiyun, Yangyingqiu, Jin, Qingwei, Ailian and Lizhi. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner(s) are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.