



# High-Velocity Shear and Soft Friction at the Nanometer Scale

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We study high-speed friction on soft polymer materials by measuring the amplitude dependence of cyclic lateral forces on the atomic force microscope (AFM) tip as it slides on the surface with fixed contact force. The resulting dynamic force quadrature curves separate the elastic and viscous contributions to the lateral force, revealing a transition from stick-slip to free-sliding motion as the velocity increases. We explain force quadratures and describe how they are measured, and we show results for a variety of soft materials. The results differ substantially from the measurements on hard materials, showing hysteresis in the force quadrature curves that we attribute to the finite relaxation time of viscoelastic surface deformation.

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## **1 INTRODUCTION**

Friction is a force that acts in opposition to the velocity of a sliding object. Unlike inertial force, which opposes a change in the velocity of an object with mass, friction is not associated with a fundamental property of matter. Friction depends on the structure and composition of the sliding surfaces, their relative velocity, the presence or absence of lubricant, and the contact force perpendicular to the plane of sliding. Most surfaces of contact are not perfectly planar and friction is concentrated at asperities or protrusions from the plane. The atomic force microscope (AFM) is an ideal instrument for measuring the force of friction on a single sliding asperity—the tip of an AFM probe. Here, we present measurements of friction forces on an AFM tip sliding on soft materials. We use a new method that allows for quantitative, nanometer-scale characterization of friction. We hope that this report will spark interest in using this method to study tribology of soft materials, a field of growing interest driven by a wide variety of applications in fields such as biology, food science, and health and personal care Liamas et al. (2020).

Friction gives rise to a lateral force **F** that is often assumed to be proportional to the contact force **N**, normal to the plane of sliding,  $|\mathbf{F}| = \mu |\mathbf{N}|$ . This contact force should include adhesion, which depends on the contact area. Adhesion can give rise to different regimes of friction with soft materials, as has been studied in macroscopic contacts Homola et al. (1990), Popov et al. (2021). At the microscopic scale of a single asperity, we expect the coefficient of friction  $\mu$  to depend on velocity. The Prandtl–Tomlinson model Popov (2010) describes velocity-dependent friction on a point-like asperity moving in a periodic potential, e.g., an AFM tip sliding along the atoms of a crystalline surface. At low velocity, the tip undergoes stick-slip motion, which crosses over to free-sliding motion at higher velocity. In a previous publication by Thorén et al. (2016), we have studied this crossover using a dynamic force measurement technique that we here apply to soft materials. Our previous results were well described by a modified Prantdel–Tomlisson model, which included an elastic or flexible AFM tip Krylov et al. (2006), Reimann and Evstigneev (2010), Martin-Jimenez et al. (2016). The Prandtl–Tomlison model may be well suited to describe friction on rigid crystalline surfaces, where the periodic atomic potential provides a natural length scale for slipping. However, this model is not a good starting point to describe friction on soft materials that are amorphous and have the ability to flow. Soft materials are both elastic and viscous and both of these properties should play a role in friction. For an asperity with a very small radius of curvature, such as an AFM tip, adhesive capillary forces can dominate the contact mechanics when the tip radius approaches the elastocapillary length  $L = \gamma/E$ , where  $\gamma$  is the interfacial energy of the contacting surfaces and *E* is the elastic modulus Style et al. (2013). In such situations, the soft material surface may appear more like a liquid than a solid to the sliding AFM tip.

Thus, a stiff tip sliding on a soft surface is related to the problem of lubrication and the question of the slip or no-slip boundary conditions at the fluid-solid interface Neto et al. (2005). AFM has been used to indirectly probe fluid slippage at the 10 µm scale by measuring the normal force needed to drain a viscous fluid when compressed between a flat surface and a colloidal probe Craig et al. (2001), Bonaccurso et al. (2002). At the macroscopic scale, the shear force between a fluid and a solid interface can be detected with a quartz crystal micro-balance (QCM) Johannsmann (2015). The QCM has MHz resonant frequency, which, together with the relatively large amplitude of the bulk shear mode, allows for sensitive dynamic measurement of force at high velocity, but without spatial resolution. Other methods detect fluid slippage on nanometer-scale particles but without the ability to scan and image a surface Chakraborty et al. (2021), Collis et al. (2020). The method presented here combines the advantages of high-frequency dynamic force measurement with the high spatial resolution of AFM.

Shear force on a sliding AFM tip is also measured with a mode of AFM known as Frictional Force Microscopy (FFM) Bennewitz (2015). FFM is often said to probe "dynamic friction" because force is measured when the tip is sliding at constant velocity. However, the measurement of force is actually quasi-static, by which we mean that the force transduction (i.e., conversion of lateral force at the tip to the measured torsion in the cantilever) is made under the assumption that the cantilever is in quasi-static mechanical equilibrium with the force of friction. While sliding, a change in the torsion signal corresponds to a change in the frictional force, allowing one to image friction. Comparing images at various load forces, controlled with the AFM scanning feedback, one can map the friction coefficient of a surface Álvarez-Asencio et al. (2013). For a fixed signal-tonoise ratio, spatial resolution scales inversely with sliding velocity.

Thus FFM relies on the notion that the lateral force due to friction is constant (quasi-static) during the time spent at each image pixel. Here, we employ a dynamic measurement of force, where the cantilever is rapidly oscillating through several hundred oscillation cycles of varying amplitude, all during the time needed to image one pixel (2 ms). The frictional force is measured as a perturbation to this oscillatory motion by capturing it in the frequency domain, where the motion consists of many frequency components close to a cantilever resonance Haviland (2017).



FIGURE 1 | Thermal noise and multifrequency lock-in spectra. (A) Measured noise-equivalent-deflection (NED) after 500 averages. The black curve is a fit to a model which sums independent contributions: a frequencydependent torsional noise of the cantilever and a frequency-independent noise of the detector. This fit calibrates the cantilever and detector, as explained in the text. (B) Measured response at 41 intermodulation product frequencies. Orange dots are the free response far away from the surface and blue bars are the engaged response. These spectra are a frequency-domain representation of the envelope modulating the rapid lateral oscillation of the tip. The time domain is shown in insets.

#### 2 MATERIALS AND METHODS

Dynamic transduction of force exploits a resonance with highquality Q to enhance the transducers' response to an external force at the oscillation frequency. This factor Q enhancement in responsivity leads to a proportional improvement in measurement sensitivity, the latter being specified by the limiting noise in the measurement. In our experiment, we use the fundamental torsional resonance of the cantilever with Q = 1,567.

Figure 1A demonstrates this enhanced sensitivity, showing a measurement of the power spectral density of the total noise when the tip is free from the surface. We express the noise as an equivalent lateral deflection of the tip. In a narrow band centered on resonance, we can resolve the transducers' intrinsic thermal noise above the detector noise background. This thermal torsion noise is actual fluctuations of the lateral motion of the tip caused by a frequency-independent torque noise (or lateral force noise at the tip). Resonance converts the torque noise to a frequency-dependent torsion noise, which comes to within a factor of two of the detector noise.

Dynamic force measurement also probes friction at a very high velocity. The high frequency of torsional resonance, in our case  $f_0 = 3.1$  MHz, results in sliding velocity  $v_{\text{max}} = A2\pi f_0 = 194$  cm/s for very small oscillation amplitude  $A \sim 10$  nm. This amplitude is roughly equal to the tip radius and it sets the image resolution when scanning.

We inertially actuate the torsional oscillation with a split-piezo shaker. As the tip oscillates back and forth in sinusodial sliding motion x(t), we resolve two components of the frictional force: a

TABLE 1   The different polymer samples studied. E-moduli for polymers a	re the
nominal value reported by the manufacturer.	

Material	E-modulus	Stiffness	<b>a</b> 0
Mica	~100 GPa	3.4 N/m	0.4 nm
Polystyren (PS)	2.7 GPa	6.5 N/m	2 nm
Low-density polyethylene (LDPE)	0.1 GPa	4.3 N/m	3 nm
Polydimethylsiloxane (PDMS)	3.5 MPa	4.2 N/m	-
Polydimethylsiloxane (PDMS)	2.5 MPa	4.1 N/m	-

conservative force  $F_I(A)$  in-phase with the harmonic motion and a dissipative force  $F_Q(A)$  in-phase with the velocity v(t) Haviland (2017).

$$x(t) = A\cos(\omega_0 t), \tag{1}$$

$$v(t) = A\omega_0 \sin(\omega_0 t), \qquad (2)$$

$$F_I(A) = \frac{1}{T} \int_0^T F(t) \cos(\omega_0 t) dt, \qquad (3)$$

$$F_Q(A) = \frac{1}{T} \int_0^T F(t) \sin(\omega_0 t) dt.$$
(4)

By slowly modulating *A* so that it remains approximately constant during the period of a single oscillation cycle  $T = 1/f_0 = 0.32\mu$ s, we reveal how these Fourier components of the frictional force behave as functions of *A*.

We perform the measurement in the frequency domain using a method called Intermodulation Frictional Force Microscopy (ImFFM) Intermodulation Products (2021). The slow modulation of *A* is made at a frequency  $\Delta f \ll f_0$  by driving the cantilever at two frequencies close to torsional resonance  $f_1 = n\Delta f$  and  $f_2 = (n + 1)\Delta f$ , where *n* is a large integer. The perturbing frictional force is nonlinear in the tip motion and therefore generates intermodulation products of the two drive frequencies, which form a dense comb of response at many frequencies close to resonance (see **Figure 1B**). A tuned multifrequency lock-in amplifier Intermodulation Products

(2021) performs the two-frequency excitation and captures the amplitude and phase of the response at 41 intermodulation product frequencies, at each pixel, while scanning at normal speeds for dynamic AFM. Application of the inverse Fourier transform allows one to directly extract the force quadrature curves  $F_I(A)$  and  $F_Q(A)$  without any assumptions or model of the interaction between the tip and surface Platz et al. (2013), Haviland (2017).

Our previous report demonstrated ImFFM on a hard surface Thorén et al. (2016). Here, we report a study of a variety of soft surfaces where we observed hysteresis in the force quadrature curves, i.e.,  $F_I(A)$  and  $F_Q(A)$ , which are different for increasing and decreasing amplitude. This hysteresis is indicative of relaxation of the surface deformation on a time-scale that is longer than the period T of the oscillatory sliding motion. We have explained the observed hysteresis of force quadratures seen in standard ImAFM using a moving surface model of the viscoelastic surface Thorén et al. (2018a). We have not yet derived a similar model for lateral surface deformation to explain the friction force quadratures presented here.

Quantitative measurement of force requires calibration of the transducer. For dynamic force measurement, we must determine three mode constants of the free resonance: stiffness k, mass m, and damping  $\eta$ , or equivalently, stiffness, resonance frequency  $\omega_0 = \sqrt{k/m}$ , and quality factor  $Q = \sqrt{km/\eta}$ . The latter two are found from the fit displayed in Figure 1A. If the detector responsivity (volt of detector signal per nanometer of lateral tip motion, V/nm) is known so that the motion noise is measured in  $m^2/Hz$ , the mode stiffness can be found through the application of the equipartition theorem with a calibrated measurement of the temperature of the surrounding medium Hutter and Bechhoefer (1993). Alternatively, we can use the "Sader method" Sader et al. (2016), whereby a model of the hydrodynamic damping is used to calculate the mode stiffness from  $\omega_0$  and Q. With this stiffness, we calibrate the detector responsivity using the equipartition theorem Higgins et al. (2006). We used this







latter approach to calibrate the single cantilever used for all measurements in this study.

We chose an AFM probe with relatively large flexural stiffness (nominal value 200 N/m, Bruker RTESPA-525) in order to counteract attractive tip-surface force so that we could adjust the loading force and avoid the jump-to-contact instability. The nominal tip radius is specified by the manufacturer to be 8 nm (max 12 nm). We measured the thermal motion noise of the lowest flexural mode, finding a resonance frequency of 516 kHz and quality factor 764. From a calculated hydrodynamic damping Sader et al. (2012), we calibrated the flexural stiffness to be 121 N/m.

The torsional mode is more difficult to calibrate because the thermal motion noise is a factor of two below the added noise of the detector. Nevertheless, with enough averaging of the noise data, a reasonable fit can be made (see **Figure 1A**), giving the lowest torsional resonance frequency  $f_0 = 3.1$  MHz and quality factor, Q = 1,500. We apply the method of Sader and Green to find the torsional stiffness Green et al. (2004), Thorén et al.

(2018b). With the manufacturer specified tip height of 17  $\mu m$ , we arrive at the stiffness to the frictional (lateral) force acting on the tip,  $k_t = 2700$  M/m Thorén et al. (2016). With this stiffness, we apply the equipartition theorem to find the responsivity of the detector to lateral tip motion.

Figure 1B shows the frequency content of torsional response when driven by two strong tones at the two central frequencies in the response spectrum. In the time domain, this free motion corresponds to a beating waveform (see inset to Figure 1B). Some weak intermodulation at non-driven frequencies is seen in the free spectrum above the noise level, indicating weak nonlinearity of the cantilever's torsional resonance. When the cantilever engages the surface, a much stronger intermodulation response is seen to very high order, well above the noise floor. Only the amplitude is plotted in Figure 1B, but the lock-in's ability to measure the phase at each frequency is crucial to the method.

The intermodulation spectrum is essentially a frequencydomain representation of the effect of friction on the envelope of the beating waveform. By downshifting the spectra and inverse Fourier transform, we compare the envelope of engaged motion to the envelope of free motion to extract the dynamic force quadrature curves  $F_I(A)$  and  $F_Q(A)$  Platz et al. (2013), Haviland (2017). When reconstructing the force quadrature curves, it is necessary to separate the tip-surface force from other long-range force contributions, such as electrostatic Law and Rieutord (2002) or lubrication Honig et al. (2010) forces. In order to isolate the frictional force from these "background" contributions, regardless of their origin, we use the method described by Borgani et al. Borgani et al. (2017).

We compare ImFFM measurements with the same cantilever and tip on five different material systems covering a wide range of stiffness, listed in **Table 1**. We perform a 2  $\mu$ m square scan of each sample, varying scanning feedback setpoint as the scan progresses. The result is a banded image shown for two representative scans in **Figure 2**, where each band corresponds to a different setpoint value, input to the software as a percentage of the free amplitude response at frequency  $f_1$ . The scanning feedback keeps the load force (vertical force) constant. However, we are not able to quantitatively measure the load force as the relatively stiff cantilever shows no discernible vertical deflection signal above the noise level.

The images of homogeneous materials are essentially featureless, as for mica (**Figure 2A**), indicating that the surfaces are either atomically flat (as expected for mica) or that our lateral force measurement is not sensitive to surface topography (roughness) at a scale corresponding to the maximum amplitude of oscillation  $A \sim 10$  nm. The polymer blend does exhibit a large circular domain of LDPE in the PS matrix (**Figure 2B**). The color in the images maps the highest velocity  $v_{max} = A2\pi f_0$  reached at every pixel.

### **3 RESULTS**

At each image pixel, we measure the amplitude dependence of frictional force quadratures  $F_I(A)$  and  $F_Q(A)$ , which are shown at a few representative pixels and setpoint values in **Figure 3**, for four different surface materials. We used a crystalline solid mica as a reference surface, on which we measured a response very similar to graphite reported on in our previous publication Thorén et al. (2016). At sufficient loading force (red curves in **Figure 3**), one observes a characteristic behavior. For small oscillation amplitude  $A \leq 0.25$  nm,  $F_I(A)$  shows a linear region. We showed that this region corresponds to the tip being stuck in a local minimum, where  $F_I(A) = \frac{1}{2}k_{tip}A$  so that the slope gives the tip stiffness.

On mica, when  $A \sim 0.5$  nm, corresponding to a few atomic lattice spacings,  $F_I(A)$  exhibits a broad minimum when the tip is sliding back and forth with stick-slip motion, oscillating between neighboring minima in the periodic atomic potential. With increasing A, stick-slip motion gives way to smooth sliding in the atomic potential, with  $F_I(A)$  typically decreasing on hard materials, such as graphite and mica. With increasing load  $|F_Q(A)|$  is always an increasing function of A, corresponding to increasing dissipation or energy loss due to friction. Qualitatively similar yet distinctly different behavior is seen on the softer materials. Recall that the same AFM tip is used for all materials. For both LDPE and PS (see **Figure 3**), we see the linear region at low A, but the measured slope is larger than on mica. The minimum in  $F_I(A)$  occurs at a much larger amplitude than it does on mica. Furthermore, we see hysteresis, where  $F_I(A)$  is larger for increasing A (lighter shade in **Figure 3**) and smaller for decreasing A (darker shade in **Figure 3**). For PDMS, we do not observe hysteresis and we find no distinct minimum in  $F_I(A)$  for the region probed in the force quadratures.

## **4 DISCUSSION**

We do not yet have a quantitative model to explain these experimental observations, but some features can be understood qualitatively. The low-amplitude slope of  $F_I(A)$  is somewhat larger for soft materials than that observed with hard materials, which may be explained by a conical tip penetrating deeper into the soft material, making the asperity stiffer to friction. This notion of deeper penetration into the material is also consistent with the minimum in  $F_I(A)$  occurring at larger A in the soft materials, compared to hard surfaces. The transition from the tip being stuck in the surface to stick-slip sliding motion is not associated with a crystalline lattice spacing in the soft material. Rather, it is conceivable that larger amplitude motion is needed to achieve free-sliding if the tip were buried deeper in a soft surface.

The hysteresis seen for LDPE and PS in **Figure 3** is indicative of a finite relaxation time for healing of the viscoelastic surface deformation caused by the sliding asperity. One observes hysteresis in  $F_I(A)$  and  $F_Q(A)$  when this relaxation or healing time is larger than the period of oscillation, in this case  $T = \frac{1}{f_0} = 0.32 \ \mu$ s. For linear viscoelastic forces, the relaxation time  $\tau = \eta/k$  is the ratio of the force constants associated with the tips lateral velocity ( $F_{\text{Visc}} = \eta \dot{x}$ ) and motion ( $F_{\text{Elast}} = kx$ ). The weak hysteresis seen in PDMS is explained by a faster relaxation time, due to its large elastic modulus (larger k) and apparently smaller viscous force constant (smaller  $\eta$ ). However, such analysis based on notions of linear force constants is only hand-waving and does not reveal any of the surely more complex nonlinear dynamics of the soft surface when subject to the sliding asperity.

### DATA AVAILABILITY STATEMENT

The raw data supporting the conclusion of this article will be made available by the authors, without undue reservation.

### AUTHOR CONTRIBUTIONS

All authors contributed to the development of the methods used in this manuscript. P-AT performed all measurements. P-AT and DH contributed to the writing of this article.

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**Conflict of Interest:** DH, RB and DF are part owners of Intermodulation Products AB, which manufactures and sells the equipment used in this research.

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