



# Nanogenerator-Based Sensors for Energy Harvesting From Cardiac Contraction

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Biomedical electric devices provide great assistance for health and life quality. However, their maintainable need remains a serious issue for the restricted duration of energy storage. Therefore, scientists are investigating alternative technologies such as nanogenerators that could harvest the mechanical energy of the human heart to act as the main source of energy for the pacemaker. Cardiac contraction is not a source for circulation; it utilizes body energy as an alternative energy source to recharge pacemaker devices. This is a key biomedical innovation to protect patients' lives from possible risks resulting from repeated surgery. A batteryless pacemaker is possible via an implantable energy collecting tool, exchanging the restriction of the current batteries for a sustainable self-energy resource technique. In this context, the physiology of heart energy in the preservation of blood distribution pulse generation and the effects of cardiac hormones on the heart's pacemaker shall be outlined. In this review, we summarized different technologies for the implantable energy harvesters and self-powered implantable medical devices with emphasis on nanogenerator-based sensors for energy harvesting from cardiac contraction. It could conclude that recent hybrid bio-nanogenerator systems of both piezoelectric and triboelectric devices based on biocompatible biomaterials and clean energy are promising biomedical devices for harvesting energy from cardiac and body movement. These implantable and wearable nanogenerators become self-powered biomedical tools with high efficacy, durability, thinness, flexibility, and low cost. Although many studies have proven their safety, there is a need for their long-term biosafety and biocompatibility. A further note on the biocompatibility of bio-generator sensors shall be addressed.

**Keywords:** pacemaker, heart, hormone, charge, nanogenerators, nanosensors, mechanical, electric energy

## INTRODUCTION

Bioelectronic device technology that can be implanted in the body has a life-saving function in organ damage, such as a pacemaker, and early diagnosis and follow-up of many diseases. Primitive electronic devices use batteries that can be controlled externally and are very sophisticated. In addition, performing long-term *in vivo* studies is not easy and may cause unintended outcomes for the patient who requires multiple high-risk operations repeatedly. For instance, sinoatrial (SA) node dysfunction and high-grade atrioventricular block require permanent pacemaker implantation (Da Costa et al., 2002). Millions of patients today use battery-dependent pacemakers, defibrillators, and other life-saving implantable devices that must be replaced every 5 to 10 years. Replacing implants after completing their lifetime requires surgery, which is costly and can cause complications and infection (Dong et al., 2019a). Current cardiac pacemakers utilize a battery power supply to maintain hearts beating regularly. In practice, a couple of problems such as difficulty in charging, insufficient battery life, and risk of restart still await solutions. This is hindered by the restricted duration of energy storage. Thus, a way for the battery-less pacemaker to harvest kinetic energy from the heart to sustainably power the device may be the ultimate solution (Melville, 2021). The body is rich in energy from the mechanical source such as the physical movements of the musculoskeletal system. Electromagnetic, piezoelectric, and triboelectric energy harvesting devices were investigated for converting biomechanical energy into electric type to be used as power for several wearable and implantable electronic devices. However, the complex construction, cost, in addition to challenges of these devices reduce the advancement and commercialization of the technology of bioenergy harvesters (Shi et al., 2019).

At this point, a nanogenerator is an ideal power supply that collects biomechanical energy from the heartbeat and harvests electrical signals for self-charging (Sun et al., 2021)

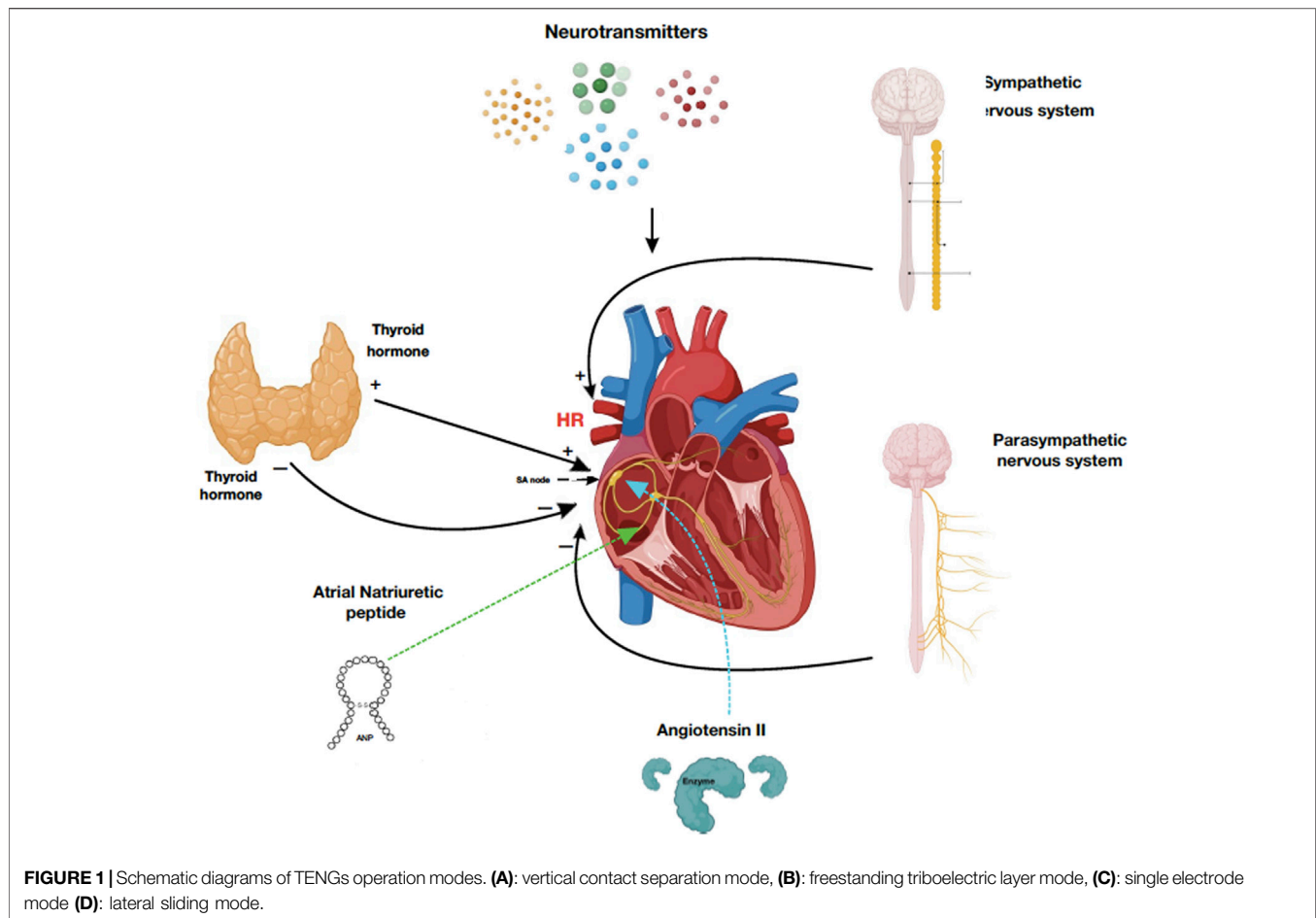
This review aims to cast some light on implantable energy harvesters and self-powered implantable medical devices, with emphasis on nanogenerator-based sensors for energy harvesting from cardiac contraction. Together with the physiology of pacemakers and the effect of hormones, limitations are comprehensively elucidated.

This review is focused on sustainable energy strategies for cardiac medical applications based on nanoscale devices. The topic covers the physiology of heart energy; pacemakers; key challenges; limitations; transformation of biomechanical activity into energy harvesters; design principles of piezoelectric, triboelectric, and pyroelectric nanogenerator-based devices; and considerations of biosafety and biocompatibility.

## PHYSIOLOGY OF NATURAL PACEMAKER AND THE EFFECT OF HORMONES

Every heartbeat is controlled and initiated by the sinoatrial (SA) node; it is the natural pacemaker of the heart. This tissue is controlled by circulating and locally released factors in addition

to the autonomic nervous system (MacDonald et al., 2020). The SA node is the natural initiator of the heart contraction and regulates the cardiac rhythm. The SA node is a collection of spindle-shaped myocytes located at the sulcus terminalis of the right atrium lateral to the superior vena cava junction. This specialized cluster of pacemaker cells generates 60–100 electrical impulses per minute that propagate through the heart conduction system, the atria, atrioventricular (AV) node, and bundle of His, reaching Purkinje fibers causing subsequent contraction. The activity of the SA node is interpreted *via* the P wave in the electrocardiogram (ECG). Dysfunctions in the SA node activity include sinus arrest, sinus arrhythmia, and SA node block characterized by an absent or varying P-P wave interval length in the ECG. Unlike other myocardial cells, the electrical activity of pacemaker cells has no resting phase, meaning that they go to the depolarization phase immediately after firing an action potential (Kashou et al., 2022). The autonomic nervous system (ANS) controls the activity of the SA node. For instance, the activation of the sympathetic nervous system increases heart rate (HR), while the parasympathetic nervous system reduces HR through its rest and digest response. This autonomic control allows for proper adaptation to physiological stressors. Neurotransmitters such as catecholamines (epinephrine and norepinephrine), serotonin, histamine, and acetylcholine influence the activity of the SA node (Gordan et al., 2015). In addition, different groups of hormones have a role in the physiology of pacemaker cells. For example, it is known that patients with hyperthyroidism experience an increase in HR (tachycardia), while those with hypothyroidism have a lower HR (bradycardia), which indicates the direct effect of thyroid hormones on the SA node (Valcavi et al., 1992) (**Figure 1**). Saito et al. found great quantities of Angiotensin II (ANGII) converting enzyme in the SA node, which may indicate its synthesis there (Saito et al., 1987). Another hormone family known as natriuretic peptides (NPs) are produced and stored in the atrial myocytes and have a role in the physiology and pathophysiology of the cardiovascular system. Brain natriuretic peptide (BNP) usually increases in conditions associated with heart failure and congestive heart failure (Cowie and Mendez, 2002). However, their direct effect on the SA node is not fully understood yet (MacDonald et al., 2020). A study conducted by La Villa et al. measured the atrial natriuretic peptide (ANP), brain NP (BNP), and arterial pressure in 15 patients with an implanted dual-chamber pacemaker and unimpaired heart function during ventricular pacing. Patients were ECG-monitored while receiving atrioventricular and ventricular pacing for 30 min with a constant rate of 80 beats/minute. An increase in plasma ANP was observed within 1 h in patients with atrioventricular dissociation with no change in both BNP and arterial pressure, while those with retrograde conduction had a significant increase in both ANP and BNP levels. However, the arterial pressure also remained unchanged. This indicates the presence of a dual NP peptide system composed of ANP in the atria and BNP in the ventricles (La Villa et al., 1994). All in all, the SA node is structurally heterogeneous. Hence, further work is needed for a complete, comprehensive understanding of the complex mechanisms involved in the neurohumoral control of SA node



function. The effects of many endocrine factors are summarized in **Table 1**.

## PHYSIOLOGY OF HEART ENERGY

The heart functions as a cyclic energy generator with two phases: internal and external loads. The internal load is the mechanical characteristics of the ventricle, while the external load is the characteristics of the arterial tree. Hydraulic energy is conveyed to blood as blood pressure and flow. Vascular resistance causes energy loss during steady flow. In contrast, the arterial tree adjusts blood pressure and flow through circulation (Muñoz and Sacco, 1997). The generally accepted paradigm of heart function is the pressure generated to maintain blood circulation. However, the heart's primary function is to generate pulse, not pressure. Blood circulation existed in the original direction even with the severe diseases of the heart valve, which is opposite to the physical law. With a non-functional heart valve, blood would flow from the main arteries toward the veins due to the pressure in the heart chamber (Papp, 2008).<sup>b</sup> Therefore, the circulation seems to be driven not only by the heart but also by a complementary driving mechanism exiting by the vessels. Blood vessels are involved in

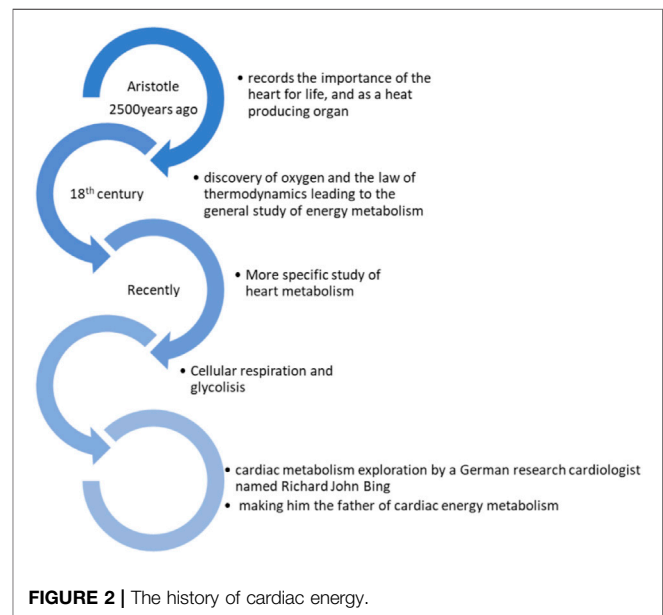
the driving mechanism for blood circulation, but the precise mechanism regarding how the blood vessels, especially the capillary, pump blood under stander pressure remains unclear (Thudichum, 1855; De Langen, 1951; Manteuffel-Szoegge, 1960; Furst, 2014). However, flow mechanisms play an essential part in the vascular system to drive from arteries to veins in the natural direction (Li and Pollack, 2020). Usually, tubular surfaces have a significant role in driving the intratubular flow due to the generated axial chemical concentration gradients (Rohani and Pollack, 2013; Yu et al., 2014; Li and Pollack, 2020). The determination of the surface-induced flow direction correlates with the intratubular concentration gradient direction. Nevertheless, certain factors control the direction of intratubular flow based on the tubular surface removal or induce substance and the change along the tube length of the surface to volume ratio. A vascular network has a group of vessels with the same diameter within each hierarchical level. According to Li and Pollack (2020), the flow can be predicted by assuming identical behavior in all vessel walls within each hierarchical level, in which the surface-to-volume ratio of these blood vessels is inversely proportional to their average diameter. Therefore, blood flow should circulate from narrower to wider vessels. Li and Pollack (2020) discovered a flow mechanism that can operate

**TABLE 1 |** Neurohormonal and endocrine control of sinoatrial node activity and heart rate.

Hormone/others	Effect on SAN	Effect on heart rate	References
Oxytocin	Unknown	Decrease	Jankowski et al. (2020)
Insulin treatment	Rescues from atrial fibrillation	Rescues	Maria et al. (2020)
Neurohormones	Increase/decrease	Increase/decrease	MacDonald et al. (2020)
Pharmacological glucagon	Increase contractility	Increase	Petersen et al. (2018)
Leptin	Deep bradycardia	Decrease	Lin et al. (2015)
Catecholamines	Increase firing rate	Increase	Larsson (2010)
Acetylcholine	Increase action potential duration	Decrease	Harvey (2012)
Histamine	Increase cAMP	Increase	Hattori et al. (2016)
Serotonin	Unknown	Increase/decrease	Linden et al. (1999)
Vasoactive intestinal peptide	Increase cAMP	Increase	Mangoni and Nargeot (2008)
Calcitonin gene-related peptide	Unknown	Increase	Fisher et al. (1988)
Neurotensin	Activation	Increase	Osadchii (2015)
Somatostatin	Unknown	Decrease	Bubiński et al. (1993)
Atrial natriuretic peptide (ANP)	Increase automaticity	Increase/decrease	Moghtadaei et al. (2016)
Adenosine	Decrease cAMP	Decrease	Headrick et al. (2013)
Angiotensin II	Decrease firing	No effect	Mehta and Griendling (2007)
Endothelin	Activation	Increase	Horinouchi et al. (2013)
Thyroid hormones	Activation	Increase	Mangoni and Nargeot (2008)
Parathyroid hormone	Increase cAMP	Increase	Potthoff et al. (2011)
Bradykinin	Unknown	Increase	Pian et al. (2007)
Relaxin	Increase firing rate	Increase	Han et al. (1994)
Nitric oxide	Increase cAMP	Modulation	Chowdhary et al. (2004)

without compulsory pressure. They used the infrared (IR) energy to verify the driving mechanism in blood vessels using an early chick embryo model. They tested the blood circulation under two states postmortem and in the normal physiological state using infrared (IR) energy. They demonstrated and confirmed the finding of the second circulatory mechanism originating from the blood vessels. Surface-induced flow originating from vessels can be driven by infrared radiation energy, which can appear naturally from metabolic heat and external sources. The metabolic activity in any organism would generate heat that is released in the IR energy form to facilitate circulation and nourish the tissues. Some cardiovascular diseases and novel therapies can be overcome in the future by appreciating this second circulatory existence (Li and Pollack, 2020).

The heart is an aerobic pump, oxidative substrates to generate energy. There is harmonic relation between myocardial oxygen use ( $MV_{O_2}$ ) and the essential factors of the systolic role: contractile state, heart rate, and wall stress. In a mechanical pump, not all the investing energy is transformed into an external force. In cardiac physiology, mechanical efficiency is the proportion of useful energy released (stroke work [SW]) to the oxygen utilized. In normal cases, this proportion is  $\approx 25\%$ , while the remaining energy at most recedes as heat, but in heart failure, mechanical efficiency is decreased, and it is supposed that the elevated expense of energy related to work participates in the progress of the disease. Therapy that enhances mechanical efficiency has evidenced its effectiveness in relation to outcome (Knaapen et al., 2007). The history of the heart discovery goes back to Aristotle's manuscripts 2,500 years ago, where he records the importance of the heart for life and as a heat-producing organ. In the 18th century, the discovery of oxygen and the idea of energy preservation (or the law of thermodynamics as known now) gave rise to the general study of energy metabolism and,

**FIGURE 2 |** The history of cardiac energy.

later, a more specific study of heart metabolism. Cellular respiration was understood more clearly with the discovery of glycolysis. Although many scientists researched energy metabolism, a German research cardiologist named Richard John Bing conducted cardiac metabolism exploration, making him the father of cardiac energy metabolism (Beloukas et al., 2013) **Figure 2**. Cardiometabolic disorders have been found to be linked to energy transduction by the myocardium. When the heart is failing, glycolysis and ketone oxidation occur, trying to meet the high energy demand of the continuously beating heart. The beneficial cardiac effects of some antidiabetic drugs are



facilitated partly by modified myocardial metabolism (Honka et al., 2021). Electrical stimulation of large mammalian ventricular heart surfaces was demonstrated at different stimulus strengths. Ventricular surfaces of pig hearts that span large areas were attached to long line electrodes and activated individually. It was found that endocardial stimulation activated more heart tissues than epicardial stimulation, making it a possible futuristic cardiac electrotherapy (Moreno et al., 2019). Batokines are secreted by brown adipose tissue (BAT), found to be the regulatory factors mostly studied in experimental models. Targets of batokines are the liver, heart, and skeletal muscle. In humans, the link between active BAT and a healthy metabolism may be explained by the endocrine role of BAT (Gavalda-Navarro et al., 2021).

## LIMITATION OF AVAILABLE CARDIAC IMPLANTABLE ELECTRONICS

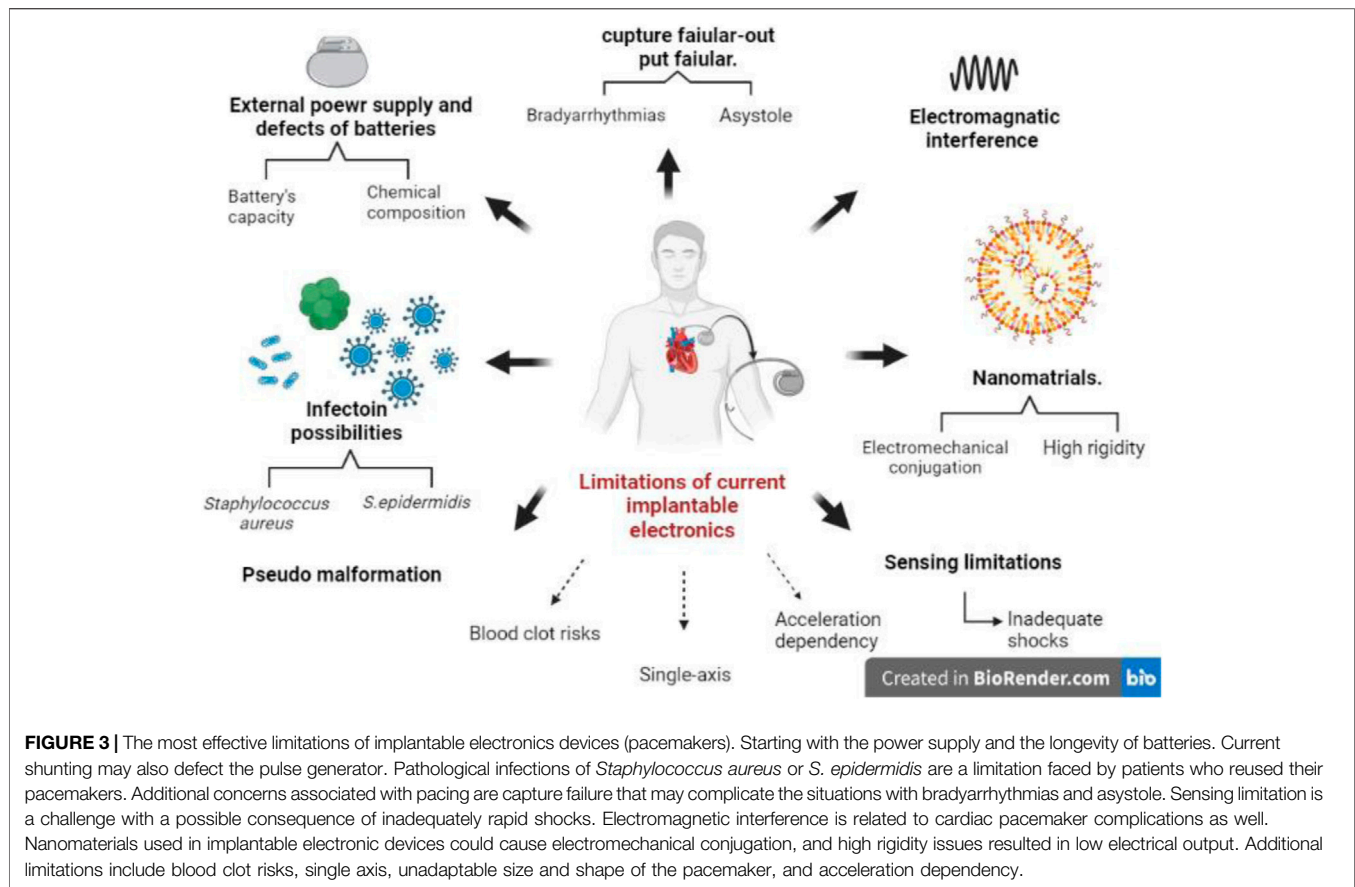
Implantable biomedical tools are commonly used for the treatment and monitoring of some disorders. An implantable heart pacemaker is the main current therapeutic device for remedying bradyarrhythmia, but its replacement surgically is unavoidable each 5–12 years because of the restricted life of its built-in battery (Li et al., 2019). Sensor technology has recorded considerable advances, particularly because of the evolution of materials and the emergence of new technologies such as nanotechnology, thereby necessitating the exploration of novel opportunities. Implantable electronic devices are examples of such explorations in the healthcare sector, largely transforming therapeutic interventions for cardiac arrhythmias (Surendran et al., 2021). However, this technology requires an external power supply, which might pose other problems (Li et al., 2020). These devices are thus associated with several complications, which must be identified and addressed to prevent undesirable outcomes. One of these limitations is associated with the external power supply, particularly the defects in batteries. According to Hauser et al., possible battery longevity issues may also be characterized by the battery's current capacity and its chemical characteristics (Hauser et al., 2021). Additional factors include housekeeping current drain, percent pacing, and lead impedance. Furthermore, current shunting challenges may also be associated with possible defects of the pulse generator. Another major limitation of cardiac pacemakers includes electromagnetic interferences from cellular devices, security systems, medical equipment, power generators, and wireless chargers. Although this limitation is scantily covered in the literature, available studies argue that electromagnetic fields can influence the performance of pacemakers by inhibiting pacing. According to Huang et al., this issue may be reduced by twisting excess leads (Huang et al., 2020). Unfortunately, even leads are bound to fail, which may aggravate the situation, potentially causing implantable cardioverter-defibrillator (ICD) system-based morbidity and mortality. Consequences of lead failure include pacing inhibition and inappropriate ICD shocks. One way of monitoring this limitation is by manipulating the Lead

Integrity Alert, which, unfortunately, is also limited by its algorithm dependence (Kella and Stambler, 2021). Additional limitations are associated with nanotechnology and nanomaterial. For instance, the piezoelectricity and biocompatibility of various nanoparticles, such as ZnO, face electromechanical coupling issues and high rigidity concerns, thereby necessitating only a considerably low electrical output, which prevents further explorations (Li and Wang, 2021). This implies that the number of usable nanocrystals is limited. The impact of cardiac pacemakers cannot be overemphasized, owing to their abilities to prolong patient life. However, access to this vital device is problematic, particularly in regions with few supporting resources. According to Khairy et al., the lack of these supportive systems inhibits re-sterilization and reuse, which in turn affects their performance or viability, mainly because of infection possibilities. According to them, patients who reused their devices had a high likelihood of contracting infections. Pathogens associated with the infections included *Staphylococcus aureus* and *S. epidermidis* (Khairy et al., 2020). Patients are also prone to other forms of problems, which are associated with either pacing or sensing. Limitations associated with pacing include output failure and capture failure. Possible consequences include bradyarrhythmias and asystole. Sensing limitations include under-sensing and over-sensing, which can deliver inappropriate shocks. Pseudomalformation limitations include fusion and pseudo-fusion, pacemaker crosstalk, and ventricular safety pacing (Liaquat et al., 2021). The upper rate behavior, pacemaker mediated tachycardia, and runaway pacemakers are additional limitations. Apart from limitations of battery, which reduced life expectancy of cardiac pacemakers, Franzina et al. noted that other concerns of invasive implantation, blood clot risks, single-axis acceleration dependency, and unadaptable size and shape of pacemakers, owing to the heart environments are considerable limitations (Franzina et al., 2020). **Figure 3** summarizes these crucial limitations and demands prompt attention to facilitate the future of implantable electronic devices.

## TRANSFORMATION OF BIOMECHANICAL VIBRATION (MOVEMENT) INTO NANO-ENERGY GENERATOR

Implantable medical devices (IMDs) are becoming an important tool for enhancing patients' longevity and quality of life. The latest research on this topic is to overcome those limitations and focus on internal charging using energy produced by body activities. Piezoelectric nanogenerator (PENG) and triboelectric nanogenerator (TENG) energy harvesters with sophisticated structural and material designs have been developed to harvest biomechanical energy efficiently. The human body holds diverse forms of energy in it, including chemical, heat, and mechanical energy. The nanogenerator, a device capable of converting mechanical energy into electric energy, was developed in 2006 and has been used in various ways as a self-powered sensor since then (Li et al., 2020).

Medical devices are powered by energy from body movements, such as contraction and relaxation of muscles,



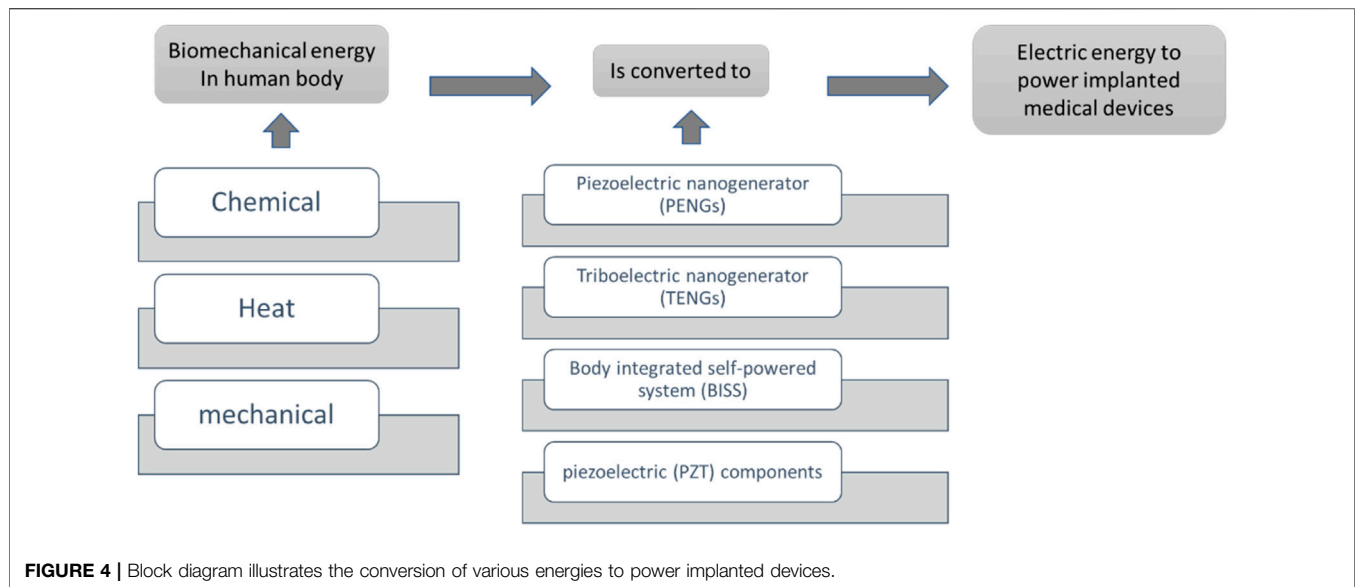
**FIGURE 3 |** The most effective limitations of implantable electronics devices (pacemakers). Starting with the power supply and the longevity of batteries. Current shunting may also defect the pulse generator. Pathological infections of *Staphylococcus aureus* or *S. epidermidis* are a limitation faced by patients who reused their pacemakers. Additional concerns associated with pacing are capture failure that may complicate the situations with bradyarrhythmias and asystole. Sensing limitation is a challenge with a possible consequence of inadequately rapid shocks. Electromagnetic interference is related to cardiac pacemaker complications as well. Nanomaterials used in implantable electronic devices could cause electromechanical conjugation, and high rigidity issues resulted in low electrical output. Additional limitations include blood clot risks, single axis, unadaptable size and shape of the pacemaker, and acceleration dependency.

motions of the heart and lungs, and circulation of the blood. More recently, PENGs and TENGs are utilized. Self-powered medical systems are futuristic opportunities for biodegradable, flexible, and intelligent devices that monitor and treat disease (Zheng et al., 2017). The body integrated self-powered system (BISS) is a highly efficient and economic technology to hunt energy from biomechanical energy in the human body, which can be harvested through an electrode tool close to the skin. The main rule of the BISS is enthused by the inclusive function of triboelectrification among soles and ground and human's electrification. The technical feasibility has been proven to power electronic devices using the BISS either *in vitro* or *in vivo*. BISS shows an amazingly simple, cost-effective, and appropriate tactic for producing energy from human movement, with promising applications for wearable and implantable electronic devices (Shi et al., 2019). Although many energy harvesting strategies were discovered in recent years, they were not efficiently applied. Thus, many strategies for straight firing a contemporary and functional cardiac pacemaker have been investigated, which pace the heart of porcine *in vivo* through harvesting its energy from heartbeats, free from any external energy source. The energy harvester consists of an elastic structure and two piezoelectric compounds that could produce an elevated-output current of  $15 \mu\text{A}$  *in vivo* with the state-of-the-art function. This strategy resolved the energy shortage of implantable devices

using energy harvesting by piezoelectric (PZT) components (Li et al., 2019).

*In vivo* real-time monitoring of human physiological activities and treatment of diseases are developed to replace the use of large instruments such as the electrocardiogram (ECG) monitor and electroencephalograph (EEG). New devices such as the pulse generator for brain stimulation and other implantable devices are rapidly developed for flexibility and portability (Xia et al., 2020; Jiang et al., 2021). However, one of the challenges of using these devices includes frequent battery replacement due to a short lifespan.

Energy harvesting and vibration sensing may utilize PZT components, which are available and well established, yet alterations are proposed to improve large-scale vibration energy harvesting (Eghbali et al., 2020). In industry, energy harvesting can be accomplished by cantilever oscillators covered by a layer of piezoelectric material (Tommasino et al., 2022). PZT components can convert mechanical pressure applied to them to electrical signals, and the opposite applies as well. This ability may be used to harvest mechanical energy from human motion and vibrations to electrical energy to power small devices (Mahapatra et al., 2021). Devices that harvest energy will avoid patients from additional surgical interventions and the possibility of miniaturizing existing pacemakers and defibrillators. Another study used an automatic wristwatch as an energy harvesting device, converting cardiac wall motion (kinetic energy) to



electrical energy. Motion analysis of the left ventricle based on MRI showed that the basal region was the most favorable for energy harvesting. It refers to the researchers of study of (Zurbuchen et al., 2013). We can say: The study also developed a mathematical model to optimize the device's configuration. An *in vitro* experiment validated the model as a robot arm reproducing the cardiac motion. Another *in vivo* experiment also validated the model as the device was attached to a sheep heart for 1 h. Both experiments generated enough energy to power a modern pacemaker (*in vitro* 30  $\mu\text{W}$  and *in vivo* 16.7  $\mu\text{W}$ ) (Zurbuchen et al., 2013). Piezoelectric energy harvesting may occur through the contractile and relaxation motion of the diaphragm, lungs, and heart. This has been studied in animal models with organ sizes close to human organ size (Dagdeviren et al., 2014). Regular medical follow-ups are required to ensure optimal functioning of cardiac pacemakers. ~25% of pacemaker replacements are due to battery depletion. In addition, the specialized wire (pacemaker lead) that delivers energy from the pacemaker to the heart muscle is subjected to dislocations and fractures, and harvesting endocardial energy at favorable locations may assist in the drawbacks of typical pacemakers (Zurbuchen et al., 2017). Researchers harvested energy from the cardiac valvular movement to power a wireless sonomicrometry sensor, where piezoelectric sutures were placed close to the valvular regions using the valve movement for self-powering. It was found that the range of harvested energy would be from nano-watts to milli-watts. The highest amount of the harvested energy was from the leaflet plane (Kondapalli et al., 2018). Wearable technologies are increasing, and the demand for novel methods for powering these devices is met through new energy harvesting materials such as the piezoelectric polymer. Mokhtari et al. developed a polyvinylidene fluoride (PVDF)/LiCl electrospun nanofiber, using it in a nanogenerator package that is flexible and lightweight. This nanogenerator could generate voltage and current output of 3 V and 0.5  $\mu\text{A}$  with a power density output of

0.3  $\mu\text{W cm}^{-2}$  at the frequency of 200 Hz. This energy harvesting material has promising applications for self-power electrical devices (Mokhtari et al., 2020). **Figure 4.**

## NANOGENERATOR-BASED SENSOR FOR ENERGY HARVESTING FROM CARDIAC CONTRACTION

The electric nanogenerator (ENG) is an ideal power supply that extracts and converts the energy from physiological activities such as blood flow, heartbeat, muscle contraction, body movement, respiration, and body heat to produce electrical energy. ENGs possess a promising role in terms of medical applications such as tissue repairing, pathological indicators, neural stimulators, and cardiac pacemakers (Bhatia et al., 2010; Sun et al., 2021). Generally, ENGs can be classified into three categories based on the electrical production mode known piezoelectric nanogenerator (PENG) (Bhatia et al., 2010), triboelectric nanogenerator (TENG) (Wang, 2013), and pyroelectric nanogenerator (PYENG) (Yang et al., 2012).

### Piezoelectric Nanogenerator

The invention of the piezoelectric nanogenerator by Z. L. Wang (Li Z. et al., 2020; Zagabathuni and Kanagaraj, 2022) was a development that led to the functioning of biological devices without the need for a battery or external power source. Bio-nanogenerators capture mechanical energy generated from body movement and convert it into electrical energy to drive the function of implanted medical devices (Li Z. et al., 2020; Jiang et al., 2021; Zagabathuni and Kanagaraj, 2022). Recently medical implants, sensors, and wearable devices harvest energy using piezoelectric nanogenerators (Jiang et al., 2020). Inorganic materials such as wurtzite semiconductors are used in piezoelectric materials utilized in different sensors and actuators (Wang R et al., 2021; Dahiya et al., 2018); piezoelectric ceramics

with high dielectric and piezoelectric properties (Dudem et al., 2018; Hyeon and Park, 2019); and organic materials, such as PVDF and its copolymer P(VDF-TrFE) (Dong et al., 2019b).

The human body contains energy in different forms, including thermal, chemical, and mechanical energy. Amongst them, mechanical energy is the most abundant form in which PENG can transform into electricity. This was firstly invented by Zhong Lin Wang in 2006 (Wang, 2007). PENG is composed of piezoelectric materials, flexible substrates, and external electrodes. The core component of PENG is piezoelectric material in which the electric current generated due to the crystal deformation in response to the changes in the condition of the body parameters includes blood vessels contractions and other physiological mechanical activities (Bhatia et al., 2010). The mutual transformation between mechanical and electrical energy can be recognized by the piezoelectric effect. Thus, when the piezoelectric material is exposed to external pressure, an electric dipole moment will be produced because of the mutual displacements of cations and anions in the crystal. As a result, the electric potential difference is generated in the tension direction of the material. Therefore, the continuous electrical pulse could be produced in the external circuit as the mechanical force applied to the PENG (Jiang et al., 2020; Li Z. et al., 2020). Typically, inorganic piezoelectric materials such as ZnO (Zhao et al., 2014; Murillo et al., 2017), lead zirconate titanate (PZT) (Dagdeviren et al., 2017), barium titanate (BT) (Jiang et al., 2019), and organic polyvinylidene fluoride (PVDF) (Yu et al., 2020) are the most commonly used in PENG for wearable and implantable medical devices. ZnO and PVDF exhibit lightweight with great flexibility; hence, they are suitable for multidimensional deformation applications, including wearable biosensors. In contrast, PZT- and BT-based devices are suitable for energy harvesting where they possess a high piezoelectric strain constant (Li Z. et al., 2020). In order to obtain good stability and high output, the appropriate structure of PENG has developed from single nanowires to films. Taking ZnO nanowires as an example, it has a wurtzite structure in which  $\text{Zn}^{2+}$  and  $\text{O}^{2-}$  coordinate to form tetrahedral in the crystal structure. The piezoelectric effect of ZnO appears in the lack of central symmetry of the wurtzite structure. In the beginning, the cations and anions centers are coincided with each other due to the absence of the strain. However, when the external force is applied, the crystal structure is deformed and the charge centers are separated from each other, resulting in an electric dipole. The generated electric potential is preserved as long as the mechanical force is applied. Thus, the output current will be driven through the external load when ZnO nanowires are connected to an external circuit. The working mechanism of the other materials is similar to ZnO nanowires (Wang et al., 2010; Li X. et al., 2020; Sun et al., 2021). Cheng et al. reported the usage of piezoelectric thin film for harvesting mechanical energy to electricity through the contraction and expansion of the aorta. They conducted an *in vivo* ENGs examination of piezoelectric PVDF *via* wrapping it around the ascending aorta of a pig. The obtained outpower was 40 nW (Cheng et al., 2016). Kondapalli et al. used PENG to harvest energy from cardiac valvular perturbations for wireless powering sonomicrometry sensors (Kondapalli et al., 2018).

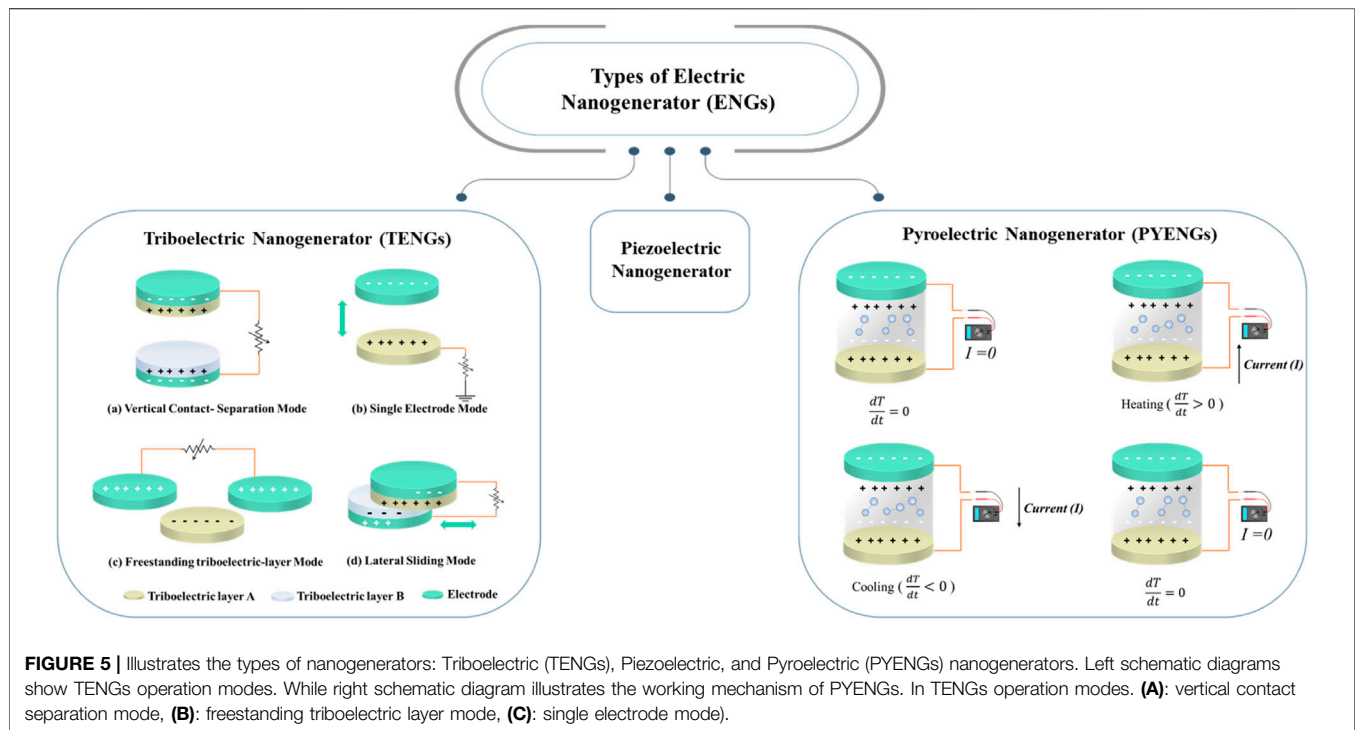
Han et al. created different three-dimensional piezoelectric microsystems and demonstrated their application in mechanical energy harvesting *in vivo* (Han et al., 2019). Two and three-component nanohybrids are used for energy harvesting in the form of a bio-based piezoelectric eggshell membrane (ESM). A bio-waste piezo-filler in a piezoelectric polymer matrix was designed using organically modified two-dimensional nanoclay. These nanohybrid materials are appropriate for energy harvesting. The effectiveness of the device was tested using a range of body movements leading to energy storage. The hybrid device is a strong nanogenerator as it is durable and mechanically stable for repeated energy conversion. Cellular studies also found it suitable for powering biomedical devices and implants (Gaur et al., 2019).

## Triboelectric Nanogenerator

Triboelectric nanogenerator sensors are highly sensitive detectors of mechanical energy and provide a high-quality amount of electrical energy output. They are easily activated by slight motions of the ribcage during respiration, heart contraction, blood flow, and gastric peristalsis (Ouyang et al., 2019; Xia et al., 2020; Sun et al., 2021). This attribute makes this sensor worthy of *in vivo* biomedical monitoring (Xia et al., 2020; Sun et al., 2021).

The triboelectrification effect is quite common in our daily life. It appears at the interface between two different contacted materials. The power generation mechanism of triboelectric nanogenerator (TENG) relies on the coupling of two principles: triboelectricity and electrostatic induction (Wang et al., 2015). The electrostatic charges are generated because of the triboelectrification effect, where the material becomes electrically charged after two friction surfaces are brought into contact. The friction layers could carry the opposite signs with the same number of triboelectric charges after separation, forming an electrostatic field and driving the electrons' movement through the external circuit (Jiang et al., 2020; Sun et al., 2021). TENG exhibited large output power with large corresponding charge transfer when the materials were significantly different in the frictional electric sequences. According to the structure of two friction layers and the connection of the external load, the working modes of TENG were categorized into four groups as shown in **Figure 5**: lateral sliding mode, vertical contact separation mode, freestanding triboelectric layer mode, and single electrode mode (Jiang et al., 2020; Li X. et al., 2020; Sun et al., 2021). TENG utilized the energy from muscle movement, heartbeat, and respiration as a source of biomechanical energy for disease treatment and physiological signal detection (Sun et al., 2021). In 2019, Ouyang et al. designed a pacemaker based on TENG, which harvested energy from heart motion (Ouyang et al., 2019). Furthermore, Shi et al. designed a body-integrated self-powered system based on TENG for harvesting biomechanical energy from body movements (Shi et al., 2019). Li et al. prepared biodegradable TENG modified by gold nanorods that possess stability for more than 28 days *in vivo* (Li Z et al., 2018). Moreover, biodegradable TENG has been fabricated by Jiang et al. and implemented in the dorsal subcutaneous region of rats, where the maximum voltage, current, and power density reach up to 55 V, 0.6  $\mu\text{A}$ , and 21.6  $\text{mW}/\text{m}^2$ , respectively.





## Pyroelectric Nanogenerator

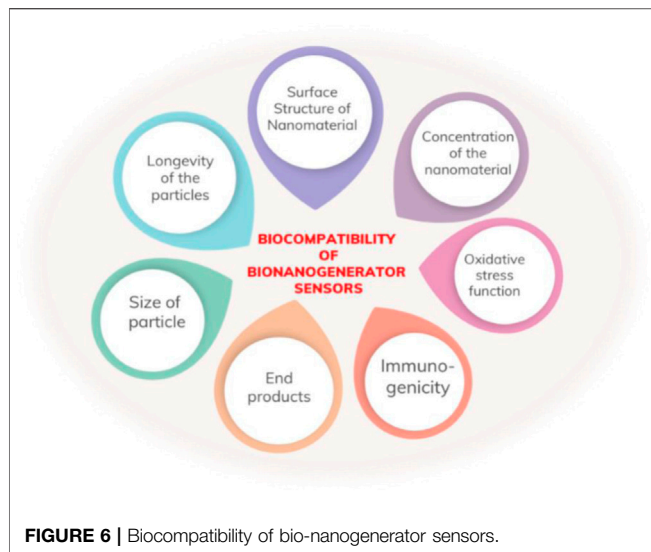
A pyroelectric nanogenerator (PYENG) is a thermoelectric energy harvesting device that can convert heat energy into electrical energy. The working principle of PYENG is based on the Seebeck effect (Yang et al., 2012), which utilizes a temperature gradient to polarize nanomaterials driving the charge diffusion. The spontaneous polarization of pyroelectric materials changes with the temperature variation when exposed to heat that transforms the surface bounded charge causing current output. In the absence of temperature difference, the spontaneous polarization of pyroelectric material remains unchanged, and no current is generated. However, once the temperature rises with time, the polarization density will decrease and generate the pyroelectric current to an external circuit until reaching the equilibrium state. On the contrary, when the temperature of the medium decreases, such as cooling the material, the polarization density will increase, generating a reverse current in the external circuit until an equilibrium is reached, as illustrated in Figure 5 (Li X. et al., 2020; Sun et al., 2021). Sultana et al. reported the fabrication of PYENG that harvested the waste body heat from the respiration process and body surface. It can detect human heat, work as a temperature sensor, and monitor the respiratory process. The produced output reached 1.5 V and 1.5  $\mu$ A (Sultana et al., 2018).

## BIOCOMPATIBILITY OF BIO-NANOGENERATOR SENSORS

Due to the persistent mechanical activities in human bodies, it is expected that materials placed inside the body should have the strength to withstand continuous movements. An implantable

cardiac device, for example, should meet certain standards so that it can stand the constant heart contractions without injuring the body through toxicity or stimulation of an adverse immune response is said to be biocompatible (Suvaneeth and Nair, 2018). Biocompatibility was defined as “the ability of a material to perform with an appropriate host response in a specific application.” This suggests that a biocompatible material is not completely non-reactive with the environment but exerts an appropriate reaction. Accordingly, a more acceptable definition of biocompatibility is the natural tendency of a material to carry out the required function, such as health monitoring or treatment, without causing unwanted effects locally or systemically on the individual (Elshahawy, 2011). Therefore, a biocompatible material is expected to react with the environment in a specific way instead of the environment refusing to notice its presence.

The biocompatibility of biomaterial is dependent on factors such as its chemical and physical components, the nature of the environment where the biomaterial will be placed, and the length of time it will remain in that location. One of the challenges of using these devices is the possibility of draining some of their component material into the body or causing undesirable effects. Therefore, it is important to make an in-depth assessment and safety evaluation of such biomaterials. Regulatory bodies and institutions, such as the U.S. Food and Drug Administration (FDA), the International Organization for Standardization (ISO), and the Japanese Ministry of Health and Welfare (JMHW), produced guidelines that made it compulsory for manufacturers of medical devices to conduct pre-clinical and clinical testing of their products before they are approved for use by the public (Suvaneeth and Nair, 2018).



A medical device that may be implanted in the human body for long-term therapy or monitoring should meet the biocompatibility requirement of not causing injury to the tissues it will be in contact with (Williams, 2008). This means that the material biocompatibility (including bio-nanogenerators) should be tested before implantation into human tissues. Ideally, three types of biocompatibility testing should be conducted, including *in vitro* testing, *in vivo* animal, and clinical testing. The clinical trials are carried out on a volunteer where the material being assessed is placed into the tissues of such an individual, and they will be observed for any reactions (Elshahawy, 2011). The physical and chemical properties of nanoparticles and their surface characteristics determine their cellular uptake and bio-distribution (Kunzmann et al., 2011; Adabi et al., 2017). Furthermore, the immune reaction caused by the interactions between the nanoparticles and the immune cells, which may have engulfed the nanoparticles, is keenly observed to understand the mechanism (Kunzmann et al., 2011; Adabi et al., 2017).

Ubiquitous mechanical energy is seen as a recent sustainable energy source, as it was successfully harvested by different types of nanogenerators. Biocompatible nanogenerators are of great interest due to their possible biomedical applications (Wang YM et al., 2021).

The most studied energy harvesting mechanisms are based on the use of piezoelectric and triboelectric effects. The biocompatible ferroelectret nanogenerator (FENG) is efficient, flexible, and biocompatible. It uses the active material of polypropylene ferroelectret (PPFE). The mechanism of the mechanical-electrical energy conversion in PPFE films is described by the finite element method (FEM). Each time the device is folded, the generated voltage and current signals are doubled (Li et al., 2016).

Implantable nanogenerators showed high efficacy for self-powered medical devices. The most needed factor is its biosafety and long term. Li J et al. (2018) have surveyed the technology of polydimethylsiloxane (PDMS), and PDMS/Parylene-C embalmed polyvinylidene fluoride (PVDF) NGs

embedded in female mice for 6 months. *In vitro*, the PVDF NG showed a constant output of 0.3 V exposed to 7,200 cycles, while *in vivo* and under distending, the output was 0.1 V. Advanced methods of imaging studies were applied, such as ultrasound, computed tomography, and photoacoustic to monitor the *in vivo* performance. NGs displayed excellent adherence to the adjoining muscle and showed steady electric energy within the study. Interestingly, there was no evidence of toxicity or incompatibility with the adjacent tissues and body systems proven by humoral biochemical and pathological examinations. The PDMS complex device displayed effective insulation from the biological environment of the body with minor loss of currents at a pA hierarchy. These multiple *in vivo* and *in vitro* examinations prove the biological achievability of applying the innovative technology of mechanical energy harvesting in the biological environment *in vivo*.

Triboelectric nanogenerators (TENGs) are considered a good choice in the energy source field due to their low cost, high durability, and processability. The addition of biomaterials to TENGs gives rise to biomaterial-based TENGs (bio-TENGs), which are more environmentally friendly, with great potential for applications in wearable and implantable devices (Li Z. et al., 2020).

A cost-effective energy harvesting technology emerged in recent years, harvesting energy from renewable and clean energy sources. This technology is a nanogenerator founded on piezoelectric or triboelectric materials. The technology is also used for biomedical wearable or implantable applications, using advances in biocompatible soft materials and nanostructures. Hybrid bio-nanogenerators (HBNGs) are hybrid systems that depend on combining piezoelectric and triboelectric devices based on biocompatible materials aiming to harvest energy from the environment or for biomedical applications (Mariello, 2022). **Figure 6** Shows biocompatibility of bio-nanogenerator sensors.

## CONCLUSION

Biomedical electric devices greatly help in managing life's quality of many patients. However, their sustainability and safety in the human body still represent considerable issues for the limitations, such as restriction of energy storage, contamination, risk of its wastes, harm reaction of chemical and physical composites with the body, and effect of external magnetic, electric sources. All these factors are unknown, and others can arise, which show the importance of considering the full biocompatibility of these devices. This attracted scientists to find out substitute technologies for energy generators, such as nanogenerators, which can utilize the mechanical energy of the human heart and other physical activities to provide a sustainable source of energy for the implantable devices, in which the cardiac pacemaker represents the most important device for maintaining human life. Cardiac systole is a source of small and systematic blood circulation, and it is used to generate pressure and energy, which could be used as identical innovative technology as an energy provider to revive the pacemaker device, to keep the patients away from potential

complications of repeated surgery. A battery-less pacemaker became an implantable energy harvesting device, overcoming the limitations of the available battery-dependent pacemaker to a maintainable and friendly self-energy resource medical tool. This review outlined the implantable/wearable energy harvester and self-recharge medical devices, highlighting the importance of nanogenerator-dependent sensors for the electrical energy generated from heart contraction. It could be summarized that recent hybrid bio-nanogenerator systems of both piezoelectric and triboelectric devices based on biocompatible biomaterials and friendly energy are potential biomedical candidates showing *in vitro* and *in vivo* self-powered biomedical tools characterized by significant value, tractability, robustness, adjustable size, and cost-effectiveness. Although many studies have proven being body friendly and biocompatible, further clinical studies and critical reviews are needed for its long-term safety, immune reactions, and biocompatibility.

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## AUTHOR CONTRIBUTIONS

EA-S designed the idea, drafted the first and final version of the manuscript, and reviewed and edited it. MA drafted, reviewed, and edited the manuscript. AH drafted and reviewed the manuscript. AB reviewed the manuscript critically. The rest of the co-authors contributed to drafting the manuscript, designing the figures, and reviewing the references.

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