



Conformational dynamics of insulin

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We have exploited a prandial insulin analog to elucidate the underlying structure and dynamics of insulin as a monomer in solution. A model was provided by insulin *lispro* (the active component of Humalog®; Eli Lilly and Co.). Whereas NMR-based modeling recapitulated structural relationships of insulin crystals (T-state protomers), dynamic anomalies were revealed by amide-proton exchange kinetics in D₂O. Surprisingly, the majority of hydrogen bonds observed in crystal structures are only transiently maintained in solution, including key T-state-specific inter-chain contacts. Long-lived hydrogen bonds (as defined by global exchange kinetics) exist only at a subset of four α -helical sites (two per chain) flanking an internal disulfide bridge (cystine A20–B19); these sites map within the proposed folding nucleus of proinsulin. The anomalous flexibility of insulin otherwise spans its active surface and may facilitate receptor binding. Because conformational fluctuations promote the degradation of pharmaceutical formulations, we envisage that “dynamic re-engineering” of insulin may enable design of ultra-stable formulations for humanitarian use in the developing world.

Keywords: diabetes mellitus, NMR spectroscopy, hydrogen bond, amide-proton exchange, protein structure, protein dynamics, protein engineering, protein therapeutics

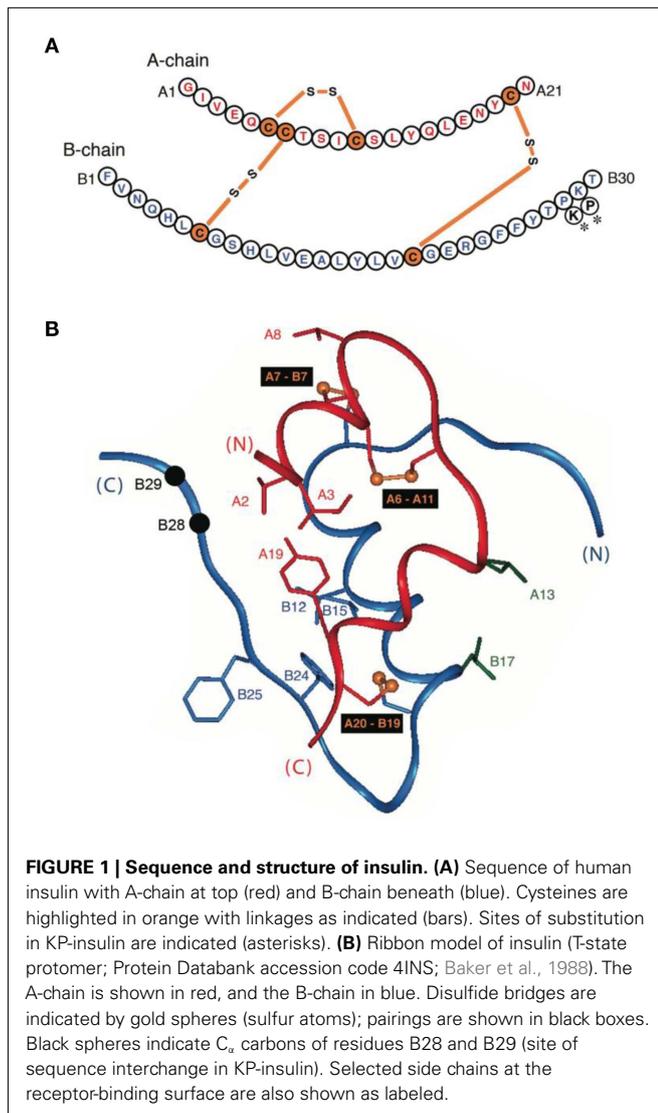
INTRODUCTION

We describe the structure and dynamics of a rapid-acting (prandial) insulin analog based on ¹H-NMR spectroscopy. Structure-based design of such analogs has enhanced the safety and efficacy of glycemic control in the treatment of diabetes mellitus (DM; Selden et al., 1986; Tripathi and Srivastava, 2006). The importance of tight control in Type 1 DM has been demonstrated by clinical trials, including the landmark DCCT (The Diabetes Control Group and Complications Trial Research Group, 1993) and its successor, the Epidemiology of Diabetes Interventions and Complications Study (Nathan et al., 2005). Although the safety of protocols to achieve tight control in long-established Type 2 DM may vary based on individual metabolic and clinical features [e.g., transient excursions in blood glucose concentration, duration of disease, and co-morbidities (Saltiel, 2001)], the United Kingdom Prospective Diabetes Study (Nicolleat, 2000) and subgroup analysis in the recent Action to Control Cardiovascular Risk in Diabetes Study (Riddle, 2010; Gerstein et al., 2011) support the appropriateness of moderate glycemic targets (Ismail-Beigi et al., 2011). To achieve these clinical objectives, rapid- and long-acting insulin analogs have been designed based on classical crystal structures (Baker et al., 1988) and general physico-chemical principles (Creighton, 1997).

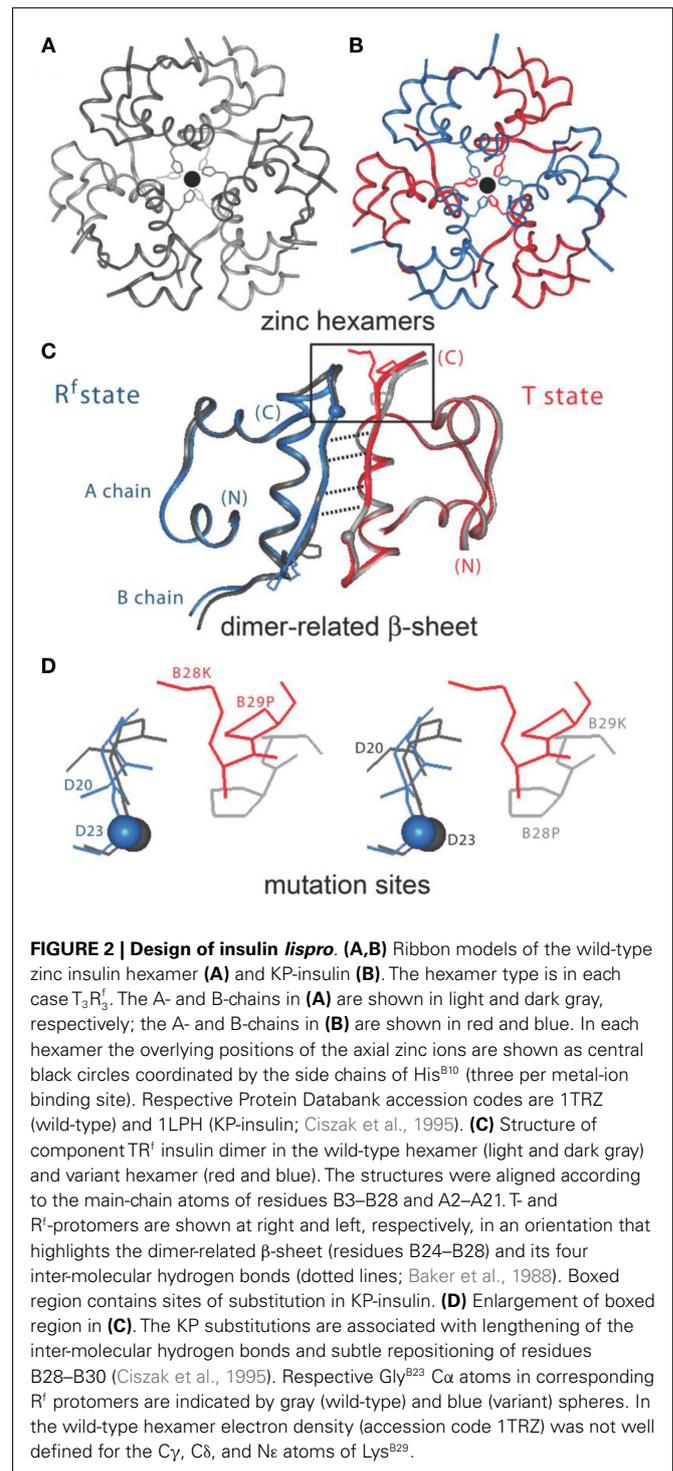
To obtain a model monomer, our studies employed insulin *lispro* (Ciszak et al., 1995; Campbell et al., 1996), the active component of Humalog® (Eli Lilly and Co.); its sequence is shown in **Figure 1A**. Approved by the United States Food and Drug Administration in 1996 (Campbell et al., 1996; Holleman and Hoekstra, 1997) and currently in broad clinical use (Hartman, 2008), this analog (also designated KP-insulin) contains paired substitutions near the C-terminus of the B-chain (Pro^{B28} → Lys and Lys^{B29} → Pro; asterisk in **Figure 1A** and black

spheres in **Figure 1B**). Interchange of residues B28 and B29, which recapitulates a feature of insulin-like growth factor I, does not perturb the receptor-binding surface of the hormone (Baker et al., 1988), and so the analog retains native potency (Shoelson et al., 1992). Subtle perturbation of the dimer interface (Ciszak et al., 1995) nonetheless leads to accelerated disassembly of the zinc insulin analog hexamer on subcutaneous injection (DeFelippis et al., 2001). Accordingly, the analog is absorbed into the bloodstream more rapidly than is wild-type insulin (Bakaysa et al., 1996). Although intrinsic rates of clearance from the bloodstream are presumably unaffected, enhanced absorption also leads to more rapid exhaustion of the subcutaneous depot and thus more limited duration of action (DeFelippis et al., 2001). The structural basis of such altered pharmacokinetics (PK) and pharmacodynamics (PD) has been investigated by X-ray crystallography (**Figure 2**; Ciszak et al., 1995). Whereas the overall structure of the variant hexamer closely resembles that of wild-type insulin (**Figures 2A,B**), superposition of component dimers reveals splaying of the C-terminal segments of the B-chain (box in **Figure 2C**) with weakening of β -sheet-related hydrogen bonds (dotted lines; Dodson et al., 1993; Ciszak et al., 1995). Such analysis highlighted the subtle contributions of Pro^{B28} and Lys^{B29} to the wild-type dimer interface (**Figure 2D**). Structure-based design of insulin *lispro* and related analog insulin *aspart* (Asp^{B28}-insulin, the active component of Novolog®; Novo-Nordisk, Ltd.) represented pioneering examples of protein engineering in molecular pharmacology (Brange et al., 1988, 1992a; DeFelippis et al., 2001).

¹H-NMR spectroscopy in principle provides an opportunity to probe the structure and dynamics of insulin as a monomer in solution and so complements crystallographic studies of insulin self-assembly (Hua et al., 1991). Such spectroscopic studies were long hampered by the complex self-association equilibria characteristic



of wild-type insulin at micromolar-to-millimolar protein concentrations (Weiss et al., 1991). In the present study we have explored a broad range of conditions to enable rigorous ¹H-NMR characterization of insulin *lispro* in aqueous solution without the need for additional amino-acid substitutions or addition of organic co-solvents (Hua and Weiss, 1991). Whereas the solution structure of monomeric insulin *lispro* closely resembles a crystallographic T-state protomer (Figures 1B and 2C, right; Baker et al., 1988), analysis of amide-proton exchange in D₂O demonstrated novel dynamic features. This technique focuses on the kinetics of exchange between peptide N-¹H protons by solvent-derived deuterons as a measure of both global stability and site-specific conformational fluctuations (Wüthrich, 1986; Englander et al., 1996). Remarkably, the majority of main-chain hydrogen-bonds observed in the crystal structure of insulin are only transiently maintained in solution: long-lived hydrogen bonds are restricted to a subset of α -helical residues flanking the A20–B19 disulfide bridge. This pattern of core conformational stability and flanking fluctuations is discussed in relation to mechanisms of receptor



binding (De Meyts and Whittaker, 2002; Nakagawa et al., 2005) and proinsulin folding (Steiner, 1967; Qiao et al., 2003; Weiss, 2009; Yang et al., 2010a).

Conformational stability and fluctuations within insulin are pertinent not only to *in vivo* biosynthesis and signaling, but also to pharmaceutical formulation (Brange et al., 1987). Rates of chemical and physical degradation, key determinants of shelf-life

above room temperature, are enhanced by transient partial unfolding processes (Brange and Langkjoer, 1993). Such degradation is accelerated among rapid-acting insulin analogs, including insulin *lispro*, and poses a particular challenge among indigent patients in the developing world (Hua et al., 2008). Indeed, the same structural perturbations introduced by substitutions at positions B28 and/or B29 to achieve accelerated absorption lead at the same time to compromised pharmaceutical stability. How may this trade-off, seemingly intrinsic to the logic of protein design, be avoided? The dynamic view of insulin provided herein by ¹H-NMR analysis promises to provide an opportunity for the “dynamic re-engineering” of favorable pharmacokinetic- and stability properties. We envisage that such second-generation analog formulations would circumvent the cold chain of insulin delivery and thereby facilitate their storage and use to address the emerging global pandemic of DM (Osei, 2003; Lefebvre and Pierson, 2004).

MATERIALS AND METHODS

SYNTHESIS OF INSULIN ANALOGS

Human insulin and insulin *lispro* were obtained from Eli Lilly Co. (Indianapolis, IN, USA). Synthetic analogs, kindly provided by Prof. P. G. Katsoyannis and coworkers, were prepared as described (Hu et al., 1993). Predicted molecular masses were in each case verified by mass spectrometry.

CIRCULAR DICHROISM

Circular dichroism (CD) spectra were obtained as described (Hua et al., 2001). Samples were dissolved in 10 mM acetic acid (0.14% v/v) at pH 3.0; the protein concentration was *ca.* 25 μM. For equilibrium denaturation studies, samples were diluted in the same buffer to 5 μM; guanidine-HCl was employed as denaturant (Hua et al., 2002a, 2006c). Data were obtained at 25 or 37°C and fitted by non-linear least squares to a two-state model (Sosnick et al., 2000).

NMR SPECTROSCOPY

Spectra were obtained at 700 MHz in 10 mM deuterioacetic acid (pH/pD 3.0; direct meter reading) at 25 and 37°C (Hua et al., 1996a); the protein concentration was *ca.* 0.5 mM. Resonance assignment was obtained by standard methods (Wüthrich, 1986). Sites of hydrogen bonds were inferred from the pattern of amide-proton protection in D₂O (Hua and Weiss, 1990). Spectra were also acquired at pH 7.4 and in 20% (v/v) deuterioacetic acid (pH 2.0).

STRUCTURE CALCULATIONS

Distance-geometry/simulated annealing calculations (DG/SA) were performed using program *DG-II* (Havel and Snow, 1991); restrained molecular dynamics (RMD) were calculated using *X-PLOR* (Brunger, 1992). Nuclear overhauser enhancement (NOE)-related and dihedral-angle restraints were used for molecular modeling as described (Hua et al., 1998).

AMIDE-PROTON EXCHANGE

¹H–²H-exchange was monitored in 10 mM deuterioacetic acid (pD 3.0) at either 25 or 37°C. The protocol is outlined in schematic form in Figure S1 in Supplementary Material. Intrinsic hydrogen exchange rates (k_{int}) were estimated using the *Sphere* program (H.

Roder, Fox Chase Cancer Center, Philadelphia, PA, USA). Protection factors (PFs) are defined as the ratio of intrinsic exchange rate constants:observed exchange rate constants ($k_{\text{int}}/k_{\text{obs}}$; Englander et al., 1996). Sites of global exchange were identified on the basis of comparative studies of protein analogs differing in thermodynamic stability but otherwise similar in structure; at such sites values of ΔG_{u} derived from denaturation studies were in accordance with values of ΔG_{HX} predicted by global PFs according to:

$$\Delta G_{\text{HX}} = -RT \ln(k_{\text{int}}/k_{\text{obs}}) = -RT \ln(\text{PF}) \quad (1)$$

where R is the Rydberg constant, and T is the absolute temperature. Values of k_{obs} and PF are provided in Table S1 in Supplementary Material.

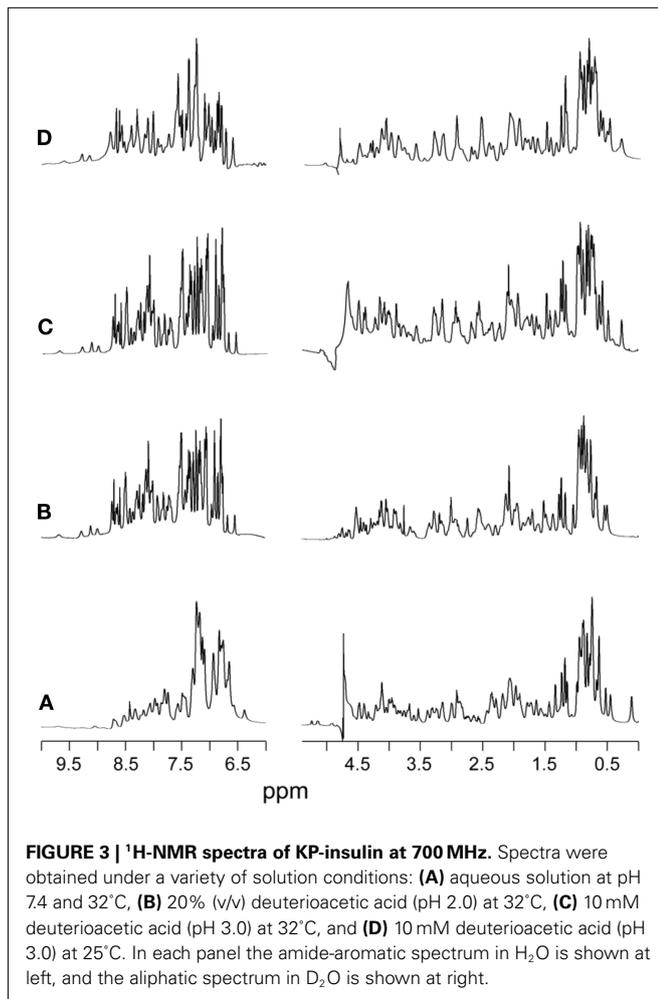
RESULTS

Twenty years ago protein engineering enabled the application of 2D ¹H-NMR methods to insulin (Weiss et al., 1991). Simultaneous substitutions were introduced at successive self-association surfaces (such as the classical B28-related dimer contact and B10-related trimer contact; **Figures 2A–C**) to achieve the millimolar protein concentrations then required for 2D ¹H-NMR study (Hua et al., 1996a). Advances in ¹H-NMR instrumentation (particularly development of ultra-high sensitivity cryogenic probes) presently enable such study at protein concentrations as low as 0.1–0.5 mM. Aided by this technology, we have found that KP-insulin is tractable in the absence of ancillary substitutions at the trimer interface, providing an opportunity to characterize a prandial insulin in clinical use.

SOLUTION STRUCTURE

Representative 1D ¹H-NMR spectra of KP-insulin under diverse solution conditions are shown in **Figure 3**; these include aqueous solution at pH 7.4 (pertinent to conditions in the bloodstream) and at pH 3.0 (optimal for analysis of amide-proton exchange). In each case KP-insulin exhibits patterns of chemical shifts, resonance line widths, and NOEs consistent with an isolated monomer (Hua et al., 1996a). Short- and medium-range NOEs characteristic of secondary structure were in each case consistent with the classical T state (Figure S2 in Supplementary Material). The set of inter-residue NOEs was found to be similar to that previously observed in 2D ¹H-NMR studies of Asp^{B10}-KP-insulin (also designated DKP-insulin; Hua et al., 1996a). Structural models were calculated by DG/RMD based on 803 distance restraints, 47 dihedral-angular restraints, and 31 hydrogen-bond restraints (Table S2 in Supplementary Material); a total of 881 restraints (*ca.* 17.3 restraints per residue) were thus employed. As expected, the resulting ensemble of structures (**Figure 4B**) closely resembles a collection of crystallographic T-state protomers (**Figure 4A**).

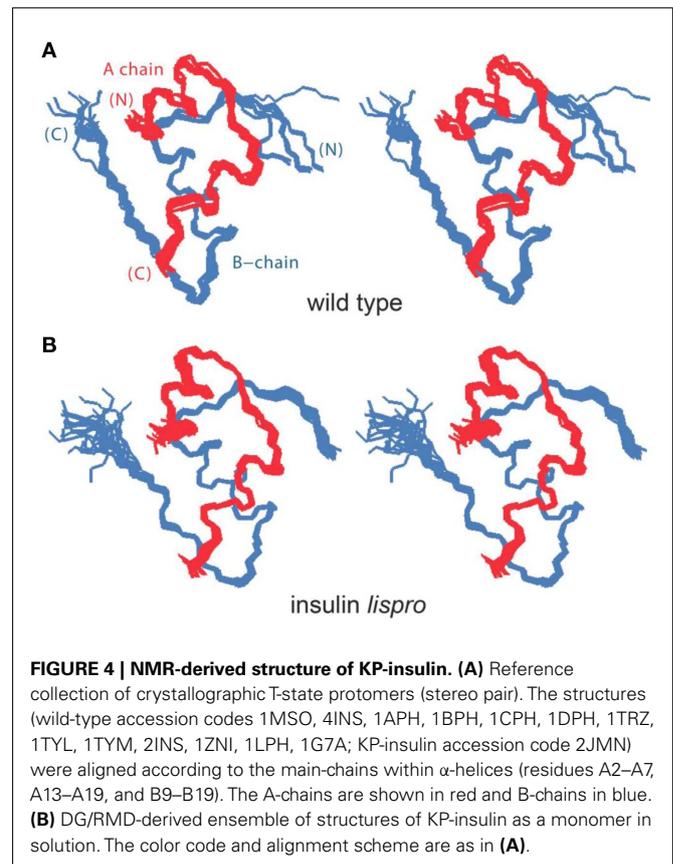
Distance-geometry/RMD ensembles of KP-insulin exhibit peptide segments of varying precision and so are evocative of dynamic variability. The C-terminal residues of the B-chain (residues B25–B30) are less well defined in solution than among crystal structures, presumably due to stabilizing effects of self-assembly (Baker et al., 1988). Conversely, positioning of the N-terminal arm of the B-chain in solution (residues B1–B4) is more precisely defined than



would be expected based on the diversity of crystallographic conformations (**Figures 4A,B**). The latter difference may reflect the DG/RMD protocol (which enforced all restraints simultaneously and so may underestimate conformational fluctuations), or conversely, variable positioning of the arm in crystals may be enjoined by lattice contacts (Baker et al., 1988). Because DG/RMD ensembles do not directly provide dynamic information, we sought an independent probe of protein stability and dynamics. ¹H-NMR analysis of amide-proton exchange in D₂O in principle provides such a probe (Wüthrich and Wagner, 1979; Englander et al., 1996).

AMIDE-PROTON EXCHANGE

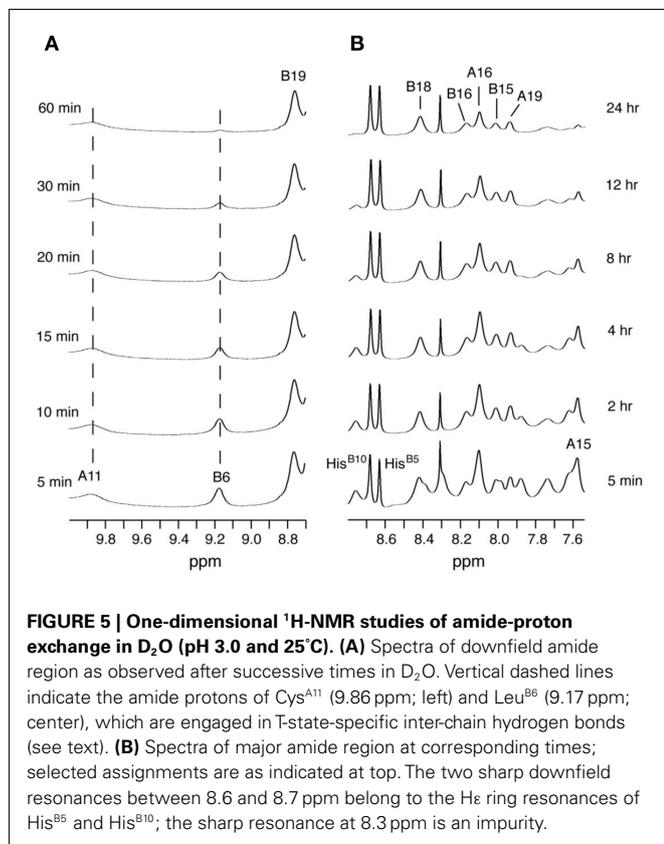
The amide proton (H_N) within each peptide-bond unit is labile, i.e., able to exchange with a solvent-derived ¹H or ²H (Englander et al., 1996). The rate of such exchange is typically measured under EX2 conditions wherein the observed rate constant (k_{obs}) is the product of a pH-dependent intrinsic rate constant (k_{int}) and the site-specific opening rate constant (k_{op} ; Bai et al., 1993). The extent to which k_{obs} differs from k_{int} enables calculation of individual PFs, defined as $k_{\text{int}}/k_{\text{obs}}$ (Roder et al., 1985). PF values depend on local structural environment and so define a residue-specific probe. In small globular proteins non-negligible PFs are ordinarily restricted to sites of hydrogen bonding. Protection



within KP-insulin might therefore be expected at H_N sites within α -helices (A3–A8, A15–A19, and B12–B19, excluding N-terminal residues), within β -turns (B7–B10 and B20–B23), or participating in inter-chain hydrogen bonds; dimer-specific protection would not be expected within the isolated B-chain β -strand (B24–B28; **Figure 2C**). The extent of protection at a given site depends on rates of structural fluctuations leading to hydrogen-bond breakage and exposure to solvent. Two limiting cases are of interest: (i) local stability is sufficiently marked that exchange requires global unfolding and (ii) local fluctuations are sufficiently marked that protection is negligible even in the presence of a non-random mean structure.

¹H–²H-exchange in KP-insulin is illustrated in **Figure 5** (1D spectra) and **Figure 6** (2D spectra). The studies were conducted at pD 3.0 and 25°C to optimize the quality of the ¹H-NMR spectrum in a pH regime between the extremes of acid and base catalysis. The majority of amide protons were found to exchange within 5 min, and so their resonances were not observed in the initial spectrum. Rates of exchange were thus measurable only for a minority of amide resonances. These reside within or adjoining α -helices (**Figure 5B**) and at inter-chain hydrogen bonds A11 H_N ⋯ O = C B4 and B6 H_N ⋯ O = C A6 (vertical dashed lines in **Figure 5A**). Resonance overlap among amide resonances in α -helices was resolved in successive TOCSY spectra (**Figure 6**). A broad range of PFs was observed (**Figure 7A**; Table S1 in Supplementary Material), suggesting uncorrelated and inequivalent segmental fluctuations. Whereas the central B-chain α -helix and

C-terminal A-chain α -helix contain sites of marked protection, exchange was rapid within the A1–A8 α -helix and the two B-chain β -turns. A summary of sites of observable protection is provided in **Figure 7B** in relation to hydrogen bonds as defined in crystal structures and as inferred from DG/RMD models.

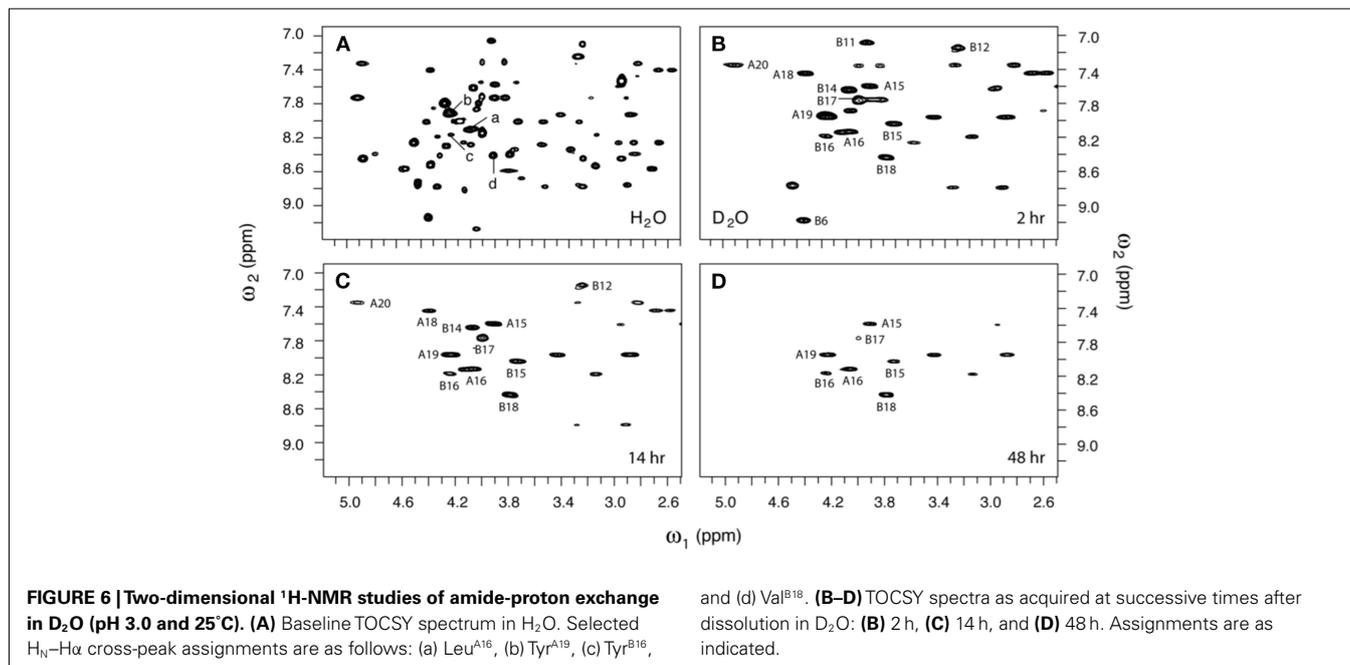


DYNAMIC CLASSIFICATION

Protection factors may be interpreted in relation to protein stability (at sites of global exchange) or protein dynamics (at sites of subglobal or local exchange; Roder et al., 1985). *Global* refers to an overall equilibrium between native and unfolded structures; such exchange implies that local or segmental conformational fluctuations either do not involve the breakage of hydrogen bonds or do not enable their exposure to solvent. *Subglobal* pertains to cooperative segmental fluctuations whereas *local* refers to uncorrelated local motions leading to hydrogen-bond breakage and exposure. The thermodynamic stability of a protein imposes an upper bound on observable PFs; intrinsic (random-coil) exchange rates impose a lower bound.

To distinguish between these modes of exchange, the global thermodynamic stability of KP-insulin was probed by chemical denaturation (Figure S3 in Supplementary Material). Cooperative unfolding at successive concentrations of guanidine-HCl was observed by CD at a helix-sensitive wavelength (222 nm). Application of a two-state model ($\text{N} \rightleftharpoons \text{U}$) enabled an estimate of the free energy of unfolding (ΔG_{U}) to be obtained as extrapolated to zero denaturant concentration (Hua et al., 2002a). The resulting estimate (3.3 ± 0.1 kcal/mol; see **Table 1**) implies a PF ceiling between 250 and 300. Because the $^1\text{H-NMR}$ studies were conducted in D_2O , comparative CD-detected studies in H_2O and D_2O were undertaken (each in 10 mM acetic acid at pH/pD 3.0); the results suggested that solvent isotope effects on stability are negligible (Figure S4 in Supplementary Material).

Four sites of global exchange were identified as depicted in **Figure 8A**. Their identification was based on PFs at or near the stability ceiling as imposed by ΔG_{U} : Leu^{A16} and Tyr^{A19} (the C-terminal segment of the second A-chain α -helix) and Tyr^{B16} and Val^{B18} (the C-terminal segment of the central B-chain α -helix). Global stability as estimated based on the average of the PFs at these sites ($\Delta G_{\text{HX}} 3.26 \pm 0.03$ kcal/mol) is in accordance with



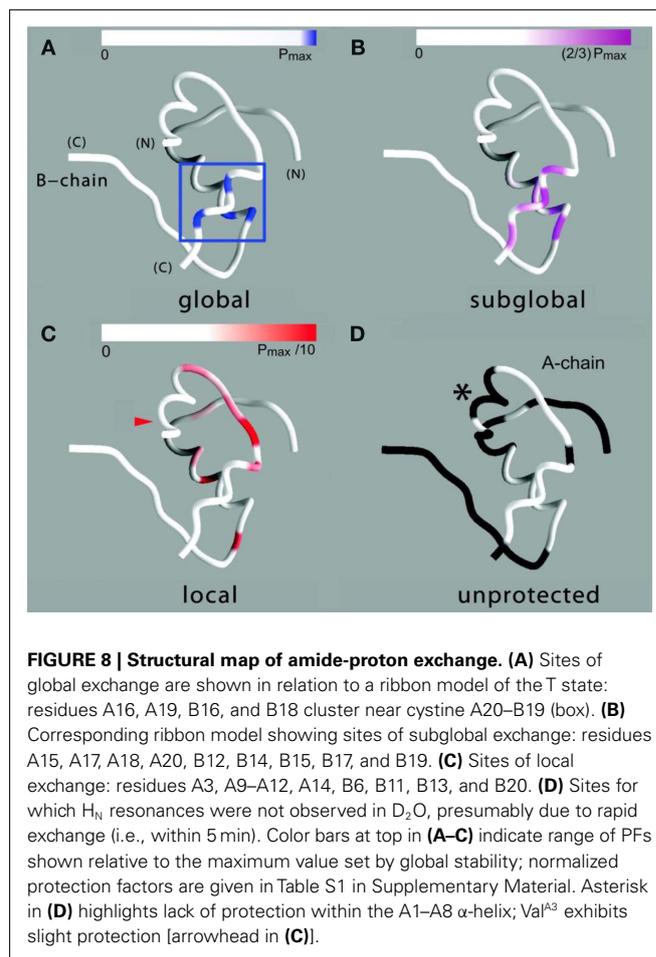
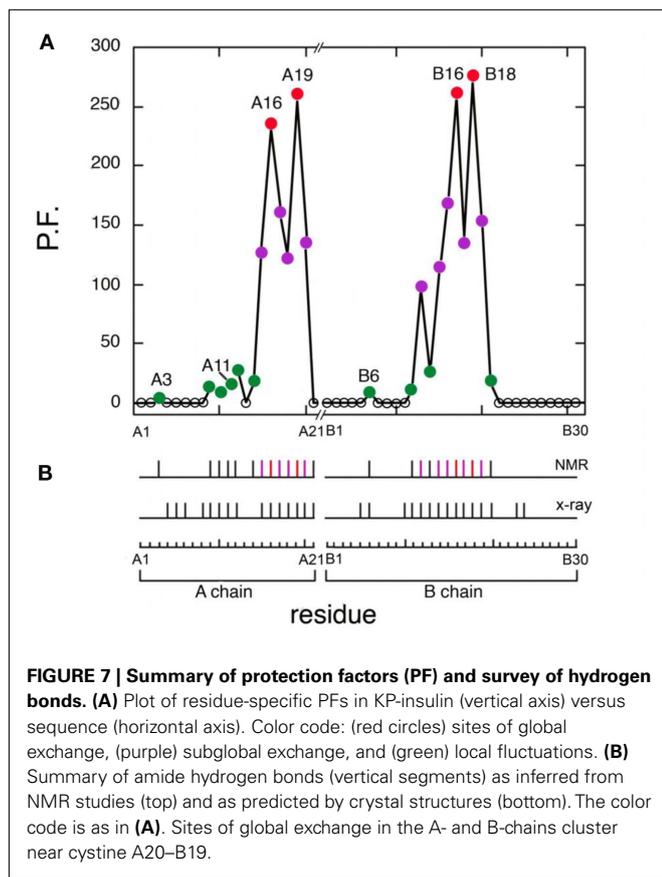


Table 1 | Estimates of global thermodynamic stability^a.

Analog	Temp (°C)	ΔG_u	ΔG_{HX}
KP-insulin ^b	25	3.3 ± 0.1	3.26 ± 0.03
Trp ^{A13} -KP-insulin	25	2.7 ± 0.1	2.73 ± 0.03
KP-insulin	37	2.6 ± 0.1	2.51 ± 0.03
Asp ^{B10} -KP-insulin ^b	37	3.0 ± 0.1	3.11 ± 0.01

^aIndependent estimates of thermodynamic stability (given in kcal/mol) were inferred from CD-detected guanidine denaturation studies (column 3) and NMR-detected 1H - 2H -exchange (column 4). CD assays were performed in 10 mM acetic acid (pH 3.0); NMR studies were performed in 10 mM deuterioacetic acid (pD 3.0).

^bKP-insulin, an analog containing IGF-I-related substitutions Pro^{B28} → Lys and Lys^{B29} → Pro (Ciszak et al., 1995). Asp^{B10}-KP-insulin (also designated DKP-insulin) contains the additional substitution His^{B10} → Asp as originally described in a monogenic syndrome of diabetes mellitus and hyperproinsulinemia (Carroll et al., 1988). Asp^{B10} enhances binding to the insulin receptor and Type I IGF-receptor (Schwartz et al., 1987; Hansen et al., 2011); its clinical use has been precluded on the basis of increased mitogenicity (Milazzo et al., 1997) and potential carcinogenicity (Hansen et al., 2011). Whereas the KP switch impairs stability, Asp^{B10} enhances stability (Kaarsholm et al., 1993).

the results of chemical denaturation (ΔG_u 3.3 ± 0.1 kcal/mol; **Table 1**). Similar consistency was observed at 37°C wherein KP-insulin exhibits both reduced stability to chemical denaturation (ΔG_u 2.6 ± 0.1 kcal/mol) and proportionately accelerated global

exchange (ΔG_{HX} 2.51 ± 0.03 kcal/mol; **Table 1**). These sites of global exchange kinetics flank internal cysteine A20–B19; their nascent folding is proposed to stabilize the folding nucleus of proinsulin (see Discussion; Hua et al., 2006a). To verify their global status, comparative amide-proton exchange studies were undertaken of analogs of KP-insulin of lower or greater thermodynamic stability (Trp^{A13}-KP-insulin and Asp^{B10}-KP-insulin; **Table 1**); surface substitutions were chosen to avoid perturbations within the hydrophobic core. Whereas substitution His^{B10} → Asp provides a more favorable C-cap to the B-chain α -helix (Weiss et al., 1990), substitution Leu^{A13} → Trp would be expected to introduce a destabilizing “reverse hydrophobic effect” (Chu et al., 1992) and potentially perturb the long-range packing of Phe^{B1}. These modifications were each associated with commensurate changes in ΔG_{HX} and ΔG_u in accordance with the global exchange model. Representative 1H -NMR data are respectively provided in Figures S5 and S6 in Supplementary Material.

Sites of subglobal exchange were identified as depicted in **Figure 8B**. Such sites (heuristically defined by PF values between 100 and 200; Table S1 in Supplementary Material) adjoin the global sites in the A-chain α -helix (residues A15, A17, A18, and A20) and B-chain α -helix (residues B12, B14, B15, B17, and B19). Sites of local exchange ($3 < PFs < 30$) were likewise identified as depicted in **Figure 8C**. These sites were observed in the A-chain at residues

A3, A9–A11, A13, and A14; and in the B-chain at B6, B11, B13, and B20. Structural correlates are as follows. (i) Protection is negligible or absent within the A1–A8 α -helix; only Val^{A3} H_N was observed in D₂O (PF_{A3} 3.6 ± 0.2). Such rapid exchange stands in contrast to retention of canonical helix-related NOEs in this segment (see above; Figure S2 in Supplementary Material). (ii) β -Turn probes Leu^{B11} (hydrogen bonded to the carbonyl oxygen of Gly^{B8}) and Gly^{B20} (hydrogen bonded to the carbonyl oxygen of B23) exhibit PFs between 10 and 20 (PF_{B11} 11.4 ± 0.4 and PF_{B20} 19.0 ± 0.6). (iii) Inter-chain hydrogen bonds (A11 H_N ··· O = C B4 and B6 H_N ··· O = C A6) are likewise transient (PF_{A11} 14.5 ± 0.5 and PF_{B6} 4.3 ± 0.3). No PFs were observed with values between 30 and 100, providing a clear empirical demarcation between segments exhibiting subglobal fluctuations and sites of local exchange.

No protection was observed at the remaining sites (Figure 8D), the majority of which are uninvolved in hydrogen bonding in crystal structures (Baker et al., 1988). Conspicuous by their absence, however, is lack of observable H_N protection at six sites of hydrogen-bonds characteristic of the classical 2-Zn (T₆) insulin hexamer. These map both within the A-chain (A20 H_N ··· O = C A17) and B-chain (B22 H_N ··· O = C B19 and B23 H_N ··· O = C B20). Accelerated ¹H–²H-exchange within the central B-chain β -turn correlates with enhanced crystallographic thermal B-factors at residues B20–B23 (Baker et al., 1988). Anomalous lack of protection was also observed at sites of inter-chain hydrogen bonds (A20 H_N ··· O = C B23, B4 H_N ··· O = C A11, and B25 H_N ··· O = C A19). Because the latter two inter-chain hydrogen bonds are broken in the crystallographic TR transition (Baker et al., 1988), such allosteric reorganization may exploit intrinsic sites of flexibility in an insulin protomer as originally envisaged by Hodgkin and colleagues (Chothia et al., 1983).

DISCUSSION

The zinc insulin hexamer exhibits representative structural features of globular proteins in general, including canonical elements of secondary structure, well-organized hydrophobic core, ligand-binding sites, and capacity for allosteric reorganization (Chothia et al., 1983). A model critical to the development and application of X-ray crystallographic techniques (Baker et al., 1988), the hexamer provides a stable storage form of the hormone both in the secretory granules of pancreatic β -cells (Steiner, 1967; Dodson and Steiner, 1998) and in pharmaceutical formulations (Brange et al., 1987). Structure-based mutagenesis of the zinc insulin hexamer (Brange et al., 1988) enabled development of rapid-acting insulin analog formulations for prandial injection and use in pumps (Zinman et al., 1997). Although originally described as “monomeric” (Brange et al., 1988), such analogs are formulated as zinc insulin hexamers (Humalog® and Novolog®; DeFelippis et al., 2001) or as an equilibrium distribution of zinc-free oligomers (Apidra®; Garg et al., 2005). The overall goal of such protein engineering is enhanced glycemic control with reduced risk of major hypoglycemic events per decrement in hemoglobin A_{1c} (Melki et al., 1998; Renner et al., 1999; Hartemann-Heurtier et al., 2003).

The present study has exploited a rapid-acting analog in current clinical use as a biophysical model of the insulin monomer. Insulin *lispro* contains paired substitutions near the C-terminus of the B-chain [Pro^{B28} → Lys and Lys^{B29} → Pro; (Bakaysa et al.,

1996)]. These changes are peripheral to the receptor-binding surface (Shoelson et al., 1992) and so are compatible with native hypoglycemic potency (Campbell et al., 1996). Although dimerization is markedly impaired in the absence of zinc ions, zinc-dependent hexamer assembly (critical to the stability of its pharmaceutical formulation) is maintained on binding of phenolic ligands (Ciszak et al., 1995). The structure and dynamics of the zinc-free monomer are of broad interest in relation to receptor-binding *in vivo* (Dodson and Steiner, 1998) and mechanisms of degradation *in vitro* (Brange and Langkjoer, 1993). Structural relationships within and between A- and B-chains are also pertinent to the folding of proinsulin (as a nascent monomer in the endoplasmic reticulum; Dodson and Steiner, 1998) and its aggregation-coupled misfolding in a newly recognized monogenic diabetes syndrome (Stoy et al., 2007; Weiss, 2009).

The solution structure of insulin *lispro* closely resembles the crystallographic T state as observed within structures of zinc insulin dimers and hexamers (Baker et al., 1988). This result was expected in light of previous NMR studies of related and unrelated engineered insulin monomers under a variety of solution conditions by several laboratories (for review, see Baker et al., 1988; De Meyts and Whittaker, 2002). Characterization of insulin *lispro* as a native-like monomer at pH 3.0 and in the absence of an organic co-solvent nonetheless provided an opportunity to obtain a quantitative assessment of amide-proton exchange in D₂O. Use of an acidic pH facilitates observation of ¹H–²H-exchange in flexible systems due to reduction in baseline rates of exchange from the random-coil state; between pH 3.0 and 4.0 the simultaneous efficiency of acid-catalyzed and base-catalyzed exchange was thus minimized (Roder et al., 1985; Wüthrich, 1986; Englander et al., 1996). In addition, the absence of an organic co-solvent permitted application of tabulated random-coil exchange rate constants (Englander et al., 1996) and hence calculation of site-specific PFs in the native state (Bai et al., 1993; Englander et al., 1996). Strikingly, at the majority of potential sites protection could not be observed, due either to absence of hydrogen bonding or local conformational fluctuations. Evidence for the latter is provided by the conspicuous absence of observable protection at sites otherwise structurally compatible with hydrogen-bond formation in the majority of DG/RMD models (e.g., A20 H_N ··· O = C A17 and A21 H_N ··· O = C B23; see Results). Because insulin is more stable under acidic conditions than at neutral pH (due to protonation of His^{B5}; Bryant et al., 1993), the present results may underestimate the extent of conformational fluctuations in the bloodstream.

From the present analysis three structural classes of hydrogen bonds may be defined: (i) those within stable α -helices, (ii) those within β -turns, or (iii) those between the A- and B-chains. Surprisingly, the majority of such hydrogen bonds are labile in solution (i.e., exhibit PFs smaller than would be predicted based on the global thermodynamic stability of the protein) irrespective of structural class. Global exchange kinetics was observed only at four sites (two per chain) flanking internal cystine A20–B19 (Figure 8A). Successive classes of exchange kinetics provide a dynamic map (Figures 8B–D). The lability of the majority of hydrogen bonds in monomeric insulin stands in contrast to the greater PFs observed in pioneering studies of bovine pancreatic trypsin inhibitor (Wagner and Wüthrich, 1986;

Roder, 1989). Previous studies have suggested that hydrogen bonds within insulin are stabilized on self-assembly (Hua et al., 1993) in accordance with high-resolution crystal structures (Baker et al., 1988).

Sites of global exchange kinetics in KP-insulin coincide with the proposed folding nucleus of proinsulin (Hua et al., 2006b). Although the latter precursor comprises a single polypeptide chain, the success of insulin chain combination (Katsoyannis, 1966) implies that chemical information required for folding is contained within the sequences of the A- and B domains (Tang and Tsou, 1990; Wang and Tsou, 1991). Studies of the disulfide-coupled folding of proinsulin and related polypeptides – foreshortened single-chain analogs (mini-proinsulin; Huang et al., 2001) and insulin-like growth factors – are notable for populated one- and two-disulfide intermediates (Hober et al., 1992; Miller et al., 1993; Qiao et al., 2001). Such intermediates are thought to acquire structure stepwise on successive disulfide pairing (for reviews see Jia et al., 2003; Weiss, 2009; Hua, 2010).

Spectroscopic studies of equilibrium peptide models support a structural pathway of disulfide pairing. In this process a key role is played by preferred initial formation of cystine A20–B19. In the native state this internal bridge connects the C-terminal α -helix of the A domain to the central α -helix of the B domain, connecting sites of global exchange kinetics as defined in the present study (Hua et al., 1995, 2002a,b). Although studies of proinsulin itself have been limited by aggregation (imposing a requirement for pH conditions >9), the disulfide pathways of mini-proinsulin and IGF-I are well characterized near neutral pH (Hober et al., 1992, 1994; Miller et al., 1993; Qiao et al., 2001). In such studies cystine A20–B19 is the only one-disulfide species to accumulate (Miller et al., 1999). We therefore envisage that the dynamic “core” of KP-insulin in its native state reflects its role in folding (Hua et al., 1996b, 2001). Impaired folding of the A20–B19-associated folding nucleus may account for the proteotoxicity and β -cell dysfunction caused by Gly^{B23} \rightarrow Val and related B-domain mutations in patients with permanent neonatal-onset neonatal DM (Weiss, 2009).

Sites of rapid, local, and subglobal exchange are prominent within the N-terminal segments of the A- and B-chains. Only limited protection was observed, for example, at the sites of key T-state-specific inter-chain hydrogen bonds (A11 H_N \cdots O = C B4 and B6 H_N \cdots O = C A6); no protection was observed corresponding to B4 H_N \cdots O = C A11. Breakage of such contacts (a prominent feature of the TR transition among zinc hexamers; Chothia et al., 1983) has been proposed to accompany binding of insulin to the insulin receptor (Baker et al., 1988; Nakagawa et al., 2005). Although co-crystal structures of the hormone-receptor complex have not been determined, evidence for such induced fit in the B-chain has been obtained through characterization of substitutions of Gly^{B8}. Formation of the A11 H_N \cdots O = C B4 and B6 H_N \cdots O = C A6 hydrogen bonds is coupled to maintenance of the adjoining T-state-specific β -turn (residues B7–B10). Remarkably, stabilization (or destabilization) of this turn by respective D- (or L) amino-acid substitutions at Gly^{B8} is associated with reciprocal effects on activity. On the one hand, because in the T state Gly^{B8} exhibits a negative ϕ dihedral angle, characteristic of D-amino acids, diverse D-substitutions at B8 are compatible with native-like

structure but low activity (Nakagawa et al., 2005; Hua et al., 2006c). On the other hand, L-amino-acid substitutions, consistent with the positive B8 ϕ angle of Gly^{B8} in the R state, can exhibit high activities despite markedly impaired stability and low yields of chain combination or yeast expression (Kristensen et al., 1997; Guo et al., 2005; Hua et al., 2006c). Accordingly, we have proposed that Gly^{B8} functions an “ambidextrous switch” between folding-competent (T-like) and active (R-like) conformations. In this model nascent T-like local structure in the proximal arm (including inter-domain hydrogen bonding and contacts by the imidazole ring of His^{B5}; Hua et al., 2006c) enhance the efficiency and fidelity of disulfide pairing. The present ¹H–²H-exchange data highlight the flexibility of T-like structure in the B-chain and hence its amenability for structural reorganization on receptor binding.

The flexibility of insulin may also contribute to its susceptibility to degradation. Whereas zinc hexamer assembly permits pharmaceutical formulation of adequate shelf life, degradation at elevated temperatures complicates the transport, storage, and use of insulin in the developing world. Brange and colleagues have characterized two modes of degradation, *chemical processes* leading to changes in covalent structure (such as formation of iso-aspartic acid or disulfide-linked polymers; Brange et al., 1992b) and *physical processes* leading to aggregation-coupled denaturation and fibrillation (Brange et al., 1997). Conformational fluctuations enhance rates of both chemical and physical degradation. The transient nature of the majority of hydrogen bonds in an insulin monomer is thus likely to play a central role in such mechanisms. In this regard the anomalous dynamic properties of the A2–A8 α -helix (as manifest by rapid amide-proton exchange and attenuated ¹³C α/β chemical shifts despite maintenance of helix-related NOE patterns) represent an “Achilles’ Heel” (Yang et al., 2010b). We speculate the molecular repair of this nascent helix may permit design of second-generation insulin analogs that are refractory to thermal degradation and so of humanitarian value in the developing world. One step in this direction has been taken based on solid-state NMR studies of insulin fibrils and analysis of β -branched side chains (Yang et al., 2010b). An alternative route toward stabilization of this segment may be provided by its tethering to the B-chain through the engineering of active single-chain analogs (Hua et al., 2008; Rajpal et al., 2009).

Following submission of this article, a complementary analysis of hydrogen bonds in insulin was presented (Antolíková et al., 2011). Remarkably, this and the present studies have put forward a similar perspective based on unrelated biophysical methodologies. Employing isothermal microcalorimetry, Brzozowski, Jiráček, and their respective colleagues exploited N-methylated insulin analogs to distinguish between the roles of inter- and intra-molecular hydrogen bonds at the dimer interface. Of particular interest, formation (or disruption) of the intra-molecular B25 H_N \cdots O = C A19 hydrogen bond (unprotected in insulin *lispro*) was observed to correlate with the relative competency of the B-chain to form inter-molecular β -sheet-related hydrogen bonds (Antolíková et al., 2011). Such coupling, supported by crystallographic analyses of variant zinc hexamers, highlights the non-local nature of a hydrogen-bond network and its potential functional relevance. The particular N-methylated insulin analogs studied by Antolíková et al. (2011) exemplify the power of chemical

modification to dissect specific dynamic features of a globular protein.

CONCLUSION

In the present study we have presented the solution structure of a prandial insulin analog as a monomer in solution. Dynamic characterization by amide-proton exchange has provided surprising insights into the lability of hydrogen bonds within and between the insulin chains. Although these hydrogen bonds are prominent features of classical crystal structures (Baker et al., 1988) and contribute to self-assembly (Dodson et al., 1993), their breakage is likely to contribute to the biological activity of the hormone as well as its degradation in pharmaceutical formulations. To our knowledge, this report represents the first quantitative analysis of ^1H - ^2H PFs in an insulin analog. We envisage that a deeper understanding of the dynamics of insulin will enable design of second-generation analogs with application to the developing world.

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SUPPLEMENTARY MATERIAL

The Supplementary Material for this article can be found online at http://www.frontiersin.org/Molecular_and_Structural_Endocrinology/10.3389/fendo.2011.00048/abstract

Six figures providing a schematic outline of the ^1H - ^2H -exchange protocol, CD-monitored guanidine denaturation assays, summary of ^1H -NMR analysis of secondary structure in Wüthrich format, and serial ID ^1H -NMR spectra of insulin analogs.

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