



Overcoming Blood-Brain Barrier Resistance: Implications for Extracellular Vesicle-Mediated Drug Brain Delivery

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Drug delivery across the blood–brain barrier (BBB) has several challenges, especially toward targeting neurological diseases, due to tight and selective barrier function of the BBB. Several structural and functional components of this barrier contribute to restricting drug entry, such as interendothelial tight junctions (TJs), efflux transporters, drug-metabolizing enzymes, and crosstalk between the cells of the neurovascular unit. Among different strategies to overcome BBB resistance to therapeutic drug delivery, the use of extracellular vesicles (EVs) gained attention in recent years. This review discusses the BBB structural and functional resistance, as well as potential avenues to overcome this challenge using EVs as drug delivery vehicles into the brain.

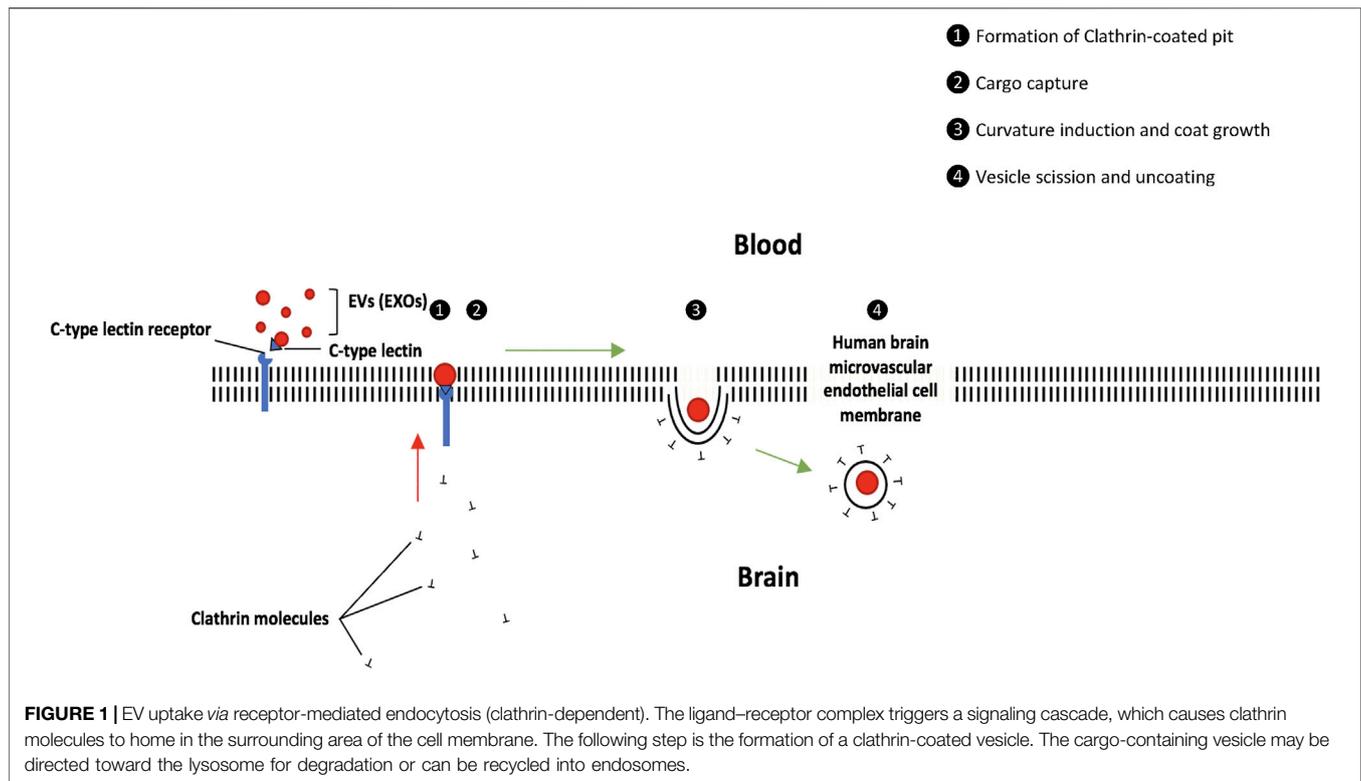
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1 THE BLOOD–BRAIN BARRIER

The blood–brain barrier (BBB) represents a microvascular interface between the circulatory system and the extracellular space of the brain (Toborek et al., 2005; Palmer and Alavijeh 2013; Osborne et al., 2020; Naranjo et al. 2021). The primary roles of this physical and metabolic entity are regulating central nervous system (CNS) homeostasis and providing the brain with a unique protection against endogenous and foreign agents (Weiss et al., 2009). Multiple cell types are interconnected at the endothelial cell lining of brain microvessels, which represent the anatomical site of the BBB. In terms of length, the BBB is the largest brain barrier, measuring approximately 650 km, and a surface of 10–20 m². Certain substances such as water, oxygen, and small lipids from the bloodstream cross the BBB by transcellular pathways or a paracellular pathway. The transcellular pathway includes a variety of mechanisms such as passive diffusion, receptor-mediated transport, and transcytosis. For the paracellular pathway, ions and solutes use concentration gradients to pass the BBB by passive diffusion (Dong, 2018). Although the BBB protects the brain's homeostasis, it may also interfere with therapeutic drug delivery into the CNS. This BBB resistance may occur *via* several mechanisms involving different structural and functional aspects of the BBB.

1.1 The Neurovascular Unit

Solute filtration at the BBB is a highly selective process that involves multiple cell types. The cells that play a role in the integrity of the BBB are collectively known as the neurovascular unit (NVU) (Abbott and Friedman, 2012). The primary component of the NVU is the brain microvascular endothelial cell (BMEC), which is a flat, sheet-like cell that forms the single-cell layer wall of brain microvessels (Kadry et al., 2020). BMECs and peripheral endothelial cells have similar functions,



such as regulating exchanges between the bloodstream and other surrounding cells. However, endothelial cells assembling the microvascular lining of the BBB lack fenestrations or small breaches in the outer membrane. They also have tight intercellular junctions. As a result, diffusion of proteins and small molecules is highly limited (Cohen et al., 2001; Stamatovic et al., 2008; Campos-Bedolla et al., 2014; Kadry et al., 2020; Walter et al., 2021). Both peripheral and brain endothelial cells have substantial proinflammatory properties (Toborek et al., 1995; Andras et al., 2005).

Astrocytes, a glial cell type, also play a critical role in the formation of the BBB. Astrocytes present projections known as astrocytic end-feet that extend to the walls of the blood vessels of the BBB (Kubotera et al., 2019). Working jointly, astrocytes and BMECs mediate signals that prompt the formation of TJs and other cell adhesion molecules necessary to fortify BBB integrity (Abbott and Friedman, 2012).

Pericytes, embedded between the parenchyma and external lamina of the BMEC, are also part of the NVU. These cells are susceptible to injury and viral infections (Nakagawa et al., 2012; Bertrand et al., 2019). They are separated from the parenchyma by the basal lamina, a thin layer that also interposes between the pericyte and endothelial cells (Bergers and Song, 2005). Pericytes have several functions; they are thought to limit angiogenesis and provide microvascular stability by inhibiting the growth of capillaries. Pericytes also possess contractile functions, which regulate capillary diameter. Effectively, the size of the diameter will have an impact on oxygen and nutrient diffusion (Kadry et al., 2020).

Surrounding neurons remain closely associated with capillaries and connect with astrocytic endfeet in the vicinity of the BBB. In addition to controlling blood flow and microvascular permeability, neurons regulate angiogenesis by releasing factors that stimulate growth of new blood vessels. Furthermore, neurons assist in the synthesis and localization of tight junction molecules in brain endothelial cell culture (Savettieri et al., 2000).

1.2 Accessory Cells of the Blood–Brain Barrier

Cells that also play a role in BBB integrity are microglia (Kovac et al., 2009), leukocytes (Engelhardt 2006), and, according to some reports, surrounding neurons of the NVU (Sonar and Lal, 2018). They typically induce an inflammatory response to stress, infection, and other altercations in the brain. Microglial cells facilitate the inflammatory response after chronic and acute central nervous system disorders, including Alzheimer's disease (AD) and Parkinson's disease. They work in conjunction with the neurovascular unit and function in BBB-sensor homeostasis, so any disturbance within the brain causes BBB dysfunction and neuroinflammation.

1.3 Interendothelial Junctions of the Blood–Brain Barrier

The unregulated passage of polar molecules, toxins, and other substances between blood and brain is highly limited. It is

primarily regulated by interendothelial junctions composed of protein complexes of tight junctions (TJ), adherence junctions (AJ), and gap junctions (GJ) (Komarova et al. 2017; Dong, 2018). TJs are transmembrane protein complexes that prohibit the interendothelial flux of solutes and ions (Hartsock and Nelson, 2008). AJs are linked to intracellular actin filaments of ECs and mainly initiate and stabilize cell–cell adhesion. Both AJs and TJs are intermembrane structures that function as seals to paracellular pathways of BMECs. Thus, the decrease in the integrity of these protein complexes results in inflammation, edema, and neuropathologies. Lastly, GJs are intercellular channels that direct electric and chemical communication between BMECs. Like TJs, GJs also regulate cell–cell transfer of ions and small molecules (Goodenough and Paul, 2009).

1.4 Efflux Transporters

An intact BBB is crucial for normal brain functions. Protecting the brain from potentially harmful endogenous and exogenous substances are physiological components such as efflux transporters and drug metabolizing enzymes. Efflux transporters of the BBB, such as P-glycoprotein (P-gp) (Cordon-Cardo et al., 1989), breast cancer resistance protein (BCRP) (Eisenblatter and Galla, 2002), and organic anion-transporting polypeptide (OATP) (Gao et al., 2000), are drug transporter proteins expressed at the luminal and abluminal BMEC membranes. P-gp and BCRP are specific membrane transporters known as multidrug resistance pumps. The role of these transporters is to detoxify the BMECs by actively pumping out compounds, such as xenobiotics, back into the blood stream (Kadry et al., 2020). P-gp can actively transport various compounds out of the cell by using ATP. Transported drugs, however, increase the enzymatic activity of ATPase by several folds. Due to their hydrophobic nature, most drugs will travel from the cytosol to the inner leaflet of the pump located in the lipid bilayer. Once inside, ATP must bind to the interior nucleotide-binding domains causing P-gp to undergo a dramatic conformational change that extrudes the drug to extracellular space. In a study involving Pgp inhibition in a rodent model, it was shown that knockout of one of the two genes that express P-gp in rodents (*mdr1a*) can increase drug penetration up to 100-fold but can sometimes lead to toxic consequences (Loscher and Potschka, 2005). Administration of P-gp inhibitors (e.g., PSC833 and GF120918) could also enhance brain entry of anticancer therapeutics (Loscher and Potschka, 2005). These data demonstrate that efflux pumps at the BBB level have a major role in the BBB resistance to therapeutic intervention.

1.5 Drug Metabolizing Enzymes of the Blood–Brain Barrier

Solute clearance is further enhanced by the presence of drug-metabolizing cytochrome P450 (CYP450) enzymes, a super-family of enzymes that are classified as monooxygenases. Located in the endoplasmic reticulum or within mitochondrial membranes of BMECs, CYP450 enzymes are responsible for the metabolism of xenobiotics and endogenous compounds, such as fatty acids in the brain microvascular area (Gherzi-Egea et al.,

1994; Zanger and Schwab 2013). This group of enzymes can also cause oxidation of a large group of drugs, including antiepileptic drugs (Kadry et al., 2020).

2 OVERCOMING BLOOD–BRAIN BARRIER RESISTANCE: EXTRACELLULAR VESICLE-MEDIATED DELIVERY INTO THE BRAIN

The integrated defense systems of the BBB impose a major challenge for effective drug delivery and the treatment of many brain diseases (Banks, 2016). Over the past decade, multiple strategies to improve drug delivery across the BBB are focused on noninvasive techniques. One of the most effective solutions to improve delivery efficiency relies on the use of extracellular vesicles (EVs).

2.1 Extracellular Vesicles

EVs are membrane vesicles from cellular origin that contain a lipid bilayer with a uniquely interactive surface area that can establish contact with surrounding cells and molecules of the extracellular microenvironment (Ratajczak et al., 2006; Zwi-Dantsis et al., 2020). The surface diameter of EVs expands from 20 nm to as large as 10 μ m. The mean diameter is approximately 30–150 nm (Subedi et al., 2019). Additional morphological characteristics of EVs, such as shape, are less versatile. They are round but can take on an elongated appearance that is not energetically favorable; therefore, it is only temporary or reversible (Zabeo et al., 2017). The general EV properties are presented in **Table 1**. The biological properties of EVs have been subject of several publications from our laboratory (Andras et al., 2017; András et al., 2020a; Cho et al., 2021). We also characterized the proteome of EVs derived from brain endothelial cells (András et al., 2020b). EVs have three main subtypes: microvesicles (MVs), exosomes (EXOs), and apoptotic bodies (Borges, Reis, and Schor 2013; Yanez-Mo et al., 2015; Zaborowski et al., 2015; Yu et al., 2019). MVs are released from the cell surface via budding mechanisms and attach to other cells where they may have surface–surface interactions (Ratajczak et al., 2006). They contain adhesion molecules, such as integrins, that can influence the diffusion of vesicles. Different proteins and lipids are involved in the vesicle trafficking processes, which in turn influence membrane curvature and rigidity (Skog et al., 2008).

A specific pool of vesicles is generated after the disassembly of apoptotic cells. These membrane-surrounded fragments are referred to as apoptotic bodies. Initially, it was believed that the primary role of vesicles pertaining to this category was harboring cellular debris of disassembled cells, and occurred spontaneously (Wickman et al., 2012; Xu et al., 2019). It is now becoming increasingly clear that these vesicles play a larger role in cellular apoptosis and, in fact, contain a wide variety of components such as micronuclei, chromatin remnants, cytosol portions, degraded proteins, DNA fragments, and intact organelles (Ma et al., 2021). Brain

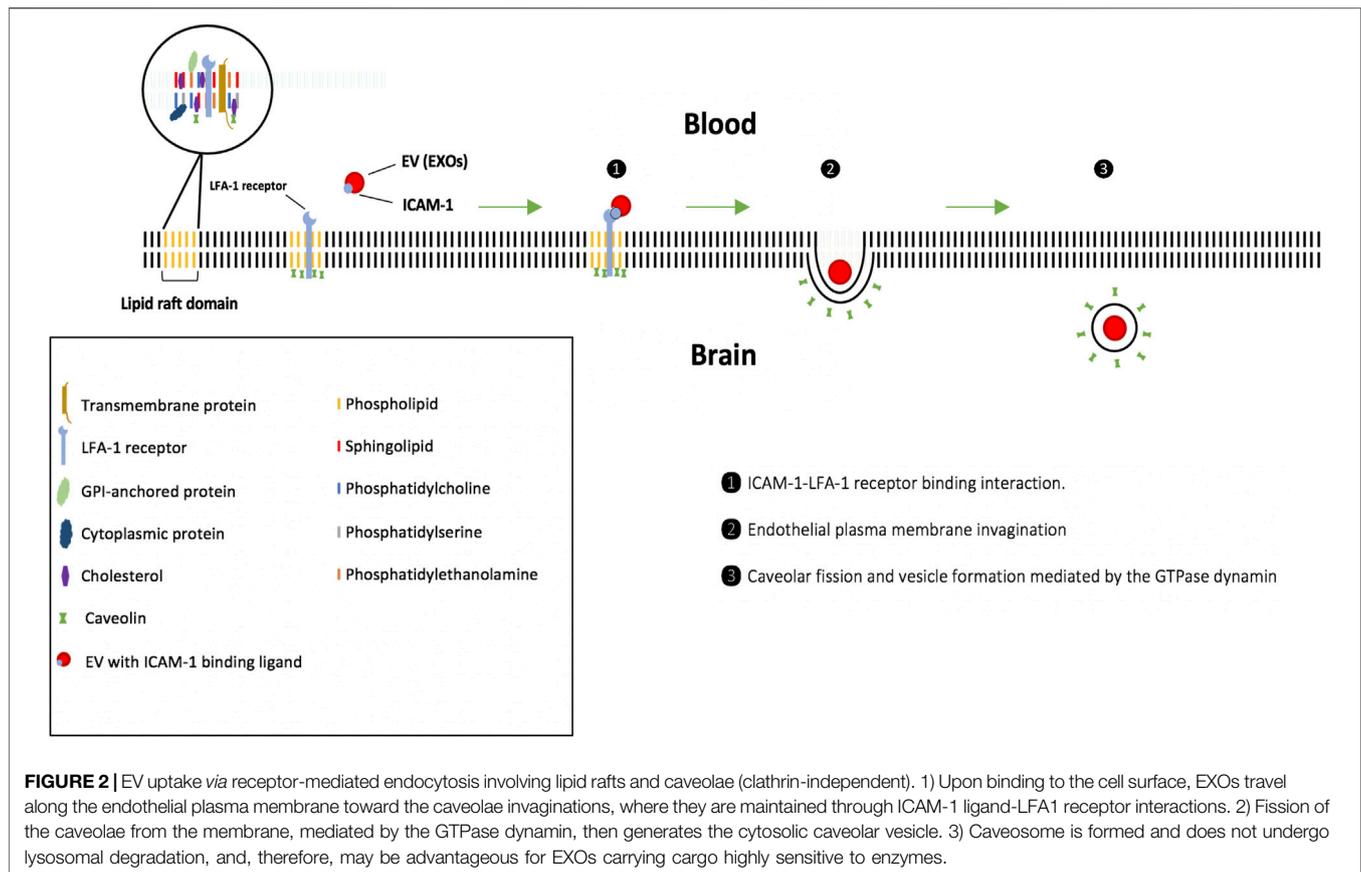


TABLE 1 | Summary of EV Properties (modified from Lee et al., 2012).

Classification	Characteristic	Biomarker	References
Microvesicles (MVs)	Heterogenous population Size: 50–1000 nm	Markers include annexin A1 and A2	Cocucci, Racchetti, and Meldolesi (2009) Jeppesen et al. (2019)
Exosomes (EXOs)	Homogenous population Size: 40–150 nm	Markers include CD9, CD63, Alix, flotillin-1, MHC class I, MHC class II, constitutive HSC70/HSP73, inducible HSP70/HSP72, and actin	Mayers and Audhya (2012) Mathivanan et al. (2012) Record et al. (2011) Kowal et al. (2016)
Ectosomes	Neutrophil- or monocyte-derived MVs Size: 50–200 nm	—	Sadallah, Eken, and Schifferli (2011)
Apoptotic bodies	Size: 50–2000 nm Cytoplasm with tightly packed organelles	Markers include caspase-2,3,7,8,9; annexin-V; nucleosomal DNA; cytokeratins; externalized phosphatidylserine; Apo-1/Fas; Fas ligand; p53; phospho-p53; p21 ^{waf1} ; and pH2AX	Elmore (2007) Stolzinger and Grune (2004) Ward et al. (2008) Masvekar et al. (2019)
EVs (general)	Size: variable	Markers include Small EVs (<150 nm): Tsg101, ADAM10, and EHD4 Large EVs (>150 nm): GP96 and other ER-associated proteins	Kowal et al. (2016)

endothelial cell death may occur in both physiological and pathological conditions. In a study on zebrafish larvae, some brain endothelial cell apoptosis could be attributed to remodeling of the brain vasculature (Zhang et al., 2018). Another study reported that the increased presence of acid sphingomyelinase

in old mice prompted apoptosis in brain endothelial cells (Park et al., 2018). In pathological conditions such as stroke, rapid and also late endothelial cell death was demonstrated (Zille et al., 2019). Programmed brain endothelial cell death can be correlated to low perfusion in capillaries (Park et al., 2018). Therefore,

apoptotic bodies resulting from these processes may profoundly impact the surrounding cells of the neurovascular unit.

Smaller vesicles, such as exosomes (EXOs), are produced by multiple vesicular endosomes that undergo invagination, resulting in their release into the intraluminal or extracellular space of the cell. Exosomes act as shuttle vectors or signal transducers that can deliver specific biological information and mediate nearby or long-distance intercellular communication. Furthermore, EXOs and other EV subtypes are non-cytotoxic and exhibit a low immunogenic profile. These characteristics place them as promising candidates for the next generation of nanomedicine for both diagnostic and therapeutic purposes (Alvarez-Erviti et al., 2011; Jang et al., 2013; Yang et al., 2015; Khongkow et al., 2019).

Throughout the article, we will use the terms EVs (extracellular vesicles in general), EXOs (exosomes), MVs (microvesicles), and apoptotic bodies.

2.2 Extracellular Vesicle Transport and Uptake

EVs can cross the BBB from the blood into the brain and from the brain into the blood. True BBB transendothelial transport of vesicles in both directions and quantitative uptake of EVs was presented in a highly cited paper (Banks et al., 2020). According to the calculations presented in this study, all EXOs crossed the BBB with an influx rate from 0.044 $\mu\text{L/g-min}$ to 0.524 $\mu\text{L/g-min}$ (Banks et al., 2020). While the routes embarked by EVs remain unclear, there is evidence that EVs may cross the BBB using a variety of mechanisms depending on their origins. The mechanisms employed for this crossing are likely to involve endocytic and transcytotic pathways, such as adsorptive transcytosis (Jarmalaviciute and Pivoriunas, 2016; Banks et al., 2020). The available evidence that EXOs indeed cross the BBB primarily by transcytotic mechanisms suggests that there may be some connections between the mechanisms of pathways used by immune cells, infectious agents such as viruses, some large proteins, as well as nanoparticles for crossing the BBB (Vorbrott and Trowbridge, 1991; Banks et al., 2012). Their convergence with viral pathways has been reviewed, summarizing how herpesviruses can merge with MVs pathways. Some proteins that are utilized for EXOs production by herpesviruses serve as functional release agents. The convergence of these pathways could explain the observation of virus-like particles, which could potentially be EXOs containing viral proteins or nucleic acids (Wurdinger et al., 2012). In addition, CD46 and mannose-6-phosphate (M6P) may also be involved in the EV crossing the BBB (Banks et al., 2020). Confocal microscopy showed that EXOs are internalized by brain endothelial cells through endocytosis, colocalize with endosomes, in effect primarily utilizing the transcellular route of crossing (Chen et al., 2016).

Receptor-mediated endocytosis *via* brain endothelial cells may be categorized into clathrin-mediated and non-clathrin-mediated (El-Sayed and Harashima, 2013). A proposed mechanism of *clathrin-dependent-receptor-mediated endocytosis* of EVs (Figure 1) is a ligand-receptor interaction between C-type

lectin and its receptor (Hao et al., 2007). Many C-type lectins participate in receptor-mediated endocytosis to transport soluble bound ligands to lysosomes (Cummings and McEver, 2015). Lectins are glycoprotein-bound receptor domains that interact with and bind to carbohydrates and glycan moieties. Among the functions of this broad subset of proteins is cell-to-cell communication, adhesion, and intracellular transport. Three categories of lectins exist, all that have been linked to EVs. They are as follows: transmembrane lectins and selectins, transmembrane sialic acid-binding immunoglobulin-like lectins (SIGLECS), and galectins found in the cytosol (Gonda et al., 2019). Selectins, however, are the best-known lectin type found to regulate the uptake of EXOs and other EVs (Johannes et al., 2016). C-type lectin receptors have been identified on both dendritic cells and brain endothelial cells. Using antibodies that bind to cellular C-type lectin receptors, it was demonstrated that the internalization of macrophage-derived EXOs occurs *via* the interaction between C-type lectin and its receptor (Hao et al., 2007). The interaction of selectins and C-type lectins with EXOs suggests an emerging area of research into the intercellular communication that enhances immune cell-antigen recognition and movement (Gonda et al., 2019). The ligand-receptor complex triggers a signaling cascade, which causes clathrin molecules to home in the surrounding area of the cell membrane. Additional stabilizing factors then pull in the lipid bilayer, allowing entry of the C-type lectin ligand into the cytosol. The following step is the formation of a clathrin-coated vesicle because of the invagination of the membrane (Kaksonen and Roux, 2018). The fate of the cargo-containing vesicle ultimately depends on the content it delivers. For example, a cargo with a pH of 4–5 is directed toward the lysosome, where the membrane is degraded, freeing its content. Vesicles can also be recycled into endosomes and repurposed to trigger signals within the cell or in surrounding ones (El-Sayed and Harashima, 2013).

Conversely, *clathrin-independent endocytosis* takes place in lipid rafts that are enriched in caveolin, which play important roles as vesicle traffic mediators and signal transducers (Zhong et al., 2008). The rafts are small, fluid domains of the lipid bilayer composed of sphingolipids and cholesterol connected to phospholipids and membrane-associated proteins. The essential membrane proteins include: 1) proteins attached to glycosylphosphatidylinositol-anchored proteins (GPI-AP) that are inserted in the outer leaflet of the membrane, 2) proteins attached to the inner leaflet of the membrane, and 3) transmembrane proteins that have a cytoplasmic domain in addition to an outer domain that is exposed on the cell surface (Simons and Ikonen, 1997; El-Sayed and Harashima, 2013). In endothelial cells, caveolae-mediated endocytosis takes place in lipid rafts that are enriched in caveolin and the resulting vesicles are stabilized by cavin. Scission of the vesicles from the cell membrane takes place via the action of dynamin (El-Sayed and Harashima, 2013). A study (Segura et al., 2005) demonstrated a possible mechanism of uptake for dendritic cell (DC) derived EXOs into B lymphocytes. Specifically, a decrease in DC-EXO uptake was observed after a blockage of intercellular adhesion molecule 1 (ICAM-1), a surface glycoprotein expressed on DC-EXO membranes, and its corresponding cell surface receptor,

lymphocyte function-associated antigen 1 (LFA-1) (Walling and Kim, 2018), suggesting the involvement of these molecules in EV uptake (Figure 2).

Characterized by its uptake at a smaller scale, micropinocytosis occurs when an intracellular vacuole of size less than 0.2 μm (Anzinger et al., 2010) forms from the invagination of the plasma membrane. EXOs interact with the surface of the recipient cell *via* surface receptor molecules and ligands (Muthu et al., 2021), and micropinocytosis plays an important role in internalizing EXOs on the cell surface. Interestingly, micropinocytosis is being seen to play a larger role in LDL uptake (Anzinger et al., 2010), where it accounts for 40% of LDL uptake. In addition, it was demonstrated in a zebrafish model that nanoparticles were able to cross the BBB with the aid of micropinocytosis uptake (Zhao et al., 2020). Hence, EXOs encapsulating nanoparticles can pave routes toward nanoparticle drug delivery across the BBB *via* micropinocytosis uptake.

In a recent paper, high-resolution electron microscopy imaging of the BBB *in vitro* revealed nanovesicles bound to the brain endothelial plasma membrane surface. These membrane-bound vesicles appeared to impact the formation of thin nanotubes in the paracellular space between the brain endothelial cells. These nanotubes may have a crucial role in the paracellular space alignment and sealing (Mentor and Fisher 2021). We can speculate that EVs may cross the BBB in pathological conditions when the BBB permeability is increased *via* the altered paracellular pathway involving these nanovesicles.

2.3 Targeting of Extracellular Vesicles for Drug Delivery

EVs can carry versatile cargo loads, including both hydrophilic and hydrophobic drugs, nucleic acids like miRNA, siRNA, and recombinant proteins, or even solid-state nanoparticles. Substantial effort has concentrated on developing EXOs as a drug delivery system as they possess the ability to undergo modification to improve delivery capacity and targeting specificity of nanomaterials. An initial report demonstrated EXO-mediated delivery of siRNA to the mouse brain by intravenous injection (Alvarez-Erviti et al., 2011). This was achieved by genetically modifying EV-producing cells to produce a targeting fusion protein, followed by loading the EVs with the siRNA cargo. The fusion protein was composed of Lamp2b, a surface protein found in the membrane of EXOs, and rabies virus glycoprotein (RVG), a neuronal cell-targeted protein.

Phosphatidylserine (PS), one of the most common phospholipids and abundantly found on the surface of EVs (Pirisinu et al., 2020), is a key player in decreasing EV time in circulation (Miyaniishi et al., 2007). Along with its receptor, phosphatidylserine receptor (PSR), the PS-PSR complex serves as a surface marker and is recognized by phagocytes as apoptotic cells (Hoffmann et al., 2005). Based on this, EVs could be potentially targeted to phagocytes and used for therapeutic purposes. For example, EVs carrying this marker and a drug

could be engulfed by brain macrophages thus having a potential for targeting HIV reservoirs in the brain. When EXOs secreted by primary oligodendrocytes were exposed to liposomes containing PS (Fitzner et al., 2011), their uptake *via* macropinocytosis was reduced. This was due to competition with the liposomes containing PS, underscoring a role of PS in EV uptake. Additionally, it was demonstrated that EXO-PS can facilitate the recognition and internalization of neuronal EXOs by microglia (Yuyama et al., 2012).

EVs may have a potential as delivery vehicles or tracking tools in pathological conditions. *In vitro* work investigating the interactions between EXOs and brain endothelial cells under conditions that mimic the healthy and inflamed BBB *in vivo* demonstrated that their transport involved endocytotic processes (Chen et al., 2016). Transwell assays revealed that luciferase-carrying EXOs can cross a brain endothelial monolayer under stroke-like, tumor necrosis factor alpha activated inflamed conditions but not under normal conditions. Confocal microscopy demonstrated that EXOs are internalized by brain endothelial cells through endocytosis, colocalize with endosomes, in effect primarily utilizing the transcellular route of crossing (Chen et al., 2016).

Extracellular vesicle-mediated repair of damaged endothelial cells in an amyotrophic lateral sclerosis (ALS) *in vitro* model was demonstrated recently. Human bone marrow endothelial progenitor cell-derived EVs ameliorated mouse brain endothelial damage, and this effect appeared to be mediated *via* EV uptake into the endothelial cells (Garbuzova-Davis et al., 2020).

Moreover, EVs derived from rat brain endothelial cells in combination with tissue plasminogen activator (tPA) were reported to have a beneficial effect on stroke outcomes by reducing neurovascular damage. These EVs improved BBB integrity, reduced infarct volume, and improved neurological outcomes in rats. Ultrastructural data from TEM images clearly showed that intravenously administered EVs crossed the BBB and were internalized by astrocytes and injured neurons (Li et al., 2021). A recent study also demonstrated that EXOs can play a protective role when delivering specific toxic viral proteins into the brain. In a study engineering EXOs containing HIV-1 Tat (EXO-Tat), Tat neurotoxicity was greatly reduced both *in vitro* and *in vivo* (Tang et al., 2020). EXO-Tat could reactivate latent HIV-1 infection but neurotoxicity was inhibited by eliminating Tat's ability to penetrate the neuronal cell membrane.

2.3.1 Intranasal Delivery of Extracellular Vesicles

EV drug delivery *via* the intranasal administration is gaining popularity due to its ability to easily bypass the BBB and retain itself at sites of injury better than the intravenous route. Two cranial nerves, olfactory and trigeminal, innervate the nasal cavity and provide direct access to the brain (Hanson and Frey, 2008). More specifically, drug administration *via* the intranasal route is narrowed down to intracellular and extracellular pathways (Crowe et al., 2018). In the intracellular pathway, the drug is engulfed *via* endocytosis by olfactory sensory cells, migrates *via* axonal transport, and is exocytosed in the olfactory bulb of the

brain. In the extracellular pathway, the drug translocates through the tight TJs of the nasal epithelium into the lamina propria, travels externally along axons *via* bulk processes into the CNS.

This route of delivery was explored in successful treatment of brain inflammation induced by administration of lipopolysaccharide, myelin oligodendrocyte glycoprotein (MOG)-induced experimental autoimmune encephalitis (EAE) and in glioma-26 tumor model (Zhuang et al., 2011). Specifically, antioxidant curcumin was encapsulated in EXOs and delivered *via* the intranasal route. Intranasal drug delivery *via* EXOs was also applied toward rectifying spinal cord injury (SCI) (Guo et al., 2019). SCI results in limited axonal growth and function due to the adult central nervous system neuron's maladaptive ability to regenerate from injury. In addition, SCI ensues major inflammation, myelin-associated inhibitors, glial components, and major blood loss. While attempts to correct spinal cord damage *via* permissive substrate grafting have proven to be ineffective (Griffin and Bradke, 2020), mesenchymal stem cell-derived EXOs (MSC-EXO) loaded with PTEN-siRNA were employed for intranasal administration to target spinal cord lesions. The PTEN gene normally functions as a tumor suppressor gene. The results indicated that EXOs migrated to the injured T10 spinal segment, suggesting a possibility of novel therapeutic approaches.

2.3.2 Extracellular Vesicles and the Choroid Plexus

The choroid plexus is characterized by its ability to secrete the majority of the central nervous system's cerebrospinal fluid (CSF), which presents potential in emerging methods of drug delivery. Injection of drugs from the bloodstream is transferred to the CSF across the choroid plexus, while in the BBB or brain capillary endothelium, drug is transferred into the interstitial fluid (ISF) from the blood, due to different endothelial/epithelial barriers (Pardridge 2011). The blood-CSF barrier is formed by TJs of the ependymal epithelium lining the ventricles. The choroid plexus contains many capillaries, but they are leaky allowing for large volume flow in the brain as opposed to the capillaries with TJs found within the BBB (Abbott, 2004). When comparing brain penetration of drugs to CSF penetration, CLogD is used to measure lipophilicity of certain compounds (Abbott et al., 2018). It turned out that brain penetration increases as drugs become more lipid-soluble (increased CLogD), but CSF penetration significantly decreases with more lipid-soluble drugs (Abbott et al., 2018). The reason is that the aqueous CSF is less favorable for lipophilic compounds than the brain, where the compounds directly meet the lipid cell membranes. In reference to efflux transporters, such as P-glycoprotein, uptake of substrates for this transporter is generally closer at any given CLogD in wild-type mice that contain the P-glycoprotein transporter (Abbott et al., 2018). In the KO mice where P-glycoprotein is missing, brain entry is increased because the drug is not effluxed back to blood. Therefore, the presence of any compound in CSF cannot be a true measure of its brain level, especially for lipophilic drugs that interact with efflux transporters (Abbott et al., 2018).

Regarding the role of the choroid plexus in the EV-mediated brain pathologies, it was previously reported that peripheral inflammation evoked increased choroid plexus epithelial cell-

derived EVs release at the blood-cerebrospinal fluid (CSF) interface into the CSF (Balusu et al., 2016). Later, the same group studied choroid plexus-mediated EV release in AD pathogenesis. They observed increased EV levels in the CSF of young transgenic APP/PS1 mice which correlated with high amyloid beta (A β) CSF levels. If they injected A β oligomers into the brain ventricles of wild-type mice, a significant increase of EVs in the CSF occurred and these EVs originated from the choroid plexus (Vandendriessche et al., 2021). Recently, it was also demonstrated that choroid plexus and CSF EVs might play a role in the pathogenesis of Niemann-Pick type C disease. Specifically, in NPC1 $-/-$ mice, enlarged CSF-EVs were observed. It turned out that EVs derived from NPC1 $-/-$ choroid plexus explants could induce typical brain pathology like microgliosis and astrogliosis (Van Hoecke et al., 2021).

2.3.3 Extracellular Vesicle-Based Brain Cancer Therapy

Several EV-based therapeutic strategies have been employed in experimental treatment of primary brain tumors, such as glioblastoma multiforme (GBM). Temozolomide (TMZ), an alkylating agent used as a first-line adjuvant drug, is at the frontline of GBM treatment; however, not all forms of GBM are sensitive to this drug. Because microRNA-9 (miR-9) is highly expressed in GBM cells that are resistant to TMZ, a strategy has been explored to deliver anti-miR-9 to TMZ-resistant GBM cells. This approach successfully sensitized the GBM cells to TMZ (Munoz et al., 2013).

Another miR, miR-146b, has also been explored as a potential contributor toward GBM cancer therapy. MiR-146b can inhibit glioma cell invasion, migration, viability, and expression of EGFR (Katakowski et al., 2013). In this context, bone marrow stromal cell-derived EXOs were tested to serve as a vehicle for miR-146b delivery into GBM cells. Administration of EXOs loaded with miR-146b *via* intra-tumor injection resulted in a significant reduction in 9 L glioma xenograft growth in a rat model (Katakowski et al., 2013).

2.3.4 Combined Extracellular Vesicle-Nanoparticle Delivery Into the Brain

Inorganic nanoparticles have an overall higher delivery efficiency compared with nanomaterials from organic origin. This is expected due to the vast range of tunable properties that inorganic nanoparticles possess, such as size, controlled release mechanisms, or active targeting (Patra et al., 2018). To improve the clinical translation of nanomedicine as an effective treatment for neurological diseases, it is important to consider these properties. The delivery efficiency of nanoparticles exhibiting neutral zeta potentials tends to be higher than that of nanoparticles with positive or negative zeta potentials. For a nanoparticle to efficiently reach the targeted tumor site, it must selectively interact with tumor cells while avoiding interaction with other cell types. If the designed nanoparticles exhibit a negative zeta potential charge, they may be repelled from the negatively charged tumor cell membrane, for example. Conversely, designing a positively charged surface for nanoparticles may allow for better interaction with the tumor cells, but may increase interaction with unwanted cell types

(Gumustas et al., 2017). Furthermore, delivery methods, such as active targeting and passive targeting, are also considered. In passive targeting, nanoparticles take advantage of the enhanced permeability retention (EPR) effect, where they cross the tumor vascular membrane through intercellular gaps and undergo a longer retention period due to the impaired lymphatic drainage of the tumor (Shi et al., 2020). Alternatively, active targeting is a more efficient targeting method, which relies on attaching targeting ligands to the surface of nanoparticles. This method potentially reduces delivery time of nanoparticles, which decreases the risk of potential phagocytosis from immunogenic cells and enhances binding specificity, since the ligands in the nanoparticle surface are functionalized to target the corresponding receptors in the tumor site (Attia et al., 2019).

Similar approaches using EVs in combination with nanoparticles can be applied to the field of brain cancer. For example, EVs can be genetically modified to produce a fusion protein containing gelonin, a cancer targeting protein (Cheng et al., 2018). Following this modification, EVs can be loaded with nanoparticles such as iron oxide, gold nanoparticles, or zinc oxide. Iron is used in various magnetic applications because it contains four unpaired electrons in its d orbital that contribute to its magnetic potential. However, it is commonly used in the form of iron oxide because it is more stable than pure iron. Iron oxide is also biocompatible and was considered nontoxic to the human body, facilitating its use in biomedical applications (Teja and Koh 2009). However, iron oxide nanoparticles can also have some toxic effects involving oxidative stress (Mahmoudi et al., 2012; Soenen et al., 2012). When administered intranasally, they evoked oxidative stress and microglial activation in the olfactory bulb, hippocampus, and striatum (Kumari et al., 2013). In a rat model, these iron oxide nanoparticles induced oxidative stress, inflammation, and apoptosis in neurons (Kim et al., 2013). Once iron oxide is delivered to the cancer cell, it can induce magnetic hyperthermia or it can serve other purposes, such as magnetic resonance imaging (MRI) and photodynamic therapy (Estelrich and Busquets, 2018). Loaded inside EVs, gold nanoparticles can also serve as agents of magnetic resonance imaging (Khongkow et al., 2019). Zinc oxide nanoparticles encapsulated inside EVs can also be efficiently internalized by cancer cells, and particularly, may trigger apoptosis (Bai et al., 2017).

3 CHALLENGES OF USING EXTRACELLULAR VESICLES FOR BRAIN DRUG DELIVERY

Despite described advantages that expand EVs' potential clinical use in cancer and CNS diseases, EV-mediated drug delivery methods are still at early stages and there are many obstacles yet to overcome. For example, achieving a large-scale production of EVs for clinical use is challenging. This process is affected by limited resources and requires cell culturing, followed by EV isolation, which potentially causes issues with vesicle purification. EVs have a complex structure as revealed by proteomic, RNA seq, and lipidomic studies, which is difficult to control, and they have the ability to manipulate cell microenvironment. For example, EVs

derived from GBM cells can change the angiogenic phenotype in brain endothelial cells, increase the proliferation of GBM cells within the surrounding area, and increase tumor growth as a result of vesicle internalization. Specifically, these EVs contain angiogenic proteins, such as angiogenin, FGF α , IL-6, IL-8, TIMP-1, VEGF, and TIMP-2, and thus stimulate tumor vascularization promoting tumor growth. The presence of low pH levels in germinating tumors may facilitate lysis of EVs, leading to increased bioavailability of intravesicular proteins. In addition, angiogenesis-promoting proteins, such as angiogenin, require membrane transport to exert their biological activity, which could be also facilitated by EVs. Therefore, tumor-derived EVs may potentially also serve as a targeted product delivery vehicle, carrying multiple components, including mRNA, miRNA, and proteins, to communicate genetic information and signaling proteins to cells within proximity (Skog et al., 2008).

Another important factor to consider is the EV half-life in different biological compartments. EV blood levels reflect a balance between secretion and clearance rates (Matsumoto et al., 2020). After intravenous administration of EVs in a mouse model, EVs had an estimated half-life of 30 min and most EVs were cleared in 6 h (Lai et al., 2014). When crossing the BBB from the blood into the brain, EV clearance from the blood occurred rapidly (1.51–7.29 min) or slowly, independent of the EVs origin. These clearance patterns reached a prolonged steady state indicative of uptake by the periphery and exchange between the circulation and the peripheral tissues (Banks et al., 2020).

4 CONCLUSION

Although its functional and structural integrity is vital in maintaining the homeostasis of the brain microenvironment, the BBB compromises the effectiveness of many CNS treatments. Among the explored strategies to overcome this challenge, EVs are becoming increasingly promising candidates to cross or bypass the BBB by their innate capability to act as efficient drug delivery vehicles alone or in combination with nanoparticles. Nevertheless, several obstacles in using EVs for drug delivery remain to be addressed, including a large-scale production of EVs for clinical use or the biological impact of their cargo, which originates from the parent cells.

AUTHOR CONTRIBUTIONS

JD, NS, IA and MT wrote or contributed to the writing of the manuscript; JD created all figures. MT provided funding.

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