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# Recent advances in lanthanide-doped up-conversion probes for theranostics

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Up-conversion (or anti-Stokes) luminescence refers to the phenomenon whereby materials emit high energy, short-wavelength light upon excitation at longer wavelengths. Lanthanide-doped up-conversion nanoparticles (Ln-UCNPs) are widely used in biomedicine due to their excellent physical and chemical properties such as high penetration depth, low damage threshold and light conversion ability. Here, the latest developments in the synthesis and application of Ln-UCNPs are reviewed. First, methods used to synthesize Ln-UCNPs are introduced, and four strategies for enhancing up-conversion luminescence are analyzed, followed by an overview of the applications in phototherapy, bioimaging and biosensing. Finally, the challenges and future prospects of Ln-UCNPs are summarized.

#### KEYWORDS

lanthanide-doped, probes for theranostics, up-conversion, up-conversion luminescence, biomedicine

#### 1 Introduction

Rare earth-based nanomaterials have attracted attention due to their superior fluorescence properties. Because of their dense energy levels that enable complex electronic transitions, rare Earth elements have become a treasure house of luminescence (Li et al., 2015a; Binnemans, 2015). Rare earth-based nanomaterials require specific wavelength of excitation to photoluminesce (Tsang et al., 2015; Adachi, 2018; Quan et al., 2018; Mintz et al., 2019; Mir et al., 2020; Gierschner et al., 2021). The emission can be characterized as up-conversion or downconversion luminescence (Reddy et al., 2018). For example, Ln- UCNPs can be excited by infrared light to emit visible light. If modified properly, they can become good candidates for tumor diagnosis and treatment.

Phototherapy (PT) (Li et al., 2018; Lan et al., 2019; Zhen et al., 2019; Xie et al., 2020), as a new type of treatment with good targeting and low toxicity, is often classified as photodynamic therapy (PDT) or photothermal therapy (PTT). Phototherapy is gradually becoming an important supplement for tumor treatment. Therefore, Ln-UCNPs can serve as a substrate for composition with other materials for phototherapy, to aid surgical navigation, to enhance the precision of imaging, and for efficient treatment (Shanmugam et al., 2014; Liu et al., 2019a).

In addition to therapy, Ln-UCNPs also have potential for use in bioimaging and biosensing (Zhang et al., 2016; Zhang et al., 2019). Functionalized Ln-UCNPs can be applied in Computed Tomography (CT) and Magnetic Resonance Imaging (MRI) among others, which adds value to the bioimaging field (Zhang et al., 2011; Sun et al., 2013; Li et al., 2019). Regardless, Ln-UCNP-based biological imaging has shortcomings and there is significant room for improvement. Ln-UCNPs also perform well in biosensing (Guo

Method	Morphology	Reaction condition	Product stability	Synthetic cost
Thermal decomposition	Controllable	Harsh	Stable	Higher
Hydrothermal/solvothermal	Controllable	Simple	Stable	Lower
Co-precipitation	Uncontrollable	Simple	Stable	Lower

TABLE 1 Typical methods of Ln-UCNPs synthesis (Li and Lin, 2010; Du et al., 2011; Lin et al., 2012).

et al., 2016; Mahata et al., 2017). Ln-UCNPs can be used as pH and temperature sensors as well as gas and DNA sensors, to name a few, due to temperature sensitivity and other optical properties. It is foreseeable that the use of Ln-UCNPs will expand in the sensor field (Wang et al., 2014a; Cui et al., 2014; Dong et al., 2015; Pan et al., 2017).

This manuscript reviews research on the synthesis, luminescence modulation, and the latest achievements in phototherapy, bioimaging and biosensing of Ln-UCNPs. Synthetic methods are summarized in Section 2, research on luminescence modulation is outlined in Section 3, and then applications for Ln-UCNPs in phototherapy, bioimaging and biosensing are introduced in Section 4. Finally, the current challenges of Ln-UCNPs and their prospects for the future are discussed.

## 2 Synthesis methods of Ln-UCNPs

Many challenges concerning the morphology and performance of Ln-UCNPs must be addressed for successful application in biomedicine. Fortunately, many kinds of Ln-UCNPs have been synthesized that enable the potential for applications. Rare Earth luminescent materials have attracted much attention because of their flexibility and easy modulation. Different nanoparticles can be synthesized by controlling the reaction conditions; these include the temperature, pH, precursor concentrations, etc. Researchers have successively realized several luminescence mechanisms such as excited state absorption (ESA), energy transfer up-conversion (ETU), cooperative sensitization up-conversion (CSU), photon avalanche (PA), and energy transfer-mediated up-conversion (EMU). This section introduces the most common methods, specifically thermal decomposition and hydrothermal/ solvothermal, as well as several other synthetic approaches. A brief comparison of these methods is provided in Table 1.

#### 2.1 Thermal decomposition method

The thermal decomposition method is the most facile to create high-quality Ln-UCNPs. Thermal decomposition is the process of pyrolyzing organometallic precursors in an organic solvent under an oxygen-free environment. In general, the precursors are organic salts of rare Earth ions, such as trifluoroacetate and acetate among others. Octadecene (ODE) is the most frequently used high-boiling organic solvent. Oleic acid (OA) and oleylamine (OM) can serve dual roles as solvents and as ligands that adsorbed onto the nanoparticles to control their size and shape. It is worth noting that the crystal nucleation and growth process that control the nanoparticle uniformity can be adjusted with the temperature, heating rate, and precursor concentrations during synthesis.

Yan and co-authors first synthesized LaF<sub>3</sub> crystals by thermal decomposition using a single-source precursor (Zhang et al., 2005). Later they pioneered the use of multi-source precursors to prepare high quality nanocrystals through thermal decomposition, which greatly promoted the development of Ln-UCNPs (Yin et al., 2010). Murray and collaborators studied the influence of reaction time and the ratio of sodium to lanthanide precursors on the morphology of  $\beta$ -NaYF<sub>4</sub>-based Ln-UCNPs in detail, thereby obtaining beautiful rare earth-based nanocrystals (Ye et al., 2010). We applied LnCl<sub>3</sub> (Ln = Y and Er) as precursors in an OA and ODE mixture that was heated to a high temperature, next NH4F and NaOH were added to obtain core nanoparticles of NaYF<sub>4</sub>:Er. Finally Lu(CF<sub>3</sub>COO)<sub>3</sub> and CF<sub>3</sub>COONa mixed with NaYF<sub>4</sub>: Er were further processed under high temperature and oxygen-free environment to obtain stable NaYF<sub>4</sub>:x%Er@NaLuF4 (Feng et al., 2018).

Ln-UCNPs synthesized using the thermal decomposition method are highly monodisperse and uniform in shape. They also display greater up-conversion emission intensity; however, the syntheses are complicated and the products are lipophilic and not stable, which limits the application of thermal decomposition in Ln-UCNPs synthesis.

#### 2.2 Hydrothermal/solvothermal method

The hydrothermal/solvothermal method is facile for synthesizing Ln-UCNPs under mild conditions at a low cost. Generally, hydrothermal syntheses are carried out in a reactor to provide a high-pressure environment. Simple rare Earth nitrates or chlorides are used as precursors for the preparation of Ln-UCNPs. The most common solvents are water, ethanol, glycol and other simple hydrophilic inorganic/organic solvents (Rafique et al., 2019). Li and co-workers introduced oleic acid into solvothermal synthesis. As an oleophilic organic solvent, it broadened the range of materials and structures that can be realized using this method (Wang et al., 2005). The selection of organic additives has a significant impact on the morphology and size of the product. Hydrophilic organic ligands that can adhere to the surface of products and inhibit particle aggregation can endow the nanocrystals with good hydrophilicity, biocompatibility, and functionalizability with biomolecules. It was reported that ethylene diamine tetra acetic acid (EDTA), polyvinyl pyrrolidone (PVP), hexadecyl trimethyl ammonium bromide (CTAB) and polyacrylic acid (PAA)/poly ethylenimine (PEI) as additives improve the morphology and dispersion of Ln-UCNPs (Mousavand et al., 2010; Li et al., 2020a). A mixed solution of  $Ln(NO_3)_3$ , Y:Yb:Tm = 70:30:0.5, was used as a rare Earth precursor with EDTA as an organic additive. NaYF<sub>4</sub>: Yb<sup>3+</sup>, Tm<sup>3+</sup> were synthesized by high temperature and pressure

#### TABLE 2 Typical cases of Ln-UCNPs for sensing.

No	Sensor system	Excitation (nm)	Emission	Sensor type	Recent advances	References
1	NaYF4:Yb,Tm-T (Thymine)	980	475 nm	ECL sensor	In the presence of $Hg^{2+}$ , the T monolayer-modified Au electrode (AuE/T) absorbed $Hg^{2+}$ and T-Ln- UCNPs by T- $Hg^{2+}$ -T matching. Surface-tethered T-Ln-UCNPs further recruited more $Hg^{2+}$ , as well as T-Ln- UCNPs, thus forming a Ln-UCNPs-T- $Hg^{2+}$ -T-Ln-UCNPs reticular architecture on the surface of the electrode	Dhal et al. (2020)
2	ssDNA-NaYF4:Yb,Er@SiO2	980	549, 654 nm	miRNA sensor	In the absence of complementary miRNA sequences, the ssDNA functionalized particles interact with the GQD leading to an enhancement of the up-conversion emission. In the presence of the target miRNA sequences, the hybridization process yields dsDNA on the surface of the Ln- UCNPs that hinders the interaction with GQD and reduces the up- conversion fluorescence enhancement.	Zhou et al. (2020)
3	NaLuGdF4:Yb,Er-Fe <sup>3+</sup> , C u <sup>2+</sup> , and Li <sup>+</sup>	980	543 nm	CAs sensor	It was found that catecholamines could be more effectively detected in the presence of Ln-UCNPs-Fe <sup>3+</sup> , whereas, dopamine and epinephrine were detected selectively using Ln-UCNPs- Li <sup>+</sup> and Ln-UCNPs-Cu <sup>2+</sup> sensors.	Hu et al. (2020)
4	APTEs-NaYF4:Yb,Er-Pt	980	543 nm	TNT sensor	The Janus capsule motors were fabricated by layer-by-layer assembly of Ln-UCNPs-functionalized polyelectrolyte microcapsules, followed by sputtering of a platinum layer onto one half of the capsule.	Zhang et al. (2020)
5	NaGdF <sub>4</sub> :Yb,Er@SiO <sub>2</sub> -Spiropyran	980	540 nm	HIS fluorescent nanosensor	HIS could specifically bind to SP, which could cause the isomerization of SP. His will lead to fluorescence quenching of the sensor based on inner filter effects (IFE)	Wu et al. (2019)
6	NaYF4:Yb,Er-pHrodo	980	550, 590 nm	pH sensor	A nanosensor based on up-conversion resonance energy transfer (UC-RET) between an upconverting nanoparticle (Ln-UCNPs) and a fluorogenic pH- dependent dye PHrodo ™ Red that was covalently bound to the aminosilane surface of the nanoparticles. The sensitized fluorescence of the pHrodo™ Red dye increases strongly with decreasing PH.	Liu et al. (2018b)
7	NaYF4:Yb,Tm-BODIPY	980	451, 475, 64 8 nm	pH sensor	The blue UCL of NaYF4:Yb <sup>3+</sup> ,Tm <sup>3+</sup> Ln- UCNPs excited at 980 nm, that overlaps with the absorption of the pH-sensitive fluorophore, provides reabsorption based excitation of the dye, the spectrally distinguishable green fluorescence of which is switched ON upon protonation, preventing photoinduced electron transfer within the dye moiety, and the pH-inert red UCL act as reference.	Park et al. (2018)

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#### TABLE 2 (Continued) Typical cases of Ln-UCNPs for sensing.

No	Sensor system	Excitation (nm)	Emission	Sensor type	Recent advances	References
8	NaGdF4:Yb,Er-mOrange	980	540 nm	pH sensor	The Ln-UCNPs-mOrange nanoprobe could be fluorescently imaged with 980 nm excitation, having deep penetration depth, by a fluorescence microscope on a coverslip, or uptaken in a single HeLa cell. Nigericin mediated intracellular pH (3.0, 5.0, and 7.0) could be accurately estimated from the CLSM derived FRET ratio.	Qiu et al. (2017)
9	La <sub>2</sub> MoO <sub>6</sub> :Er	379	555 nm	Temperature Sensor	By means of a fluorescence intensity ratio (FIR) technique, the temperature sensing performances in the temperature range of $303-463$ K were investigated based on thermally coupled levels, <sup>2</sup> H11/2 and <sup>4</sup> S3/2, of Er <sup>3+</sup> ions. The sensor sensitivity of Er <sup>3+</sup> - activated La <sub>2</sub> MoO <sub>6</sub> nanoparticles can be greatly affected by the doping concentration and the maximum sensor sensitivity was determined to be about 0.0097 K <sup>-1</sup> at 463 K.	Du et al. (2020)
10	NaGdF <sub>4</sub> :1%Tm/49%Yb@NaGdF <sub>4</sub> :15%Tb/1.5%Eu	980	545 nm	Temperature sensor	The large difference in energy between the emission of Tb <sup>3+</sup> and Eu <sup>3+</sup> made the spectra easier to be detected and calculated based on relative intensity measurement compared to single-ion based systems.	Zhao et al. (2020)
11	NaLuF <sub>4</sub> :Mn,Ln-PNIPAM-Au	980	544, 660,	Temperature sensor	By utilizing red/near-infrared dual emitting NaLuF4: $Mn^{2+}$ , $Ln^{3+}(Ln^{3+} =$ Yb <sup>3+</sup> , Er <sup>3+</sup> , Tm <sup>3+</sup> ) Ln-UCNPs as the energy donor and Au nanoparticles as the acceptor, the temperature resolution of the Ln-UCNPs is significantly increased from 3.1°C to 0.9°C in the physiological temperature range.	Luo et al. (2020)
12	NaY(WO <sub>4</sub> ) <sub>2</sub> :Er,Yb	980	552, 655 nm	Temperature sensor	The maximum relative sensitivity (Srel) and absolute sensitivity (Sabs) were determined to be ~1.2% K <sup>-1</sup> at 293 K and ~0.9% K <sup>-1</sup> at 503 K, respectively. The excellent repeatability of fluorescence intensity ration (FIR) and low temperature uncertainty $\Delta$ Tmin of ~0.4 K at 293 K make this optical nanothermometry cover a wide temperature range of 293–503 K.	Li et al. (2014)
13	Bi <sub>2</sub> Ti <sub>2</sub> O <sub>7</sub> :Yb,Ho	980	550,665,750 nm	Temperature sensor	The maximum relative sensitivity is calculated to be 2.44% at 498 K, obtained from the temperature- dependent spectra by recording in the range of 298–498 K. The samples also provide excellent repeatability and chromaticity stability.	Tse et al. (2019)
14	NaYF4:Yb,Er	980	525,548 nm	Temperature sensor	The spider silks were drawn directly from Araneus ventricosus and were decorated with core–shell Ln-UCNPs <i>via</i> a photophoretic effect. By measuring the fluorescence spectra of the Ln-UCNPs on the spider silks, the membrane temperature of a single breast cancer cell was obtained with absolute and relative sensitivities ranging from 3.3 to $4.5 \times 10^{-3}$ K <sup>-1</sup> and 0.2-0.8% K <sup>-1.</sup>	Yang et al. (2016)

(Continued on following page)

TABLE 2	(Continued)	Typical	cases	of	Ln-UCNPs	for	sensing.
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No	Sensor system	Excitation (nm)	Emission	Sensor type	Recent advances	References
15	NaYF4:Yb,Er-polystyrene	980	542,657 nm	Gas sensor	PS is chosen as a matrix because it displays permeation selectivity for $CO_2$ and rejects protons. The luminescence intensities of the Ln-UCNPs at 542 and 657 nm increase with increasing concentration of $CO_2$ , and the detection limit is 0.11% of $CO_2$ .	Cao et al. (2013)
16	NaYF4:Yb,Tm@PEP	980	474 nm	Fe <sup>3+</sup> sensor	Limit of detections (LOD) of 0.2 $\mu$ M and recoveries of 94.5–102.5%, Ln-UCNPs@PEP was shown to have low cytotoxicity and was used for monitoring Fe <sup>3+</sup> in HeLa cells by fluorescence microscopy.	Gerelkhuu et al. (2019)



in a reactor (Xu et al., 2020). The advantages of hydrothermal/ solvothermal method include the potential for large-scale production. Moreover, the reaction is always carried out under closed conditions without harmful gas leakage, so it is environmentally friendly and non-toxic. However, these conditions also make it impossible to observe the crystal growth process, which impede the studies into the reaction mechanisms.

#### 2.3 Co-precipitation methods

The products of the co-precipitation method are usually chemically homogeneous and uniformly distributed; however, the surfaces are rough and difficult to control. Coudret et al. obtained ultra-small Na(Gd-Yb)F<sub>4</sub>:Tm through an improved co-precipitation method (Figure 1). In addition to the synthesis of specific precursors and microwave-assisted heating, the influence of oleic acid content on heating efficiency was discussed (Amouroux et al., 2019). In 2014, Liu and co-workers demonstrated a simpler co-precipitation method to prepare core-shell NaGdF4 nanoparticles doped with luminescent lanthanide ions that did not require precise control of the feeding rate of shell precursors. However, the large core-shell nanocrystals had a low up-conversion efficiency (Wang et al., 2014b). Jin and co-workers synthesized a near-infrared (NIR) fluorescence "turn-on" kit based on rare Earth ion-doped nanoparticles and gold nanoparticles, which created an HIV-1 based DNA detection system that was simple, homogeneous, and highly selective (Zhou et al., 2019). Chen and co-workers were the first to report the synthesis of CaS:Eu<sup>2+</sup>,Sm<sup>3+</sup> near infrared photostimulated luminescence nanocrystals by a high temperature co-precipitation method. The materials exhibited a fast response to stimuli over 800–1,600 nm (Gao et al., 2019). In conclusion, the application of the co-precipitation method creates products that have biomedical applications; however, they are limited by defects. Regardless, this simple process is conducive to industrial production.

#### 2.4 Other methods

In addition to the processes discussed previously, several novel methods have been developed for the synthesis of Ln-UCNPs. For

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instance, microemulsions and ionic liquids have been applied, and Ln-UCNPs have been prepared using microwave heating. The microemulsion method creates materials in droplets that contains the surfactant, cosurfactant, solvent and water. Few product nanoparticles are prepared this way; furthermore, the dispersion is poor because the growth of the particles is affected by the size of the micelle. Li and colleagues reported a method of microemulsion assisted synthesis of functionalized Ln-UCNPs. The nanoparticles was synthesized in a heterogeneous oil-water microemulsion phase, and the product had a high cross-section and adjustable pore size (Dai et al., 2020).

Microwave synthesis has unique properties, including increased speed and heating efficiency, which contributes to energy savings and environmental protection. It was reported that NaGdF<sub>4</sub>:Yb, Er can be directly synthesized using a microwave digestion/extraction system; furthermore, the produced have good biomedical application prospects (Li et al., 2012).

# 3 Up-conversion luminescence modulation

Key issues concerning the optical properties of Ln-UCNPs include the small absorption cross-section, fluorescence quenching, and the electronic structure that may result in multiple emission lines despite excitation at a single wavelength. As a result, Ln-UCNPs should be classified according to the requirements of applications (Li et al., 2015b). In recent years, a series of Ln-UCNPs with enhanced upconversion luminescence (UCL) have been obtained by adjusting the composition and structure. This provides a deeper understanding of the characteristics and nature of rare Earth luminescence and broadens the potential for applications (Wu et al., 2016; Garfield et al., 2018).

#### 3.1 Species and concentration of doping ions

Up-conversion is the process of converting low-energy photons into high-energy luminescence, which relies on energy transfer within the 4f electron manifold of the luminescent ions. Luminescence mechanisms include excited state absorption (ESA), energy transfer up-conversion (ETU), and cooperative sensitization up-conversion (CSU). The ESA process occurs within a single ion that continuously absorbs photons to create upconverted luminescence. The ETU process involved in a pair of neighboring rare Earth ions, a sensitizer as energy donor, and an activator as energy acceptor. After excitation, the ground state sensitizer ion becomes electronically excited, the energy from which is transmitted to activators. In turn the activator ion transitions to a higher electronic state, and then luminesces to the ground state. The CSU process requires at least three ion centers. Two of them are the same element that act as sensitizers. They can interact with activators simultaneously in the excited state, which in turn transfers energy to activators. Consequently, the doping of rare Earth ions is closely related to the up-conversion luminescence ability of the nanoparticles, and the luminescence intensity can be regulated by adjusting the species and concentration of rare Earth ions.

Ln-UCNPs are composed of activators and sensitizers within a matrix. For up-conversion, the matrix must have excellent optical properties and stability. The most studied are fluoride materials NaYF<sub>4</sub>, LaF<sub>3</sub>, LiYF<sub>4</sub>, and NaGdF<sub>4</sub> among others (Wang et al., 2011; Liu et al., 2012; Wang et al., 2014b; Zhang et al., 2015). To achieve up-conversion luminescence, the energy difference between at least three adjacent energy levels of the activator should be in close proximity. Therefore,  $Er^{3+}$ ,  $Tm^{3+}$  and  $Ho^{3+}$  are the most important due to their step-like energy levels. Sensitizer ions are usually introduced due to the fact that the luminous efficiency of single-doped Ln-UCNPs is not high. Yb<sup>3+</sup> has become the most common sensitizer due to its unique energy level structure (Han et al., 2014).

We synthesized highly doped Er<sup>3+</sup> core-shell nanoparticles of  $NaYF_4:x\%Er@NaXF_4$  (x = 5, 25, 50, and 100; X = Lu and Y). The effect on luminescence as a function of Er<sup>3+</sup> concentration was studied. There was a significant enhancement of red emission at 100% Er<sup>3+</sup> doping (Feng et al., 2018). In a sensitizer and activator codoped system, the concentration of activator generally does not exceed 5% while the sensitizer concentration is relatively high, on the order of 15%–40%. The emission of Yb<sup>3+</sup>/Er<sup>3+</sup> co-doped systems range from 510 nm to 560 nm (green) and 640 nm-670 nm (red). This system can emit with multiple colors as a combination of green and red can produce yellow light. Er3+/Yb3+ co-doped Na<sub>0.5</sub>Gd<sub>0.5</sub>Mo<sub>O4</sub> was reported to emit with characteristic peaks at 531/552/667 nm; furthermore, the intensity of UCL increased with higher Yb<sup>3+</sup> concentration over a certain range (Du et al., 2016). Similarly, the intense emission of the Yb<sup>3+</sup>/Tm<sup>3+</sup> co-doped system was in the blue region, while the Yb<sup>3+</sup>/Ho<sup>3+</sup> co-doped system mostly emitted green light with improved efficiency due to the sensitizer. Rare Earth ions have further utility. For example, multi-doped systems empower enhanced luminescence modulation. Liu et al. reported white light emission from Er<sup>3+</sup>/Tm<sup>3+</sup>/Yb<sup>3+</sup> triple-doped SrLu2O4. The Yb<sup>3+</sup> concentration and pump power can be tuned to modulate the emission color. The optimal doping ratio of 0.5% Er<sup>3+</sup>, 0.5% Tm<sup>3+</sup>, and 20% Yb<sup>3+</sup> created the best balance of red, green and blue luminescence to produce bright white light emission (Liu et al., 2018a). Dammak and coworkers designed a white light modulation system, Yb<sup>3+</sup>/Er<sup>3+</sup>/Tm<sup>3+</sup> doped GdPO<sub>4</sub> at a high concentration of Yb<sup>3+</sup> (35%mol), which emitted white light with excitation by an appropriate laser power (Hassairi et al., 2018). β-NaYF<sub>4</sub>: Yb<sup>3+</sup>, Ho<sup>3+</sup>, Tm<sup>3+</sup> triple-doped Ln-UCNPs can create multicolor UCL by adjusting the doping concentration and excitation power, which resulted in both white and red light output (Gao et al., 2017).

#### 3.2 Surface plasmon resonance modulation

Metal nanoparticles exhibit a strong plasmon resonance intensity due to electron delocalization over a large surface area. The surface plasmon resonance (SPR) effect will occur when the frequency of the incident photon is the same as the surface plasma oscillation. At this time, a strong local electric field is generated around the metal nanostructure, which further increases the excitation and radiation decay rates of Ln-UCNPs and thus enhances the up-conversion luminescence. UCL can be enhanced by SPR (Thariani and Yager, 2010), which prompted us to theoretically explore the effects of metal nanoparticles on Ln-



UCNPs luminescence using the Discrete Dipole Approximation (DDA). The DDA algorithm can calculate the electromagnetic properties of nanoparticles as a function of shape. We synthesized La2O3:Yb/Er@Au, the gold coating of which significantly enhanced the emission intensity of La2O3:Yb/Er@Au by 16.8 times. Experiments demonstrated that the amount of Au added affects the particle spacing and the intensity of UCL. The increase in the electric field simulated by DDA was in good agreement with the observations made in the presence of an Au coating (Lv et al., 2014a). Light exposure and heating of the metal were shown to result in drug release in Na5Lu9F32:Yb/Er@Au. Both DDA simulation and experimental studies of Ln-UCNPs revealed that the coating of Au enhanced the absorptivity, which in turn resulted in a temperature increase upon excitation that facilitated the release of doxorubicin (DOX). Therefore, this system can be used for controlled drug release by the photothermal effect (Lv et al., 2014b). In the first two systems, we only performed electromagnetic calculations on single Au nanoparticles. DDA was used for the first time to perform extinction calculations on the rare earth-metal model of Ln-UCNPs@SiO<sub>2</sub>-Au (Figure 2A) (Lv et al., 2018a). The results revealed the potential to use DDA to guide the construction of rare earth-metal composite materials.

Although considerable progress has been made, many issues remain to be addressed. In the simulations discussed above, gold shells were used to simulate gold coatings. To obtain more accurate results, the Au shells were replaced with randomly distributed gold spheres to simulate Ln-UCNPs@mSiO<sub>2</sub>-Au. Both DDA simulation and experiments demonstrated that the presence of 5 nm Au spheres results in enhancements; however the experimental results on 20 nm Au sphere were inconsistent with the DDA simulations due to insufficient uniformity and aggregation. Regardless, the overall accuracy of the model on the modulation of the luminescence was improved (Lv et al., 2020). Next, we synthesized Au/Ag@Ln-UCNPs, and used DDA to simulate the enhancement on UCL due to the presence of gold nanocages of different sizes and thicknesses. Optical characterizations revealed that the luminous intensity of Au/ Ag@Ln-UCNPs is twice that of Ln-UCNPs alone. In addition, Au/ Ag@Ln-UCNPs were also effective for PTT/PDT treatment of tumors (Liu et al., 2019b). Additionally, Ln-UCNPs@SiO2@Au (SPS@Au) was synthesized and coated with ZnPc (zinc phthalocyanine) to produce SPS@Au/ZnPc. DDA was used to simulate the extinction of SPS@Au/ZnPc as a function of gold particle content (Figure 2B), the results from which revealed enhanced luminescence properties (Lin et al., 2020).

The finite difference time domain (FDTD) method can be used to simulate the enhancement of UCL due to metal SPR. Song and coworkers used FDTD to simulate NaYF<sub>4</sub>: Yb<sup>3+</sup>, Er<sup>3+</sup> up-conversion luminescence in the presence of a gold rod. Single-layer gold nanorod (GNRs) and Ln-UCNPs were assembled on both sides of an isolating MoO<sub>3</sub> layer to demonstrate a luminescence enhancement effect of more than 35 times (Yin et al., 2016). Zhou and coworkers used FDTD to model Ag@SiO<sub>2</sub> to calculate the optimal Ag particle size and silicon layer thickness. The prepared Ag@SiO<sub>2</sub>@YF<sub>3</sub>:Ho<sup>3+</sup> nanoparticles exhibited better luminous



intensity (Xu et al., 2019). Although enhancements are realized using the current strategy of metal modulation to enhance UCL, the effects are actually quite modest. Methods to achieve greater optical enhancements is a problem to be solved in the future.

#### 3.3 Algorithm optimization

A large number of experiments are usually required to determine the optimal doping concentration for Ln-UCNPs.

However, computer technology has revolutionized the traditional screening method. Using algorithms to guide this process can greatly simplify experimental realization. The doping optimization of rare Earth luminescent powder is essentially a combination optimization problem. A product can be designed on a computer and then experimentally realized; these steps are repeated to obtain a material with the best properties. In this process, heuristic algorithms based on natural body algorithms, have been used to guide the synthesis of rare earth-doped luminescent powders with high quantum yield. Heuristic algorithms include the genetic algorithm (GA), particle swarm optimization (PSO), and simulated annealing (SA) (Hopper and Turton, 2001; Hamza et al., 2017; Ozdemir and Karaboga, 2019). GA is a global random search optimization algorithm that uses the "survival of the fittest" mechanism to derive relationships between the material properties and the mole percentage of each raw material, and is often used to guide chemical synthesis optimization problems (Katoch et al., 2021). PSO simulates "bird predation." The algorithm is easy to understand and program, has global search ability; as a result it has been applied in the field of combinatorial chemistry. Annealing is the process in which the temperature of the system decreases with time (Thangaraj et al., 2011). SA continuously iterates a simulated annealing process to find a solution that meets design specifications (Suman and Kumar, 2006). This algorithm has not yet been applied to combinatorial chemistry problems. Therefore, the most widely used optimization algorithm is the genetic algorithm (Lv et al., 2018b).

Our group has studied the pros and cons of SA, the improved SA of harmony search, PSO, and GA for guiding the synthesis of luminescent powders (Figure 3). The efficacy of the four

algorithms were evaluated by taking the same first-generation luminescent powder as the starting point for optimization and performing 5 iterations. SA had no obvious optimization effect; however, better results were obtained when combined with the harmony search. The genetic algorithm was better than PSO; however, generational analysis found that the brightness of the luminous powders as guided by PSO was more gradual (Lv et al., 2019).

In recent years, it was reported that the regression equation was built through the experimental results, which showed the relationship between luminescence and doping concentration. Then genetic algorithm was used to get the doping concentration corresponding to the maximum luminescence intensity (Sun et al., 2015). Coincidentally, Zhao et al. (2019) used the genetic algorithm to modulate  $Er^{3+}/Yb^{3+}$  co-doped Ba5Gd8Zn4O21, resulting in efficient red light emission.

#### 3.4 Dye sensitization

Ln-UCNPs are challenged with weak absorptions and narrow optical excitation regions. These issues can be addressed using the dye sensitization strategy in which organic near-infrared chromophores are coordinated to the surface of Ln-UCNPs. Examples include IR783, IR806, IR808, and indocyanine green (ICG) which act as "antennas" to capture photons and transfer energy to the up-conversion rare Earth particles to improve UCL (Hazra et al., 2018). In 2012, Zou et al. (2012) used IR806 to sensitize β-NaYF<sub>4</sub>: Yb, Er for the first time. In this study, the intensity of upconversion luminescence via excitation with an 800 nm laser increased by 1,100 times compared to that realized from excitation at 980 nm. This work prompted widespread application of this strategy for up-conversion luminescence enhancement. Han and coworkers synthesized (β-NaYF4: 20% Yb<sup>3+</sup>, 2% Er<sup>3+</sup>) Ln-UCNPs without hydrophobic organic ligands, and then explored the best ratio of near-infrared dyes to Ln-UCNPs to enhance luminescence. They coordinated IR783, IR808, IR820 and IR845 to Ln-UCNPs, and found enhancements of 80, 200, 70 and 10, respectively. To explore the sensitization effect of multiple dyes, IR783 and IR845 were simultaneously coordinated to



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the same Ln-UCNPs. The multidye-sensitized Ln-UCNPs showed a wider wavelength range and were applied for orthogonal bioimaging (Wu et al., 2015). Chen et al. proposed a new concept of energy-cascaded up-conversion (ECU) through the design of an IR808-sensitized core/shell Ln-UCNPs. IR808 was coordinated to the Ln-UCNPs and acted as an antenna to collect excitation energy that was transferred to Nd<sup>3+</sup>, Tm<sup>3+</sup> and Yb<sup>3+</sup> through a multi-step process. This approach achieved a high up-conversion quantum efficiency of 19% (Chen et al., 2015).

Although the sensitization strategy can significantly enhance UCL, the dyes are quenched in water which greatly limits potential applications. Researchers have explored the synthesis of more stable and brighter dye-sensitized Ln-UCNPs. It was reported that LnUCNPs sensitized with Cy7 enhanced UCL in ethanol by ~30 times, although the effect was limited in water by ~2 times. To address this problem phosphatidylcholine was introduced to improve water dispersibility, which resulted in an increase of 17 times efficiency and enabled lymphatic imaging (Zou et al., 2016). Liu and coworkers revealed that quenching of dye sensitized Ln-UCNPs in water is the result of dye aggregation. Generally, near-infrared dyes are coupled to Ln-UCNPs through chemical coordination; in contrast, Liu and coworkers constructed dye-sensitized systems through hydrophobic interactions. The amphiphilic molecule DSPE-PEG (1,2-distearoyln-glycerol-3-phosphoethanolamine-N- [(polyethyleneglycol)methoxy]) was used to coat the dye Car-Cl. As a result, the sensitization was improved 85 times in water. Unfortunately, aggregation-induced quenching was nonetheless observed at high concentrations.

To further eliminate strong coordination between the dye and rare Earth ions, Liu and coworkers used two long hydrophobic alkyl chains to replace the carboxyl group of the dye Car-Cl to produce a new dye (Alk-Cl), the use of which achieved enhancement of UCL of 215 times (Figure 4) (Liang et al., 2020a). In addition, NIR-II dye (IR-1061) was used to sensitize core-shell Ln-UCNPs and solve the problem of quenching in water. It was worth noting that the purpose of this research was not to enhance up-conversion, rather, to obtain a strong near-infrared signal. Application of this strategy resulted in an increase in the 800 nm emission of Tm<sup>3+</sup> ions by 2.83 times. Furthermore, the near-infrared emission had a deeper tissue penetration depth, which is more conducive for biological imaging compared to visible emitters (Hazra et al., 2018). Although Ln-UCNPs have multicolor emission, it should be noted that red light has the advantages of deep penetration depth and imparts minimal damage to tissues in biological application.

#### 3.5 Surface modification

During the synthesis of nanoparticles, long-chain polymers like oleic acid always were wrapped on the surface of Ln-UCNPs. In this way, the stability and luminescence intensity in aqueous are decreased compared with organic solvents, which limits the application in organisms. The following methods are usually used to deal with synthesized Ln-UCNPs. 1) Acid or excess ethanol was added. The ligands on the surface of Ln-UCNPs can be removed under the ultrasound. Capobianco and co-workers successfully removed the oleic acid ligands on the surface of NaGdF4: Yb<sup>3+</sup>,Er<sup>3+</sup> by the means of acid treatment (Bogdan et al., 2011) 2). The hydrophobic ligands were replaced by hydrophilic ligands, such as PEI, PAMAM, and PAA, to increase the water solubility of the nanoparticles. (Kovalenko et al., 2009; Kovalenko et al., 2010; Tangirala et al., 2010) 3) Inorganic material shells were coated on the surface of Ln-UCNPs, such as SiO2. This method can improve the water solubility of the nanoparticles effectively. It is worth noting that, thickness of the SiO<sub>2</sub> needs to be determined by multiple experiments. Since too thick or too thin SiO<sub>2</sub> layers may affect the luminescence intensity of Ln-UCNPs and make the synthesis process more difficult. (Li and Zhang, 2006)

#### 4 Ln-UCNPs-based theranostics

The traditional treatment for tumors, chemotherapy and surgical resection, have disadvantages that must be addressed. Several new therapies have attracted recent attention (Atmaca et al., 2021; Kobayashi et al., 2021; Lu et al., 2021; Pedziwiatr-Werbicka et al., 2021; Zhu et al., 2021). PT mainly includes photodynamic therapy and photothermal therapy. In PDT, irradiating a photosensitizer produces reactive oxygen species (ROS) that cause oxidative damage to cells (Yan et al., 2021a). In PTT, light-induced heating damages cancer cells (Shi et al., 2021). Combining photosensitizer or photothermal agent with Ln-UCNPs can achieve PT with near-infrared light.

#### 4.1 Ln-UCNPs-based drug delivery

Drug delivery is an important part of cancer treatment. Generally, Ln-UCNPs can be used as a vehicle for drug delivery to achieve a specific therapy. Mechanisms for drug delivery using Ln-UCNPs include passive, active, and physical targeting. In the passive targeting strategy, drugs are combined with Ln-UCNPs to achieve targeted therapy with the help of the enhanced permeability and retention (EPR) effect. In the active targeting strategy, drugs are combined with Ln-UCNPs, and the interaction between a ligand and receptor, or antigen and antibody, is used to specifically recognize cells to achieve the targeted delivery of drugs. Chen et al. (2017) designed Tm<sup>3+</sup>-doped UCNPs and combined them with lightactivated Ru complexes, so that enzyme inhibitors can be released by NIR excitation. In the physical targeting strategy, designer nanoparticles can be used to release drugs in specific locations by external environmental stimulus, such as changes in pH or temperature, photoexcitation, or magnetic targeting. Lin and coworkers designed Ln-UCNPs doped with Yb3+ and Tm3+ with additional modification of hydrazine monohydrate on the surface. In an acidic environment, the hydrogen bonds in the nanoparticles dissociate, enabling drug release (Yang et al., 2014). Mykhaylyk et al. (2001) designed magnetic nanoparticles that can deliver drugs to penetrate the blood-brain barrier and enter the mouse brain (Mykhaylyk et al., 2001). De et al. designed a polyelectrolyte complex based on Yb<sup>3+</sup> and Er<sup>3+</sup> to deliver pharmaceutical grade protein (De et al., 2022). The modified nanosystem overcame the problem of protein aggregation in the cell membrane and protected the protein drugs from destruction by proteases and the action of heat. At the same time, the nanoscale drug carrier system responded to the 980-nm NIR light, and realized the imaging of the protein delivery process.

#### 4.2 Ln-UCNPs-based phototherapy

PDT has been clinically applied as a supplement to traditional therapy. Porphyrin is the first photosensitizer approved for this purpose (Tian et al., 2020), and mTHPC (meso-tetra hydroxy phenyl chlorin), a second generation photosensitizer, has shown many excellent characteristics in photodynamic therapy (Pinto et al., 2021; Yakavets et al., 2021; Yuan et al., 2021). In addition, chlorin dihydrogen E6 (Chlorin e6, Ce6), ZnPc and other photosensitizers have been widely used in scientific research although they have not been clinically approved (Chen et al., 2021a; Zhang et al., 2021a; Chen et al., 2021b; Hu et al., 2021; Lee et al., 2021; Shen et al., 2021; Zheng et al., 2021). Most photosensitizers are hydrophobic and easily aggregate in solution, which introduces practical difficulties (Liu et al., 2021a; Lin et al., 2021; Wei et al., 2021; Wu et al., 2021). Compared with PDT, there are less examples of the clinical application of PTT for tumor treatment. ICG is a dye that has been widely used in clinical diagnosis (Lutken et al., 2021; Teng et al., 2021). It can absorb in the near-infrared (600-900 nm) which enhances tissue penetration. In addition to its use in imaging and diagnosis, ICG has high photothermal conversion efficiency for photothermal therapy which is helpful for follow-up treatment of tumors (Ravichandran et al., 2020; Zhang et al., 2021b).



(A) In vitro P11 confocal images of ECA109 cells treated with PBS and BINS@NaLnF4, with or without NIR irradiation. [Reprinted with permission from Ref. (Ma et al., 2021a) Copyright 2021: Royal Society of Chemistry]. (B) Images of tumor after treatment. [Reprinted with permission from Ref. (Wang et al., 2020) Copyright 2020: Royal Society of Chemistry]. (C) Photographs of female BALB/c nude mice bearing T24 tumors when treated with DNA–Ln-UCNPs-Au hydrogel, Ln-UCNPs-Au, and PBS samples over a period of 21 days after NIR irradiation in 3 min (1 W cm<sup>-2</sup>); s.c., subcutaneous injection. [Reprinted with permission from Ref. (Liu et al., 2020) Copyright 2020: John Wiley & Sons, Inc.].

Currently, most of the photothermal agents are still applied in preclinical or early clinical research due to the fact that photothermal reaction cannot not completely eradicate a tumor; furthermore, there are additional risks due to overheating caused by laser ablation (Gao et al., 2020; Guo et al., 2021; Li et al., 2021; Pang et al., 2021; Zhao et al., 2021).

Ln-UCNPs are candidates for phototherapy due to their low toxicity and ability to be excited by near-infrared light. Ln-UCNPs are often used to deliver other molecules or add modifiers, for which the ability to upconvert expands the range of usable therapeutic agents making it more suitable for cancer phototherapy. In most cases, PDT and PTT effects exist simultaneously (Yang et al., 2021a; Bian et al., 2021; Yang et al., 2021b).

Generally, Ln-UCNPs is used in phototherapy to convert near infrared into visible light to trigger a photodynamic response. Guang and co-workers synthesized BiNS@NaLnF<sub>4</sub>(Ln = Gd) using a solvothermal method (Figure 5A). Specifically, NaGdF4 was loaded onto Bi ultra-thin nanosheets, and up-conversion was observed under 980 nm laser irradiation to stimulate ROS generation. NaLnF<sub>4</sub> has a light-to-heat conversion efficiency of



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35.3% (Ma et al., 2021a). Ln-UCNPs can also be used as a light energy converter to participate in the reconstruction of a tumor's microenvironment (Figure 5B). The emitted light of a Ln-UCNPs can activate a photoacid to release H<sup>+</sup>, which reduced the pH value of the tumor environment and improved the release of ROS in the cell in response to acid environment (Wang et al., 2020). Liu et al. (2020) synthesized an injectable DNA-Ln-UCNPs-Au hydrogel, which enhanced the aggregation of Ln-UCNPs-Au through electrostatically complexed DNA strands and achieved a photothermal conversion efficiency of 42.7% (Figure 5C). In in vivo experiments, DNA-Ln-UCNPs-Au showed good stability and anti-cancer activity. In these preclinical studies, Ln-UCNPs have played an important role for tumor treatment. Since the excitation wavelength is in near-infrared band, phototherapy based on Ln-UCNPs can avoid the self-absorption problem of biological tissues and increase the penetration depth.

#### 4.3 Ln-UCNPs-based phototherapy with chemotherapy

Chemotherapy can address the shortcomings of phototherapy, while phototherapy can more accurately target tumors and can be used to visually monitor drug release when combined with bioimaging (Andre et al., 2020; Birtle et al., 2020; Zheng and Xu, 2020; Yan et al., 2021b). A Ln-UCNPs-based multifunctional platform, Ln-UCNPs@PDA@Cy3-pep, that has treatment and real-time monitoring functions was reported (Liu et al., 2021b). The Ln-UCNPs comprised the core, while the chemotherapeutic drug staurosporine (STS) was loaded on the polydopamine (PDA) shell. The complex was shown to be effective for both photothermal therapy and chemotherapy under near infrared light irradiation. The quenching and restoration of Cy3 fluorescence was used to monitor the anti-cancer efficiency of the complex in real time (Liu et al., 2021b). Ju and coworkers reported a combination of chemicalphotodynamic therapy based on a dual emitting Ln-UCNPs that was functionalized with a photosensitizer and the prodrug camptothecin. The surface was modified to enhance water solubility and targeting. Near-infrared excitation resulted in ultraviolet emission that activated the toxicity of CPT, and additional blue emission activated the photosensitizer to produce singlet oxygen to kill cancer cells (He et al., 2021). Huang and coworkers modified the photosensitizer to the surface of Ln-UCNPs to obtain Ln-UCNPs@PFNS. AQ4N, a hypoxia-activated prodrug that displays high toxicity selectively to hypoxic environment, was added to the pH-sensitive surface coating for chemotherapy (Figure 6). The surface coating decomposed at the tumor site due to the acidic environment, resulting in exposure of AQ4N and the photosensitizer. Under near-infrared excitation the photosensitizer generated ROS and aggravated the hypoxia at the tumor site which enhanced the therapeutic effect of hypoxia-activated AQ4N (Ji et al., 2019). It is promising to actively explore therapies that can assist chemotherapy given its role as the dominant cancer treatment. It is foreseeable that the structure and optical properties of Ln-UCNPs will add value in chemotherapeutic approaches to treat cancer more effectively (Liang et al., 2020b).



(A) Scheme of synergistic phototherapy for augmentation of antitumor immunity. Upon laser irradiation, nanoparticles ablate the primary tumor through phototherapy. (Reprinted with permission from Ref. (Yan et al., 2019) Copyright 2019: John Wiley & Sons, Inc.). (B) Schematic depiction of the experimental approach for the evaluation of the abscopal effects induced by Ln-UCNPs/ICG/RB-mal based phototherapy. (Reprinted with permission from Ref. (Wang et al., 2019) Copyright 2019: John Wiley & Sons, Inc.). (C) Schematic of the design of a photoactivatable immunodevice through the integration of Ln-UCNPs with the UV light-responsive photoactivatable CpG (PCpG). Ln-UCNPs act as transducer to upconvert NIR light into UV light locally, thus liberate CpG oligonucleotides (ODN) from PCpG to achieve refined temporal control on its immunoactivity. [Reprinted with permission from Ref. (Chu et al., 2019) Copyright 2019: Nature Publishing Group].

#### 4.4 Ln-UCNPs-based phototherapy with immunotherapy

In recent years, immunotherapy has attracted attention due to the targeting capability and increased safety. Tumor immunotherapy does not reply on external stimuli, rather, it activates the immune response and cultivates immune cells to attack cancer cells (Tan et al., 2020a). Unlike traditional therapies, cancer cells can be removed continuously and quickly. Due to the efficacious anti-cancer effects of anti-CTLA-4 and anti-PD-1 antibodies, immunotherapy has the potential to revolutionize tumor treatment (Kamata-Sakurai et al., 2021; Tay et al., 2021). Many studies have demonstrated the potential for immunotherapy to improve the survival rate of patients and improving quality of life (Borcoman et al., 2019; Wallis et al., 2019; Mpekris et al., 2020). The combination of Ln-UCNPs-based phototherapy and immunotherapy may augment each other's therapeutic effects. Liu et al. prepared a core-shell structure with a core PDA, a NaGdF<sub>4</sub>:Yb/Er shell, and modified it with the photosensitizer Ce6 (Figure 7A). When irradiated with a 980 nm laser, the PDA component of the PDA@Ln-UCNPs-PEG/Ce6 acted as a photothermal agent while the Ce6 functioned as a photodynamic therapy agent. Phototherapy stimulated the body to produce an immune response, activated T lymphocytes and T memory cells, and helped to inhibit tumor metastasis and recurrence. However, it did not protect the mice from death threats caused by cancer. When combined with the immunosuppressant PD-1, the survival rate of mice was significantly improved to 77.8%, demonstrating the advantages of immunotherapy in long-term survival (Yan et al., 2019). Similarly, Chen and co-authors constructed a Ln-UCNPs/ ICG/rose bengal (RB-mal) system (Figure 7B) that triggered enhanced phototherapy by ICG under near-infrared irradiation. Tumor-derived protein antigen was captured by the nano-platform and kept in place to trigger a systemic anti-tumor immune response.

Experiments in mice proved that Ln-UCNPs/ICG/RB-mal can not only cure tumors *in situ*, but also inhibits the growth of distant tumors, illustrating the generation of a tumor-specific immune response (Wang et al., 2019a). In addition, Ln-UCNPs can stimulate the immune response. Li and co-workers combined Ln-UCNPs with PCpG for immunotherapy (Figure 7C). The core-shell nanoparticles NaGdF<sub>4</sub>:70%Yb, 1%Tm@NaGdF<sub>4</sub> emitted at 313, 363, 453 and 478 nm under 980 nm laser excitation. The UV light activated PCpG to release the immunotherapy agent CpG. In mouse experiments, it was worth noting that the CpG/UCs conjugate proved more effective compared to PCpG/UCs + NIR; however, the former caused severe systemic toxicity which reveals the advantages of using Ln-UCNPs in this process (Chu et al., 2019).

When combining phototherapy with immunotherapy, both the near-infrared irradiation and phototherapy reagents elicit the body's immune response (Hou et al., 2018; Dai et al., 2020; Sun et al., 2020). However, the process is not clear, and as such exploring complex systems that can cause an immune response is still an urgent issue to be solved.

### 5 Ln-UCNPs-based bioimaging

Recent research in biological imaging has centered on the design of new optical molecular probes (Yao et al., 2020).

Since biological tissue is a high-scattering medium, current imaging technology has disadvantages such as low penetration depth, interference from biological autofluorescence, and may cause tissue damage which greatly limits the application of biological imaging (Jia et al., 2020). Ln-UCNPs have a strong anti-Stokes shift, and the ability to absorb near-infrared light helps avoid biological background fluorescence interference (Dhal et al., 2020). Furthermore, near-infrared light has a deep tissue penetration depth. However, Ln-UCNPs cannot be directly applied to biological imaging due to fluorescence quenching, hydrophobicity, biological toxicity and other problems. Addressing these issues requires modification to their structure (Zhou et al., 2020).

#### 5.1 Ln-UCNPs-based fluorescence imaging

Fluorescence imaging generally uses photoluminescence probes, for which Ln-UCNPs are excellent candidates as their application does not result in tissue damage (Hu et al., 2020; Zhang et al., 2020). Recently, Hao and co-workers synthesized polyacrylic acid-modified NaLnF4: 40Gd/20Yb/2Er, (Ln = Y, Yb, Lu, PAA-Ln-NRs). PAA-Ln-NRs with bright NIR II emission were injected into the tail vein of mice, and under excitation from a 980 nm laser they achieved highprecision imaging of small tumors and metastases that enabled early cancer diagnosis (Wu et al., 2019). Liu et al. synthesized dyesensitized Ln-UCNPs with a reduced propensity for aggregation in water through hydrophobic coordination. Issues with the quenching of Ln-UCNPs luminescence in water was addressed by adjusting the dye absorption band (Liang et al., 2020a). Chen et al. designed an ingenious NaYF4@NaYbF4@NaYF4:Yb3+/Tm3+@NaYF4 structure for multi-channel fluorescence imaging. After intravenous and subcutaneous injection of the Ln-UCNPs, clear in vivo color imaging was obtained (Li et al., 2020b). The Fuyou group (Qiu et al., 2017; Liu et al., 2018b; Park et al., 2018) recently synthesized a rareearth probe with NIR-II imaging capability.  $Ce^{3+}$  doping significantly increased the intensity of NIR-II luminescence, resulting a higher resolution in *in vivo* tumor imaging (Cao et al., 2020).

There are some interesting new studies for Ln-UCNPs outside *in vivo* imaging. Giri et al. coated Ln-UCNPs with oleylamine to obtain OA-Ln-UCNPs, and then further processed it to make a Ln-UCNPs oleogel with better skin permeability. The loading of Ln-UCNPs in the oleogels was varied to study the relationship between concentration and fluorescence intensity. For *in vitro* experiments, the Ln-UCNPs oleogel could penetrate the skin more deeply than free OA-Ln-UCNPs and be used as a skin tissue imaging agent under near-infrared excitation. Xu and co-workers reported the application of Ln-UCNPs in plant cell imaging, whereby LiErF4:1%Tm<sup>3+</sup>@LiYF4 with a core-shell structure could enter the cell membrane easily and emit bright red light (Qiao et al., 2021).

# 5.2 Ln-UCNPs-based computed tomography

Computed tomography (CT) is based on the difference in the absorption and transmittance of X-rays among various tissues of the human body. The data is scanned by an instrument and processed to determine the pathological condition (Pfeiffer, 2018). Lanthanides have high X-ray attenuation coefficients (Issa et al., 2018), for example, the atomic number and electron density of Lu and Yb are greater than iodine which is currently used in CT. Du et al. reported the synthesis of core-shell nanoparticles NaYF4:Yb/Er@ NaLuF<sub>4</sub>:Nd/Yb@NaLuF<sub>4</sub> and surface modification of chitosan. Next, Ag<sub>2</sub>Se was grown in situ to form NaYF<sub>4</sub>:Yb/Er@NaLuF<sub>4</sub>: Nd/Yb@NaLuF4@CS@Ag2Se. In vivo imaging experiments with these agents demonstrated potential for clinical CT (Du et al., 2020). Bismuth doping of materials significantly improves CT imaging as Bi has better X-ray attenuation ability compared to lanthanides. You et al. reported the synthesis of a porous BiF3:Yb, Er nanomaterial that generated an in vivo CT signal as demonstrated with concentration dependence. The CT value curve showed that the Hounsfield unit (HU) value of the sample was higher than observed in commercial Iohexol (Zhao et al., 2020). Gao and co-workers reported the synthesis of BaYF5 with different bismuth doping ratios: Yb, Er, Bi-x (x = 0-3). Under the excitation of a 980 nm laser, the up-conversion luminescence was enhanced with increasing Bi content, reaching a maximum at x = 2.5. Then Ln-UCNPs was coated with citrate for biological imaging. Both in vitro and in vivo experiments demonstrated that the Ln-UCNPs can be successfully used in X-ray CT imaging by accumulating at the tumor site (Luo et al., 2020).

# 5.3 Ln-UCNPs-based magnetic resonance imaging

Magnetic resonance imaging is a technique in which radio frequency pulses are applied to generate structural information



Positive contrast enhancement evaluation *in vivo*. (**A**, **B**) T1-weighted MRI and corresponding pseudocolor images of tumor-bearing mice after intravenous injection of cell membrane coated-BSNPs (MSNPs) (**A**) and Magnevist (**B**) with the same dosage (2.5  $\mu$ mol of Gd<sup>3+</sup> for each mouse). Images were captured before and at different time points after the administration of contrast agents. The time points were collected at the midpoint of the time interval during each imaging acquisition. The dotted circles represent the regions of interest: 1) tumor, 2) muscle, 3) background, and 4) bladder. Scale bars are 5 mm for all images. The small spots on the corners are from the circulation apparatus in the MRI scanner. (**C**, **D**) Tumor-to-background (T/ B) and tumor-to-muscle (T/M) contrast ratios based on the corresponding MRI images. Values represented as means  $\pm$  s.d. (*n* = 3). [Reprinted with permission from Ref. (Yi et al., 2019) Copyright 2019: John Wiley & Sons, Inc.].

(Tirotta et al., 2015; Clough et al., 2019). The signal is generated from relaxation of nuclei from the excited state to equilibrium over the relaxation time. There are two relaxation times, labeled T1 and T2, where T1 is the spin-lattice or longitudinal relaxation time and T2 is the spin-spin or transverse relaxation time. Therefore, MRI is divided into T1 MRI and T2 MRI. The lanthanide gadolinium is the main contrast agent for T1 MRI due to its paramagnetic properties (Li et al., 2014; Yang et al., 2016; Tse et al., 2019). Liu et al. reported a T1-weighted nanocontrast agent with smart MRI switch based on NaGdF<sub>4</sub>. Ultra-small NaGdF<sub>4</sub> and pH-sensitive CaCO<sub>3</sub> generated self-assembled bare self-assembled nanoparticles (BSNPs) in organic solvents (Figure 8). The addition of a tumor targeting coating on the surface effectively guided the BNSPs to the tumor location, and then CaCO3 reacted with the acidic environment to release NaGdF4 to achieve MRI with 60 times higher contrast compared to the commercial contrast agent Magnevist (Yi et al., 2019). Superparamagnetic Fe<sub>3</sub>O<sub>4</sub> nanoparticles combined with Ln-UCNPs are often used in T2 MRI. Li et al. synthesized Fe<sub>3</sub>O<sub>4</sub>@  $NaGdF_4$ :Yb:Er-HMME with a core-shell structure, which was used for both treatment and imaging. The super paramagnetism of the sample was first confirmed, and its T2-weighted MRI performance was studied. Compared with the commercial T2 contrast agent Feridex, the samples performed better, and were effective for use in *in vivo* T2 MRI (Wang et al., 2019b).

### 5.4 Other imaging based on Ln-UCNPs

Single-Photon Emission Computed Tomography (SPECT) and Positron Emission Tomography (PET) are two techniques in nuclear medicine. PET is the only imaging technique that can interrogate biomolecular metabolism, receptors, and neuromediator activity *in vivo*. Generally, substances necessary for metabolism, such as glucose, are labeled with short-lived radionuclides such as <sup>18</sup>F and <sup>11</sup>C. After injection into the human body, metabolic activities are reflected by the accumulation of the radiolabeled probes to enable diagnosis. Fang et al. (2020) used cancer cell membrane-modified NaGdF<sub>4</sub>:Yb,Tm@ NaGdF<sub>4</sub> for UCL/MRI/PET trimodal tumor imaging and successfully differentiated triple-negative breast cancer subtypes MDA-MB-231 and MCF-7. Sun et al. (2011) used an efficient strategy for labeling Ln-UCNPs with <sup>18</sup>F, and successfully applied the materials in sentinel lymph nodes mapping with PET imaging and detection. The materials were realized by the reaction between rare Earth cations and fluoride ions. The process was simple, fast, and efficient as no organic reagents were applied.

The principle of SPECT is to label probes with short half-life nuclides and inject them intravenously. The nuclides emit y-rays through decay, and the y-rays are then converted into electrical signals and input into a computer for tomography reconstruction. A cross-section or three-dimensional image reflecting the physiological condition of organs in the human body can be obtained. Li et al. (2020b) prepared radioactive PEG-modified NaYF4:Yb, Er, Sm. These 10-nm nanoparticles were detected in kidney and urine by SPECT imaging and gamma counter analysis, confirming the potential for these probes as a biodistribution markers (Cao et al., 2013). Ma et al. (2021b) prepared a platelet membrane-coated nanostructure (PM-PAAO-Ln-UCNPs) containing Ln-UCNPs and Ce6 photosensitizer (PAAO = poly(noctylamine) acrylate), and injected them into mice models. SPECT/CT dual-mode imaging was performed and the precise location of an atherosclerotic plaque was demonstrated.

#### 6 Ln-UCNPs-based biosensing

The unique optical properties of Ln-UCNPs make them effective for biological analysis and sensing. First, they are easily incorporated into a fluorescence analysis scheme due to their robust emission properties and high chemical stability. Second, the near-infrared excitation of Ln-UCNPs can effectively avoids autofluorescence of biological tissues. The use of Ln-UCNPs as fluorescent sensors has been extensively studied (Laurenti et al., 2016; Gerelkhuu et al., 2019; Yuan et al., 2019; Su et al., 2020; Gu et al., 2021). This section introduces the application of Ln-UCNPs-based pH and temperature sensors, as well as gas and ion sensors and some other platforms. And the typical cases of Ln-UCNPs for sensing are shown in Table 2.

#### 6.1 Ln-UCNPs-based pH sensors

The pH of the cell can reflect its condition; for example, abnormal cells are acidic. Furthermore, as some viruses and germs are most active under acidic conditions, (White et al., 2017) it is important to monitor intracellular pH. Ratiometric (dual color) Ln-UCNPs-based pH ratiometric sensors can be prepared by first analyzing the emission spectrum of Ln-UCNPs to ensure that it has a pH-insensitive component to serve as a reference, and then coupling it to a fluorescent pH indicator. Proper spectral matching results in fluorescence resonance energy transfer that can generate pH-dependent emission. The Schaferling group coupled Ln-UCNPs to a fluorescent pH-dependent dye pHrodoTM Red. The NaYF<sub>4</sub>:Yb<sup>3+</sup>, Er<sup>3+</sup> material emits at 550 and 660 nm under laser excitation at 980 nm. As the emission peak at 550 nm was found to be invariant to changes in pH, it was used as a reference signal. The dye pHrodoTM Red emitted at

590 nm with an intensity that is dependent on pH. As a result, the combination of the two chromophores created a ratiometric fluorescence probe that displayed a linear response to pH over the range 3-6.7 (Arppe et al., 2014). Likewise Resch-Genger et al. combined NaYF4:Yb3+, Tm3+ with a pH-sensitive BODIPY dye to create a ratiometric pH sensor (Figure 9). Excitation at 980 nm resulted in 475 nm emission of Tm<sup>3+</sup> that was absorbed by the dye, while the pHinsensitive 648 nm emission of Tm<sup>3+</sup> was used as a calibrant against the 528 nm emission of BODIPY. This two-component sensor was successfully applied for pH monitoring in Escherichia coli (Radunz et al., 2019). Ln-UCNPs can also be coupled to pH-dependent fluorescent proteins to create ratiometric sensors. Recently, it was reported that Ln-UCNPs were combined with mOrange fluorescent protein. Excitation at 980 nm resulted in UCL green emission by the Ln-UCNPs, which subsequently excited the mOrange fluorescent protein. The ratio of the pH independent Ln-UCNPs emission at 655 nm to the pH- dependent emission of mOrange fluorescent protein was a quantifiable metric that was shown to have good stability and reversibility (Ghosh et al., 2020).

#### 6.2 Ln-UCNPs-based temperature sensors

Sensitive, convenient, and biocompatible temperature sensors are needed for biological studies (Tran Quang et al., 2016; Ge et al., 2020). Some rare Earth particles have temperature sensitive luminescence properties, which makes them good candidates for biological thermal sensing (Du et al., 2014; Zheng et al., 2014; Wang et al., 2015; Du and Yu, 2017). Lin et al. synthesized doubly-doped NaLuF4:Mn<sup>2+</sup>,  $Ln^{3+}(Ln^{3+} = Yb^{3+}, Er^{3+}, Tm^{3+})$ , which have red/NIR dual emission that can be enhanced by the SPR effect of proximal Au nanoparticles. Embedding both these materials into the thermoresponsive polymer poly(N-isopropylacrylamide) (PNIPAM) resulted in a temperature dependent modulation of the Ln-UCNPs and Au nanoparticle distance. The effect was to modulate the red to NIR emission ratio, which was the metric of the temperature-sensitive sensor that had a resolution of 0.9°C (Xiao et al., 2014). Shahzad et al. (2019) co-doped microfibers with LiYF<sub>4</sub>:Yb<sup>3+</sup>/Er<sup>3+</sup>, polymethyl methacrylate, and silver to create temperature sensors. The temperature dependent ratio of the emission intensity at 522 nm and 541 nm of the Ln-UCNPs was quantified over the range of 303-348 K. Doping with Ag was shown to significantly improve the photostability and temperature response of the composite (Shahzad et al., 2019). A study on the temperature sensitivity of ZnO:Yb3+/Tm3+ has been reported. The Ln-UCNPs was excited using a 980 nm laser to produce blue and red UCL emission. The UCL decreased at lower temperatures in the range of 300°C-780°C. The ratio of the intensities of the blue and red emission was modulated by 2.1% K<sup>-1</sup> at 293 K (Li et al., 2017a). Zhong et al. synthesized a new type of 8.5 nm  $\times$  12.5 nm nanoparticle of NaY(WO4)2:Er<sup>3+</sup>, Yb<sup>3+</sup> that were shown to be temperature sensitive over the range 293 K-503 K (Lin et al., 2019). In addition to explore the relationship between luminescence of Ln-UCNPs and temperature, researchers have combined various fiber optic probes and temperature-sensitive Ln-UCNPs. Kumar et al. designed Ln-UCNPs coated with polydimethylsiloxane (PDMS) to obtain better fluorescence emission. The pure Ln-UCNPs and Ln-UCNPs-PDMS composite materials were coated on optical fibers for temperature sensing. The sensor coated with composite material displayed a linear response from 295 to 473 K



(Kumar et al., 2020). A recent report demonstrated the coating of a temperature-dependent Ln-UCNPs onto the surface of spider silk, a natural optical fiber, to construct a temperature sensor with good biocompatibility. The change in fluorescence intensity of Ln-UCNPs reflected the temperature change of cancer cells. In addition, the sensor successfully detected temperature changes during apoptosis (Gong et al., 2021). Meiling et al. designed a lanthanide nanoscale temperature measurement system that can be used for the diagnosis of in vivo inflammation. The structure included an inert core, an active shell and an inert shell. The thermosensitive lanthanide elements were localized in the intermediate shell to shield from interference of the bioactive environment. This ternary structure enabled nanothermometers to continuously measure temperature changes of up to 4 mm depth in biological tissues, with high temperature sensitivity over a physiological temperature range of 10°C–64°C (Tan et al., 2020b). Although Ln-UCNPs are not the only material used for temperature sensors, their use imparts unique advantages. Ln-UCNPs have adjustable excitation wavelengths and can be excited by nearinfrared light, making such temperature sensors beneficial for in vivo applications. Additionally, Ln-UCNPs have multi-color luminescence, which enables a wide selection of emission for construction of a temperature sensor.

#### 6.3 Ln-UCNPs-based gas sensors

Gas molecules are of great significance in many biological processes. For example, O<sub>2</sub> is important for maintaining

metabolism (Mates et al., 2012). CO<sub>2</sub> can regulate breathing and the acid-base balance in the body. NO regulates cardiovascular function and improves the immunity of white blood cells (Carpenter and Schoenfisch, 2012; Lundberg et al., 2015; Farah et al., 2018). As a result, the sensing of gas molecules can elucidate the internal physiological behaviors of organisms. In 2010, Achatz et al. (2011) reported a CO<sub>2</sub> gas sensor based on Ln-UCNPs for the first time. In their system bromothymol blue was used as the luminescence intensity modifier of Ln-UCNPs on polystyrene. Specifically, bromothymol blue the absorption of bromothymol blue quenched the emission of the Ln-UCNPs; however, the presence of acidic CO<sub>2</sub> changed the pH which instigated a color change. Thus, when the CO<sub>2</sub> concentration increased, the absorption of bromothymol blue was minimized which resulted in higher intensity Ln-UCNPs fluorescence that enabled a quantitative detection of CO<sub>2</sub> with a detection limit of 0.11% (Ali et al., 2010). The same group created other gas sensors using Ln-UCNPs. They reported the first application of NaYF<sub>4</sub>:Yb, Tm excited by near-infrared light as an O<sub>2</sub> sensor. First, an iridium (III) oxygen probe, Ln-UCNPs, and ethyl cellulose were dissolved in tetrahydrofuran. The solvent was evaporated to yield a sensor film. The Ln-UCNPs was excited by a 980 nm laser and emitted at 455 nm and 475 nm. These two emission peaks overlapped the absorption of the iridium complex at 468 nm. Therefore, Ln-UCNPs acted as a nanolamp in the sensor. The fact that the iridium complex's emission at 568 nm is quenched by O<sub>2</sub> enabled quantitatively oxygen detection (Achatz et al., 2011).



#### 6.4 Ln-UCNPs-based ion sensors

Although the content of metal ions in organisms is small, they play an important role in maintaining the acid-base balance of cells and organisms and other metabolic activities, and are components of many complex biological compounds. The luminescence properties of Ln-UCNPs show great advantages for metal ion detection. Many studies have demonstrated that ion sensors based on Ln-UCNPs have high sensitivity and selectivity, the results from which can be visualized for convenient operation. Iron directly participates in the transport and storage of oxygen. It is a component of hemoglobin, myoglobin and cytochrome, and is necessary for many metabolic processes (Abbaspour et al., 2014; Sangkhae and Nemeth, 2017). The Lee group reported that adrenaline-modified NaYF4:Yb, Tm was used for intracellular Fe3+ detection. PEP can complex with Fe3+, and the energy transfer with the Ln-UCNPs occurred through non-radiative electron transfer and energy return (EBT), resulting in reduced Ln-UCNPs emission at 474 nm. The detection limit of the Fe<sup>3+</sup> sensor was 0.2  $\mu$ M over a range of 1–10  $\mu$ M (Gerelkhuu et al., 2021). The content of zinc in the human body can affect the activity of many enzymes, and as a result Zn<sup>2+</sup> has an important role in human health (Maret, 2013). Chang et al. synthesized a Zn<sup>2+</sup> sensor composed of a Ln-UCNPs and a Zn<sup>2+</sup> sensitive dye.

NaYF<sub>4</sub>:Yb/Tm@NaYF<sub>4</sub> has a multi-peak emission; the blue component at 475 nm was within in the absorption range of the dye while the 654 nm emission was not affected. When  $Zn^{2+}$  was added, the absorption of the dye shifted to 360 nm, which led to an increase in the ratio of I475 nm/I654 nm. The sensor successfully detected  $Zn^{2+}$  in a live animal model of zebrafish (Peng et al., 2015).

Copper is an indispensable component in blood and participates in hematopoietic process and iron metabolism. It was reported that core-shell Ln-UCNPs were electrostatically adsorbed onto flexible carbon fiber cloth (CFC) to create Cu2+ sensors (Figure 10). The absorption of Cu<sup>+</sup> and Cu<sup>2+</sup> coincided with the emission of Ln-UCNPs, which is a sensing mechanism. It was the first time that electrochemical technology was used to improve the sensing performance. Cu2+ accumulated when a voltage of 0.3 eV was applied. CFC reduced the quenching of Ln-UCNPs in water. The synergy of the electrochemical technology and the CFC protective layer resulted in a detection limit of 82 ppb (Wong et al., 2019). Trace fluoride can promote the normal development of teeth and bones, but excessive fluoride causes dental and skeletal fluorosis. Dualfunctional gallic acid-Fe(III) modified Ln-UCNPs was reported with a 654 nm emission that was quenched by the Fe-complex. The presence of F<sup>-</sup> destroyed the Fe-complex, which imparted a sensing mechanism between the UCL and F- ion analyte (Ma et al., 2017).

#### 6.5 Other new sensors

Recently there have been many reports on the use of Ln-UCNPs for the detection of miRNA and other biologically active molecules (Yuan et al., 2015; Li et al., 2016). Trypsin is an activating enzyme that plays an important role in food digestion and has anti-inflammatory and swelling functions (Plattner and Noe, 2015; Wattanasiritham et al., 2016). Guo et al. synthesized Ln-UCNPs-peptide-AuNP for the detection of trypsin and its



inhibitors. The peptide, DDDDARC, is sensitive to trypsin. In the initial state, the emission of UCL was quenched by the Au NP due to Förster Resonance Energy Transfer (FRET) energy transfer. After adding trypsin the peptide was cleaved and UCL was restored. The detection limit of the trypsin sensor was 4.15 ng/mL (Wu et al., 2017). Cytochromes are involved in cell redox reactions and take part in cell energy transfer (Zanger and Schwab, 2013). Wang et al. attached a Cy3-labeled aptamer to the surface of a Ln-UCNPs wrapped with PDA (Figure 11). The aptamer responded to cytochrome c to trigger changes in the fluorescence intensity of Cy3, and the internal UCL served as a reference signal. The sensor reflected the level of Cytc through a ratiometric fluorescence signal, with a detection limit of 20 nM over a range of 50 nM to 10  $\mu$ M (Ma et al., 2017).

Recent studies have demonstrated that a single sensor can be used for the simultaneous detection multiple biomolecules. Xu et al. developed an Au-Au-Ln-UCNPs with an aptamer with sensitivity for both alpha-fetoprotein (AFP) and mucin 1. The sensor generated both Raman and fluorescence signals. Mucin 1 concentration was detected through the change of surface enhanced Raman scattering intensity, and AFP was sensed by the change of fluorescence intensity. The detection limits of both proteins were at an attomolar level (Qu et al., 2017).

Thrombin acts on the last step of the blood coagulation process. It can be used to stop bleeding and is a relevant marker for tumor diagnosis. Prostate-specific antigens are abundantly present in prostate tissue and semen, with extremely high tissue organ specificity, and are currently the first-choice marker for the diagnosis of prostate cancer. Kuang et al. used a Raman signal and fluorescence of Au-Ln-UCNPs in conjunction with aptamers to respond to thrombin and prostate specific antigen (PSA). The signal intensity of SERS was affected by the concentration of thrombin. The fluorescence signal was affected by PSA, and the detection limit was  $3.2 \times 10^{-20}$  M (Hao et al., 2017).

# 7 Biological toxicity of Ln-UCNPs

Despite the great potential in applications such as biotherapy, biological imaging and biosensing, the biotoxicity remains a major problem hindering the clinical application of Ln-UCNP. Most of the current studies on in vivo toxicity of Ln-UCNPs focus on mice. Ln-UCNPs enter mice in tail vein injection and reach the whole body by blood circulation. Due to the high permeability effect of capillaries to nanoparticles, the liver and spleen become the main aggregate organs of Ln-UCNPs (Li et al., 2017b; Abualrejal et al., 2019; Chen et al., 2019; Guryev et al., 2019; Shan et al., 2020). Chen and co-workers designed targeted contrast agents modified by PEI and FA (Chen et al., 2019). At 24 h and 18 days after the injection, the aggregation of nanoions in liver was higher than that in other tissues. Ln-UCNPs injected into the body can be eliminated by the hepatobiliary and renal metabolic systems. Tian and co-workers (Tian et al., 2019) found that the rate of excretion of Ln-UCNPs is independent of the modified groups. Other studies have shown that the modified group species can influence the toxicity of Ln-UCNPs. Chen and co-workers (Chen et al., 2018) designed a kind of unmodified nanoparticles (NaYF4:Er and NaGdF4:Yb,Er), which caused mild liver toxicity and nephritis. This can be considered as the unmodified Ln-UCNPs would release rare Earth ions under biological conditions, which will react with the phosphate group of ATP, cause ATP inactivation and tissue damage. Vedunova and co-workers (Vedunova et al., 2016) polymaleic anhydride octadecene, PEI, tetramethyl ammonium hydroxide modified Ln-UCNPs (NaYF<sub>4</sub>:Yb,Tm@NaYF<sub>4</sub>) respectively. The nanoparticles caused the morphological changes of the hippocampal cells, reduction in Ca2+ activity and cellular damage. Moreover, the nanoparticle size, concentration, and treatment time can also affect the biotoxicity of Ln-UCNPs (Xu et al., 2016; Chen et al., 2018; Rafique et al., 2018).

### 8 Conclusion and future prospects

In this review, we summarize the latest progress in the synthesis, optimization and application (especially for therapy) of Ln-UCNPs. The high-temperature pyrolysis method and hydrothermal/ solvothermal procedure are still the most widespread protocols for their syntheses. In terms of improving up-conversion emission, through algorithm optimization, dye sensitization and other methods, the up-conversion emission intensity can be increased by multiple orders of magnitude. The fluorescent properties of lanthanide upconverting nanoparticles have also advanced the field of biomedicine. Near-infrared excitation addresses the limitations of ultraviolet to visible light excitation, penetrates deeper into tissue, and makes nanotherapeutic materials with light as the main excitation source a strong competitor for clinical drugs. Although lanthanide up-conversion has advanced significantly, there are still a large number of obstacles to address. We posit that the future direction of Ln-UCNPs research in the field of biology consists of: 1) Existing luminescence enhancement strategies are either ineffective or easily quenched when exposed to water. Better results may be obtained starting from the principle of up-conversion luminescence to explore optimization methods. 2) Cancer treatment drugs based on Ln-UCNPs have not been reported clinically, which may be related to long term toxicity in the body. It may be possible to extend the in vivo experiment period and minimize other factors that affect drug metabolism to simulate the therapeutic effects to the greatest extent. 3) Although the synthesis technology of Ln-UCNPs is very mature, the products are often hydrophobic. Surface modification for in vivo application will improve biocompatibility; however, this process will affect the efficiency. Finding the balance luminescence between biocompatibility and luminescence is a difficult problem. 4) Ln-UCNPs-based biosensors have been developed. However, few studies have evaluated the sensitivity and stability of Ln-UCNPs sensors for in vivo sensing. The in vivo environment is complex, and

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#### Author contributions

RL, DX, and BL contributed to conception and design of the study. DX organized the database. CL performed the statistical analysis. DX wrote the first draft of the manuscript. BL, CL, and WL wrote sections of the manuscript. All authors contributed to manuscript revision, read, and approved the submitted version.

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### Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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