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Dedicated to the memory of Dr. Majid Rezayi

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Two-dimensional-Ti₃C₂ magnetic nanocomposite for targeted cancer chemotherapy

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Introduction: Cervical cancer is the leading cause of cancer-related death in women, so novel therapeutic approaches are needed to improve the effectiveness of current therapies or extend their activity. In recent decades, graphene analogs, such as Mxene, an emerging class of two-dimensional (2D) graphene analogs, have been drawing considerable attention based on their intrinsic physicochemical properties and performance as potential candidates for tumor therapy, particularly for therapeutic purposes. Here we explored the targeted drug delivery in cervical cancer in *in vivo* model. Mxene-based nanocarriers are not able to be precisely controlled in cancer treatment.

Method: To solve this problem, the titanium carbide-magnetic core-shell nanocarrier (Ti_3C_2 -Fe₃O₄@SiO₂-FA) is also developed to provide synergetic anticancer with magnetic controlling ability along with pH-responsive drug release. A xenograft model of the cervix was used to investigate the effects of Cisplatin alone, or in combination with Ti_3C_2 @FA and Ti_3C_2 @ Fe₃O₄@SiO₂-FA, on tumor growth following histological staining for evaluation of necrosis.

Result and Discussion: A significant tumor-growth suppression effect is shown when the Ti_3C_2 -Fe₃O₄@SiO₂-FA nanocarrier is magnetically controlled Cisplatin drug release. It reveals a synergistic therapeutic efficacy used in conjunction with pharmaceuticals (p < .001). According to the *in vivo* study, the Ti_3C_2 @FA@Cisplatin nanocomposite exhibits less tumor growth than the drug alone or Ti_3C_2 @FA@Cisplatin via increasing necrosis effect (p < .001). Through this study, Mxene nanosheets are expanded for biomedical applications, not only through the fabrication of biocompatible magnetic Mxene nanocomposite but also through the development of functionalization strategies that enable the magnetic Ti_3C_2 nanocomposite to load high levels of Cisplatin for cervical cancer treatment (242.5%). Hence, Ti_3C_2 -Fe₃O₄@SiO₂-FA nanocarriers would be promising candidates to improve cancer treatment efficiency.

KEYWORDS

drug delivery, cervix cancer, pH-responsive, magnetic nanocomposite, *in-vivo*, stimuli drug release

1 Introduction

There are several different types of cancer, but cervical cancer is the one that has emerged as the primary cause of death among females. The number of cervical cancer cases diagnosed is estimated to be around 500,000 annually (Jasrotia et al., 2022). Based on their histology, cervical cancers are generally classified as squamous cell carcinoma, adenocarcinoma, and adenosquamous carcinoma (Jiang et al., 2020). The Human papillomavirus (HPV) is believed to cause 90% of cervical cancer cases (Pokhriyal et al., 2019). Traditional cancer treatments, such as surgery, radiotherapy, ablation, and chemotherapy, are often unsatisfactory because they involve invasive procedures, high recurrence rates, and side effects (Siegel et al., 2019). During the last decade, medical nanotechnology has been driving the design of new intelligent nanosystems that can respond to the pathological environment of tumor tissue with physicalmorphological modifications. Nanotechnology-based therapeutics are gaining increasing attention in cancer treatment due to their multiple advantages, including a low level of invasiveness and few side-effects compared to other clinical treatments (Yu et al., 2022). In terms of clinical use, however, some limitations remain, including considering the composition and structure of nano agents, the complex physiological system, and their interactions rather than their therapeutic aspects. According to the reductionist viewpoint, the therapeutic route for nanoparticle-based therapies entails the delivery of nanoparticles to the tumor site, the treatment of the tumor with exogenous excitations, and the expulsion of nanoparticles from the body over time slowly (Liu et al., 2022).

On the other hand, it has been demonstrated that organic nanosystems possess a high potential for turning conceivable solutions to current therapeutic and diagnostic challenges into options that are more efficient and effective (Chen et al., 2021; Li et al., 2021). It has gained significant accomplishments in the fight against viruses, cardiovascular diseases, cancer, etc. (Qiu et al., 2022). Organic nanocarriers are especially appealing in cancer therapies due to their biocompatibility, enhanced cell permeability, high content of payloads, and selectivity for tumor accumulation (Zhang et al., 2021). Organic nanosystems are currently being developed based on biodegradable polymers and non-biodegradable polymers (Yu et al., 2021). Due to the absence of chronic toxic and inflammatory reactions, biodegradable organic nanocarriers are superior to their non-biodegradable counterparts (Blasi, 2019). A number of studies have demonstrated that drug carriers can significantly increase drug accumulation in specific organs and cells (Ulbrich et al., 2016), thus enabling the delivery of drugs to areas that require therapeutic effects, such as in tumor matrixes and/or in cancer cells, through controlled release (or activation). (Pecorino, 2012). Furthermore, it is possible to limit the toxicity of a drug by selective activation, which would reduce or eliminate any adverse effects and invasiveness (Nestler and Lüscher, 2019). In addition, several nanomaterials have been demonstrated to possess unique therapeutic potential, such as two-dimensional nanomaterials (Gong et al., 2017b; 2017a; Darroudi et al., 2022).

Therapeutic nanomedicine extensively explored the possibility of two-dimensional (2D) nanosheets being the wonder material of this era of science (Chen et al., 2015; Ranjbari et al., 2022), which benefited from their unique physiochemical properties and nanostructures, including their unique ultrathin nanostructure and associated desirable physiochemical and biological properties (Li X. et al., 2008; Chen et al., 2016b; Liu et al.,

2018c). There are numerous 2D nanosystems, including graphene (Huang et al., 2019; Liu et al., 2021; Koutsioukis et al., 2022), black phosphorus (Qian et al., 2017; Wang et al., 2017), metals and metal oxides (Tang et al., 2014; Sun et al., 2018; Li et al., 2019), and transition metal dichalcogenides (TMDCs) (Chou et al., 2013; Shi et al., 2020), which have been applied in a variety of applications, including molecular imaging, drug/gene delivery, biosensing, photothermal/photodynamic therapy, antibacterial activity, and even tissue engineering (Khafaji et al., 2019; Zhang et al., 2020). An emerging component of 2D nanomaterials is Mxene, a new and emerging compound that represents a large group of transition metal carbides as well as carbonitrides (Naguib et al., 2011; Bai et al., 2021; Shen et al., 2021). Mxene is prepared through the ablation of A elements from ternary-layered carbides of MAX phases in which M represents a transition metal carbide, A represents an element of the A group, and X represents a C or N element (Karlsson et al., 2015; Wang et al., 2015; Ferrara et al., 2021). Furthermore, in addition to the most extensively investigated applications of Mxene in the energy storage field, we, along with other researchers, recently demonstrated that ultrathin titanium carbide (Ti₃C₂) nanosheets could be intrinsically engineered to be highly effective in theragnostic and tumor therapy (Xuan et al., 2016; Li R. et al., 2017; Song et al., 2021). The development of 2D Ti₃C₂ Mxene for antibacterial, fluorescent imaging, and biosensing applications has opened a new research frontier for using Mxene in biomedical applications. In recent years, therapeutic nanomedicine has proven effective at treating various diseases by combining diagnostic imaging and therapeutic functionality (Lee et al., 2015; Liu et al., 2015; Chen et al., 2017). In order to achieve the specific functionalities and performances, it would be highly beneficial if this 2D Ti₃C₂ Mxene could be integrated with other functional moieties; however, it is still a challenge and unattainable as of yet (Zhang et al., 2018; Yang et al., 2021). In order to fully functionalize Ti₃C₂ Mxene, the functional moieties must be directly decorated onto the surface of nanosheets while maintaining the intrinsic Mxene properties and framework (Zhang et al., 2022). Taking this into account, we present the development of magnetic Ti₃C₂ Mxene for cancer therapy applications by directly coating Ti₃C₂ Mxene with magnetic iron oxide nanoparticles. Based on the specific surface chemistry and versatile properties of magnetic iron oxide nanoparticles, Mxene nanosheets provide an ideal surface for the application (Liu et al., 2018b; Ma et al., 2021). Despite this, Mxene-based nanosheets led to a lack of controllability as nanocarriers and have a low drug loading content, so many nano vehicles can't remain in the tumor site continuously due to blood circulation, resulting in the inevitable damage to normal tissues as well as a decline in anticancer effectiveness (Xing et al., 2018).

It is still a challenge to improve the drug-loading capability of Ti_3C_2 -based nanocarriers for cancer treatment while providing controllability to confine them inside cancer cells. It has been demonstrated in previous studies that superparamagnetic nanomaterials can control the movement of nanoscale drug carriers (Shahzad et al., 2018; Yang et al., 2018). Using cobalt ferrite/graphene oxide (CoFe₂O₄/Go), Wang et al. revealed that the nano platform could be controlled due to its magnetic properties (Wang et al., 2016). There have been a few studies in which magnetic material has been introduced into drug delivery systems to demonstrate high levels of

drug-loading ability (Chan et al., 2017). According to the above studies, by combining magnetic materials with Ti_3C_2 -based nanocarriers, it might be possible to resolve the dilemma.

When a magnetic nanomaterial was introduced into Ti_3C_2 nanosheets to form a drug nanocarrier, the magnetic nanocarriers would be confined in cancer cells under an external magnetic field, and then nanocarriers would be efficiently contacted by cancer cells. In response to endogenous or exogenous stimulation, the nanocarrier releases the anticancer drug (Cisplatin), resulting in more effective responsive therapy for localized tumor eradication. According to our knowledge, a controllable nanocarrier for combating cancer cells has not yet been achieved by combining Ti_3C_2 nanosheets with magnetic core shells. Therefore, for the first time, we investigated the effect of combining Ti_3C_2 nanosheets with magnetic core shells on the suppression of cervical cancer tumor growth.

2 Material and methods

2.1 Materials

Ti₃AlC₂ (powder, 200-meshes), HF, HCl (36%, w/w, purity >98%), TMAOH (25 wt% in water), AlCl₃ 6H₂O, and Folic acid, sodium dodecyl sulfate (SDS), phosphate buffer saline (PBS), high glucose cell culture medium, and a tetrazolium-based assay were purchased from Sigma-Aldrich. No further treatment was applied to the chemicals unless otherwise stated. An aqueous solution of monobasic potassium phosphate (KH₂PO₄) and dibasic potassium phosphate (K₂HPO₄) was utilized to produce PBS at pH 7. We used ultrapure water throughout all experiments.

2.2 Characterizations

Bruker diffractometers (PW1730) were used to carry out X-ray diffraction (XRD) with Cu Ka radiation ($\lambda = 1.5406$ Å). In order to characterize the morphology of the samples, transmission electron microscopes (TEM, Philips EM208S 100 KV) and field emission scanning electron microscopes (FESEMs, Hitachi, Japan) were used. To measure absorbance from 200 to 800 nm, Uv/Vis spectrometer (Perkin Elmer Lambda 25) was used. In addition, a JASCO FT-IR-460 spectrometer was utilized to obtain Fourier transform infrared spectroscopy (FT-IR) in the 400 to 4,000 cm⁻¹ range. Using vibrating sample magnetometers (VSM), magnetic nanocomposites were measured at Mahamax, Tehran, Iran).

2.3 Fabrication of titanium carbide (Ti_3C_2) nanosheets

A sample of 1 g of Ti_3AlC_2 powder was etched in a solution containing 1 g of LiF and 0.3 g of AlCl₃ 6H₂O for 3 days at room temperature with 10 mL of HCl (9 M) (Liu P. et al., 2018). The etching materials were centrifuged several times before being dispersed in 10 mL of TMAOH for 3 days, followed by centrifugation and washing to remove the intercalated Ti_3C_2 . In order to prepare a colloidal suspension of Ti_3C_2 nanosheets, a clay-like solid was dispersed in water for hours under bath sonication, then the supernatant was centrifuged at 7,000 rpm, and then a freeze-drier was used to collect the dried samples.

2.4 Fabrication of Ti₃C₂-Fe₃O₄@SiO₂-FA

As part of the preparation of Ti₃C₂-Fe₃O₄@SiO₂ nanocomposites, 50.0 mg of Fe₃O₄@SiO₂ nanoparticles synthesized hydrothermally (Darroudi et al., 2020; Ghasemi et al., 2021) was dispersed ultrasonically in 20 mL deionized water, and 100.0 mg of Ti₃C₂ nanosheets were dispersed in 80 mL deionized water and stirred for 30 min (Dai et al., 2017). In both solutions, ultra-sonification was performed for 120 min under an Ar atmosphere. After filtering the suspension to obtain the Ti₃C₂-Fe₃O₄@SiO₂ nanocomposite, it was dried in a vacuum overnight at 60°C. Afterward, 100.0 mg of the prepared Ti₃C₂-Fe₃O₄@SiO₂ and 0.5 g of folic acid were dispersed in 60 mL of deoxygenated water for 1 h with ultrasound. Then, the reaction system was kept in an Ar atmosphere in an oil bath at 60 C for 4 h. Finally, the obtained Ti₃C₂-Fe₃O₄@SiO₂-FA was washed with water and dried with a freeze-dryer.

2.5 Fabrication of Ti₃C₂@FA-Cisplatin

As part of the preparation of Ti₃C₂@FA nanocomposites, 5.0 mg of folic acid (FA) functionalized polymer was dispersed ultrasonically in 10 mL deionized water, and 100.0 mg of Ti₃C₂ nanosheets were dispersed in 50 mL deoxygenated water and stirred for 30 min, and then mixed through sonicating for extra 90 min under an Ar atmosphere. After filtering the suspension to obtain the Ti₃C₂@FA nanocomposite, it was dried in a vacuum overnight at 60°C. Finally, the obtained Ti₃C₂@FA was washed with water and dried using freeze-dryer.

2.6 Drug loading and release of Ti_3C_2 -Fe₃O₄@ SiO₂-FA-Cisplatin

2.6.1 Drug adsorption study

As part of the cisplatin adsorption study, the following nanocarriers (Ti_3C_2 -Fe₃O₄@SiO₂-FA and Ti_3C_2 @ FA) (1 mL) loaded formulations were mixed separately with various masses of Cisplatin (0.5, 1, 1.5, 2, 3 mg) of Cisplatin in 20 mL of Phosphate-buffered saline solution (PBS) under an ice-cooled dark environment (Jermy et al., 2019; 2021). After overnight stirring and sonication at room temperature, the solution mixture was centrifuged at 8,000 rpm for 10 min. Then, the product was collected and washed with 15 mL of standard saline solution. Based on the equation, the amount of Cisplatin adsorption was calculated using UV visible spectroscopy at 293 nm.

The supernatants were centrifuged for different intervals of time (0, 0.5, 1.5, 2.5, and 6 h). A UV-vis spectrometer was used to measure the absorbance of supernatants and then to calculate the Cisplatin concentration based on a standard calibration curve based on the characteristic absorbance peak of Cisplatin (293 nm) in 2 mL.

Drug loading of Cisplatin: (w/w%) = (the weight of final Cisplatin in Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin)/(weight of initial Ti₃C₂-Fe₃O₄@SiO₂-FA) \times 100%.

2.6.2 Drug release study

The cumulative cisplatin release was studied using the prepared nanoformulations Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin and Ti₃C₂@FA -Cisplatin (Ramezani Farani et al., 2022). Drug delivery was performed by immersing 10 mg of drug formulations in 20 mL of phosphate-buffered saline (PBS) at pH 4.5 and pH 7.4 (for selected samples). The release condition was performed at a constant temperature of 37°C. A specific volume of solution (2 mL) was removed at regular intervals, replaced with fresh PBS solution, and analyzed using UV-visible spectrometry. In order to calculate the weight of the final Cisplatin, the amount of the original Cisplatin was subtracted from the concentration of the loaded nanocarrier. A standard calibration curve was used to calculate Cisplatin concentration based on absorbance at 293 nm. As a means of designing the standard calibration curve, six different concentrations of Cisplatin solution (1, 5, 10, 25, 50, 100 µg/mL) were tested by UV-Vis spectrophotometer at the characteristic peak of Cisplatin absorbance (293 nm).

2.7 *In-vivo* intraperitoneal administration under an external magnetic field

In order to examine Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin's anticancer properties, it was examined on the cervix tumor model. The C57BL/ 6 mice (25-30 g) were purchased from the Laboratory Animal Center of Mashhad University of Medical Sciences (MUMS), Mashhad, Iran. The Ethical Committee approved animal experimentation protocols of the Experimental Animal Center at MUMS, Mashhad, Iran. Standard food and water were provided during the experiments, and mice were housed in a laboratory environment. The TC1 cells (murine cervix cancer cell lines) were obtained from Pastour Institute (Tehran, Iran) and cultured in RPMI-1640 medium with 10% heat-inactivated FBS and 1% streptomycin at 5% CO₂ at 37°C. 2.5 \times 10⁶ TC1 cells per 100 mL were injected in the left flank region of the mouse subcutaneously injected into mice, and approximately 2 weeks later, the tumor size reached 80-100 mm3 (Ghaemi et al., 2012). The participants were divided into four groups randomly according to the following instructions (n = 6 in each group): I. Control group (Untreated group), II. Cisplatin as a standard regimen for the treatment of cervical cancer (administered twice at a 3-day interval using 5 mg/kg, intraperitoneally; IP), III. Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin (administered twice at a 3-day interval using 5 mg/kg, IP), and IV. Ti₃C₂@Cisplatin (administered twice at a 3-day interval using 5 mg/kg, IP), followed by applying an external circular magnet (10 mm by 10 mm, 0.4 T surface field strength). The tumor size of the animals was measured once every other day. In order to determine the tumor volume (V), the formula $V = AB^2/$ 2 was used, where A is the primary axis length and B is the minor axis length (Ghaemi et al., 2012). The cervical tumors of each mouse were removed on day 18 to undergo further investigation by hematoxylin and eosin staining (H&E).

2.8 In-vitro studies

2.8.1 Growth inhibition studies

Cisplatin, Ti $_3C_2@FA@Cisplatin$, and Ti $_3C_2-Fe_3O_4@SiO_2-FA-Cisplatin$ have been evaluated for their growth inhibitory properties

after 24-h and 72-h treatments. After seeding cells (5×10^6) in 96-well plates, they were grown for 24 and 72 h. In the next step, cells were treated with 10 µL concentrations of Cisplatin (1–1,500 µg), Ti₃C₂@ FA@Cisplatin (1–1,500 µg), and Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin (1–1,500 µg) in the total volume of 200 µL cells per well. As previously described, the plates were then processed (Hashemzadeh et al., 2022).

2.8.2 Formation of multicellular spheroids

A total of 200 μ L of RPMI-1640 and GlutaMAX-I (1:1) in agarosecoated 96-well plates were seeded at a density of 5 × 10⁴ cells per well and later treated with Cisplatin, Ti₃C₂@FA@Cisplatin, and Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin in the total volume of 200 μ L per plate. On a Leica Microsystems GmbH inverted phase contrast microscope (Wetzlar, Germany), the cell connections and cytotoxic effects were assessed over 3 days. Images of spheroid sizes were analyzed with ImageJ ver. 1.8.0–112 (National Institutes of Health, Bethesda, MD, United States) (Hashemzadeh et al., 2022).

2.9 Statistical analysis

The results of all experiments are expressed as the mean and standard error. One-way ANOVA using LSD *post hoc* test was used to analyze the significance of the results using SPSS software (SPSS Inc., Armonk, NY, USA). Statistical significance was determined by *p* .05.

3 Result and discussion

3.1 Fabrication and characterization of the Ti_3C_2 -Fe₃O₄@SiO₂-FA-Cisplatin composite nanosheet

Through sonication treatment, multi-layer Ti₃C₂ was converted into ultrathin Mxene nanosheets (Figure 1A). After this step, magnetic nanoscale Mxene sheets exhibited a large planar structure and good dispersity, which are ideal for biomedical applications (Soleymaniha et al., 2019). An HCl/LiF etchant was used initially to remove the Al layer from Ti₃AlC₂. In this manner, the Ti₃AlC₂ can be exfoliated using HCl/LiF etching, but the resulting multi-layer Ti₃C₂ nanosheets remain close together, exhibiting large particle sizes, which is incompatible with the demands of biomedicine (Naguib et al., 2011). Due to this, ultrasonication was used to complete the separation process and simultaneously reduce particle size. To increase controllability, magnetic nanoparticles were intercalated into Mxene layers to form heterostructures, thereby ensuring the confinement of Ti₃C₂ nanosheets. The Ti₃C₂-Fe₃O₄@SiO₂-FA nanocarrier can store the charged functional groups of the anticancer drug (Cisplatin) owing to adequate hydroxyl groups on the surface (Figure 1A). For chemotherapy purposes, Cisplatin can be targeted released from nanocarriers under inner or external stimulation. As a result of their nanoscale size, Ti₃C₂-Fe₃O₄@ SiO₂-FA nanocarrier would circulate easily within blood vessels and could passively penetrate tumor cells (Li X. et al., 2017). The Ti₃C₂-Fe₃O₄@SiO₂-FA nanocarrier can be reached cancerous cells using an external magnetic field and would not leave the cancer cells with blood circulation (Figure 1B).



The morphology and structure of constructed nanocomposites are characterized using TEM and FESEM images. As illustrated in Figure 2A, the Mxene Ti₃C₂ nanosheet, after etching the Al layer and following intercalation by TMAOH, the FESEM image depicted that closely pack layer structure of MAX phase exfoliating into nano size thickness sheets. Also, the EDAX analysis of the etched sample confirmed the surface modification by Al ion. TEM image also revealed that the titanium carbide nanosheets have an average lateral size of approximately 35 nm (Figure 3A). Furthermore, the formation of Mxene nanosheets is confirmed by XRD analysis, in which no peak at 38° was exhibited through intercalation, while the characteristic peaks from stacked Mxene nanosheets appeared. As shown in Figure 2C, the Brightfield FESEM image of Ti₃C₂-Fe₃O₄@ SiO₂-FA composite nanosheets revealed a small Fe₃O₄@SiO₂ magnetic core-shell with an average size of approximately 31.3 nm on the surface of Ti₃C₂ Mxene nanosheets with a thickness of ~31 nm. It is clear from the TEM image (Figure 3A) that the core shells of Fe₃O₄@ SiO₂ species are in core-shell morphology. As shown in Figure 2D, the TEM and SEM images of functionalized Ti₃C₂ Mxene by FA had a surface of sheet-like morphology with a thickness of around ~29.3 nm (Figure 2B). According to FESEM images of Ti₃C₂@FA nanosheet surface become roughened and covered by some spheres composed of Ti₃C₂@FA nanocomposite. Furthermore, the vanishing or decreasing peaks in the 30-40-degree range confirm the 2D structure of functionalized Ti₃C₂ nanosheets (Figure 4D).

Along with characterized nanocarrier, it exhibited a multi-layer structure of constructed Ti_3C_2 -Fe₃O₄@SiO₂-FA-Cisplatin nanosheets that Fe₃O₄@SiO₂ component in core-shell morphology is firmly attached to the surface of Ti_3C_2 nanosheets in the average size of 27.2 nm on the sheets with thickness 30.5 nm (Figure 2E). In Figure 2F, FESEM images of Ti_3C_2 @FA and the multi-layer Ti_3C_2

are shown, where a typical accordion-like structure of the multi-layer ${\rm Ti}_3C_2$ can be observed with a thickness of approximately 38.5 nm.

The FESEM of MAX phase exhibited in Figure 2, confirmed the accordion-like structure of Ti3AlC2 structure, in which, through the ultrasonic process, the weak covalent bonds between the multi-layer Ti₃C₂ nanosheets are destroyed, confirmed through TEM image (Figure 3B). The EDAX analysis also confirmed the presence of Ti, Al, and C elements in the structure of the MAX phase (Figure 5A). Overall, the TEM image of Ti₃C₂ nanosheets revealed further details about their morphology and structure (Figure 3), which are approximately 29-41 nm in transverse dimension. Further, TEM results suggest that Ti3C2 nanosheets could be used as drug delivery nanocarriers due to their small thickness and size, which enhances blood circulation (Wang et al., 2013). An XRD pattern for Ti₃C₂ nanosheets, shown in Figure 4, demonstrates the etching of Al layers from Ti₃AlC₂ by using LiF/HCl etchant successfully removed Al layers from Ti₃AlC₂ through the most intense XRD peak (104) of Ti_3AlC_2 (2 $\theta \approx 39^\circ$). As a consequence of the introduction of lithium and hydroxyl ions into the Ti₃C₂ layers, the main peak (002) of Ti₃AlC₂ moved from 10.5° to 9.2°, since the distance between adjacent Ti₃C₂ layers in Ti₃C₂-Fe₃O₄@SiO₂-FA, Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin, and Ti₃C₂@FA is augmented by the presence of these ions (Wang et al., 2021). The aqueous dispersion of Ti₃C₂ nanosheets appears dark-colored, with the incident light scattered by colloidal nanosheets. The formation of Ti₃C₂ is also confirmed by X-ray diffraction (XRD).

As indicated by previous studies (Ma et al., 2021), Ti_3C_2 MXene exhibited negatively charged oxygen-containing groups, which could absorb the positively charged $Fe_3O_4@SiO_2$ (Zhang et al., 2022). Analysis of this reaction procedure was conducted using Fourier transform infrared (FTIR). Following iron oxide and silane core



FIGURE 2

FESEM analysis of (A) Fe₃O₄@SiO₂, (B) MAX phase, (C) Ti₃C₂-Fe₃O₄@SiO₂-FA, (D) Ti₃C₂@FA, and (E) Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin, and (F) Ti₃C₂@FA-Cisplatin.



TEM analysis of (A) Fe₃O₄@SiO₂, (B) Ti₃C₂@FA, and (C) Ti₃C₂-Fe₃O₄@SiO₂-FA.

shells, Fe₃O₄@SiO₂, Ti₃C₂-Fe₃O₄@SiO₂-FA, and Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin FIT-IR profiles are illustrated in Figure 6. FT-IR spectroscopy was used to verify the chemical modifications. According to the spectra analysis of Ti₃C₂-Fe₃O₄@SiO₂-FA, the FTIR spectrum showed C-H stretch at 2,820–2,950 cm⁻¹, and C-O stretch at 1,335–1,192 cm⁻¹. In the range between two peaks of 1,620 and 1,440 cm⁻¹, strong bond vibrations are observed for NH and NH₂. The NH₃⁺ stretch is a wide peak at 3,230–2,600 cm⁻¹. In

addition to C=O stretch at 1,694 cm⁻¹ and C-O stretch at 1,340–1,180 cm⁻¹, C=C stretch in aromatic compounds was also found at 1,600–1,450 cm⁻¹ in the FA molecule (Figure 6). The FTIR spectra of Ti₃C₂-Fe₃O₄@SiO₂-FA exhibited a strong band at 1,626 cm⁻¹ attributing to the N-H vibration of FA. Furthermore, the FTIR spectrum of Ti₃C₂-Magnetic nanosheets showed a new peak at 575 cm⁻¹, correlated with Fe-O stretching vibration of Fe₃O₄, demonstrating Fe₃O₄ deposition on Ti₃C₂ nanosheets in





comparison with the FTIR spectrum of Ti₃C₂ nanosheets. Ti₃C₂-Magnetic NPs exhibit a significant reduction in the FTIR band associated with hydroxyl group at 3,411 cm⁻¹ and carbonyl group at 1,690 cm⁻¹ (Figure 6). The Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin showed weak amine bands, suggesting that the NH₂ was conjugated with the OH groups of the nanocomposites and Folic acid towards the Cisplatin. Moreover, the bending vibration at 1,650 cm⁻¹ indicates that Cisplatin has been functionalized, as well as the reaction between the Folic acid and Pt (II) complex.

In order to examine the presence of synthetic magnetic core shells and nanosheets, SEM and EDAX were used. As shown in Figure 5, magnetic nanoparticles with an average width of 27–40 nm have a microstructure.

The distribution maps of Ti, Fe, Si, C, and O elements on Ti₃C₂-Fe₃O₄@SiO₂-FA composite nanosheets confirmed the coexistence of Ti and Fe elements and the uniform distribution of Fe₃O₄@SiO₂ on the surface. An EDAX analysis of Ti₃C₂-Fe₃O₄@SiO₂-FA composite nanosheets (Figure 6B) shows that Ti, Fe, and Si elements are present, indicating that Fe₃O₄@SiO₂ was successfully functionalized on the surface of Ti_3C_2 Mxene nanosheets. Furthermore, through loading Cisplatin on the nanocarrier, the existence of Pt would be exhibited in the EDAX analysis, confirming the construction of the Ti3C2-Fe3O4@SiO2-FA-Cisplatin and Ti₃C₂@FA-Cisplatin (Figures 6E, F). Insets in Figure 5 provide a list of results of the elemental analysis of Fe₃O₄@SiO₂-uncoated, Ti₃C₂-Fe₃O₄@SiO₂-FA-coated, and Ti₃C₂@



FA-coated nanoparticles, in which 6.76%, 10.79%, and 15.62% of nanoparticles' weights can be found to be respectively. Ti_3C_2 -Fe₃O₄@SiO₂-FA-Cisplatin contains 2.89% Pt, while Ti_3C_2 @FA-Cisplatin contains 1.92% Pt. The elemental analysis indicates that since Fe₃O₄@SiO₂ and adsorbed-Mxene on Fe₃O₄@SiO₂, the remaining weight is comprised of Fe and Ti (from Fe₃O₄ and Ti_3C_2). Thus, the weight% of Fe and Ti is estimated to be 26.63% and 16.13%. The number ratio of compounds is determined to be C (8): Fe (26): Ti (16), using the mentioned weight% ratio. Therefore, 3.03:1 and 2.05:1 have been determined for the Fe₃O₄:Ti₃C₂ number and weight ratios. FT-IR analysis illustrates the existence of Ti_3C_2 MXene nanosheets as indicated by the elemental analysis results.

Regarding the elemental analysis of Ti₃C₂@FA nanosheets, it should be noted that the weights% of C and Ti atoms are, respectively, determined to be 84.38% and 15.62% (Figure 6D). The C: Ti ratio is determined to be 5.41:1. In this case, C is attributed to both Ti₃C₂ and Folic acid coated on the nanosheets. Therefore, we conclude that the Fe₃O₄@SiO₂:Ti₃C₂ weight% ratio is 26.53:16.13, with a 25.5% weight ratio of Fe in the total weight of the nanocarrier.

Due to the presence of magnetic Fe_3O_4 nanoparticles in Ti_3C_2 -Magnetic composite nanosheets, the Mxene can modulate their magnetic properties by applying an external magnetic field (Figure 7), which suggests that magnetic fields can be used for further nanomedicine applications. Figure 7 shows the unique



magnetic property of $\rm Ti_3C_2\text{-}Magnetic$ NPs composite nanosheets, which exhibit a saturation magnetization of 23.5 emu g^{-1} .

3.2 The magnetic properties of Ti_3C_2 -Fe_3O_4@ SiO_2-FA and Ti_3C_2 -Fe_3O_4@SiO_2-FA-cisplatin

Considering the magnetic properties of Fe₃O₄ core-shell nanomaterials (Gao and Wang, 2014; Oravczová et al., 2021), a magnetically controlled nanocarrier based on Ti₃C₂-Fe₃O₄@SiO₂-FA was investigated. It is shown in Figure 7B that Fe₃O₄@SiO₂, Ti₃C₂-Fe₃O₄@SiO₂-FA, Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin and nanocarriers show field-dependent magnetization curves. It was determined that Fe₃O₄@SiO₂ has the highest saturation magnetization (60.0 emu/g) (Figure 7A), whereas Ti_3C_2 -Fe₃O₄@ SiO₂-FA-Cisplatin nanocarrier (6.5 emu/g) exhibits significantly lower saturation magnetization than Ti₃C₂-Fe₃O₄@SiO₂-FA (23.5 emu/g), owing to the presence of Ti₃C₂ nanosheets, the remanence of Ti₃C₂ nanocarriers is lower than the remanence of $Fe_3O_4@SiO_2$ nanosheets (Liu et al., 2008). In conclusion, the $Ti_3C_2\text{--}$ Fe₃O₄@SiO₂-FA and Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin nanocarriers show hysteresis loops, suggesting they could be magnetically controlled drug carriers. Furthermore, previous studies have indicated that saturation magnetizations of 16.3 emu/g would be sufficient for magnetic control (Deng et al., 2014).

3.3 The loading/releasing Cisplatin capability of Ti_3C_2 -Fe₃O₄@SiO₂-FA and Ti_3C_2 @FA

It has been demonstrated that Ti_3C_2 nanosheets (Karlsson et al., 2015) and Fe_3O_4 (Darroudi et al., 2020) can be further developed into drug delivery nanocarriers for cancer therapy due to the abundance of hydroxyl functional groups and their large surface areas. For evaluating the drug loading/release ability of Ti_3C_2 - $Fe_3O_4@SiO_2$ -FA and $Ti_3C_2@FA$ nanocarriers, Cisplatin, a chemotherapy drug used to combat cancer, was used as a model drug. After vigorous stirring and sonication under an Ar atmosphere, Cisplatin was loaded on the surface of Ti_3C_2 - $Fe_3O_4@SiO_2$ -FA nanocarrier. Due to the strong electrostatic interactions between the negatively charged surface of the Ti_3C_2 - $Fe_3O_4@SiO_2$ -FA and $Ti_3C_2@FA$ nanocarriers and the positively charged Cisplatin, we

achieved a high drug loading content (Liu et al., 2019). This can be seen in the shaded part of the UV–Vis spectrums (Figure 8A), where the acquired Ti_3C_2 -Fe₃O₄@SiO₂-FA and Ti_3C_2 @FA exhibit the characteristic absorption peak of Cisplatin compared to the Ti_3C_2 -Fe₃O₄@SiO₂-FA after loading with Cisplatin. In this case, the combination between both Ti_3C_2 -Fe₃O₄@SiO₂-FA and Ti_3C_2 @ FA nanocarriers and Cisplatin would be a successful result of the interaction between the hydroxyl groups of Ti_3C_2 -Fe₃O₄@SiO₂-FA and Ti_3C_2 @FA nanocarriers and Cisplatin (Zhao et al., 2019). Furthermore, since the constructed titanium carbide nanocarriers are negatively charged, it may offer better cell accessibility and hydrophilic properties (Chen et al., 2016a).

A UV-vis spectroscopy study was conducted to assess the capacity of the Ti₃C₂-Fe₃O₄@SiO₂-FA and Ti₃C₂@FA nanocarriers to load different weight ratios of Cisplatin (0.5, 1, 1.5, 2, 3). By using a standard calibration curve for Cisplatin under 293 nm irradiation (Figure 8C), the concentration of Cisplatin was calculated and incorporated into the drug loading equation. As shown in Figures 8A-C greater ratio of Ti₃C₂-Fe₃O₄@SiO₂-FA results in an increase in the drug loading capacity. In accordance with the equation for drug loading, the drug loading efficiency at a mass ratio of three of the Ti₃C₂-Fe₃O₄@SiO₂-FA nanocarrier was calculated to be 244.01% based on the drug loading formula, while the Ti₃C₂@FA-Cisplatin loading efficiency was 134.01%. These are considerably higher than the average drug loading efficiency for single Ti₃C₂ nanosheets (89%) and most drug delivery nanocarriers (10%-50%) (Liu et al., 2020). It is assumed that the increase in drug loading capacity can be attributed to two factors: 1) In the case of the Ti_3C_2 -Fe₃O₄@SiO₂-FA nanocarrier, there are more electrostatic sites available for loading Cisplatin 2) The Ti₃C₂-Fe₃O₄@SiO₂-FA nanocarrier provides sufficient surface area for Cisplatin to be loaded.

This study examined the pH-dependent drug release of Ti_3C_2 -Fe₃O₄@SiO₂-FA-Cisplatin and Ti_3C_2 @FA-Cisplatin under several pH values (7.4 and 4.5, respectively). Figure 8D exhibited that at pH 7.4 and 4.5 during a 6-h period, 31.59%, and 89.01%, of Cisplatin are released from Ti_3C_2 -Fe₃O₄@SiO₂-FA -Cisplatin, respectively, suggests that it is more readily released in an acidic microenvironment. In comparison, Ti_3C_2 @FA-Cisplatin exhibited a pH-responsive release profile; during 6 h, Cisplatin release was measured to be 44.31% and 23.04%, corresponding to pH 4.5 and 7.4, respectively. Due to the altered interaction between Cisplatin and Ti_3C_2 -Fe₃O₄@SiO₂-FA nanocarriers and the greater solubility of



FIGURE 8

I) UV-Vis absorbance of Cisplatin, Ti_3C_2 - Fe_3O_4 @SiO_2-FA, Ti_3C_2 - Fe_3O_4 @SiO_2-FA-Cisplatin, and Ti_3C_2 @ FA-Cisplatin. II) Standard calibration curve for different concentrations of Cisplatin (2.5, 5, 10, 20, 50, 100) irradiation at 293 nm, III) Cisplatin release profile of Ti_3C_2 - Fe_3O_4 @SiO_2-FA and Ti_3C_2 @FA at different drug/nanocarrier ratios (0.5, 1, 1.5, 2, 3) irradiation at 293 nm, and IV) The Cisplatin release from Ti_3C_2 - Fe_3O_4 @SiO_2-FA-Cisplatin (**A**, **C**) and Ti_3C_2 @FA at A-Cisplatin (**B**, **D**) in PBS (0.1 M) solution at two pH 4.5, and 7.4, respectively (n = 3).



FIGURE 9

(A) Ti3C2-Fe3O4@SiO2-FA-Cisplatin reduces tumor size and weight in cervical cancer tumors. Effect of Ti_3C_2 -Fe_3O4@SiO2-FA-Cisplatin, $Ti_3C_2@$ Cisplatin, and Cisplatin on tumor size (B) during experiment and tumor weight (C) in a cancerous mouse model of cervical cancer at the last of experiment.



The combination of Ti_3C_2 -Fe_3O_4@SiO_2-FA-Cisplatin promotes necrosis in cervical cancer tumors compared to $Ti_3C_2@FA@Cisplatin$ and Cisplatin alone. The tumor necrosis is indicated by H&E staining under a light microscope **(A)**; necrosis areas are indicated with arrows. **(B)**Using the image J software, quantify the necrotic area.



FIGURE 11

The MTT assay was used to assess cell viability after 24 h and 48 h incubation in TC1 cervix cancer cells to determine the ability of $Ti_3C_2@FA@Cisplatin$ and $Ti_3C_2-Fe_3O_4@SiO_2-FA-Cisplatin$ to inhibit cell growth.

Cisplatin at lower pH values, this result can be attributed to the altered interaction between drug and Ti_3C_2 -titanium carbide nanocarriers. Notably, at pH 7.4, a large number of hydroxyl groups on the surface of Ti_3C_2 -Fe₃O₄@SiO₂-FA become deprotonated and negatively charged, in contrast to Cisplatin's positive charge (Gong et al., 2016). The solubility and hydrophilic properties of Cisplatin increase with an increase in protonation of the amino group under

a pH value of 4.5 (Du et al., 2010). Meanwhile, the hydroxyl groups on the surface of the nanocarrier Ti_3C_2 -Fe $_3O_4@SiO_2$ -FA are protonated in this process, would result in a repulsive interaction between Cisplatin and Ti_3C_2 -Fe $_3O_4@SiO_2$ -FA nanocarrier (Mu et al., 2019). Since Cisplatin releases from Ti_3C_2 -Fe $_3O_4@SiO_2$ -FA-Cisplatin in an acidic environment, the pH-triggered drug release action has a significant impact.



3.4 In vivo effects of Ti_3C_2 -Fe₃O₄@SiO₂-FA-Cisplatin magnetic nanosheets and Ti_3C_2 @ Cisplatin on cervical cancer and necrosis

This study aimed to determine whether Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin and Ti₃C₂@Cisplatin inhibited the growth of cervical carcinomas in mice using a tumor model. Figure 9A in each group of mice, Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin, Ti₃C₂@Cisplatin, and Cisplatin alone were treated, and tumor weight and size were measured. The results of in vivo experiments indicated a decrease in tumor size and weight in mice after treatment with Ti₃C₂-Fe₃O₄@ SiO₂-FA-Cisplatin (Figures 9B, C). This cervical cancer model shows that Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin exhibits enhanced anticancer activity compared with Cisplatin alone Ti₃C₂@Cisplatin nanosheets, which significantly increases Cisplatin's antitumor activity. According to the in vivo release profile of nanocomposite, Cisplatin alone and $\mathrm{Ti}_3\mathrm{C}_2@\mathrm{Cisplatin}$ nanosheets follow a onecompartment model in vivo. Since these magnetic nanocomposites consist of multiple compartments, they would be released sequentially, followed by the continuous release resulting from burst releases.

A significant challenge facing the treatment of cervical cancer is how to prevent the accumulation of cancer-fighting drugs in healthy tissue while improving the local accumulation of these drugs at the tumor site (Koning et al., 2010). A new therapeutic approach for treating localized cancer may be possible with nanoparticles with magnetic properties (Kumar and Mohammad, 2011). Recent research reports that a polymeric nanocapsule containing 5-Fu could treat colon cancer similarly (Li S. et al., 2008). A study by Shakeri-Zadeh et al. found that 5-Fu had an increased tendency to cause colon tumors when loaded into magnetic nanoparticles (Shakeri-Zadeh et al., 2014). In this regard, our in vivo experiments have shown that when Cisplatin is loaded into Mxene-magnetic nanosheets, it would have a sustained release in a pH-responsive manner, prolonged half-life, and significantly increased tumor uptake, while there was no predicted efficiency for Mxene Ti₃C₂@Cisplatin.

An increased area of tissue necrosis was observed in the cervix tumor after Ti_3C_2 -Fe₃O₄@SiO₂-FA-Cisplatin treatment (Figure 10A). It was revealed that Ti_3C_2 -Fe₃O₄@SiO₂-FA-Cisplatin increased percentages of necrosis in cervical tissue compared to Cisplatin alone and Ti_3C_2 @Cisplatin as the standard chemotherapeutic

regimen in cervical cancer (Figure 10B; p = .05). Using H&E staining, arrows indicate the necrosis area.

4 In vitro effects of Ti_3C_2 -Fe₃O₄@SiO₂-FA-Cisplatin magnetic nanosheets and Ti_3C_2 @Cisplatin on cervical cancer

4.1 Ti $_3$ C $_2$ -Fe $_3$ O $_4$ @SiO $_2$ -FA-Cisplatin magnetic nanosheets and Ti $_3$ C $_2$ @Cisplatin inhibit cell viability

To examine the anti-proliferative potential of Cisplatin, $Ti_3C_2@FA@Cisplatin, \quad and \quad Ti_3C_2\mbox{-}Fe_3O_4@SiO_2\mbox{-}FA\mbox{-}Cisplatin,$ cells were exposed to the rising concentrations (0-1,500 ppm) for 24 h and 72 h. A reduction of nearly 90% in cell viability was observed at the highest concentration of free Cisplatin. In contrast, although both Ti3C2@FA@Cisplatin and Ti3C2-Fe₃O₄@SiO₂-FA-Cisplatin had radical negative effects on cell viability, neither was as effective as Cisplatin. This finding also reflects in the determined IC50 values and could be attributed to variations in the drug loading/release profiles between Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin and Ti₃C₂@FA@Cisplatin. IC50 values were found to be for Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin (24 h): 855 µg/mL, (72 h): 60 µg/mL. Additionally, IC50 in terms of the amount Ti₃C₂@FA@Cisplatin (24 h): 130 µg/mL, (72 h): 30 µg/mL (Figure 11).

4.2 Cancer spheroids are inhibited by $Ti_3C_2@$ FA@Cisplatin and Ti_3C_2 -Fe_3O₄@SiO₂-FA-Cisplatin

In a 3-D cell structure (Figure 12), Ti₃C₂@FA@Cisplatin and Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin were assessed for their specific anti-cancer abilities. The spheroid size of the treated group differed significantly from the control group after 3 days. Spheroid area did not change significantly after 3 days in the control group, while it significantly decreased in Cisplatin, Ti3C2@FA@Cisplatin, and $\mathrm{Ti}_3\mathrm{C}_2\text{-}\mathrm{Fe}_3\mathrm{O}_4@\mathrm{SiO}_2\text{-}\mathrm{FA}\text{-}\mathrm{Cisplatin}$ treated groups. As a result of the loss of cell membrane integrity and the loss of viability of the core cells of Ti₃C₂@FA@Cisplatin and Ti₃C₂-Fe₃O₄@SiO₂-FA-Cisplatin spheroids, the peripheral cells have already disappeared. A threedimensional model of cervical cancer cells showed that treatments could prevent proliferation and progression, and consequently, the cancerous cells are more likely to die (Figure 12). Spheroid growth is not only significantly retarded in the presence of nanoforms, but also a corona of dead and fragmented cells is visible after approximately 3 days of treatment.

5 Conclusion

In conclusion, we present an efficient cancer treatment based on the magnetic functionalization of Mxene (2D Ti_3C_2). As a result of the in-situ growing of Mxene onto Ti_3C_2 Mxene surfaces, a heterostructure of Mxene-based magnetic nanoplatforms was developed. This nanoplatform can be used for synergistic therapy with pH-dependent drug release and controlled magnetic therapy for targeted effects for target therapeutic agents. In the case of Cisplatin, Ti_3C_2 - $Fe_3O_4@SiO_2$ -FA nanocarriers demonstrated high drug loading capacities (234%) and were capable of exhibiting a drug release behavior as a result of pH stimulation. Furthermore, Ti_3C_2 - $Fe_3O_4@SiO_2$ -FA nanocarrier could be controlled under the external magnetic field due to its magnetic properties. Finally, a first report on the multifunctionalities of Mxene, combined with Cisplatin, has been presented to demonstrate that Mxene can be elaborately engineered to fabricate magnetic nanocomposite materials using their surface chemistry and that this paradigm can be applied to a variety of therapeutic applications.

Accordingly, it was exhibited that Ti₃C₂@Cisplatin nanosheets do not have the anticipated efficiency in the drug delivery system. The development of magnetic Mxene-based 2D materials is expected to significantly expand the areas and potent applications, particularly in nanobiotechnology and nanomedicine of Mxene-based 2D materials. Therefore, it is anticipated that Ti₃C₂-Fe₃O₄@SiO₂-FA nanocarriers will be an effective method for improving the cancer treatment's efficiency.

Data availability statement

The raw data supporting the conclusions of this article will be made available by the authors, without undue reservation.

Ethics statement

The animal study was reviewed and approved by Experimental Animal Center at Mashhad University of Medical Sciences.

Author contributions

All authors contributed to the article and approved the submitted version. MD: Visualization, investigation, formal analysis, analysis data, Writing original draft, methodology. SE: Conceptualization, methodology, visualization, investigation, formal analysis, MK: Investigation, methodology, writing—review and editing. FA: Analysis data, methodology, investigation, writing—original draft. NK-T: Methodology, visualization. SA: Methodology, visualization. SR: Methodology. MR: Supervision, funding acquisition, conceptualization, writing-review and editing. MK: supervision, funding acquisition, conceptualization, writing-review and editing, validation.

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Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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Supplementary material

The Supplementary Material for this article can be found online at: https://www.frontiersin.org/articles/10.3389/fbioe.2023.1097631/full#supplementary-material

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