



Graphene-Based Nanomaterials for Dental Applications: Principles, Current Advances, and Future Outlook

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With the development of nanotechnology, nanomaterials have been used in dental fields over the past years. Among them, graphene and its derivatives have attracted great attentions, owing to their excellent physicochemical property, morphology, biocompatibility, multi-differentiation activity, and antimicrobial activity. In our review, we summarized the recent progress about their applications on the dentistry. The synthesis methods, structures, and properties of graphene-based materials are discussed. Then, the dental applications of graphene-based materials are emphatically collected and described. Finally, the challenges and outlooks of graphene-based nanomaterials on the dental applications are discussed in this paper, aiming at inspiring more excellent studies.

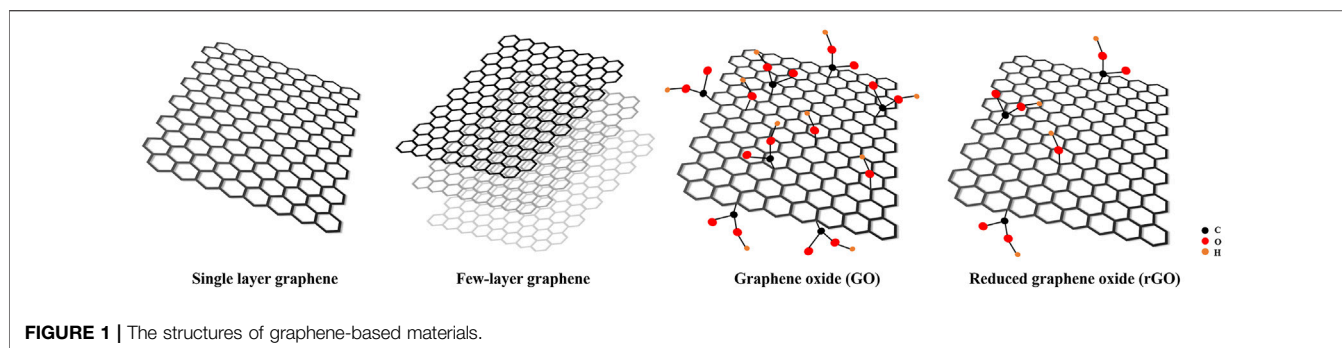
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INTRODUCTION

Oral health is quite important because it can deeply affect human health and quality of life (Lamster, 2021). However, World Health Organization (WHO) had reported that over 70% world's population suffered the dental-related diseases in 2016 (Gordon and Donoff, 2016). At the 74th World Health Assembly of WHO in 2021, oral health has been highly concerned (Lamster, 2021). The main common oral diseases include dental caries, periodontal diseases, tooth loss, and oral cancer. Nowadays, maintaining oral health is challenging. Although, many techniques and methods have been adopted to treat oral diseases, yet there was no ideal method. To improve these methods, many kinds of biomaterials have been applied.

Tissue defects (especially bone defect) caused by traumas, infections, or tumors are one of the most common diseases in dental field (Liu et al., 2020). Currently, many efforts have been taken to repair tissue defects. Moreover, the regeneration of dental-like tissues were harder than tissues like bone, and muscle, because cementum regeneration is slow and pulp regeneration is hard. Besides, the regeneration of alveolar bone is relative active and rapid (Riccardo et al., 2018). Tissue engineering is commonly considered as a superior treatment strategy, where scaffolds played a vital role. Nowadays, most commercial biomaterials lack osteoinductive properties, which are very important for bone regeneration (Wu et al., 2017). Therefore, it is vital and urgent to discover an osteoinductive biomaterial for bone reconstruction.

In the field of dentistry, dental implants have been widely applied to restore the missing teeth due to their various advantages. It is well known that osseointegration is the gold standard for successful dental implantation. Titanium and its alloy have been applied as dental implant materials because of



its good biocompatibility, mechanical properties, and so on. Except for all its merits, titanium implants also have failures due to the poor osseointegration. Therefore, it is important to improve the performance of titanium dental implants, and modifications of dental implant surfaces played an important role (Steflik et al., 1999). Various biomaterials have been widely applied to enhance the osteogenic properties of dental implants. In addition, the peri-implantitis is also the main failure reason for dental implants (Hideaki et al., 2019). Therefore, it is of great importance to explore new excellent antibacterial surfaces of dental implant.

Nanomaterials have showed wonderful performances in improving the strength and resist wear of tooth fillers and sealants. Moreover, nanomaterials also performed excellent antimicrobial properties in the application of restorative materials (Sharan et al., 2017). Owing to the above advantages, outstanding nanomaterials are widely applied in the dental fields of restorative materials, adhesives, cements, primers, and so on.

Among various nanomaterials, graphene, as a promising two-dimensional (2D) carbon-based nanomaterial, is the thinnest and strongest material. In 2004, it was first isolated by Novoselov and Geim using mechanical exfoliation with a sticky tape and they won the Nobel Prize in 2010 (Novoselov et al., 2004). Graphene-based materials could be divided into four categories: single-layer graphene, few-layered graphene, graphene oxide (GO) and reduced graphene oxide (rGO) (Figure 1) (Bei et al., 2019). Owing to perfect physical properties, well electrical conductivity, and excellent biocompatibility, graphene and its derivative have attracted much attention in the field of medicine and biomedical fields. Moreover, graphene and its derivatives have also aroused great attentions in the field of dentistry and tissue engineering, dental implant coatings, bone cements, resin additives, and tooth whitening.

During the past 20 years, significant advances have been achieved in regulating properties of graphene and its derivatives, elucidating their underlying mechanisms, and broadening potential applications. Up to now, there are more than 2,942 studies related to graphene-based materials for dental applications. Although numerous excellent reviews have been published, most of those reviews were mainly focused on certain specific aspect. Therefore, a comprehensive review is needed to summarize and analyze all the progress, especially the achievements from more than 2,271 research papers published

in the past 5 years (Figure 2). Such an analysis is necessary to help researchers to better understand graphene-based materials. To highlight the recent progress, various types, performance, and the applications of graphene-based materials such as graphene, GO, and rGO are summarized in this review. Finally, the challenges and future perspectives of graphene-based materials are also discussed. The purpose of this review aimed at summarizing the dental application of graphene-based materials and proposing the challenges and prospects.

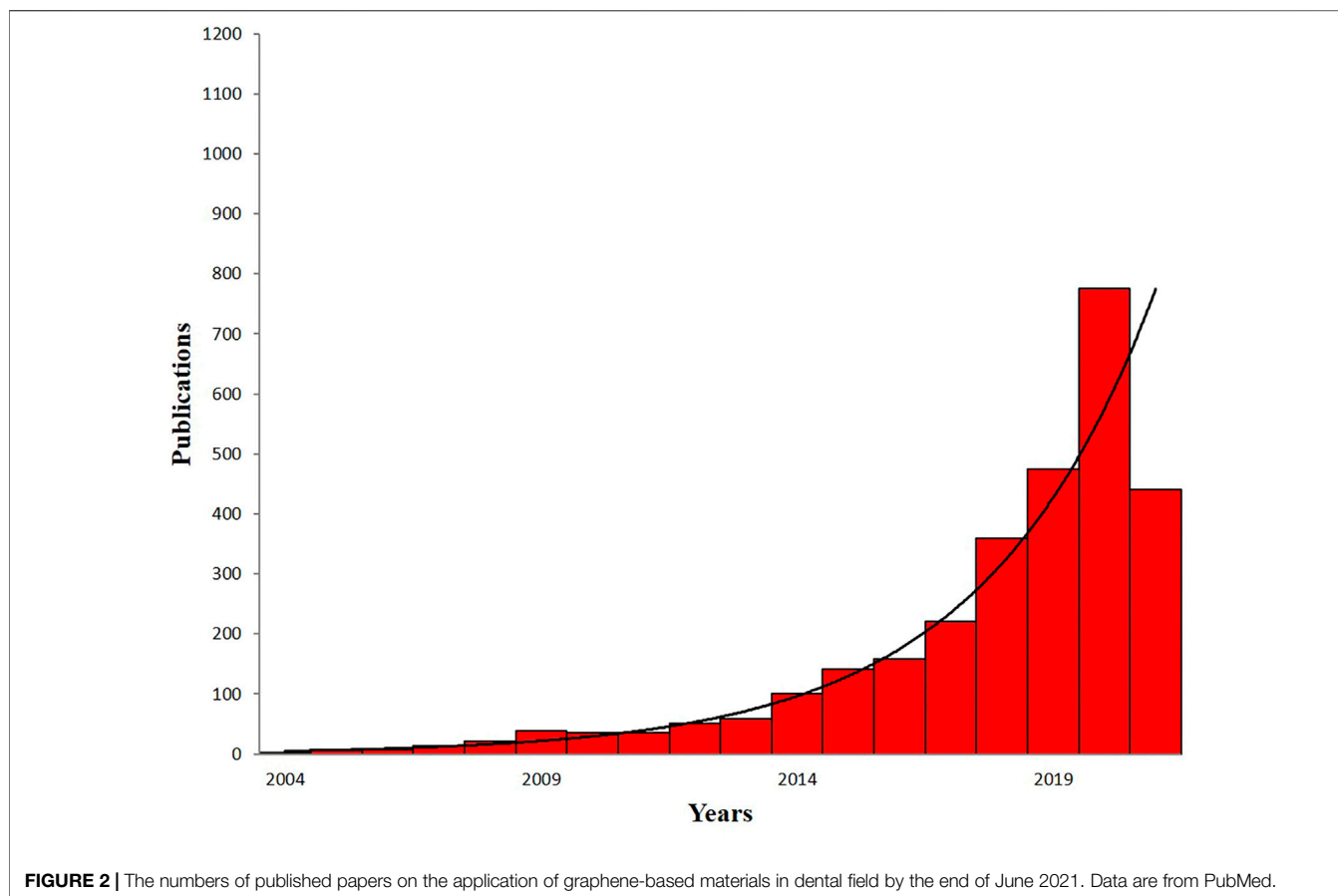
SYNTHESIS AND STRUCTURE OF GRAPHENE AND ITS DERIVATIVE

Graphene, as a promising one-atom thick, 2D carbon-based nanomaterial, is currently the thinnest and strongest material. GO and rGO are the two main derivatives of graphene. Graphene and its derivatives have similar structures but different functional groups, which could lead to the differences in the physical and chemical properties. In this part, the synthesis and structure of graphene and its derivatives will be discussed.

Synthesis and Structure of Graphene

In 2004, the Novoselov and Geim group firstly isolated graphene by mechanical exfoliation method with a sticky tape (Novoselov et al., 2004). Graphene made up of sp^2 hybridized carbon atoms arranged in honeycombed lattice, and the structure of graphene is composed of six-membered rings stacked in parallel shape with no chemical groups on the surface of graphene (Zhang et al., 2019). Graphene aroused great interest, owing to its high mechanical strength, large surface area, good conductivity, and so on (Du et al., 2020).

Graphene from mechanical exfoliation has high purity and low defect, yet the yield is very low. To enhance the yield of graphene, many synthesis methods have been developed. There are two main synthesis approaches: top-down approach and bottom-up approach (Huang et al., 2012; Liao et al., 2018). On the one hand, the bottom-up approach includes the direct synthesis of graphene from the carbon materials, such as chemical vapor deposition (CVD) methods, graphitization of carbon-containing substrates by high temperature annealing, solid-phase deposition (Guo et al., 2009; Xiao et al., 2011). On the other hand, the top-down approach involves micromechanical cleavage, chemical exfoliation of GO followed by reduction treatment, and liquid-phase exfoliation.



Mechanical Exfoliation

In 2004, Geim group firstly obtained monolayer graphene by mechanical exfoliation method (Novoselov et al., 2004). The mechanical exfoliation of graphene is realized with a sticky tape from graphite crystals. Then, the tape was treated with specific solvents (such as acetone), and then, graphene was desorbed and harvested (Phaedon and Christos, 2012). Although the resulting graphene was highly pure without any chemical groups and defects, the yield was very low (Phaedon and Christos, 2012).

Liquid-Phase Exfoliation

Liquid-phase exfoliation is a good technique for a small scale of synthesis of graphene. First, graphite suspension is prepared in an organic solvent to weaken the van der Waals forces between the graphite layers. The graphite was then stripped into graphene sheets by ultrasound at a certain voltage. After further centrifugation, large quantities of single and multilayer graphene were obtained (Ghugue et al., 2016). The graphene is pure but small, and the number of layer is uncontrollable. Moreover, the use of surfactants and organic solvents leads to environmental pollution. The residual surfactants are difficult to remove in the process of exfoliation graphene. N,N-dimethylformamide (DMF), N-methyl-2-pyrrolidone (NMP), and dichlorobenzene (DCB) are the most frequently used organic

solvents. However, they are toxic and detrimental to cells (Liao et al., 2018).

Chemical Vapor Deposition

CVD, one of the most successful approaches, has been widely employed for the low-cost and high-yield preparation of high-quality monolayer or few-layer graphene, where a large area monolayer graphene film formed on the metal (Ming et al., 2014). As for the synthesis process, methane, ethane, or propane is pyrolyzed at high temperature to form carbon onto the metal foils, such as Cu, Ni, Fe, Pt, and Ru. Then, the graphene film formed from free carbon atoms (Liao et al., 2018).

Chemical Exfoliation

Among various methods, chemical methods are one of the most productive ways in the synthesis of graphene-based materials. GO is firstly obtained by the Hummers method, which involves stirring or ultrasonic reaction of graphite with sulfuric acid, sodium nitrate, and potassium permanganate in water. Then, GO is kept at 1,000°C to exfoliate GO. GO is then reduced to rGO with reducing agents. Finally, rGO is converted to graphene by thermal or chemical treatments. However, it is difficult to remove all the oxygen-containing molecules in the GO. Besides, the long processing times and the toxic gases such as NO₂ and N₂O₄ are also adverse factors during the synthesis progress.

Epitaxial Graphene

Epitaxial graphene could be fabricated on the SiC wafers under ultra-high vacuum and high temperatures. During the process, Si atoms on the surface of SiC wafers are sublimated and carbon domains are stayed on the SiC wafer surface, eventually forming graphene (Norimatsu and Kusunoki, 2014). However, because of the simultaneously growth of graphene in different position, the as-prepared graphene is not homogenous compared to other exfoliation methods.

In addition, Nickel diffusion approach is also a good alternative to SiC crystals. Nickel has a lattice structure similar to graphene with a thin nickel layer evaporated onto a SiC crystal. Being heated, the carbon diffuses through nickel layer and forms a graphene layer on the surface. The above methods make it easier to detach graphene layer from SiC crystal (Park and Ruoff, 2009).

GO exfoliation is also involved in other method such as laser ablation, anodic bonding, and photoexfoliation (Ansari et al., 2019). Laser ablation is the use of laser energy to peel graphene. In addition, the density of laser plays an important role in dominating the thickness and quality of graphene flakes (Kazemizadeh and Malekfar, 2017). Moreover, electrochemical exfoliation of graphite could obtain graphene nanosheets (Liu et al., 2008).

Synthesis and Structure of GO

GO, achieved by the oxidation of graphene, presented various reactive oxygen functional groups (e.g., hydroxyl, carboxyl, and epoxy groups) located on the basal plane and the edges of GO, which are beneficial to combine different biomolecules such as proteins and drugs. The function of the above groups aims at interacting with proteins in the form of covalent, electrostatic, and hydrogen bonding. Considering the structure of GO, the amount of carbon atoms in GO has declined to 40%–60%, which are replaced with oxygen atoms. Therefore, GO displays the hydrophilic property. Although GO has shown more hydrophilic than graphene, GO displays defective structure, poor insulating property, and mechanical property (Reina et al., 2017).

The most well-known method of GO synthesis was proposed by Hummers and Offeman in 1958, in which graphite was oxidized by potassium permanganate and sulfuric acid (Hummers and Offeman, 1958). In the Hummers method, NaNO_3 and KMnO_4 , as oxidants, were dissolved in concentrated H_2SO_4 to oxidize graphite. However, the Hummers method has the drawbacks of generation of toxic gas such as NO_2 and N_2O_4 , residual nitrate (Yu et al., 2016). To solve this problem, Kovtyukhova et al. used $\text{K}_2\text{S}_2\text{O}_8$ and P_2O_5 to peroxide the graphite (Kovtyukhova et al., 1999). The mixture was then thermally isolated and cooled at room temperature for 6 h. Then, the mixture was rinsed with water until neutral pH. Finally, GO was obtained by the Hummers method. GO with high degree of oxidation was obtained by the oxidation of KMnO_4 and NaNO_3 . In addition, Marcano et al. used KMnO_4 rather than NaNO_3 from the Hummers method. In addition, a mixture of $\text{H}_2\text{SO}_4/\text{H}_3\text{PO}_4$ was further used to enhance the effect of oxidization (Marcano et al., 2010). The modified method showed many advantages, such as high yields, no generation

of toxic gas, and the controlled temperature. As we know, oxidization is the most important factor for fabricating the GO. Furthermore, Li et al. fabricated a high quality of GO with a green method within 1 h (Peng et al., 2015). The abovementioned improved method obtained a large-scale of graphene by using a strong oxidant K_2FeO_4 without producing heavy metals and toxic gases.

Synthesis and Structure of rGO

rGO is mainly acquired by the reduction of GO. After reduction, the structures and properties of rGO have been greatly changed. Many oxygen-containing groups are removed from GO, and the sp^2 structure of GO was restored to some extent, achieving a low carbon to oxygen ration (Lazauskas et al., 2018). As a result, the electrical conductivity is significantly enhanced. However, the conductivity of rGO is still inferior to graphene because of the residual oxygen and defects structure during the synthesis of GO.

The rGO could be obtained by the reduction of GO with different reduction conditions such as chemical reduction, thermal reduction, photochemical production, photothermal reduction, biological reduction, and electrochemical reduction (Cote et al., 2009; Guo et al., 2009; He et al., 2011; Mao et al., 2010; Williams et al., 2008; Yin et al., 2010). Among them, chemical reduction of GO is the most widely used technique to synthesize rGO with hydrazine, ascorbic acid, and bovine serum albumin (BSA) as reducing agents (Phaedon and Christos, 2012) (Rai et al., 2020) (Liu et al., 2010). Hydrazine is widely used in the chemical reduction of GO, but it is toxic and detrimental to cells. To overcome the limitations of these toxic-reducing agents, various green reduction agents have been investigated. For example, Cherian et al. used ascorbic acid as a reducing agent and stirred for 2 h in 95°C water bath to produce high-yielding black rGO (Cherian et al., 2019). Except for chemical reduction, thermal reduction of GO is employed under vacuum inert or other conditions suitable for reduction between 300°C and $2,000^\circ\text{C}$ (Pei and Cheng, 2012; Wang et al., 2017). Photothermal reduction of GO can also be produced using laser with wavelengths under 390 nm (Lazauskas et al., 2018). Moreover, Li et al. reported that microwave heating could be used for the reduction of rGO in microwave ovens (Li et al., 2010).

DENTISTRY-RELATED PROPERTY OF GRAPHENE AND ITS DERIVATIVES

Biocompatibility and Cytotoxicity

To develop the application of graphene-based materials in dentistry, it is necessary to evaluate the biocompatibility and cytotoxicity of graphene-based materials (Olteanu et al., 2015). Many researchers have been discussed the cytotoxicity of graphene and its derivatives. Up to date, the affected factors involved concentrations, surface functionalization, and so on.

Many studies have shown a dose-dependent effect on the biocompatibility and toxicity of graphene and its derivatives. Some researchers showed that the toxicity of GO to fibroblast cells was little when the concentration of GO was lower than $20\ \mu\text{g}/\text{ml}$ (Kan et al., 2011). Whereas, the cytotoxicity of GO

increased when the concentration was up to 50 $\mu\text{g/ml}$. Wang et al. investigated the cytotoxicity of GO in mice and the results demonstrated a dose-dependent toxic behaviors *in vivo* (Wang et al., 2011). When the concentrations of GO were 0.1 and 0.2 mg, there was no toxicity was detected. With the increase concentration to 0.4 mg, chronic toxicity was observed in mice.

Some studies have also focused on the effect of surface functionalization on cytotoxicity. Diana et al. investigated the cytotoxicity of GO, nitrogen-doped graphene (N-Gr), and thermally reduced GO (TRGO) on human dental follicle stem cells and analyzed the involved specific mechanism (Olteanu et al., 2015). The result showed the lowest cytotoxicity of GO and the highest cytotoxicity of TRGO. However, Malgorzata et al. also compared the viability of leukocytes with GO, rGO, and rGO-PEG (Podolska et al., 2020). The results showed that there was no significant difference in the viability of leukocytes at the concentration of 50 $\mu\text{g/ml}$, indicating that the surface functionalization had no effect on the cell viability.

When the biomaterials were implanted to the tissue, the inflammation would be provoked by the protein interactions. During this process, many factors such surface charge, topography, and chemical compositions were involved and affected the resorption of protein. Besides, many molecules also played an important role in the process of inflammation such as betaines (D'Onofrio et al., 2019). Moreover, the tissue inflammation caused by graphene-based materials should be attracted on much attention. Eriberto et al. had reported that titanium nanoparticles released from dental implants could cause the chronic inflammation on the soft and bone tissue around the dental implants (Bressan et al., 2019).

Therefore, when using graphene-based nanomaterials as the coatings of dental implants and so on, we should also focused on its effect on the surrounding tissue inflammation. In the study of Rosa et al., they confirmed that friction during the dental implants emplaces when the loads is over 400 mN (Rosa et al., 2021). However, they also investigated that graphene nanocoatings did not activate the high expression of inflammatory markers such as TNF- α from macrophages. Of course, more and more studies should be done to prove this result.

Stimulation of Cell Differentiation

Ideal biomaterials in the tissue engineering show the ability to induce the adherence, proliferation, and differentiation of cells. Many *in vitro* studies have shown that graphene and its derivatives showed the multi-differentiation ability such as osteogenic differentiation and regeneration of dental pulp.

Many studies have proved that graphene-based materials have the potential in promoting the osteogenic differentiation of various cells including MC3T3-E1, bone marrow mesenchymal stem cells (BMSCs), periodontal ligament stem cells (PDLs), dental pulp stem cells (DPSCs), etc. (Lee, Shin, and Lee et al., 2015a; Norahan et al., 2019; Xie et al., 2016; Zhou et al., 2016). The osteogenic differentiation of graphene, GO, and rGO has all been tested in different forms and synthesis methods. DPSCs, PDLs, dental follicle progenitor cells (DFPCs), and BMSCs are used to induce the osteogenic

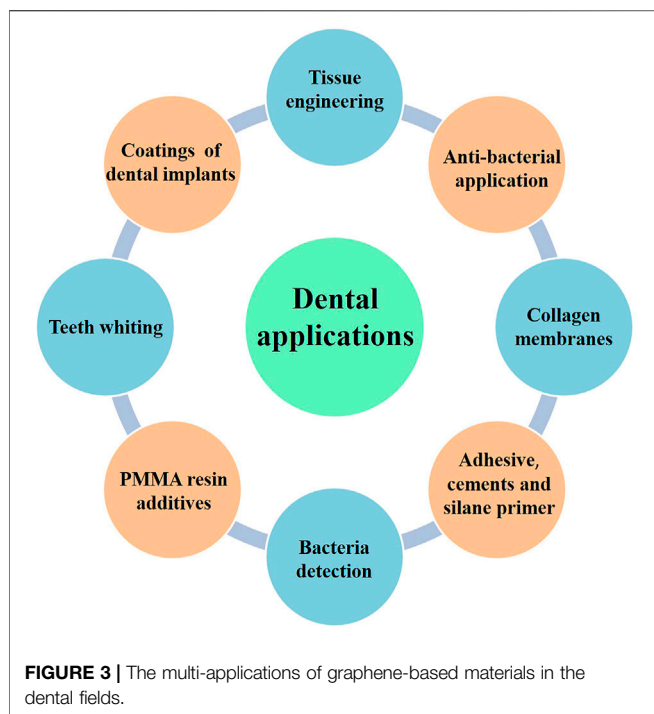
differentiation. For example, Han et al. prepared a monolayer graphene on copper foils by CVD method and studied the ability to induce the osteogenic differentiation of DPSCs (Xie et al., 2016). The results showed that osteogenic genes and proteins runt-related transcription factor 2 (RUNX2), osteocalcin (OCN), and collagen (COL) were upregulated on graphene, after the culture of 14 and 28 days. Erika et al. fabricated GO-coated COL sponge scaffolds and evaluated the ability of bone formation in tooth extraction socket (Nishida et al., 2016). After the GO scaffolds were implanted into the tooth extraction sockets of dogs, the radiological density and histological results showed that the GO promoted bone formation was fourfold compared with the control. To further investigate the osteogenic ability of rGO, Lee et al. constructed rGO coating on the HAP composites, which confirmed the osteogenic effect of rGO on human mesenchymal stem cells (hMSCs), the improved mineralization of calcium and phosphate and enhanced ALP activity (Lee et al., 2015b, Shin, and Jin et al., 2015).

To investigate the ability of graphene-based materials on the dental pulp regeneration, some researchers had focused on the neurogenic differentiation of graphene-based nanomaterials. For example, Seonwoo et al. prepared nanofibers (NFs) with electrospinning technique by incorporated with rGO and polycaprolactone (PCL) and investigated their enhanced neurogenesis of DPSCs (Seonwoo et al., 2018). The results showed that NFs with rGO showed high expression of Tuj-1 (the early marker of neurogenesis) and NeuN (the late marker of neurogenesis).

Scaffolds are an important part in the bone tissue engineering. Similarly, periodontal tissue engineering also required scaffolds to achieve an ideal therapy for periodontitis. Kawamoto et al. studied the GO modified COL sponge scaffold and evaluated the regeneration of periodontal tissue *in vivo* (Kohei et al., 2018). The rat cranial defect model was constructed, and the results showed that the new formed bone in the GO scaffolds was more than that of the control. To stimulate the therapy of periodontitis in human, the class II furcation defects of dog were conducted. CT results showed that the radiopacity of GO scaffolds was obviously increased. In addition, the histological results showed that more new formed alveolar bone was found and the furcation defect was filled without severe root resorption. More interestingly, periodontal ligament-like and cementum-like tissues were also occurred, showing an ideal therapy effect.

Antibacterial Property

As an excellent biomaterial in dentistry, low cytotoxicity and multi-differentiation ability are necessary. Except for these, antibacterial property cannot be ignored. The antibacterial effect of graphene-based materials was firstly discovered by Hu et al. (Hu et al., 2010). Then, more and more researchers had confirmed the antibacterial effect. For example, Gholibegloo et al. found that the bacterial survival rate of *S. mutans* treated with GO, GO-carnosine (GO-Car), and GO-Car/hydroxyapatite (HAP) can decrease by 67%, 86.4%, and 78.2%, respectively (Gholibegloo et al., 2018). Many composites had been



fabricated to study its antibacterial property, and some researchers fabricated the graphene-based materials into glass ionomer cements (GICs), polymethyl methacrylate (PMMA), and dental adhesive (Bregnocchi et al., 2017; Lee J.-H. et al., 2018; Sun et al., 2018).

DENTAL APPLICATIONS OF GRAPHENE-BASED MATERIALS

With the improved synthesis methods, expanded types of graphene-based materials, and engineered properties, various applications have been collected and discussed as follows (Figure 3). In addition, a main summary of graphene-based materials used in the dental field is given in Table 1.

Tissue Engineering

Tissue engineering is widely used in the repair and regeneration of various defects caused by tumors, traumas, infections, and so on. It is well known that the scaffolds provide a platform for the attachment, proliferation, and differentiation of different stem cells in the tissue engineering. Many researchers proved that graphene-based materials were suitable for fabricating or coating for scaffolds in the tissue engineering.

TABLE 1 | The graphene-based materials used in the main study of dental fields.

Applications	Types of graphene	Properties	Application types	References
Bone tissue engineering	Graphene/HA	Biomimetic mineralization	Scaffolds	Fan et al. (2014)
	Monolayer graphene	Osteogenic differentiation	Coatings	Xie et al. (2016)
	rGO/BCP	Osteogenic differentiation	Coatings	Jeong-Woo et al. (2017)
	rGO/HA	Mineralization	Scaffolds	Lee et al. (2015b)
	Silk fibroin/GO/BMP-2	Osteogenic differentiation	Scaffolds	Wu et al. (2019)
	GO/chitosan	Osteogenic differentiation	Scaffolds	Amiryaghoubi et al. (2020)
Dental pulp regeneration	Graphene dispersion	Neural differentiation	Scaffolds	Jelena et al. (2018)
	NFs/rGO/PCL	Neural differentiation	Scaffolds	Seonwoo et al. (2018)
	GO	Osteogenic differentiation	Scaffolds	Vinicius et al. (2016)
		Odontogenic differentiation		
Periodontal tissue regeneration	3D collagen sponge/GO	Osteogenic differentiation periodontal ligament-like tissue regeneration	Scaffolds	Kohei et al. (2018)
	Silk-fibroin/GO	Cementum-like tissue regeneration Osteogenic differentiation Cementoblast differentiation	Scaffolds	Vera-Sánchez et al. (2016)
Dental implant and abutment	Single-layer graphene sheets	Osteogenic differentiation	Coatings	Ming et al. (2018)
	GO/CS/HA	Osteogenic differentiation	Coatings	Suo et al. (2018)
	GO	Osteogenic differentiation	Coatings	Zhou et al. (2016)
	rGO/Dex	Osteogenic differentiation	Coatings	Jung et al. (2015)
	rGO nanosheets	Osteogenic differentiation	Coatings	Lu et al. (2020)
	GO/Minocycline hydrochloride (MH)	Antibacterial property	Coatings	Qian et al. (2018)
	GO/Ag	Antibacterial property	Coatings	Jin et al. (2017)
Collagene mmember	GO	Roughness and stiffness Osteogenic differentiation Inflammation effect	Coatings	Marco et al. (2017)

TABLE 2 | The abbreviations and full name used in this paper.

Abbreviations	Full name
WHO	World health organization
GO	Graphene oxide
rGO	Reduced graphene oxide
CVD	Chemical vapor deposition
DMF	N,N-dimethyl-form amide
NMP	N-methyl-2-pyrrolidone
DCB	Dichlorobenzene
BSA	Bovine serum albumin
N-Gr	Nitrogen-doped graphene
TRGO	Thermally reduced graphene oxide
BMSCs	Bone marrow mesenchymal stem cells
PDLCS	Periodontal ligament stem cells
DPSCs	Dental pulp stem cells
DFPCs	Dental follicle progenitor cells
RUNX2	Proteins runt-related transcription factor 2
OCN	Osteocalcin
COL	Collagen
hMSCs	Human mesenchymal stem cells
NFs	Nanofibers
PCL	Polycaprolactone
GICs	Glass ionomer cements
HAp	Hydroxyapatite
BCP	Biphasic calcium phosphate
EMFs	Electromagnetic fields
SCPAs	Stem cells of apical papilla
GNPs	Graphene nanoplatelets
FG	Fluorinated graphene
PMMA	Polymethyl methacrylate
nGO	Graphene oxide nanosheets
hGFs	Human gingival fibroblasts
hASCs	Human adipose-derived stem cells
hBMSCs	Human bone marrow mesenchymal stem cells
Dex	Dexamethasone
MH	Minocycline hydrochloride
H2O2	Hydrogen peroxide
PDT	Photodynamic therapy
IL-8	Interleukin-8
WSL	White spot lesion
BAG	Bioactive glass
GBR	Guided bone regeneration
GTR	Guided tissue regeneration
AMOX	Amoxicillin
SRP	Solid rigid polyurethane

Bone Tissue Engineering

Many studies confirmed that graphene-based materials can promote the osteogenic differentiation of various cells including osteogenic cells such as MC3T3-E1 and stem cells such as BMSCs, PDLCS, and DPSCs. As for bone tissue engineering, graphene-based materials could be used in various forms (such as composite powers, scaffolds, and surface coatings) (Yong et al., 2018).

Many studies have reported that graphene could stimulate different types of stem cells to form osteoblasts. Fan et al. reported that graphene/HAp composite sheet displayed good biomimetic mineralization (Fan et al., 2014). The similar osteogenic differentiation has been proved by Xie et al. (Xie et al., 2016). They prepared monolayer graphene with CVD and further evaluated the degree of mineralization and expression of osteogenic genes and proteins. They found that graphene

induced RUNX2 and OCN expression and stimulated high expression of OPN and OCN in DPSCs. Moreover, Li et al. showed that graphene could induce the higher expression of osteogenic-related genes (OCN, OPN, BMP-2, and Runx2) compared with the control (Li et al., 2015). In addition, the enhanced osteogenic effect had also been confirmed by the high OCN expression at the protein level.

To confirm the osteogenic differentiation of rGO, some researchers had fabricated rGO coatings and composites (Norahan et al., 2019). Kim et al. successfully fabricated rGO coating on the biphasic calcium phosphate (BCP) (Jeong-Woo et al., 2017). The results showed that the regeneration of new bone volume was higher in the rGO groups compared with the control (Figures 4–6). Except for coatings, composites are also the new strategy to confirm the osteogenic property of rGO. Lee and his colleagues also constructed the rGO composites with HAPs to further prove the promoted osteogenic properties of rGO (Lee et al., 2015a). The results showed that rGO/HAP composites at 10 µg/ml induced more calcium deposits at day 14 and 21, whereas the rGO group induced more calcium deposition at day 21. The rGO/HAP composite group also showed more mineralized bone nodules than the control at day 28 in von Kossa staining. Interestingly, Lim et al. creatively studied the synergistic effect of electromagnetic fields (EMFs) and reduced rGO on the osteogenic, neurogenic, and audiogenic differentiation of hMSCs (Lim et al., 2016). The ALP activity showed that rGO + PEMF group showed the highest ALP expression after incubation of 7 days.

To confirm the osteogenic differentiation of GO, diverse functionalizations of GO had been done such as scaffolds and nanosheets. As used for the scaffolds, Wu et al. modified the silk fibroin scaffold with GO-functionalized BMP-2 peptide. The results showed that the expression of OPN and COL-1 was upregulated by GO-P24 both in the osteogenic medium and non-osteogenic medium, demonstrating the synergistic effects of GO and BMP-2 (Wu et al., 2019). The experiment *in vivo* also confirmed the above results. Then, Azadian et al. also successfully fabricated the polyvinylidene fluoride (PVDF)–polyvinylalcohol (PVA)–GO scaffold and evaluated the ALP activity, calcium contents assays, and expression of osteogenic gene markers (Azadian et al., 2020). After 7 and 14 days, ALP expression and calcium content in PVDF-PVA group were higher than the other groups and PVDF-PVA-GO group, which also achieved the highest expression of Col-1, Runx2, and OCN in hiPSCs for 7 and 14 days. Besides, GO coatings are also constructed to prove the osteogenic property of GO. Recently, Amiryaghoubi and his co-workers reported a new injectable hydrogel composed with GO and chitosan (CS) as stem cells scaffolds for bone regeneration. According to the results, GO improved the mechanical properties of hydrogel and achieved an excellent performance in bone tissue engineering (Amiryaghoubi et al., 2020). Besides, Wei et al. testified the effect of pristine GO nanosheets on the proliferation and osteogenic ability of BMSCs by two biomimetic cell culture methods (Wei et al., 2017). When the concentration of GO nanosheets was 10 µg/ml, the proliferation of BMSCs with both seeding methods was inhibited at 3 days. Nowadays, phosphorene is a new 2D nanomaterials, which attracted great attentions after graphene (Tatullo et al., 2019a). The properties of phosphorene

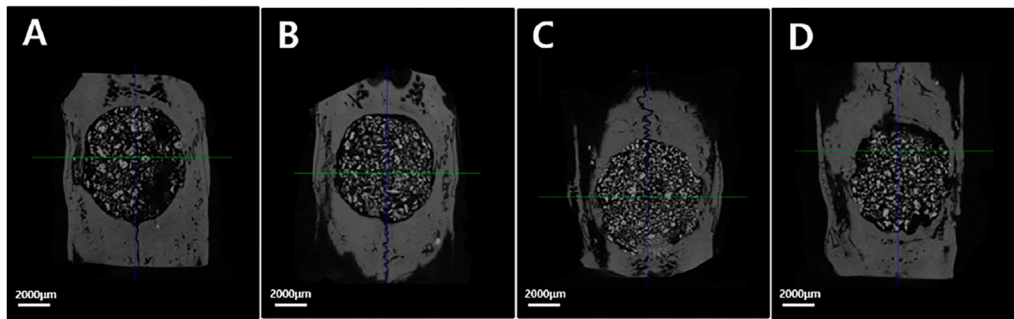


FIGURE 4 | The micro-CT images of different groups. (A) Control group; (B) rGO2 group; (C) rGO4 group; (D) rGO6 group (Jeong-Woo et al., 2017). Open access, 2017, Jeong-Woo Kim.

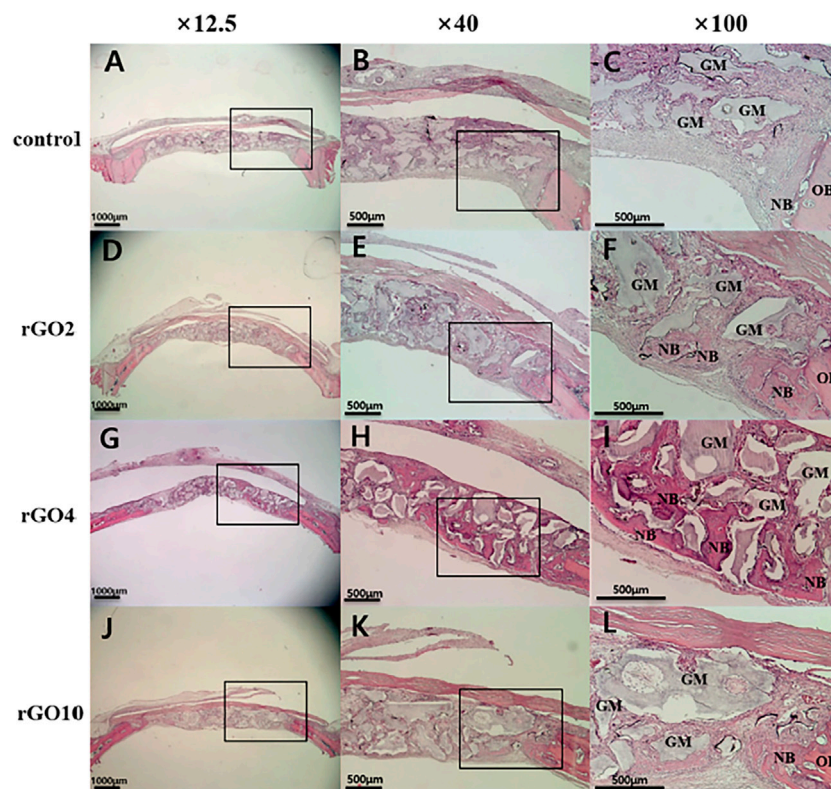


FIGURE 5 | Histological images of specimens at 2 weeks after surgery. Black box is the interest area. (A–C) Control group; (D–F) rGO2 group; (G–I) rGO4 group; (J–L) rGO10 group. NB, new bone; OB, old bone; GM, bone graft material (Jeong-Woo et al., 2017). Open access, 2017, Jeong-Woo Kim.

were quite similar to graphene-based materials, and they had wonderful biodegradability and biocompatibility compared with graphene-based materials. Liu et al. also investigated the synergistic effect of GO and phosphorene on the osteogenic differentiation (Liu et al., 2019).

Dental Pulp Regeneration

The neural and odontogenic differentiation induced by graphene-based materials were also observed. Graphene dispersion can be

applied on the neural differentiation of stem cells of apical papilla (SCPAs) (Jelena et al., 2018). A good neuron-like cell bodies with long process were found in the graphene dispersion group. The graphene dispersion group showed high expression of NF-M and β III-tubulin and showed strong β III-tubulin and NeuN immuno-reactivity 7 days after nerve induction, indicating that graphene enhanced the neural differentiation of SCPAs.

To intensify the neural differentiation of graphene-based materials, Seonwoo et al. prepared a NFs incorporated with

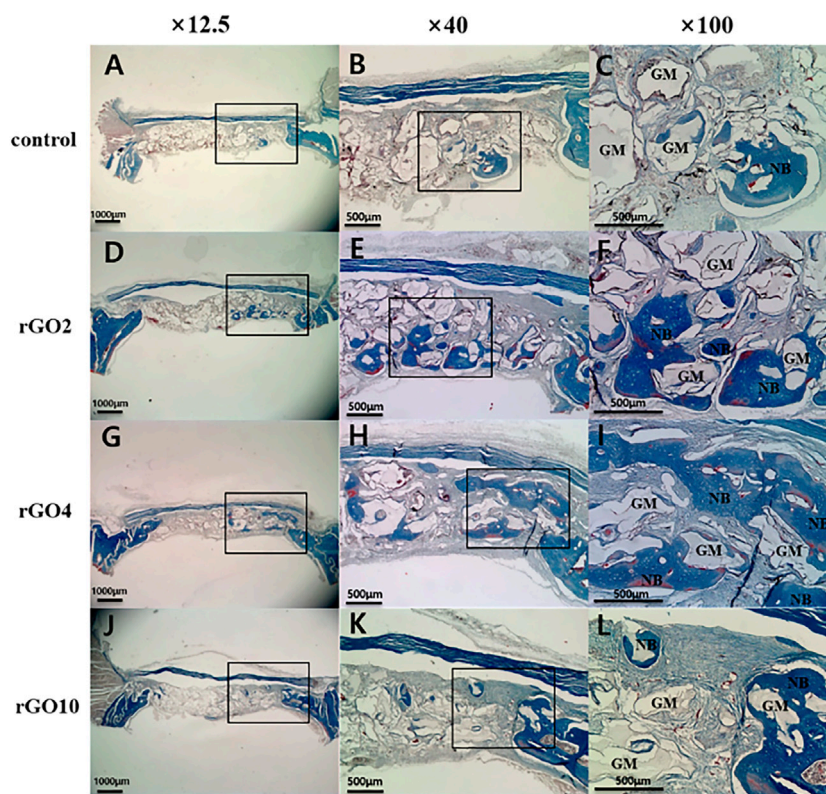


FIGURE 6 | Histological images of specimen at 8 weeks after surgery with Masson's trichrome staining. Black box is the interest area. (A–C) Control group; (D–F) rGO2 group; (G–I) rGO4 group; (J–L) rGO10 group. NB, new bone; OB, old bone; GM, bone graft material (Jeong-Woo et al., 2017). Open access, 2017, Jeong-Woo Kim.

rGO and PCL by electrospinning technique and investigated the enhanced neurogenesis of DPSCs (Seonwoo et al., 2018). The results showed that NFs with 0.1% and 1% rGO exhibited high expression of Tuj-1 and NeuN, whereas NFs with higher rGO concentration only achieved intense expression of NeuN on days 3 and 7. To prove the neural differentiation of GO, Rosa et al. investigated the effect of GO on the differentiation of DPSCs (Vinicius et al., 2016). Except for the high expression of Runx2 and OCN, GO also significantly upregulated DMP-1 and DSPP with the odontogenic differentiation of DPSCs.

Periodontal Tissue Regeneration

As we know, periodontitis is an inflammatory disease with dramatic destruction in periodontal tissue such as periodontal ligament, alveolar bone, and cementum. With the deterioration of periodontitis, the tooth faced the fate of losing, which led to many functional disorders. Therefore, it is quite urgent to regenerate and appealed many researchers. Compared with graphene and rGO, GO showed the hydrophilic surface and good dispersibility, which facilitated the absorption of some related proteins. Kawamoto et al. conducted 3D COL sponge scaffold with GO dispersion (Kohei et al., 2018). The histometric analysis showed that new formed bone in the GO group was, respectively, 2.7- and 2.3-fold greater than the control. In *in vivo* experiment, more new alveolar bone was found and filled the furcation defect. Even

more interestingly, periodontal ligament-like, cementum-like tissue was also observed in the GO group (Figures 7, 8). To investigate the related mechanisms, Vera-Sánchez et al. had fabricated the GO and silk-fibroin composites and evaluated their osteogenic differentiation and cementoblast differentiation (Vera-Sánchez et al., 2016). The results of RT-PCR showed that the cementum related genes PTPLA/CAP and CEMP1 were highly expressed after incubating for 10 days. They further ascertained the cementoblast differentiation by evaluating the expression of cementum-related protein CEMP1 on days 10.

Adhesives, Cements and Silane Primer

Adhesives and cements are two kinds of common materials in the dental restorations. Although they showed the advantages of aesthetic effect and high hardness, the problems of high polymerization shrinkage and bad antibacterial property limited their development. Silane primer played an important role in the bonding of zirconia.

Owing to various advantages of graphene-based materials, it has been applied to reinforce the properties of adhesive materials (Farooq et al., 2021). Graphene nanoplatelets (GNPs) are usually prepared as fillers of polymer dental adhesives because of the antimicrobial and antibiofilm activity. The nanocomposites filled with GNPs have been shown to effectively inhibit the active of *S. mutans* cells without compromising the bonding properties

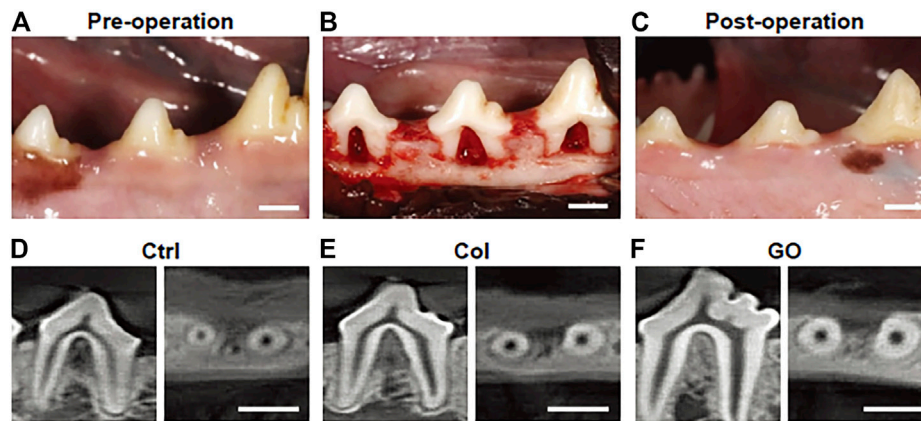


FIGURE 7 | The photographs and CT images of class II furcation defects of dog. **(A)** Pre-operation; **(B)** class II furcation defects in the surgery; **(C)** postoperation; **(D–F)** CT images after 4 weeks surgery. **(D)** No implantation group; **(E)** collagen scaffold group; **(F)** GO scaffold group (Kohei et al., 2018). Free full-text article, 2018, Kohei Kawamoto.

(Bregnocchi et al., 2017). Therefore, GNPs may be an ideal filler for dental adhesives, whose antibiofilm activity did not reduce mechanical performances.

When graphene nanosheets were added to two kinds of calcium silicate cements in powder form of different proportions, GNP–cement composites do well in shortening the bonding time and increasing the hardness of both cements. However, the bonding properties of one cement named Endocem Zr (ECZ) were impaired significantly, indicating that the addition of GNPs may improve the physico-mechanical properties of materials but not ideal for all materials in terms of bonding properties (Nileshkumar et al., 2017). Unlike gray GNPs, bright white fluorinated graphene (FG) may be a better filler in dentistry. FG has been used to the modification of GICs, presenting great advantages on the mechanical, tribological, and antibacterial properties. Compared with traditional GICs, the composites not only increase the Vickers micro hardness and compression strength but also decrease the friction coefficient. In the antibacterial properties, the GIC/FG composites achieve good antibacterial properties against *Staphylococci aureus* and *Streptococcus mutans* (Sun et al., 2018).

Considering the bonding properties of resin composites to ZrO_2 , silane primers formed adhesive layer show the poorest mechanical properties (Fallahzadeh et al., 2017). Therefore, the corporation of GO sheets into the silane primers may be a good choice to improve the mechanical properties of the adhesive layer. The results showed that the addition of GO sheets significantly increased the shear bond strength between resin composite and ZrO_2 , improved the surface roughness, and slightly increased the water contact angle (Khan et al., 2019). Therefore, graphene-base materials are ideal filler for adhesive, cements, and silane primers with proper materials.

Polymethyl Methacrylate Resin

PMMA resin has been used in prosthetic dentistry, especially complete and removable partial dentures over the past 80 years

(Bacali et al., 2019), possessing many advantages such as easy manufacturing process, low cost, low modulus of elasticity, easy repair, and good aesthetics. However, the limitations of PMMA such as low mechanical properties, large polymerization shrinkage, and the poor inhibition of biofilms formation still exist (Bahra et al., 2013; Gad et al., 2019; Matsuo et al., 2015; Ruse and Sadoun, 2014). Recently, the graphene family has exhibited good mechanical and desirable antibacterial properties in different forms in other fields. Because of the mechanical effect of graphene on PMMA, Azevedo et al. has achieved the definitive maxillary full-arch rehabilitation by incorporating GO into the PMMA resin (Azevedo et al., 2019). After 8 months later, there were no mechanical, aesthetic, and other complications found, indicating that the addition of GO to PMMA resin would be a good choice for prosthetic rehabilitation. Bacali et al. reported PMMA with graphene-silver nanoparticles (Gr-Ag), and the mechanical properties, hydrophilic abilities, and the morphology of the composites were further evaluated (Bacali et al., 2019). The results showed that the compression parameters, bending, and tensile strength of the Gr-Ag fillers were significantly higher than the pure PMMA group, indicating that the addition of Gr-Ag improved the mechanical properties of PMMA resin. Moreover, Bacali and his co-workers also assessed the antibacterial properties of Gr-Ag-modified PMMA (Bacali et al., 2020), and the results confirmed that Gr-Ag-modified groups showed higher inhibition effect in all Gram-negative strain, *Staphylococcus aureus*, *E. coli*, and *Streptococcus mutans* (Bacali et al., 2020). In conclusion, graphene-based materials may be an ideal filler to promote the physical-mechanical and antibacterial properties of PMMA.

Meanwhile, graphene oxide nanosheets (nGO) have been used to improve the antimicrobial-adhesive effects of PMMA resin by Lee and his co-workers (Lee SM. et al., 2018). The immediate antimicrobial-adhesive effects showed that nGO-incorporated groups exhibited stronger antimicrobial effect against *C. albicans*, *E. coli*, *S. aureus*, and *S. mutans* after 1 h of

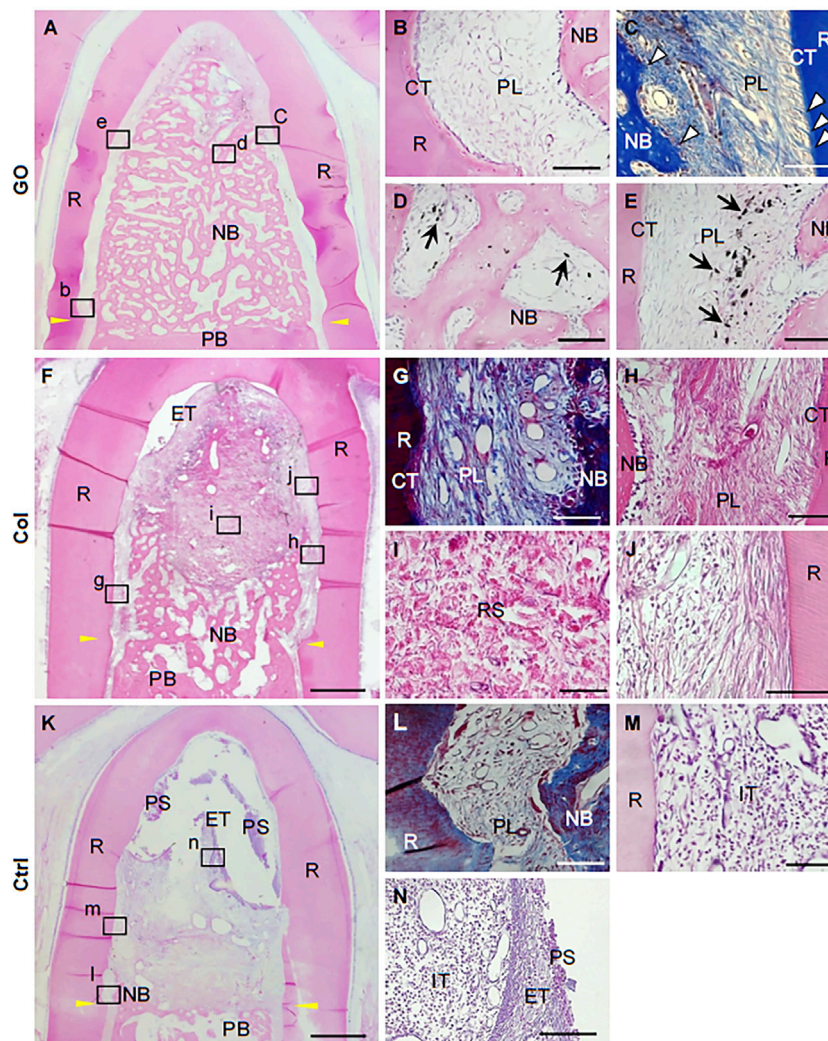


FIGURE 8 | Histological images after GO scaffold implantation into class II furcation defects of dog. **(A–E)** GO scaffold group; **(F–J)** collagen scaffolds group; **(K–N)** no implantation group. **(A)** Periodontal ligament-like tissue, cementum-like tissue, and alveolar bone with Sharpey's fiber. **(B–E)** High magnification of the black box areas **(B–E)** in **(A)**. **(G–J)** High magnification of the black box areas **(G–J)** in **(F)**. **(K–N)** High magnification of the black box areas **(L–N)** in **(K)** (Kohei et al., 2018). Free full-text article, 2018, Kohei Kawamoto.

attachment than only PMMA group except for 0.5% nGO-incorporated group against *E. coli* and *S. mutans*. Furthermore, PMMA with 2% nGO showed greater anti-adhesion effects than the PMMA resin after culturing for 28 days of *C. albicans*, indicating that the hydrophilicity of PMMA could be improved by the incorporation of nGO. Bacali et al. evaluated the antibacterial activity, cytotoxicity, monomer release, and mechanical properties of PMMA resin by adding graphene-Ag nanoparticles (G-AgNp) (Bacali et al., 2020). The results showed that G-AgNp-containing group displayed good antibacterial effects on both Gram-positive and Gram-negative strain and exhibited better antibacterial effect on Gram-positive strain *Staphylococcus aureus* than PMMA. Besides, Gram-negative strain *E. coli* also was sensitive to G-AgNp. Therefore, graphene family proved to be promising filler mixed with PMMA in antibacterial applications.

Coatings for Dental Implants and Abutments

Titanium and its alloys have been widely used in dental implants, owing to their various advantages such as good biocompatibility, high mechanical property, and corrosion resistance (Fe Ridoun et al., 2017; Jeong et al., 2017; Xie et al., 2014). However, implant failure still occurs. Because of the poor osseointegration and peri-implantitis of titanium and its alloys (Berglundh et al., 2019; Smeets et al., 2014; Kordbacheh et al., 2019). Therefore, many surface modifications by graphene-based materials have been used to improve the bioactivities of titanium and its alloys (Barfeie et al., 2015; Chouirfa et al., 2018; Li et al., 2009; Souza et al., 2019).

It is well known that the osseointegration is the gold standard of the success of dental implants. Therefore, the new bone

formation between dental implants and bone tissues is of great significance. In regard to the superior osteogenic differentiation of graphene in bone tissue engineering, they also attracted much attention in the modification of dental implant. Park et al. reviewed that the strategies of graphene-based modifications could be mainly divided into four categories: 1) a layer-by-layer assembly; 2) PMMA-mediated method; 3) electrophoretic deposition; and 4) APTES-induced method (Park et al., 2017).

To promote the osteogenic properties, many researchers have made many efforts. Gu et al. successfully constructed single-layer graphene sheets on the titanium substrates by PMMA-mediated method (Ming et al., 2018). The result showed that graphene sheets exhibited superior adhesion and proliferation properties of human gingival fibroblasts (hGFs), human adipose-derived stem cells (hASCs), and human BMSCs (hBMSCs) compared with the control. The osteogenic differentiation of hASCs and hBMSCs was also improved by graphene sheets. Otherwise, the above study recommended that PMMA treated at 160°C for 2 h enhanced the adhesion strength between graphene and titanium. Meanwhile, Suo et al. successfully constructed a homogeneous GO/CS/HAp composites on Ti substrates by electrophoretic deposition, improving the osteogenic property of Ti substrates *in vitro* and osseointegration *in vivo* (Suo et al., 2018). Besides, some other researchers have tried the APTES inducement to fabricate the graphene coatings (Jung et al., 2015; Lu et al., 2020; Zhou et al., 2016). Zhou et al. modified the Ti substrates with 3-APTES and then immersed it in the GO solution for 24 h (Zhou et al., 2016). PDLCs were used to evaluate the cell attachment, morphology, proliferation, and osteogenic differentiation *in vitro*. All the results indicated that GO coating showed a positive effect on improving the bioactivity of PDLCs. Jung and his colleges prepared a dexamethasone (Dex)-loaded rGO coating on Ti13Nb13Zr (MPCr-TNZ) multipass rolled titanium alloy surface by using the spin coating technology after pretreatment with APTES, showing a stable long-term release behaviors of Dex (Jung et al., 2015). A possible mechanism is π - π stacking. In conclusion, the Dex-loaded rGO-MPCr-TNZ achieved an enhanced proliferation and facilitated differentiation of MC3T3-E1 cells into osteoblasts. Besides, an implantation of a prototype dental implant was modified with Dex-loaded rGO to an artificial bone block, demonstrating the feasibility of the stable surface modification for further clinical applications. Recently, Lu and his coworkers ascertained the improved osteogenic effect of rGO nanosheets on the surface of titanium (Lu et al., 2020). Compared with the control, rGO groups achieved more growth factors absorption especially BMP-2, IGF, and TGF- β . Moreover, rGO-modified group displayed a more stretch cell cytoskeleton and excellent osteogenic differentiation of BMSCs. In conclusion, graphene-based material is a good candidate for dental implant surface modification material, which can improve the osseointegration of implants with proper methods.

Moreover, the excellent antibacterial activity of graphene also captured a tremendous interest in dental implant surface coatings. It is generally accepted that the failures of dental implants are still the occurrence of bacterial infections. Therefore, the titanium surface antibacterial modification is

very necessary. Qian et al. reported an electrostatically prepared GO coating that loaded the Minocycline hydrochloride (MH) on titanium (Qian et al., 2018). According to the results, GO-modified surface could prohibit the growth of *Staphylococcus aureus*, *Streptococcus mutans*, and *Escherichia coli*. Whereas MH-loaded GO coating showed superior antibacterial property with the synergistic effect of GO and MH, which were contact-killing and release-killing. Jin et al. prepared GO film and Ag nanoparticles on the titanium substrates by electroplating and ultraviolet reduction methods (Jin et al., 2017). In addition, GO-Ag-Ti composite exhibited a prominent antibacterial activity to *S. mutans* and *P. gingivalis* compared with the Ti substrate. Therefore, it can be inferred that graphene-based materials showed outstanding antibacterial activity when combined with proper materials.

Besides the titanium dental implants, zirconia has also been used for dental implant materials (Priyadarsini et al., 2017). To improve its inert properties, many surface modifications have been used. Graphene shows obvious merit in zirconia implant surface modifications (Cho and Ko, 2013; Schunemann et al., 2019). Li et al. reported a zirconia/graphene (ZrO₂/GNs) composites, which were coated on the surface of zirconia by an atmosphere plasma spray technique (Li et al., 2014). The results indicated that ZrO₂/GNs composites showed the excellent wear resistance and zirconia's tribological behavior.

Peri-implantitis has become a common disease that threatened the survival rates of dental implants. Many strategies have been adopted to avoid the happening of peri-implantitis (Jansäker et al., 2010; Koldstrand et al., 2018). Abutments are also an important part of implant system, and medicated abutments may be a good option for preventing the peri-implantitis. Qian et al. successfully fabricated a MH-loaded GO coating on the dental implant abutment and further evaluated the antibacterial activities and the adhesive ability of gingival fibroblasts with beagle dogs model (Qian et al., 2019). The results showed that MH/GO/Ti group achieved least bone loss, which could be negligible, whereas Ti and MH/Ti groups showed more bone loss by micro-CT analysis. Histological analysis showed that there were fewer neutrophils and more osteocytes in the MH/GO/Ti group than in the Ti and MH/Ti groups. Therefore, it can be inferred that MH-loaded GO films on abutment surfaces may be a superior option for prohibiting the progress of peri-implantitis in the future.

Teeth Whitening

As we know, hydrogen peroxide (H₂O₂) has been widely utilized for in-office whitening for a long time. The H₂O₂ molecules can penetrate deep the teeth and carry out the bleaching process. However, the relative high concentrations of H₂O₂ caused some side effects such as tooth sensitivity and gingival irritation (Carey and Clifton, 2014; Kwon and Wertz, 2015). Therefore, many improved strategies have been made to accelerate the tooth whitening and decrease the side effects. Su et al. reported a cobalt (Co)/tetraphenylporphyrin (TPP)/rGO nanocomposite, which showed better tooth-whitening efficacy stained with dyes, tea, and betel nuts compared with the H₂O₂ only (I-Hsuan et al., 2016). In addition, H₂O₂ produces an extremely

short lifetime of the active free radical. Therefore, to achieve a good bleaching effect, H_2O_2 must first penetrate into the teeth and quickly produce active free radicals. However, the Co/TPP/rGO nanocomposite can be used as a catalyst to produce more reactions between the staining molecules and H_2O_2 , which accelerate the bleaching process. In summary, graphene-based materials are a promising catalyst for tooth whitening application with proper types and concentrations.

Antibacterial Property

Bacterial biofilms formation plays an important role in the development of dental caries, periodontitis, and peri-implantitis (Berglundh et al., 2019; He et al., 2015; Kulshrestha et al., 2014; Slots, 2017; Ucja et al., 2017). Traditionally, antibiotics have been used for controlling the biofilms formation, whereas they faced a serious problem of antibiotic resistance, owing to the abuse of antibiotics. Many new methods for inhibiting the biofilms formation were explored. The antibacterial effect of graphene-based materials was firstly discovered by Hu et al. (Hu et al., 2010). Nowadays, more and more researchers have confirmed its effect in a various form.

Photodynamic therapy (PDT) is known as an alternative method for treatment of periodontitis and peri-implantitis. Pourhajibagher et al. investigated the effect of graphene quantum dot (GQD)-curcumin (Cur) on the perio-pathogen biofilms combined with PDT (Pourhajibagher et al., 2019). The production of reactive oxygen species (ROS) by GOD-Cur-PDT showed a dose-dependent tendency. In addition, the expression of *A. actinomycetemcomitans rcpA* gene, *P. gingivalis fimA* gene, and *P. intermedia inpA* gene was, respectively, reduced by 8.1-, 9.6-, and 11.8-fold. To improve the ICG photodynamic effect, Gholibegloo et al. fabricated the ICG-loaded GO, GO-Car, or GO-Car/HAp nanocomposites and investigated the antibacterial effect of *S. mutans* in planktonic forms and biofilms (Gholibegloo et al., 2018). Compared with the control group, GO, GO-Car, and GO-Car/HAp group decreased the survival of bacteria to 67%, 86.4%, and 78.2%, respectively. In preventing the biofilm formation of *S. mutans*, GO-Car group acquired the best effect. When treated with aPDT, the GO, GO-Car, and GO-Car/HAp group suppressed the biofilm formation up to 1.4%, 63.8%, and 56.8%, respectively. Then, the expression of *S. mutans gtfB* gene was decreased 6.0-, 9.0-, and 7.9-fold in GO, GO-Car, and GO-Car/HAp group, respectively, when without irradiation. Akbari et al. constructed the nano-GO (NGO)-ICG composite to enhance the efficiency of ICG (Akbari et al., 2017). The results showed that the NGO-ICG group achieved a significant decrease in the count of *E. faecalis* and significantly suppressed the formation of *E. faecalis* biofilms.

Besides, some researchers fabricated the graphene-based materials into GICs, PMMA, and dental adhesives to improve the physical properties and antibacterial ability (Bregnocchi et al., 2017; Lee J.-H. et al., 2018; Sun et al., 2018). Interestingly, Sun et al. evaluated the antibacterial effect of GIC/FG composites on *S. aureus* and *S. mutans*, showing that the highest antibacterial ability of FG (4 wt%) for *S. aureus* and *S. mutans* was 88.1% and 85.3%, respectively (Sun et al., 2018). Lee et al. constructed an nGO-PMMA and achieved a sustained antibacterial effect against

C. albicans over 28 days (Lee SM. et al., 2018). Bregnocchi et al. added the GNP into the dental adhesive with different content and 0.2% GNP group, showing a significant decrease on the *S. mutans* (Bregnocchi et al., 2017).

Jin et al. studied the antibacterial effect of Ti-GO-Ag *in vitro* and *in vivo* (Jin et al., 2019). The GO group significantly suppressed the bacterial activity of *S. mutans* and *P. gingivalis* with the increasing concentration after 24 h. Zhao et al. confirmed the antibacterial activity of GO on *S. mutans* (Zhao et al., 2020). Ioannidis et al. synthesized the Ag-GO composites, showing obviously decreased bacterial activity (Ioannidis et al., 2019). Qiu et al. testified that GO had excellent antibacterial properties against *S. aureus* and *E. coli* (Jiajun et al., 2017). Potential mechanisms were further analyzed, including nanoknives, wrapping or trapping, and ROS production. rGO was also used as an antimicrobial agent in suppressing *S. mutans* by Wu et al. (Wu et al., 2018).

Inhibition of the Growth of Fungal

Peri-implantitis is a common reason for the failure of dental implant. In addition, *Candida albicans* was found in the 31% peri-implantitis sites, which quickly attracted much attention (Schwarz et al., 2015). The species of *Candida albicans* in peri-implantitis patients were five times more than the health individuals (Alrabiah et al., 2019; Alsahhaf et al., 2019). Moreover, owing to the high resistant property of *Candida albicans*, the antifungal treatments are usually failure. The modification of dental implant coatings is a good method to prevent the formation of biofilms. Agarwalla et al. constructed a graphene nanocoating for twice (TiGD) and five times (TiGV) to evaluate the inhibition properties of *Candida albicans* biofilms (Agarwalla et al., 2020). According to XTT reduction assay, TiGD and TiGV group showed a lower absorbance compared with the control. Then, the colony-forming unit assay that displayed less viable yeast units on the TiGD and TiGV groups at all time points, indicating the inhibition effect of graphene on the fungal biofilm formations.

Biosensor for Biomarker Detection From Saliva

Dental disease diagnosis can reduce the mortality rates of some serious diseases and improve the quality of life of patients. Owing to its superior electrical and mechanical ability, graphene-based materials are widely used on dental disease diagnosis (Goldoni et al., 2021).

Detection of Bacterial and Viral Markers

In 2012, Mannoor et al. made the first graphene nano-sensors on tooth enamel (Mannoor et al., 2012). They fabricated a graphene sensing element with wireless readout coil attached to the silk fibroin and then transferred onto tooth enamel. The specific biological recognition was acquired by self-assembling AMP-graphene peptides onto the graphene. The reduction of electrical resistance displayed the binding of a single *E. coli* on the bare graphene nanosensor. The AMP-modified graphene nanosensor that showed a strong connection between peptides

and bacteria realized the detection and wireless remote monitoring of *Helicobacter pylori* in saliva. Gandouzi et al. build an electrochemical platform using rGO and gold nanoparticles, and the sensor showed high sensitivity to the markers (Islem et al., 2019). To diagnosis of periodontal disease in early stage, Lee et al. developed a sandwich-type biosensors to detect the human odontogenic ameloblast-associated protein (ODAM) (Wu et al., 2017). Chekin et al. fabricated an rGO/MoS₂ glassy carbon electrode for detecting the human papillomavirus type 16 (HPV-16), showing the high stability and storage performance (Chekin et al., 2018).

Detection of Drugs

Saliva is a body fluid that could be used to monitor the drugs and other harmful substances. The biosensor is a good way to detect the analytes of drugs and harmful substances. Graphene-based materials are applying to fabricate the portable biosensors. For example, Mohamed and his coworkers constructed a bio-sensing platform for detecting two drugs: the benzocaine and the antipyrine. To increase the selectivity of biosensor, they decorated the GO sheets with metal nanoparticles, achieving the high reproducibility and good selectivity (Mohamed et al., 2017). Parate and his coworkers modified the electrochemical biosensors with graphene to monitor the byproducts of smoke and tobacco with a wide linear range of 1–100 nM and the sensitivity of 1.89 μ A/decade (Parate et al., 2019).

Detection of Cancer Markers

Early diagnosis of disease is especially important for patients. Biomarker is a biological molecule which indicated the incidence of disease such as infections and cancers (Henry and Hayes, 2012). The overexpression of interleukin-8 (IL-8) has been reported to indicate the tumor progression in the oral cancer. Verma and his colleges fabricated a biosensor with rGO-modified ITO glass modified with rGO and then coated with Au NPs to detect IL-8 in saliva (Verma et al., 2017). The biosensor showed a high reproducibility and a long-term stability. After 3 months of dry storage, the retainment of biosensor is 94.3%. The performance of the biosensor was 91.8% even after 4 months of dry storage. To improve the performance of the biosensors, they also modified the GO with zinc oxide reduction and functionalized with IL-8 antibodies, showing that the sensitivity of the biosensor increased and the reproducibility was low with a RSD of 3.2% (Verma and Singh, 2019).

Owing to its excellent electrical properties, graphene-based appliances are reckoned as the gold standard in the biosensor fields. Nowadays, borophene has the similar anisotropic property with graphene (Tatullo et al., 2019b and Zavan et al., 2019). Song et al. had reported that, if the combination with borophene, graphene, and hydrogel in proper way, then it will improve the effect of implantable and wearable biosensors (Song et al., 2017). Therefore, when graphene combined with proper 2D nanomaterials, the efficiency of biosensors will be improved significantly. This may be also a good tendency in the development of graphene-based biosensors before the final clinical usage.

Prevention of Enamel and Dentin From Demineralization

White spot lesion (WSL) is one of the most common side effects of orthodontic treatment, which is caused by enamel surface demineralization (Bishara and Ostby, 2008; Nam et al., 2019). Therefore, it is of great significance to overcome WSL in the process of orthodontic treatment. Nowadays, many researchers are focusing on the studying of new bonding agent composites to prevent enamel demineralization caused by bacteria. Owing to the prominent antibacterial activity of GO, Lee and his colleges added GO to a bioactive glass (BAG) (Lee J.-H. et al., 2018). With the increase of GO concentrations, the length of anti-demineralization of the GO group increased. Besides, GO-containing groups also showed superior antibacterial effect after 24 and 48 h. The anti-demineralization mechanism of the composites may be attributed to the synergic effect of antibacterial effect of GO and the ion-releasing effect of BAG. In conclusion, GO is a promising addition in the anti-demineralization of enamel in proper style.

Dental caries and dental erosion were associated with the demineralization of dentin, which caused by acids from bacteria, food, and environments, leading to dentin hypersensitivity and pain (Addy, 2005). Nizami et al. synthesized five different functionalized GO nanocomposites and evaluated the biological and prevention of demineralization effects (Nizami et al., 2020). Compared with the control, the dentin slices coated with GO-Ag, GO-Ag-CaF₂, and GO-CaF₂ all exhibited superior prevention of decalcification. Besides, GO-Ag and GO-Ag-CaF₂ group showed better antibacterial activity compared with other groups, which may be related to the synergic effect of GO and Ag. Moreover, the color variation of f-GO coatings on the dentin surface is negligible, showing that GO is a promising dentin anti-demineralization resistant material.

Collagen Membranes

COL membrane has been widely used in guided bone regeneration (GBR) and guided tissue regeneration (GTR) as barrier membrane to hinder the soft tissue invasion of new bone (Chu et al., 2017a, Deng, and Sun et al., 2017; Elgali et al., 2017; Wessing et al., 2018). Although COL membrane has many good properties such as facilitated manipulation and less surgical intervention, it still needs various modifications to improve the biocompatibility (Chu et al., 2017b, Deng, and Hou et al., 2017). Marco et al. enriched the COL membranes with GO *via* a non-covalent functionalization by the interaction between oxygenated carbon functional parts and COL through hydrogen bonding (Marco et al., 2017). The membranes enriched with GO displayed lower deformability, increased roughness, and higher stiffness. The stability of GO in the COL membranes was evaluated, and there was no obvious GO dissolution found in the bulk solution compared with the control. After cultured on membranes with 2 and 10 μ g/ml GO for 3 days, the cell proliferations of hGFs were significantly higher than the control. With regard to the inflammatory response, the secretion of IL-6 and PGE2 showed significantly lower in cells cultured on the GO-coated membranes at day 3 compared with the control.

When it comes to DPSCs, Radunovic et al. confirmed the superior cell proliferations on the GO-coated membranes at days 14 and 28 (Li et al., 2015). Meanwhile, the expression of BMP2 on the GO-coated membranes showed higher at days 3 and 7, whereas the expression of RUNX2 and SP7 on the GO-coated membranes showed augmented after 21 and 28 days when compared with the uncoated membrane. Moreover, LDH assay also confirmed that there was no cytotoxicity of GO coating on the COL membrane. Although GO displayed superior effect on the cell growth, osteogenic differentiation, and inflammation response on the COL membrane, more studies *in vitro* and *in vivo* also needed to testify their definitive effect.

Drug Delivery

There is close interaction between bacteria and dental caries, and endodontic and periodontal diseases. Several groups of bacteria that require a common antibacterial strategy are usually involved. Amoxicillin (AMOX) is a kind of broad-spectrum antibiotic that is the first-choice antibiotic in the treatment of endodontic infection in Asian and European countries. In the conditional paste, the dose is not accurately controlled (Nan, 2016). Drug carrier can realize the gradual releasing of antibiotic drugs to easily achieve effective drug concentrations in the infected site. Trusek et al. found that GO had the potential in acting as a drug carrier especially in the therapy of dental inflammation (Trusek and Kijak, 2021). They linked the AMOX to GO using a peptide linker, which is Leu-Leu-Gly and then dispersed in the hydrogel. AMOX was released by enzymatic hydrolysis, showing the effective release of AMOX and the inhibition of bacteria strain growth.

CHALLENGES AND PERSPECTIVE

Graphene-based materials, the promising candidate for dentistry materials, have been widely used in dentistry research, owing to its cell differentiation and antibacterial property. This review summarized recent advances in expanding the types of graphene-based materials and the studies about dentistry-related properties, deepening the understanding of categories of graphene-based materials. Compared with other related studies, it displayed a quite comprehensive and detailed review about the great achievements in dental applications such as bone tissue engineering, coatings for dental implants, antibacterial properties, and COL membranes. Except for the usage in the tissue engineering, dental implant coatings, COL membrane, and adhesive, we also focused on some new fields such as drug delivery, prevention of enamel and dentin from demineralization, biosensor for oral biomarker detection, and inhibition of the growth of fungal. For the application of graphene nanomaterials in the biosensor, it could be used to detect bacterial and viral markers, drugs, and cancer markers. With the development of the application of graphene in dentistry, there are still some challenges remaining to be tackled until the final commercialized (Figure 9).

The Long-Term Cytotoxicity *in Vivo*

The excellent biomaterials should have a good biocompatibility without long-term cytotoxicity *in vitro* and *in vivo*. Because of the

limited understanding of graphene and its derivatives, a major challenge in clinical applications is the uncertainty of its cytotoxicity *in vitro* and *in vivo* and its potential mechanisms. Up to date, there is not an agreement on the cytotoxicity and potential hazards of graphene-based materials according to various studies. The factors that involved in the cytotoxicity include concentrations, surface functionalization, types of graphene family and synthetic methods, and the layer numbers. Many studies have focused on the dose dependent effect on the cytotoxicity, yet there is still no agreement for the upper limit concentration (Duch et al., 2011). When it comes to the mechanisms of cytotoxicity, ROS may play a critical role in it. When it comes to the synthetic methods, graphene films with CVD method were reckoned to be biocompatible without obvious cytotoxicity. However, when the graphene is dispersed in solution, the cytotoxicity of cells may increase, which may be caused by the accumulation or the sharp-edge penetration into the cells. Therefore, we expect to see more and more studies for long-term biocompatibility *in vivo* and *in vitro*.

The Method to Solve the Biodegradation

Another challenge of graphene-based materials is biodegradation, especially in the tissue engineering. With the formation of new tissue, the ideal biomaterial should be free of any toxic products. Up to date, there are limited literatures related to the biodegradation of graphene-based materials. Therefore, graphene-based material as an ideal biomaterial should be considered and explored to solve this problem.

The Defects Formed During the Production Process

Although the graphene used in the current study is a controlled and uncontaminated defect-free sample, the synthesis quality still should be highly examined when it was used in the clinic. Actually, the formed variety of unpredictable defects is mainly due to the differences in the synthesis methods. Once the defects occurred, the properties such as susceptibility and electronic structure will be changed (Riccardo et al., 2018). Therefore, the study of controlling the formation of defects during the graphene synthesis would be a big challenge but rewarding research areas.

Disturb the Cell Cycle

Little of the current studies are focused on the effect of GO on the cell cycle. Nowadays, Hashemi et al. innovatively focused on the effect of GO on the cell cycle (Hashemi et al., 2020). In the process of cell division, the synthesis of DNA is an important process. Certain mutagenic materials may cause the increased DNA synthesis in the S phase of cell cycle. In the study of Hashemi et al., GO increased the synthesis of DNA according to some underlying mechanisms such as damaged DNA, ROS production, and the double-strand breaks in the DNA. Cell apoptosis in mGO and nGO were greater, displaying a concentration and size-dependent effect. According to the result of cell cycle, there is a block occurred in the G₂/M phase in the GO groups. Thus, the

Dental applications	Challenges in the dental applications
Tissue engineering	<ul style="list-style-type: none"> • The long-term cytotoxicity in vivo • The biodegradation property • The defects formed in the production process
Adhesive, cements and resins	<ul style="list-style-type: none"> • The long term cytotoxicity in vivo
Anti-bacterial application	<ul style="list-style-type: none"> • The long-term cytotoxicity and genotoxicity
Biosensor for biomarker detection	<ul style="list-style-type: none"> • The methods about the functionalization of graphene sensors is needed to be explored
Coatings for implant and abutment	<ul style="list-style-type: none"> • The long-term cytotoxicity in vivo • The delamination of graphene coating • The defects formed in the production process
Collagen membrane	<ul style="list-style-type: none"> • The long-term cytotoxicity in vivo
Drug delivery	<ul style="list-style-type: none"> • Multi-antibiotics carriers for endodontic and periodontal diseases are uncertain
Teeth whitening	<ul style="list-style-type: none"> • The effect on the dental pulp sensitivity is uncertain
Prevention for demineralization	<ul style="list-style-type: none"> • Cytotoxicity in high concentrations • The effect on the vitality of dental pulp is confused

FIGURE 9 | Challenges on the different applications in the dental fields.

effect of GO on the cell cycle should be carefully considered and explored before the final clinical use.

The Delamination of Graphene Coatings

Although graphene has many advantages in the dental field, its clinical translation still needs to be carefully considered. Graphene-based materials had been used as coatings mostly in tissue engineering and dental implants surfaces. When used as the dental implant coatings, friction could cause the delamination of carbon-based coatings on the titanium with the loads over 400 mN (Rosa et al., 2021). Rosa et al. reported that there was no significant difference between the solid rigid polyurethane (SRP) and the control following the integrity of graphene nanocoatings by stimulating in the SRP and pig maxilla. However, there was a 35% decrease in the coverage area in ROI C from the bone group. Therefore, the delamination of graphene should be considered carefully (Agarwalla et al., 2019; Ming et al., 2018). How to improve the bonding strength of graphene-based materials and substrates is a question needed to be carefully investigated. Up to date, the methods of graphene-based materials coatings on the titanium surfaces are mainly based on the physical methods such as spin-coating techniques and layer-by-layer self-assembly methods. There are still technical difficulties in the chemical combinations with graphene and titanium. Compared with the chemical methods, the physical combination is weak and unstable. Therefore, the delamination of graphene coatings is a risk factor when used as

coatings. Some researchers had reported that titanium nanoparticles released from dental implants could cause the chronic inflammation on the soft and bone tissue around the dental implants. Therefore, when used graphene-based nanomaterials as coatings of dental implants, we should focus on the delamination of graphene coatings on the surrounding tissue inflammation.

The Improved Methods About the Functionalization of Graphene Sensors

When used as a biosensor, the large surface of graphene-based nanomaterial provided good adhesive conformability and the functionalization of graphene could be achieved by AMP-graphene peptide for biological recognition. However, there are different kinds of bacteria in the mouth. Therefore, more strategies should be made to recognize more bacteria, and the methods for the functionalization of graphene biosensor are quite important.

Single-Antibiotic Carrier for Endodontic and Periodontal Diseases

GO had been successfully used as a drug carrier for AMOX, which is a broad-spectrum antibiotic and could be used to control dental infections. However, the limitation is that whether two or more different drugs could be carried simultaneously is not sure and more studies are needed.

Eventually, graphene and its derivatives will be of great interest for a long time in the dental field. Although there are some limitations in the real clinical usage of dentistry, graphene, as a more reliable and more friendly biomaterial, can prompt more effective dental treatments in the near future.

The Unfavorable Antibacterial Effect on the Polymicrobial Biofilms

Although there are many studies focused on the antibacterial effect of graphene-based materials on the single strain of bacteria or monoclonal biofilm, yet no study revealed the antibacterial effect on the mature polymicrobial biofilms. On the basis of the above limitations, there is still a long way before the final clinical usage of graphene-based materials in the dental fields.

CONCLUSION

All acronyms and abbreviation used in the text are explained in **Table 2**. Just as we know, there are many advantages of graphene-based materials for the dental fields. However,

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- many challenges also existed and need to be solved. All in all, we should confirm that the usage of graphene-based nanomaterials in dental fields deserved to be deeply studied and it can bring a quite new dental treatment concept in the near future.

AUTHOR CONTRIBUTIONS

XL and XLi contributed equally to this review paper. LH, BZ, and XL conceived the content of paper. XL, LH, and XLi wrote the paper. YW, DW, HX, and MT took part in the collecting some related papers. XL draw all the flow charts. All authors reviewed and commented on the manuscript.

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