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## EDITED BY

Dumitru Trucu,  
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## REVIEWED BY

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Kanazawa Medical University, Japan  
Arran B. J. Hodgkinson,  
Queen's University Belfast, United Kingdom

## \*CORRESPONDENCE

Erin Munro Krull  
✉ munrokrulle@ripon.edu

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# Why strengthening gap junctions may hinder action potential propagation

Erin Munro Krull<sup>1\*</sup> and Christoph Börgers<sup>2</sup>

<sup>1</sup>Department of Mathematical Sciences, Ripon College, Ripon, WI, United States, <sup>2</sup>Department of Mathematics, Tufts University, Medford, MA, United States

Gap junctions are channels in cell membranes allowing ions to pass directly between cells. They are found throughout the body, including heart myocytes, neurons, and astrocytes. In cardiac tissue and throughout the nervous system, an action potential (AP) in one cell can trigger APs in neighboring cells connected by gap junctions. It is known experimentally that there is an ideal gap junction conductance for AP propagation—lower or higher conductance can lead to propagation failure. We explain this phenomenon geometrically in branching networks by analyzing an idealized model that focuses exclusively on gap junction and AP-generating currents. As expected, the gap junction conductance must be high enough for AP propagation to occur. However, if the gap junction conductance is too high, then it dominates the cell's intrinsic firing conductance and disrupts AP generation. We also identify conditions for *semi-active* propagation, where cells in the network are not individually excitable but still propagate action potentials.

## KEYWORDS

gap junctions, excitability, excitable tissue, action potential propagation, cardiac tissue, safety factor, reaction-diffusion

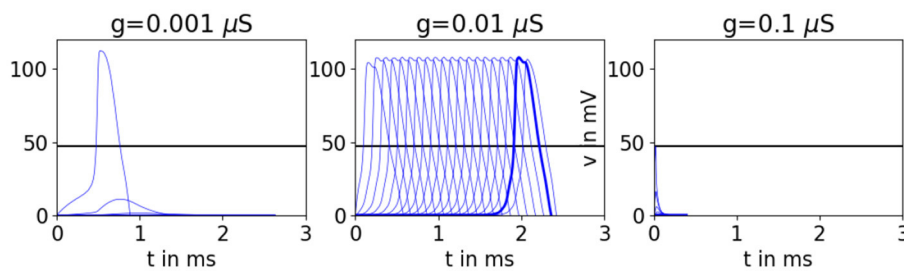
## 1 Introduction

Gap junctions are found throughout the body [1–3]. In particular, gap junctions connect astrocytes [4], neurons [5–8], especially during development [9, 10] and heart myocytes [11–13]. More recently, gap junctions were observed in cancer cells [14, 15] and between soma and germline cells [16].

Gap junctions allow ions to pass between cells, and so the voltage in one cell directly influences the voltage in the neighboring cell. Suppose two excitable cells are connected, a “trigger” cell and a downstream neighbor, and both are at rest. If there is a small voltage deflection in the trigger cell, then we will see a proportional deflection in the neighbor. This proportion is often referred to as the coupling coefficient [17]. If the gap junction conductance is low, then an action potential (AP) in the trigger cell may only yield a subthreshold response in the neighbor. This response is called passive propagation since the neighbor's firing currents are never fully activated. On the other hand, if the gap junction conductance is high, then an AP in the trigger cell may yield an AP in the neighbor. We call this active propagation since the neighbor's firing currents amplify the response.

Active propagation of APs across gap junctions is seen in cardiac tissue [11–13] and throughout the nervous system [18–25]. More recently, gap junctions were found to mediate propagating calcium waves through smooth muscle tissues [26], neural progenitor cells [27], possibly astrocytes [28–30], and retinal cells [31].

Several studies have reported that APs propagate most easily across a given network for intermediate gap junction conductances; see [Figure 1](#). Experiments in heart tissue



**FIGURE 1**  
 Simulations of Hodgkin-Huxley-type neurons [39] connected by gap junctions in a 20-layer tree network where each cell has one upstream neighbor and two downstream neighbors. The lead cell is stimulated until its voltage reaches approximately 1/2 the AP height of an unconnected cell, marked by a black horizontal line. (See section 4 for simulation details.) We see propagation failure when the gap junction conductance  $g$  is either too high or too low, and AP propagation when  $g$  is set to a medium amount.

show that reducing the gap junction conductance can allow APs to propagate through expanding tissue [12, 32, 33]. These results are corroborated in computational models of heart tissue, which show that there is an ideal gap junction conductance that maximizes the number of downstream neighbors that APs may propagate across [34] and that maximizes the “safety factor,” a measure of ease of propagation in terms of source-sink mismatch [34–38].

To understand these results, we consider a network of cells connected by gap junctions with possibly many downstream neighbors. If the gap junction conductance between cells is zero, clearly APs cannot propagate through the network. As the gap junction conductance is raised, propagation becomes possible. However, if the conductance is raised too much, current shunted to downstream neighbors may prevent APs from propagating.

Extending the study in [40] and [41], we use a one-dimensional simplification of the FitzHugh-Nagumo equations to analyze when active AP propagation is possible in branching networks. In particular, our framework explains why increasing gap junction conductance may hinder AP propagation beyond pointing to a source-sink mismatch: AP propagation is the easiest when the total gap junction conductance is large enough to overcome the cell’s intrinsic conductance below the firing threshold, but small enough to not interfere with the cell’s conductance above the firing threshold. We illustrate this phenomenon for AP propagation into a single cell and branching networks. We then verify that our conclusions hold qualitatively for more realistic biophysical models. Our analysis also predicts that if the gap junction conductance reaches a threshold, we may see semi-active propagation where individual cells in the network cannot fire an AP independently from their neighbors, but the network can still propagate APs.

## 2 Propagation into a single cell

### 2.1 Model of a single cell

We model a single cell using the equation

$$\frac{dv}{dt} = v(v - v_T)(1 - v) \tag{1}$$

where  $v_T$  is a parameter with  $0 < v_T < 1$ . We let  $F(v)$

stand for the right-hand side of Eq. (1), illustrated in Figure 2. We think of  $v$  as a non-dimensionalized membrane potential and will therefore refer to it as *voltage*. We also think of  $F(v)$  as the inward activation current (more accurately, current divided by capacitance) and therefore may interpret  $F'(v)$  as the intrinsic conductance of the cell. Equation (1) is one half of the FitzHugh-Nagumo model [42]. We omit the other half, the slow variable that drives  $v$  down when it is high. Our focus, for now, is on the *initiation*, not on the *termination* of spikes. Single cell simulations in the [Supplementary material](#) show that slow gating variables do not appreciably change during AP initiation.

Equation (1) has a stable equilibrium at  $v = v_R = 0$ , an unstable one at  $v = v_T$  representing the intrinsic threshold, and a stable one at  $v = v_F = 1$  representing the AP firing voltage. If  $v$  is perturbed slightly from 0, it returns to 0, but if it is raised above  $v_T$ , it rises further to 1 instead. While we technically have a bi-stable differential equation, since we are using this model to focus on AP initiation, we still think of this as a model for excitability. In this study, *excitability* always means the co-existence of a stable resting state and an unstable *threshold*, with the property that perturbation away from the stable resting state and past the threshold results in a large excursion to the *AP firing voltage*. Once the voltage reaches the AP firing voltage, we assume the recovery currents of the full FitzHugh-Nagumo model would take the voltage back to rest.

The graph of  $F$  has a local minimum  $v_{\min}$  and an inflection point at  $v_i = (v_T + 1)/3$ . We assume  $v_T < v_i$ , which is equivalent to

$$v_T < \frac{1}{2}.$$

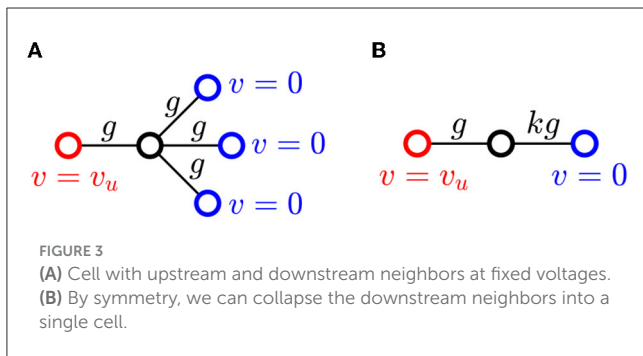
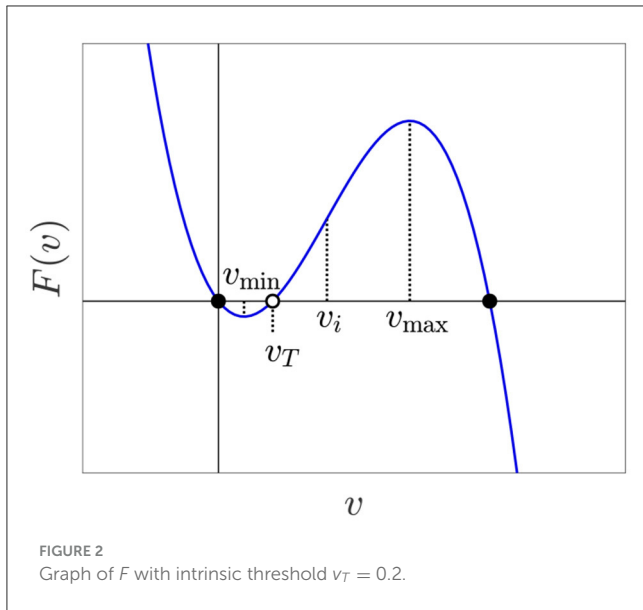
For neurons and myocytes, this is a natural assumption: The firing threshold is closer to the resting voltage ( $v = 0$ ) than to the peak voltage ( $v = 1$ ). So

$$v_{\min} < v_T < v_i$$

as illustrated in Figure 2.

### 2.2 Gap junction connections with neighbors held at fixed voltage

Consider a cell described in the previous section that is connected by gap junctions to one *upstream* neighbor with voltage



$v_u$  and  $k$  downstream neighbors with voltage  $v_d = 0$ . The upstream and downstream voltages are assumed fixed for now. Only the central cell has dynamics. Simulations (not shown) verify that the assumption  $v_d = 0$  is reasonable as long as the central cell's voltage is below threshold. We assume that all gap junction conductances have the same strength  $g$ , and stimulation comes from the upstream neighbor. See Figure 3 for an illustration with  $k = 3$ .

Our model now becomes

$$\frac{dv}{dt} = v(v - v_T)(1 - v) + g(v_u - v) - gkv. \tag{2}$$

As is customary, we assume here that gap junctions are governed by Ohm's law—current is proportional to voltage difference. The term  $g(v_u - v)$  models the effect of the upstream cell and  $-gkv$  models the effect of the downstream cells. With the notation

$$G(v) = g(k + 1)v - gv_u, \tag{3}$$

Eq. (2) becomes

$$\frac{dv}{dt} = F(v) - G(v).$$

Figure 4A shows  $F$  and  $G$  in one figure. The graph of  $G$  intersects the horizontal axis at  $(v_u/(k + 1), 0)$ , and the vertical axis at  $(0, -gv_u)$ .

In general, there may be more upstream cells than just one. There may also be more or fewer downstream cells coupled to the central cell with varying conductances. What matters is that  $g$  is the total gap junction conductance of connections between the central cell and upstream cells and  $kg$  is the total gap junction conductance of connections between the central cell and downstream cells. Therefore, we will not assume  $k$  to be an integer any more, simply thinking of it as the ratio of total downstream conductance over total upstream conductance.

### 2.3 All neighbors at rest

We first discuss the equilibria of the central cell when the upstream neighbors of the central cell are at rest ( $v_u = 0$ ) just like the downstream neighbors. The formula for  $G(v)$  is now

$$G(v) = g(k + 1)v.$$

Fixed points of Eq. (2) are solutions of

$$F(v) = G(v). \tag{4}$$

If  $g(k + 1)$  is not too large, then there are three equilibria, depicted in the left panel of Figure 4B. As  $g(k + 1)$  increases, the graph of  $G$  becomes steeper. This raises the threshold  $v_t$  and lowers the AP firing voltage  $v_f$  but does not affect the resting voltage. Eventually, the threshold and firing equilibrium points collide at a voltage which we denote by  $v_E$ ; see the middle panel of Figure 4B. For larger  $g(k + 1)$ , there is only one equilibrium at  $v = 0$ .

We say that the cell is *excitable* if there are three equilibria—an unstable threshold surrounded by two stable equilibria. This is consistent with the common notion of an excitable cell, where a small deflection in voltage across a threshold can cause a large excursion to a much higher voltage. Hence, the cell is excitable if

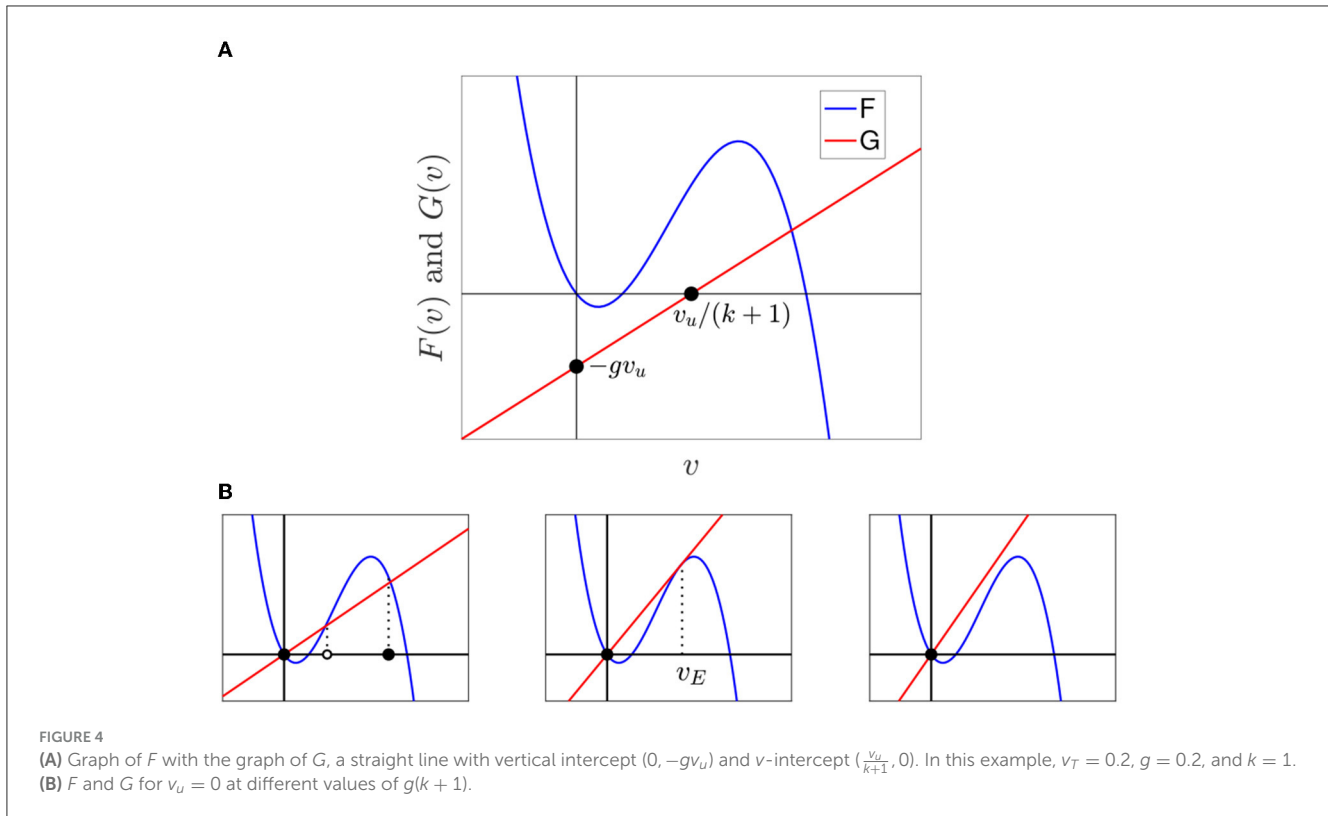
$$g(k + 1) < F'(v_E) \tag{5}$$

and is not for higher values of  $g(k + 1)$ . So gap junction connections with neighbors held at rest, if they have high conductance or are numerous enough, can make excitability disappear altogether. We will see below that non-excitable cells can still amplify a response—just not independently from other cells.

### 2.4 Firing triggered by raising the upstream voltage

As  $v_u$  is raised from 0 to some maximum value  $V_u > 0$ , the graph of  $G$  moves downward. Depending on the values of  $V_u$ ,  $k$ , and  $g$ , the threshold and resting voltages may eventually collide and annihilate each other in a saddle-node bifurcation, leaving the AP firing voltage as the only equilibrium. We let  $v_{u,c}$  be the bifurcation point, where  $v_{\min} < v_{u,c} < v_i$ ; see Figure 5A.

As the right panel of Figure 5A shows, even when the central cell is not excitable because it is too strongly connected to resting



neighbors, raising  $v_u$  may restore excitability by making the threshold and AP firing voltage equilibria re-appear via a saddle-node bifurcation. Then, at  $v_u = v_{u,c}$ , the resting and threshold equilibria collide and disappear.

**Definition 1.** We say that the central cell *fires* or has a *firing response* when  $v_u$  rises from 0 to  $V_u$  if there is a saddle-node bifurcation between the rest and threshold fixed points at some critical value  $v_u = v_{u,c}$  with  $v_{\min} < v_{u,c} < v_i$ .

**Definition 2.** The *critical segment* is the segment between  $v = v_{\min}$  and  $v = v_i$  on the graph of  $F$ .

The left panel of **Figure 5B** shows the critical segment in bold. The collision between the rest and threshold fixed points must occur on the critical segment. Therefore, the following proposition holds.

**Proposition 1.** Let  $g > 0$  and  $k \geq 0$ . The central cell fires when  $v_u$  is raised from 0 to  $V_u$  if and only if  $L_{g,k}$  (the graph of  $G$  with  $v_u = V_u$ ) satisfies the following two conditions.

- (1)  $L_{g,k}$  lies strictly below the critical segment
- (2)  $L_{g,k}$  has slope  $< F'(v_i)$ .

We say  $L_{g,k}$  is *admissible* if it satisfies the conditions in Proposition 1, as illustrated in the left panel of **Figure 5B**.

## 2.5 Region in $(g,k)$ -plane with firing response

We use Proposition 1 to derive a detailed description of the set of the parameter pairs  $(g, k)$  for which the central cell has a firing response. First, we note that  $L_{g,k}$  cannot be admissible if  $V_u \leq v_T$ . We will therefore assume

$$v_T < V_u.$$

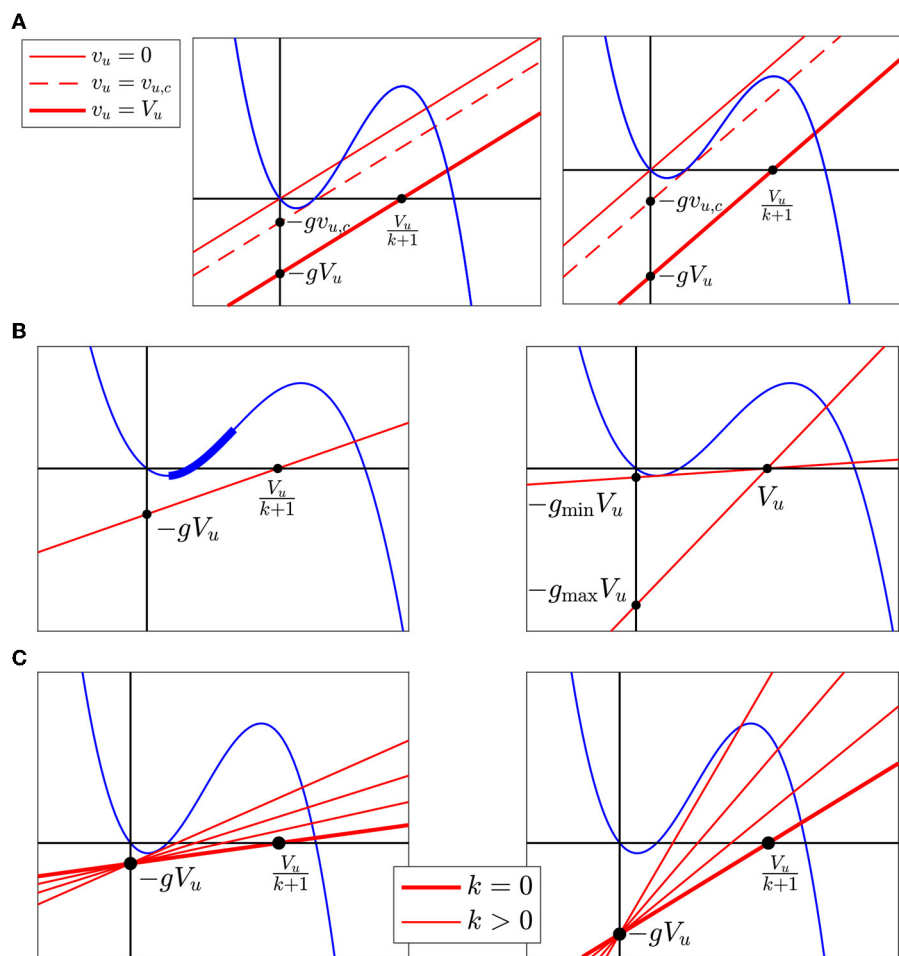
Furthermore, since lowering  $k$  rotates  $L_{g,k}$  clockwise around the point  $(0, -gV_u)$ , lowering  $k$  makes it easier to fire: For  $L_{g,k}$  to be admissible for a given  $g$ ,  $L_{g,0}$  has to be admissible (this makes sense, since lowering  $k$  lowers the current shunted to the downstream neighbors). Therefore, we first analyze the case  $k = 0$ . Note that  $L_{g,0}$  passes through  $(V_u, 0)$ . For  $L_{g,0}$  to be admissible,  $g$  must satisfy

$$g_{\min} < g < g_{\max}$$

where  $L_{g_{\min},0}$  is tangent to the critical segment and  $L_{g_{\max},0}$  has slope  $F'(v_i)$ , as illustrated by the right panel of **Figure 5B**. Since the slope of  $L_{g,0}$  is  $g$ , then  $g_{\max} = F'(v_i)$ .

Now, we consider  $k > 0$ . Suppose  $g$  lies between  $g_{\min}$  and  $g_{\max}$ . Then,  $L_{g,0}$  is admissible. Other admissible lines, for the same value of  $g$ , are obtained by rotating this line around the point  $(0, -gV_u)$  in the counter-clockwise direction until it touches the critical segment or reaches slope  $F'(v_i)$ —whichever comes first.

Which of these two does come first depends on  $g$ . If  $g$  is smaller than some threshold value  $g_*$  (discussed further below), then as the line rotates counter-clockwise around  $(0, -gV_u)$ , it touches the critical segment before it reaches slope  $F'(v_i)$ ; see the left panel of



**FIGURE 5**  
**(A)** Raising  $v_u$  shifts the graph of  $G$ . **(B)** The left panel shows an example of an admissible line  $L_{g,k}$ . The *critical segment* is the bold blue segment along  $F$ . The right panel shows the lines  $L_{g,k}$  for the minimum and maximum values of  $g$  allowing a firing response. Both occur when  $k = 0$ . **(C)** The left panel shows an example where the maximum  $k$  occurs when  $L_{g,k}$  is tangent to the graph of  $F$ . The right panel shows an example where the maximum  $k$  occurs when  $L_{g,k}$  reaches  $F'(v_i)$ .

**Figure 5C.** If  $g$  is larger than  $g_*$ , the line reaches slope  $F'(v_i)$  before it touches the critical segment; see the right panel of the figure.

From **Figure 5C**, we see that  $g_*$  is determined by the tangent to  $F$  at  $(v_i, F(v_i))$ , which intersects the vertical axis at  $-g_*V_u$ . That is,

$$F'(v_i) = \frac{F(v_i) + g_*V_u}{v_i}, \quad \text{or}$$

$$g_* = \frac{F'(v_i)v_i - F(v_i)}{V_u}. \quad (6)$$

Is it possible that  $g_* \geq g_{\max} = F'(v_i)$ ? According to (6), this means

$$\frac{F'(v_i)v_i - F(v_i)}{V_u} \geq F'(v_i)$$

or

$$V_u \leq v_i - \frac{F(v_i)}{F'(v_i)}. \quad (7)$$

The right-hand side of this inequality is the  $v$ -intercept of the tangent to  $F$  at  $(v_i, F(v_i))$ . So,  $g_* \geq g_{\max}$  only if  $V_u$  happens to be very small, just above  $v_T$ .

For every  $g \in (g_{\min}, g_{\max})$ , the slope  $g(k+1)$  of the admissible line  $L_{g,k}$  is bounded above and the upper bound on  $g(k+1)$  translates into an upper bound on  $k$ . So, the parameter regime where there is a firing response is of the form

$$g_{\min} < g < g_{\max}, \quad 0 \leq k < k_{\max}(g),$$

and our next goal will be to understand what the graph of the function  $k_{\max}$  looks like.

When  $g_* \leq g < g_{\max}$ , the constraint on the slope of  $L_{g,k}$  is  $g(k+1) < F'(v_i)$ , and therefore

$$k_{\max}(g) = \frac{F'(v_i)}{g} - 1. \quad (8)$$

For  $g_{\min} < g < g_*$ ,  $k_{\max}(g)$  is obtained by computing the  $k$  where  $L_{g,k}$  is tangent to the critical segment. The two pieces match up



continuously at  $g_*$ , and we set

$$k_* = k_{\max}(g_*).$$

Our conclusions are summarized in Figure 6A. When  $V_u$  is so small that  $g_* \geq g_{\max}$ , the dashed part of the blue boundary in Figure 6A is simply absent. The dotted and dashed parts of the upper boundary of the blue region in Figure 6A fit together continuously but not differentiably.

In Figure 6A, we also indicate the regions in the  $(g, k)$ -plane, where the central cell is excitable when the upstream cell is at rest ( $v_u = 0$ ). From Eq. 5, the boundary of this region is defined by

$$k < \frac{F'(v_E)}{g} - 1. \tag{9}$$

We let  $k_{\text{exc}}(g)$  stand for the right-hand side of (9) and describe how excitability affects behavior in more detail in section 2.7.

## 2.6 Ideal gap junction conductance

In Figure 6A, we see that  $k_{\max}(g)$  reaches a maximum point at  $(g_{\text{peak}}, k_{\text{peak}})$  at some  $g \in (g_{\min}, g_*)$ . We also see that for all  $k < k_{\text{peak}}$ , as  $g$  increases AP propagation will first appear and then disappear as illustrated in Figure 1. To understand precisely how  $(g_{\text{peak}}, k_{\text{peak}})$  corresponds to our model, we will examine what happens to  $L_{g,k}$  when it is tangent to the critical segment. In particular, we will follow what happens to the  $v$ -intercept  $(V_u/(k_{\max}(g) + 1))$  as  $g$  increases. As shown in Figure 6B, initially, the  $v$ -intercept falls as  $g$  increases until it reaches  $v_T$ . As  $g$  continues to increase, the  $v$ -intercept rises again. Therefore,  $k_{\max}$  rises until the  $v$ -intercept reaches  $v_T$  and then falls. We can solve for  $(g_{\text{peak}}, k_{\text{peak}})$  by setting  $V_u/(k_{\text{peak}} + 1) = v_T$ , and therefore

$$k_{\text{peak}} = \frac{V_u}{v_T} - 1. \tag{10}$$

and since  $g_{\text{peak}}(k_{\text{peak}} + 1) = F'(v_T)$ ,

$$g_{\text{peak}} = \frac{F'(v_T)}{k_{\text{peak}} + 1} = \frac{F'(v_T)v_T}{V_u}. \tag{11}$$

In other words, AP propagation is the easiest when the total conductance  $g(k + 1)$  is the same as the cell's intrinsic conductance when  $v = v_T$ . At lower conductances, the gap junction current may not overcome the cell's current below threshold. At higher conductances, the gap junction current may interfere with the cell's firing currents.

## 2.7 Active, semi-active, and passive propagation

In Figure 6A, we see several distinct regions defined by  $k_{\max}(g)$  and  $k_{\text{exc}}(g)$ . Notably,  $k_{\text{exc}}(g)$  intersects  $k_{\max}(g)$  so that a cell may fire without being excitable. Here, we describe these parameter regions.

**Definition 3.** The *propagation region* is the region of parameter pairs  $(g, k)$  with  $0 \leq k < k_{\max}(g)$ . The *active propagation region* is the section of the propagation regions where  $k < k_{\text{exc}}(g)$ , while the *semi-active propagation region* is the section where  $k \geq k_{\text{exc}}(g)$ . The *passive propagation region* is the region where  $k \geq k_{\max}(g)$ .

When  $(g, k)$  lies in the active propagation region (illustrated in Figure 6A where the red and blue regions overlap), the central cell is excitable for  $v_u = 0$  and fires when  $v_u$  is set to  $V_u$ . When  $(g, k)$  lies in the semi-active propagation region, the central cell is not excitable for  $v_u = 0$ , but as  $v_u$  rises from 0 to  $V_u$ , first excitability is restored, and then there is a firing response. In the passive propagation region, raising  $v_u$  from 0 to  $V_u$  still causes the voltage of the central cell to rise but does not trigger firing.

To illustrate the difference between the three parameter regions, Figure 7A shows solutions of (2) with  $v(0) = 0$  and

$$v_u = \begin{cases} 1 & \text{for } 0 \leq t \leq 30 \\ 0 & \text{for } t > 30. \end{cases}$$

In the active propagation region, the central cell's voltage rises and converges to the AP firing voltage, indicating an AP would occur in the full FitzHugh-Nagumo model. (Recall that our model includes no explicit mechanism for bringing the voltage back down after firing.) In the semi-active propagation region, the central cell's voltage also rises but drops back down to rest once  $v_u$  is set back to 0—no matter how high the central cell's voltage gets. In the passive propagation region, the voltage rises much less and returns to zero soon after  $v_u$  is switched back to zero.

## 2.8 AP height can depend discontinuously on $g$ and $k$

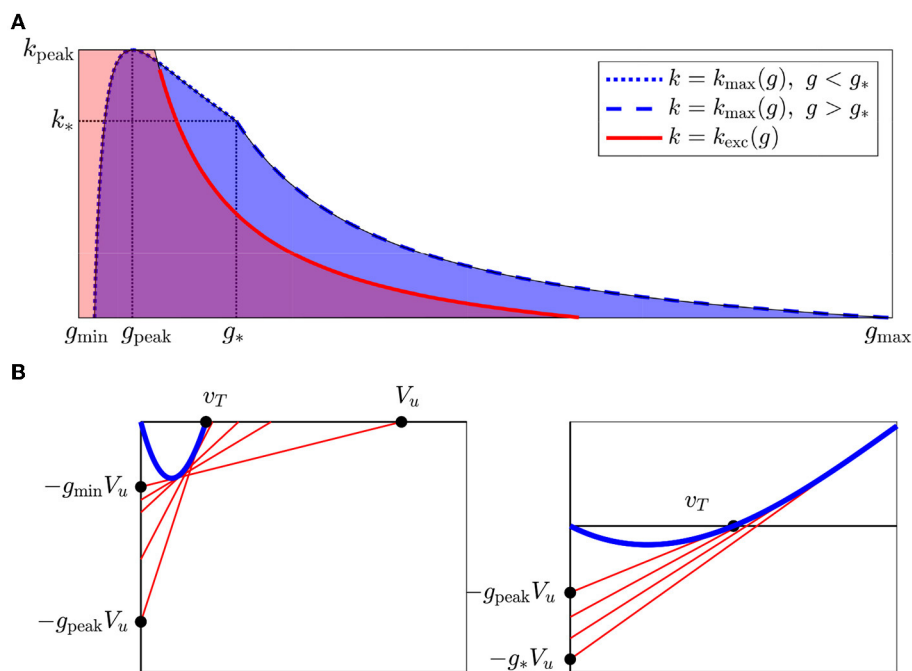
For  $g > 0$  and  $k \geq 0$ , let  $v = v(t)$  be the solution of (2) with  $v_u = V_u$  and  $v(0) = 0$ . Let

$$v_\infty = \lim_{t \rightarrow \infty} v(t). \tag{12}$$

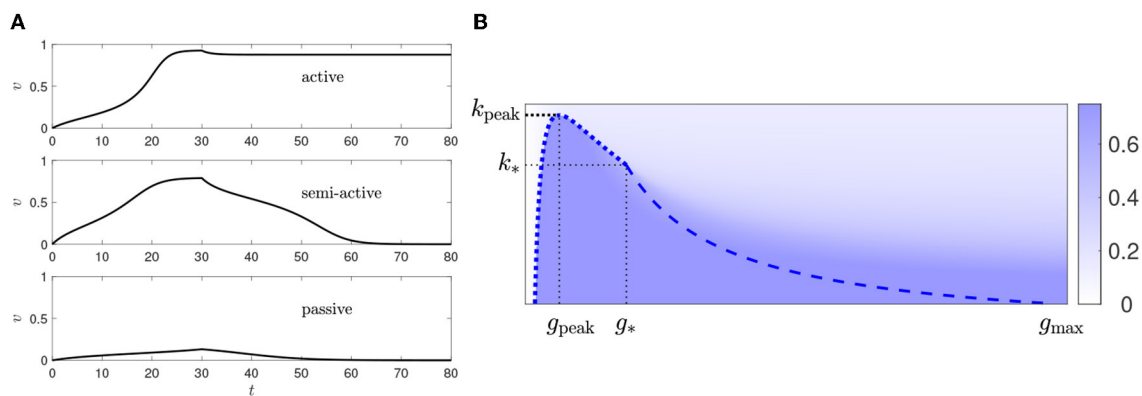
In other words,  $v_\infty$  is the voltage obtained by setting the voltage in the upstream cell to  $V_u$ , letting the voltage in the central cell equilibrate, starting at  $v = 0$ ; so,  $v_\infty$  is the smallest equilibrium. We view  $v_\infty$  as a function of  $g$  and  $k$ , as illustrated in Figure 7B. Notably, there is a discontinuous jump along the boundary defined by  $k_{\max}$  (the dotted blue curve). This boundary is discontinuous in general, as stated in the following theorem.

**Theorem 1.**  $v_\infty(g, k)$  has jump discontinuities at parameter pairs  $(g, k)$  with  $g_{\min} \leq g < g_*$  and  $k = k_{\max}(g)$  and is continuous everywhere else.

*Proof.* Let  $g > 0$  and  $k \geq 0$ . As before, denote by  $L_{g,k}$  the graph of  $G$  with  $v_u = V_u$ . Then,  $v_\infty(g, k)$  is the  $v$ -coordinate of the left-most intersection point of  $L_{g,k}$  and the graph of  $F$ . As illustrated in Figure 5A,  $v_\infty$  depends discontinuously on  $(g, k)$  if and only if  $L_{g,k}$  is tangent to the graph of  $F$  along the critical segment. The  $(g, k)$  for which  $L_{g,k}$  is tangent to the graph of  $F$  at the critical segment are precisely the ones that define  $k_{\max}(g)$  where  $g < g_*$ .



**FIGURE 6** (A) Firing occurs in the region in the  $(g, k)$ -plane below  $k_{\max}$  (blue), and the region where the cell is excitable with all neighbors at rest is below  $k_{\text{exc}}$  (red).  $v_T = 0.15, V_u = 1$ . (B) As  $g$  increases from  $g_{\min}$  to  $g_*$ , the  $v$ -intercept of the tangent through  $(0, -gV_u)$  first moves left (left panel), then right (right panel). Therefore,  $k_{\max}(g)$  first increases until  $\frac{V_u}{k+1}$  reaches  $v_T$  and then decreases.



**FIGURE 7** (A) Responses to setting  $v_u = 1$  for  $0 \leq t \leq 30$  and then setting it back to 0, for  $k = 2$  and  $g = 0.03$  (top),  $g = 0.07$  (middle), and  $g = 0.01$  (bottom). (B) Heat plot of  $v_{\infty}$  as a function of  $g$  and  $k$  for  $v_T = 0.15, V_u = 1$ . The blue curves are from Figure 6A. We see that  $v_{\infty}$  is discontinuous along the dotted blue curve but not along the dashed blue curve.

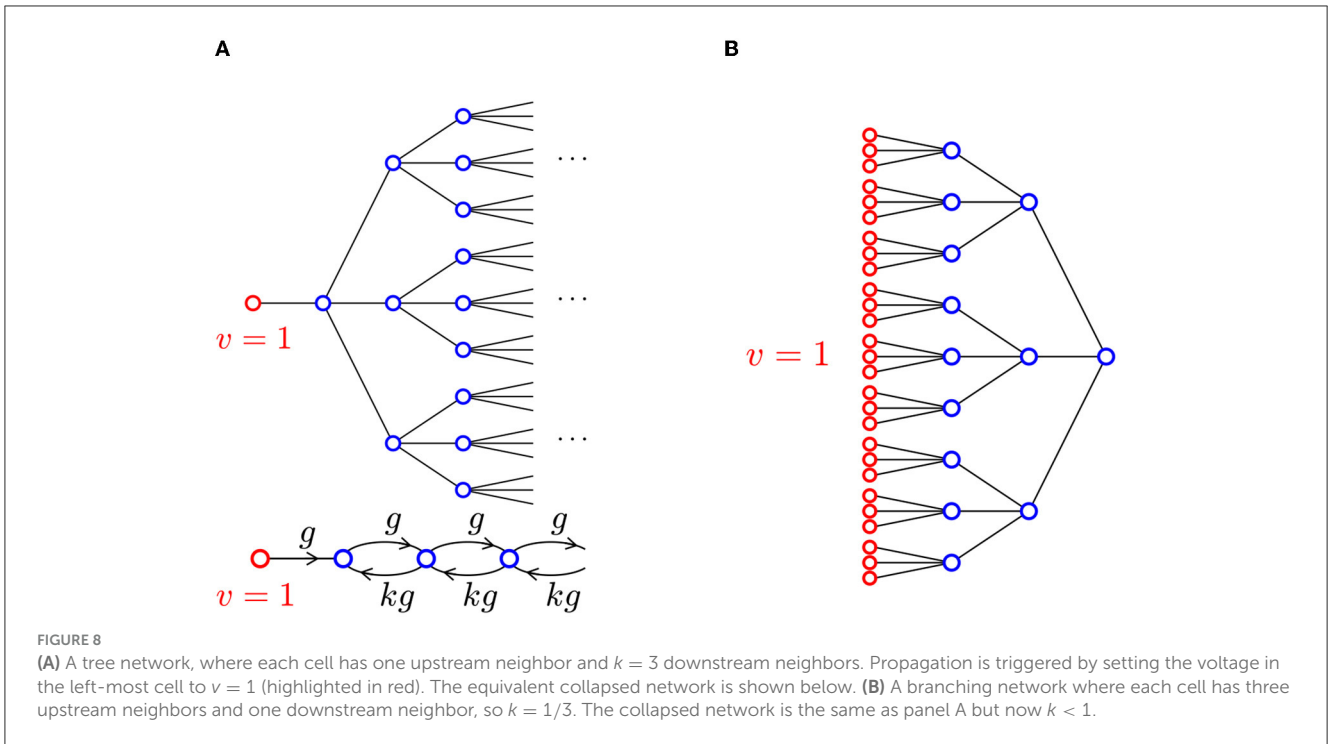
### 3 Propagation through branching networks

#### 3.1 Model

For motivation, first think about AP propagation through a tree of cells connected by gap junctions, as shown in Figure 8A. Assume that the cells are identical and each cell has exactly one upstream and  $k$  downstream neighbors.

Propagation is triggered by raising the voltage of the leftmost cell to  $v = 1$ .

By symmetry, the voltages in cells that are vertically aligned in Figure 8A are identical. We therefore collapse vertically aligned cells into a single cell and obtain the equivalent chain shown at the bottom of Figure 8A. In this chain, gap junction conductances are not symmetric:  $g$  for upstream connections and  $kg$  for downstream connections.



As we did earlier, we now drop the assumption that  $k$  is an integer, viewing it more abstractly as the ratio of downstream conductance over upstream conductance. We even allow  $k$  to be less than 1. This models a situation in which a signal originates from a large array of cells, propagating into a narrowing network: Think of a signal propagating through a tree from the tips of the outermost branches to the root, as shown in Figure 8B. We therefore consider the collapsed chain in Figure 8A as a mathematical idealization of many different kinds of branching networks.

We make the additional simplification that each cell responds only to the voltage upstream of it and behaves as though its downstream neighbors were held at zero voltage; its voltage therefore rises to  $v_\infty$ , as defined in Eq. 12. Propagation through the chain amounts to iterating the map

$$\varphi: v_u \mapsto v_\infty,$$

which maps  $[0, 1]$  into  $[0, 1]$ .

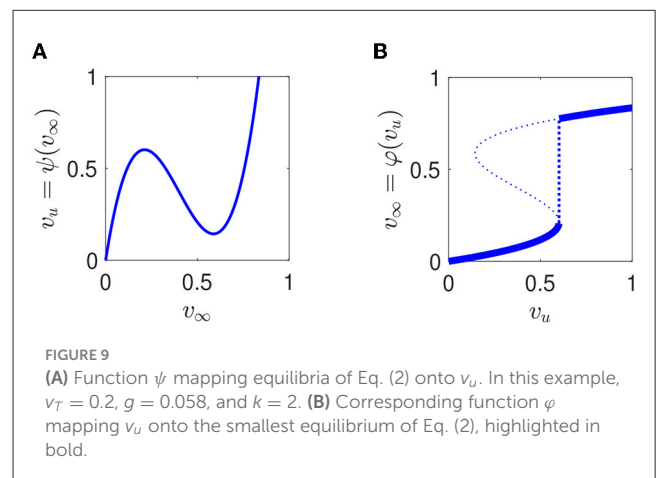
### 3.2 AP propagation determined by sequence of max voltages

A complication in our analysis is that the map  $\varphi$  need not be continuous. To see this, first note that for any equilibrium  $v_\infty$  of eq. (2), that is, for any solution  $v_\infty$  of

$$F(v_\infty) + g(v_u - v_\infty) - gkv_\infty = 0,$$

we can solve for  $v_u$  in terms of  $v_\infty$ :

$$v_u = -\frac{F(v_\infty)}{g} + (k + 1)v_\infty.$$



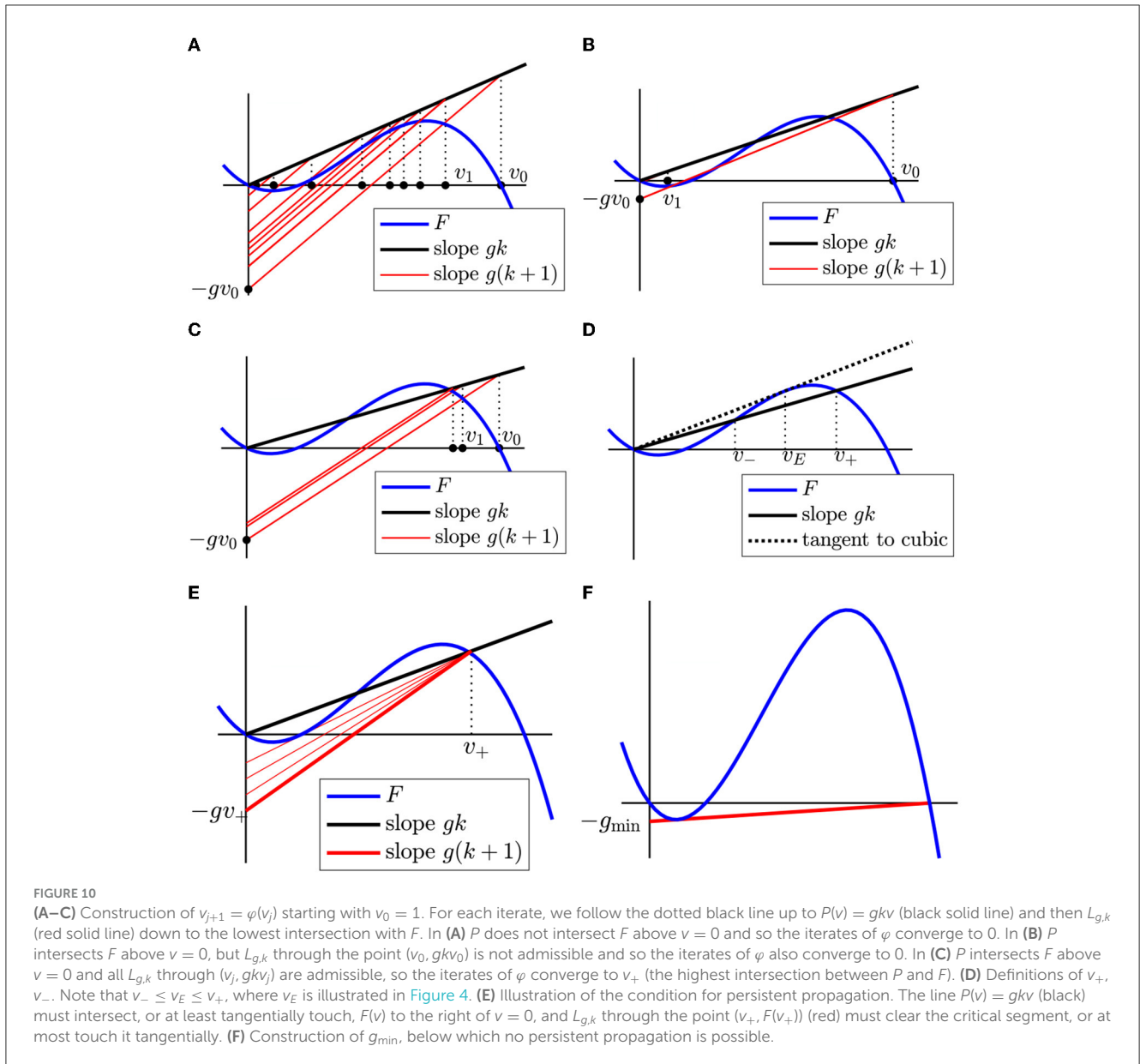
We denote the right-hand side of this equation by  $\psi(v_\infty)$ ; Figure 9A shows an example. The graph of  $\varphi$  is obtained by swapping the  $v_\infty$ - and  $v_u$ -axes, and using the minimum value of  $v_\infty$  for a given  $v_u$  when there is ambiguity; see Figure 9B.

Because of the discontinuity, we will not use the standard theory of iterated one-dimensional maps to understand the effect of iterating  $\varphi$ , but explicitly construct the iterates. Starting with  $v_0 = 1$ , we define  $v_1, v_2, \dots$  by  $v_{j+1} = \varphi(v_j)$  and  $j = 0, 1, 2, \dots$ . Given  $v_j$ ,  $v_{j+1}$  is the smallest solution of  $F(v) + g(v_j - v) - gkv = 0$  or

$$F(v) = g(k + 1)v - gv_j. \tag{13}$$

The graph of the right-hand side of this equation is the line  $L_{g,k}$  with  $V_u = v_j$ , which passes through the point  $(v_j, gkv_j)$ . To find  $v_{j+1}$  from  $v_j$ , we first draw the line  $P(v) = gkv$  as a reference and





**FIGURE 10** Construction of  $v_{j+1} = \varphi(v_j)$  starting with  $v_0 = 1$ . For each iterate, we follow the dotted black line up to  $P(v) = gkv$  (black solid line) and then  $L_{g,k}$  (red solid line) down to the lowest intersection with  $F$ . In (A)  $P$  does not intersect  $F$  above  $v = 0$  and so the iterates of  $\varphi$  converge to 0. In (B)  $P$  intersects  $F$  above  $v = 0$ , but  $L_{g,k}$  through the point  $(v_0, gkv_0)$  is not admissible and so the iterates of  $\varphi$  also converge to 0. In (C)  $P$  intersects  $F$  above  $v = 0$  and all  $L_{g,k}$  through  $(v_j, gkv_j)$  are admissible, so the iterates of  $\varphi$  converge to  $v_+$  (the highest intersection between  $P$  and  $F$ ). (D) Definitions of  $v_+$ ,  $v_-$ . Note that  $v_- \leq v_E \leq v_+$ , where  $v_E$  is illustrated in Figure 4. (E) Illustration of the condition for persistent propagation. The line  $P(v) = gkv$  (black) must intersect, or at least tangentially touch,  $F(v)$  to the right of  $v = 0$ , and  $L_{g,k}$  through the point  $(v_+, F(v_+))$  (red) must clear the critical segment, or at most touch it tangentially. (F) Construction of  $g_{\min}$ , below which no persistent propagation is possible.

then draw  $L_{g,k}$  through the point  $(v_j, gkv_j)$ . The  $v$ -coordinate of the smallest intersection of  $L_{g,k}$  with  $F$  is  $v_{j+1}$ . The construction of  $v_{j+1}$  from  $v_j$  is illustrated by Figures 10A–C.

From Figure 10, we read off the following theorem on the convergence of the  $v_j$ . In this theorem,  $v_E$  is defined as in Section 2.3 (Figure 4).

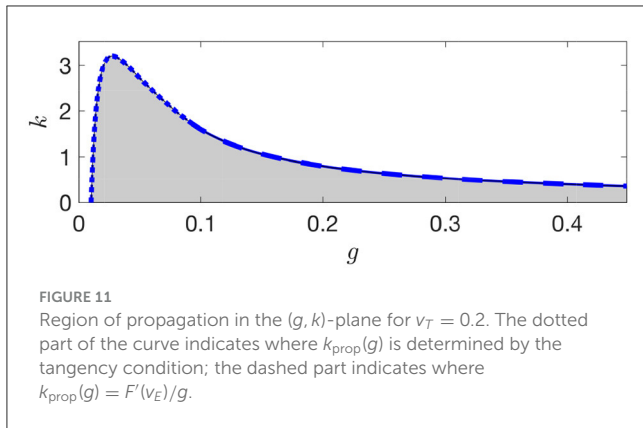
**Theorem 2.** Suppose  $gk \leq F'(v_E)$  and  $v_+$  is the maximum solution to  $F(v) = gkv$ . Then  $\lim_{j \rightarrow \infty} v_j = v_+$  if the line  $L_{g,k}$  through  $(v_+, F(v_+))$  is admissible or is tangent to  $F(v)$  along the critical segment. In all other cases,  $\lim_{j \rightarrow \infty} v_j = 0$ .

If  $\lim_{j \rightarrow \infty} v_j = v_+$ , we say that there is *persistent propagation*. If the line  $L_{g,k}$  through  $(v_+, F(v_+))$  is tangent to  $F(v)$ , we say it satisfies the *tangency condition*.

### 3.3 The region of persistent propagation

Our aim now is to understand for which values of  $g$  and  $k$ —that is, for which total upstream gap junction conductances and degree of expansion in our branching network—there can be persistent propagation. The result will be that the region of persistent propagation in the  $(g, k)$ -plane is of the form  $g \geq g_{\min}$  and  $0 \leq k \leq k_{\text{prop}}(g)$ , as shown in Figure 11. In particular, there is an “ideal” conductance which maximizes the  $k$  that can support persistent propagation.

The geometric construction described by Figures 10A–C and theorem 2 mean that there is persistent propagation precisely if the line  $P(v) = gkv$  (depicted in black in Figure 10E) intersects or at least touches  $F(v)$  at some positive value  $v_+ \geq v_E$  and with  $v_u = v_+$  (depicted in red) lies below the critical segment or at most touches it in a single tangency point.



To better understand the shape of the region of persistent propagation (Figure 11), we fix  $g$  and ask how Figure 10E changes as  $k$  is increased (illustrated in Figure 12). The slopes of both  $P(v)$  (black) and  $L_{g,k}$  (red) increase with  $k$ . Because the slope of  $P(v)$  increases,  $v_+$  decreases. Therefore, the vertical intercept of  $L_{g,k}$  ( $-gv_+$ ) also increases. This implies that  $L_{g,k}$  rises and is closer to the critical segment if it was admissible before.

We conclude that for a fixed  $g$ , the range of values of  $k$  that allow persistent propagation is either empty or an interval of the form  $[0, k_{\text{prop}}(g)]$  with  $k_{\text{prop}}(g) \geq 0$ . In particular, if there is persistent propagation for any  $k$  at all, there is persistent propagation for  $k = 0$ . Since the vertical intercept of  $L_{g,0}$  (red) is  $-g$ , the minimum possible  $g$  is  $g_{\text{min}}$ , where  $L_{g_{\text{min}},0}$  is tangent to the critical segment (Figure 10F).

For a given  $g > g_{\text{min}}$ , we obtain the range of values of  $k$  for which there is propagation by watching how  $P(v) = gkv$  and  $L_{g,k}$  (black and red lines) rotate as  $k$  increases, starting at  $k = 0$ . Figure 12 shows two examples. This leads to the following result.

**Theorem 3.** The region of persistent propagation in the  $(g, k)$ -plane is defined by

$$g \geq g_{\text{min}}, 0 \leq k \leq k_{\text{prop}}(g),$$

where  $L_{g_{\text{min}},0}$  is tangent to the critical segment and  $k_{\text{prop}}$  is continuous with  $k_{\text{prop}}(g_{\text{min}}) = 0$ . For small  $g$ ,  $k_{\text{prop}}$  is defined by the tangency condition (described in Theorem 2 and illustrated in Figure 10E). For large  $g$ ,  $k_{\text{prop}}(g) = F'(v_E)/g$ .

Since  $k_{\text{prop}}$  is 0 at  $g_{\text{min}}$  and tends to zero as  $g \rightarrow \infty$ , there is always a value of  $g$  that is “optimal” for propagation in the sense that  $k_{\text{prop}}$  is maximal. Figure 11 shows the region of propagation for  $v_T = 0.2$ . Numerical simulations suggest that the peak still occurs approximately where  $g(k+1) = F'(v_T)$ . This reflects our results for a single cell, that AP propagation is the easiest when the total gap junction conductance and cell’s intrinsic conductance at the threshold balance.

## 4 Comparison with more realistic models

We apply our analysis to see if we can predict AP propagation in simulations using more realistic models of a neuron and a

cardiac myocyte. We use a four-dimensional Hodgkin-Huxley-type model of the neuronal axon [39], which serves as a base model for hippocampal axons connected by gap junctions in several studies [43, 44]. For the cardiac myocyte, we use the eight-dimensional Luo-Rudy model [45], which captures many of the complexities in the cardiac action potential [46]. We used Anaconda Jupyter notebooks [47] with Python 3 to run simulations and apply our analysis. Numerical simulations were conducted using `solve_ivp` in the Scipy Integrate library (version 1.10.1, [48]) using implicit differentiation specified by the ‘BDH’ option. The code for all simulations and analysis are available in the [Supplementary material](#).

### 4.1 A neuronal model

To start, we compare the single cell analysis of Section 2 with simulation results for a model of the neuronal axon. We consider a single cell with downstream neighbors held at rest ( $v_R = 0$  in [39]). To apply our analysis, we construct the activation curve for this model,  $F_{\text{HH}}$ , by taking the right-hand-side of the voltage differential equation and replacing  $m$  with  $m_{\infty}(v)$ , and keeping  $n$  and  $h$  (which are slower than  $v$  near  $v_R$ ) fixed at resting values. Using  $F_{\text{HH}}$ , we calculate  $v_F$ , the AP firing voltage of the disconnected cell, and  $v_E$ , the maximum possible threshold voltage (see Figure 4 and the [Supplementary material](#)).

Using the full four-dimensional model, we run simulations of a single cell connected to fixed up- and downstream neighbors (Figure 3) for many  $(g, k)$  pairs under two different conditions:

1. The upstream cell is held at  $v = v_F$  for the entire simulation.
2. The upstream cell is held at  $v = v_F$  until the cell’s voltage reaches  $v_E$ .

For each simulation, we calculate the maximum voltage of the cell over the entire simulation for conditions 1 and 2. If the cell’s voltage rises beyond  $v_E$  under both conditions, then we say that active propagation is possible. However, if the cell’s maximum voltage goes beyond  $v_E$  only under the first condition, then only semi-active propagation is possible since the cell cannot maintain a full AP on its own. These results are shown in Figure 13A.

We then calculate  $k_{\text{max}}(g)$  and  $k_{\text{exc}}(g)$  using  $F_{\text{HH}}$ , and compare them directly to the simulation results. Figure 13A shows that  $k_{\text{max}}(g)$  for a single cell matches the simulated active propagation region boundary quite well for small  $g$ , with a discontinuous jump in the voltage height up to  $g_*$ . While the simulated boundary for the semi-active propagation is sharp as predicted in our framework, the simulated boundary lies to the left of the predicted boundary. The boundary matches the simulated active propagation regions, especially for  $g < g_*$ , which confirms that fast activation currents are primarily responsible for AP initiation in a single cell.

For the branching network, we make modifications in both the analysis and the simulations. In the simulations, we model 20 layers of cells and record the maximum voltage of the penultimate cell to indicate whether APs propagated through the network. We also only hold downstream neighbors for the last cell fixed at  $v = 0$ . In our analysis, we therefore adjust the assumption that downstream neighbors are held at  $v = 0$ . Instead, we make a cell’s

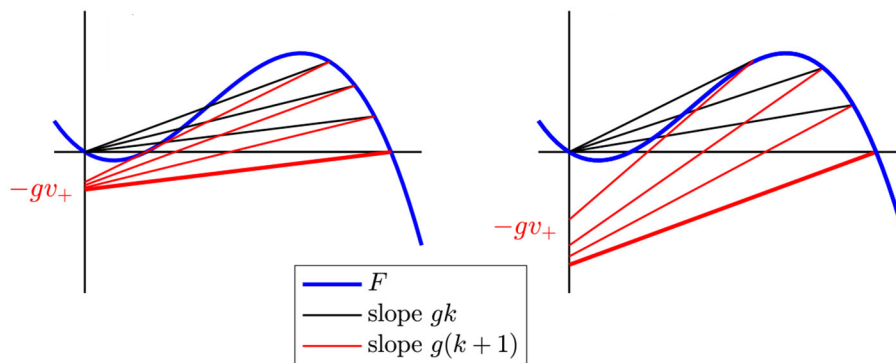


FIGURE 12

**Left:** For small  $g$ , the largest  $k$  for which there is persistent propagation is determined by the condition that the line  $L_{g,k}$  through  $(v_+, gkv_+)$  with slope  $g(k + 1)$  touches  $F$  tangentially. Here, we see  $P(v)$  and  $L_{g,k}$  for  $k = 0$  (highlighted in bold) and then see how  $P(v)$  and  $L_{g,k}$  move as  $k$  increases, until  $L_{g,k}$  is tangent to  $F$ . **Right:** For large  $g$ , the largest  $k$  for which there is persistent propagation is determined by the condition  $gk = F'(v_E)$ . Again, the case  $k = 0$  is highlighted in bold.

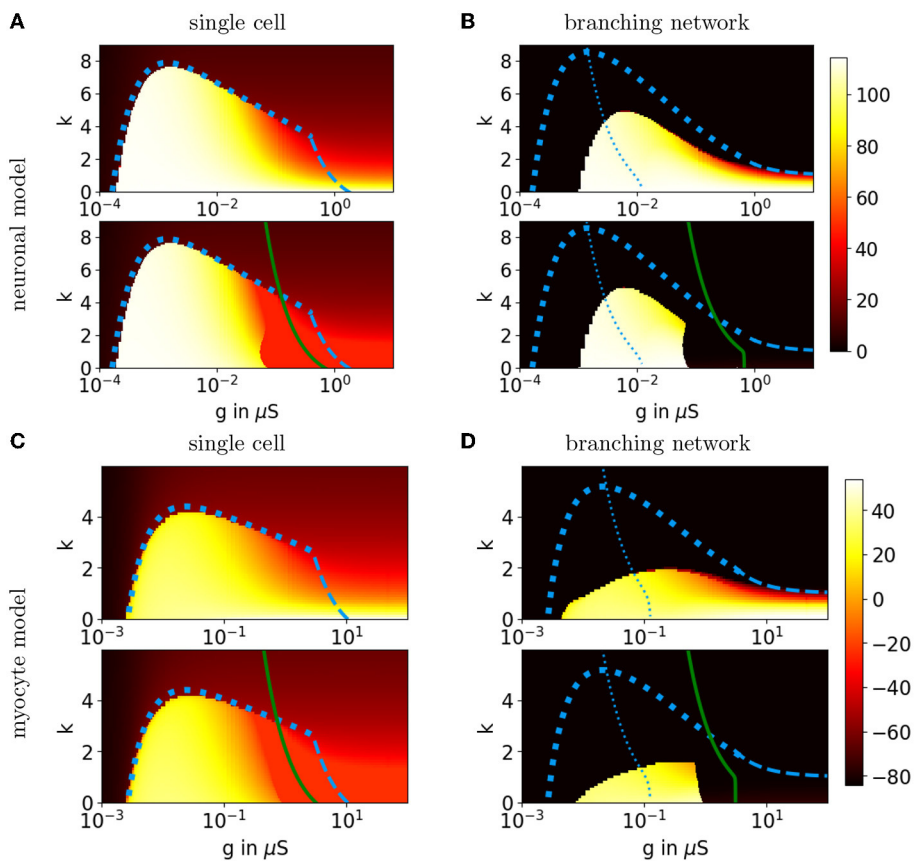


FIGURE 13

Behavioral regions for a Hodgkin-Huxley-type neuronal model and the Luo-Rudy myocyte model. **(A)** The heat map in the top graph shows the maximum voltage in mV over the entire simulation for a single Hodgkin-Huxley-type neuron where the upstream cell's voltage is held at  $v_u = v_f$ . The heat map in the bottom graph shows the maximum voltage when we only hold  $v_u = v_f$  until  $v = v_E$  and then set  $v_u = 0$ . Both heat maps range from  $v_R$  to  $v_f$ . The dashed blue curves show the predicted  $k_{max}$ . The solid green curve shows the predicted active-passive boundary  $k_{exc}$ . **(B)** The heat maps show the maximum voltage in mV for the penultimate cell in a branching network of Hodgkin-Huxley-type neurons, where  $v_0 = v_f$  for the entire simulation in the top graph and  $v_0 = v_f$  only until  $v_1 = v_E$  in the bottom graph. Both heat maps range from  $v_R$  to  $v_f$ . The curves  $k_{prop}$  (dashed blue),  $g(k + 1) = F'_{HH}(v_T)$  (dotted blue), and  $k_{exc}$  (solid green) are both adjusted for the assumption that the downstream cell's voltage is proportional to the cell's voltage. **(C, D)** Single cell and branching network results for the Luo-Rudy myocyte model. Interestingly, the shape of the simulated propagation region in the branching network is different than the predicted shape and the shape for a single cell possibly due to activation of slower calcium currents.

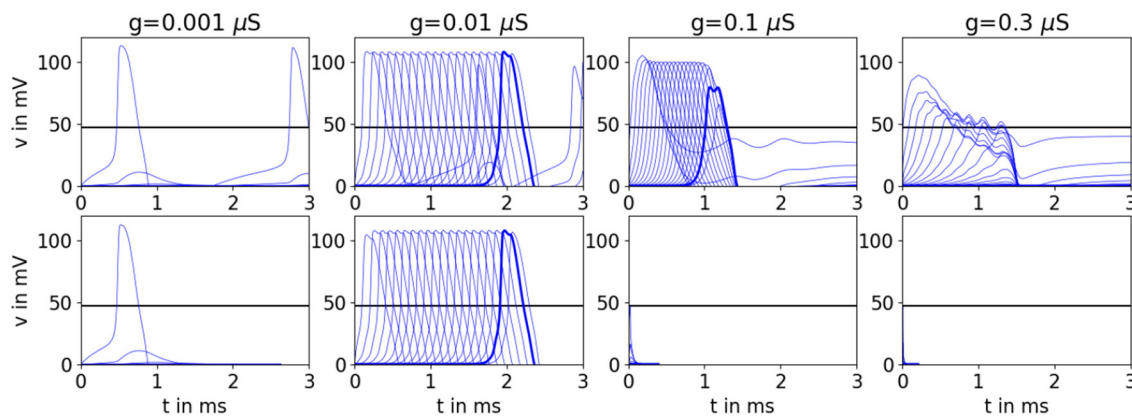


FIGURE 14

Simulations of the branching network for Hodgkin-Huxley-type neurons with  $k = 2$  showing the full range of behaviors. The top row shows results for condition 1, while the bottom panel shows results for condition 2 (also shown in Figure 1). In Figure 1, we saw propagation failure for  $g = 0.1 \mu\text{S}$ . In this figure, we see that the network will propagate if we hold the stimulation until more of the network is depolarized. However, we will always get propagation failure for very high values of  $g$ , such as  $g = 0.3 \mu\text{S}$ . The black horizontal line marks  $v_E$ . There are 20 cell layers in the network. The penultimate cell is highlighted in bold.

downstream neighbor voltages proportional to the cell's voltage [49], which follows the steady-state condition when there are only passive currents. The details of this modification are explained in the Appendix in the Supplementary material.

In Figure 13B, we see that the simulated active propagation region for the branching network lies entirely within the predicted region and has a similar shape. That  $k_{\text{prop}}$  over-estimates the boundary for AP propagation is to be expected since our analysis does not take the duration of an AP into account. (Though higher-order factors may shape the region as well, see section 5.) Regardless, we may still use the curve  $g(k+1) = F'(v_T)$  to estimate the peak, where the total gap junction conductance matches the cell's conductance at the intrinsic threshold. In Figure 13B, we see that the peak of the simulated active propagation region lies to the right of the peak curve. As predicted, there is a sharp boundary between the simulated semi-active propagation and active propagation regions. However,  $k_{\text{exc}}(g)$  lies to the right of the simulated boundary. Figure 14 illustrates the behavior seen in each region of Figure 13B for  $k = 2$ , and Figure 15 gives an example of AP propagation on both sides of the simulated semi-active propagation boundary. In particular, in Figure 15, we see APs propagate in the branching network only if cells in multiple layers are depolarized enough to fire.

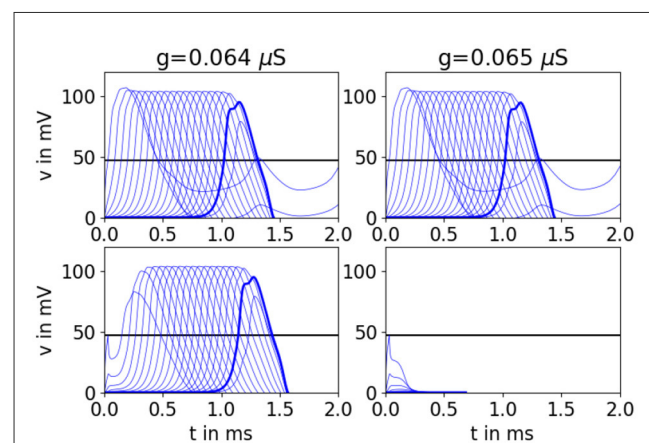


FIGURE 15

Simulations on both sides of the semi-active propagation boundary reveal that AP propagation may depend on depolarization of multiple downstream cells. Simulations of the branching network for Hodgkin-Huxley-type neurons with  $k = 2$ . **Top panels** show results for condition 1, **bottom panels** show results for condition 2. Under condition 2 on the **left**, the first cell's voltage dips down immediately after stimulation ends but is eventually pulled up when multiple layers fire. On the **right**, the downstream cells pull the first cell down, and they never recover. They all fail to propagate an AP at once. The black horizontal line marks  $v_E$ . There are 20 cell layers in the network. The penultimate cell is highlighted in bold.

## 4.2 A myocyte model

We compare simulations using the full eight-dimensional Luo-Rudy myocyte model [45] to our analysis in a similar manner to the neuron model above. We construct the activation curve  $F_{LR}$  by replacing  $m$  with  $m_{\infty}(v)$  and holding all other gating variables (which are slower than  $v$  near  $v_R$ ) fixed at their resting values. For ease of calculation, we also re-center  $F_{LR}(v)$  so that the resting fixed point is  $v_R = 0$ . Using the same simulation setup as in section 4.1, in Figures 13C, D, we again see that simulated AP propagation into a single cell matches the predicted boundaries very well, especially for

small  $g$ . Similarly, for the branching network, the simulated active propagation region lies entirely within the predicted boundary but does not quite have a similar shape. This may be due to the fact that slower calcium currents in the Luo-Rudy myocyte model allow APs to propagate for low  $g$  [38]. Similar to the neural model, the peak of the simulated active propagation region lies to the right of the peak curve. There is a sharp boundary between the semi-active and active propagation regions, which lies to the left of the predicted boundary.



## 5 Discussion

We explained why AP propagation through a branching network of excitable cells connected by gap junctions depends non-monotonically on gap junction conductance. We did this by reducing models to one-dimensional firing currents, which allows us to visualize how the firing currents and gap junction currents interact. From this visualization, we estimate that AP propagation is easiest when the total gap junction conductance matches the cell's conductance at its intrinsic threshold. We also found a discrete behavioral region where cells may propagate APs but are so strongly connected that they are no longer individually excitable.

We believe this framework can give a simple and efficient method for understanding where AP propagation may occur and may add guidelines on whether to raise or lower gap junction conductance to enhance propagation. For example, cells in realistic networks have a heterogeneous number of connections. Our framework may predict when AP propagation failure and subsequent re-entry occurs at cells with higher connectivity [12, 43, 50]. Currently, simulations are used to determine whether APs will propagate through any given network. For instance, whole heart simulations are a promising diagnostic tool in heart patients but can be computationally costly [51]. While cellular automata may alleviate the computational cost [52], our framework can inform phenomenological rules and greatly reduce the parameter space that needs to be searched. Finally, our framework outlines how the AP height, threshold, and subthreshold response changes with gap junction conductance [53]. These measures may be useful in determining the state of a network and predicting network-wide phenomena such as synchronization.

Moreover, this framework may be used to understand how network behavior may change with changes in connectivity, gap junction conductance, and firing currents. Cardiac arrhythmia can be brought about by pathogenic stressors [54, 55], adrenergic stimulation [56], or myocardial ischemia (buildup of plaques) associated with decreased gap junction coupling [57, 58]. Abnormal gap junction ubiquitination can affect both the heart and nervous system [59]. Gap junctions may be sensitive to toxins [60]. Epilepsy has been tied to gap junctions connecting networks of pyramidal cell axons, interneurons, and astrocytes, each of which play a different role in network excitability [61–64]. Furthermore, gap junctions are indicated in Parkinson's disease [65], Alzheimer's disease [66], nerve injury [67–69], and degenerative diseases in the retina [70]. Modulating gap junction conductance may help with several of these conditions; however, questions remain on how much gap junctions can be modulated without producing adverse side effects [71, 72]. An alternative may be to modulate firing currents through gene therapy [73]. There are also many conditions where external stimulation is applied as a part of therapeutic treatment [51, 74–77]. We hope that our framework can give insight on appropriate ranges to maintain proper function in a variety of networks.

Our study is closely related to several other studies. We directly extend the theory presented by Keener [40], which addresses the conditions where AP propagation may occur in a chain of cells with no branching. Our study also extends the study of Kouvaris et al. [41], who analyzed a bistable system where both the high and low resting voltages are fixed. This matches our analysis for AP

propagation into a single cell, so their bifurcation diagram matches our bifurcation diagram for a single cell (Figure 6). We take a more geometric approach, which clearly shows that the analysis depends only on the qualitative shape of the activation curve. This allows us to analyze the peak value of  $k$  for AP propagation. We also show how connectivity affects the AP firing voltage, which then determines whether persistent propagation is possible. Wang and Rudy first showed a biphasic relationship between gap junction conductance and an expansion ratio using simulations of cardiac tissue [34]. Several experimental and computational studies show a biphasic relationship between gap junction conductance and the safety factor [34, 38, 78, 79]. While our framework can predict where AP propagation is possible, the safety factor measures the source-sink mismatch from a recording or simulation based on the incoming current vs. outgoing current in a single cell. Finally, there are other studies that show an ideal gap junction conductance for propagation using a mean-field model [80], in a network using small-world topology [81], and an ideal cable diameter for AP propagation [82, 83].

We note that our framework only provides simple guidelines outlining where AP propagation may occur. While this theory can give a first estimate on when to expect AP propagation, there are many ways we could increase the accuracy of this prediction. For instance, we could link different versions of  $\varphi(v)$  to model AP propagation through a network with heterogeneous numbers of downstream neighbors. We may also improve the prediction by taking the connectivity of downstream neighbors more fully into account. In fact, AP propagation may not only depend on the number of immediate downstream neighbors, but on the number of neighbors several steps away [43]. Future studies may incorporate multiple layers of downstream neighbors. The predicted AP propagation regions in our framework overestimate the regions found in the original models. Preliminary results show that for the Fitzhugh-Nagumo model, the simulated boundary may be better predicted by taking into account the time to reach the threshold. However, a correction based on the timing still does not quantitatively predict the region in higher-order models. This may be due to higher-dimensional interactions within the cell, such as calcium currents in the Luo-Rudy myocyte model which may allow APs to propagate for low  $g$  [38].

Our framework studies propagation assuming the first cell is firing. It does not address getting the first cell to fire in the first place but rather reproduces the situation where the cell is voltage clamped. As gap junction conductance increases, it may take an increasing amount of current to bring the first cell to the desired voltage. In some cases, we may need to depolarize multiple downstream neighbors in the network to get AP propagation, similar to what is seen in semi-active propagation.

Overall, reduction of cell models to one-dimensional firing currents gives insight into how gap junction currents allow active propagation, semi-active propagation, or passive propagation. The shape of the firing currents explains how the threshold and peak firing voltage change with gap junction conductance and allows us to approximate an ideal gap junction conductance for AP propagation. This framework gives further insight into the mechanisms of these networks - which play a key role in both normal biophysiological function and disease.

## Data availability statement

The original contributions presented in the study are included in the article and [Supplementary material](#). Further inquiries can be directed to the corresponding author.

## Author contributions

EM developed the original concept and analysis. EM and CB revised the analysis and visualization and wrote and edited the manuscript.

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## Conflict of interest

The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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## Supplementary material

The Supplementary Material for this article can be found online at: <https://www.frontiersin.org/articles/10.3389/fams.2023.1186333/full#supplementary-material>

### PRESENTATION 1

Appendix.

### DATA SHEET 1

Code for all simulations and analysis.



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## Glossary

- active response:** a cell is excitable and fires as  $v_u$  increases from 0 to  $V_u$
- admissible:**  $L_{g,k}$  lies below the critical segment
- AP:** action potential
- critical segment:** segment on the graph of  $F$  between  $v_{\min}$  and  $v_i$
- excitable cell:** a cell with a stable resting voltage and unstable threshold when  $v_u = 0$
- fire:** in a single cell, a saddle-node bifurcation occurs on the critical segment as  $v_u$  increases from 0 to  $V_u$
- $F(v)$ :** inward activation current
- $g$ :** total upstream gap junction conductance
- $g_{\min}$ :** minimum  $g$  where firing is possible
- $g_{\max}$ :** maximum  $g$  where firing is possible in a single cell
- $g_{\text{peak}}$ :**  $g$  where  $k_{\max}(g)$  attains its maximum
- $g_*$ :** value of  $g$  where the condition determining  $k_{\max}(g)$  changes
- $G(v)$ :** outward gap junction current (see Eq. 3)
- $k$ :** ratio of downstream gap junction conductance over upstream conductance
- $k_{\text{exc}}(g)$ :** maximum  $k$  where a single cell is excitable
- $k_{\max}(g)$ :** maximum  $k$  where a single cell can fire
- $k_{\text{peak}}$ :** maximum value of  $k_{\max}(g)$
- $k_{\text{prop}}(g)$ :** maximum  $k$  where  $\lim_{j \rightarrow \infty} v_j = v_+$  as a function of  $g$
- $k_*$ :**  $k_{\max}(g_*)$
- $L_{g,k}$ :** graph of  $G$  when  $v_u = V_u$
- passive response:** single cell doesn't fire as  $v_u$  increases from 0 to  $V_u$
- semi-active response:** single cell isn't excitable but fires as  $v_u$  increases from 0 to  $V_u$
- $v_d$ :** voltage of a downstream cell
- $v_E$ :** value  $v$  where a saddle-node bifurcation occurs as  $g(k+1)$  increases and  $v_u$  is fixed at 0, rendering the cell unexcitable
- $v_F$ :** intrinsic AP height of single cell without gap junction connections
- $v_f$ :** AP height of a single cell with gap junction connections
- $v_i$ :** inflection point of  $F(v)$
- $v_j$ :** voltage of cells in the  $j$ th layer of a branching network
- $v_{\min}$ :**  $v$  where  $F(v)$  attains its local minimum
- $v_R$ :** the resting equilibrium point of a single cell
- $v_T$ :** intrinsic threshold of single cell without gap junction connections
- $v_t$ :** threshold of a single cell with gap junction connections
- $v_u$ :** voltage of an upstream cell
- $V_u$ :** maximum voltage or AP height of an upstream cell
- $v_{u,c}$ :** bifurcation value of  $v_u$  as a single cell fires
- $v_{\infty}$ :** lowest fixed point in a single cell when  $v_u = V_u$
- $v_+$ :** maximum intersection of  $F$  and  $P(v) = gkv$  if  $gk \leq F'(v_E)$
- $\varphi(v_u)$ :**  $v_{\infty}$  as a function of  $v_u$
- $\psi(v)$ :**  $v_u$  that will produce a fixed point at  $v$