



Assessing Brain–Muscle Connectivity in Human Locomotion through Mobile Brain/Body Imaging: Opportunities, Pitfalls, and Future Directions

Federico Gennaro^{1*} and Eling D. de Bruin^{1,2}

¹Institute of Human Movement Sciences and Sport, Department of Health Sciences and Technology, ETH Zurich, Zurich, Switzerland, ²Division of Physiotherapy, Department of Neurobiology, Care Sciences and Society, Karolinska Institutet, Stockholm, Sweden

OPEN ACCESS

Edited by:

Parashkev Nachev,
University College London,
United Kingdom

Reviewed by:

Niall Twomey,
University of Bristol, United Kingdom
Mitsunori Ogihara,
University of Miami, United States

*Correspondence:

Federico Gennaro
federico.gennaro@hest.ethz.ch

Specialty section:

This article was submitted
to Digital Health,
a section of the journal
Frontiers in Public Health

Received: 02 August 2017

Accepted: 01 February 2018

Published: 26 February 2018

Citation:

Gennaro F and de Bruin ED (2018)
Assessing Brain–Muscle Connectivity
in Human Locomotion through
Mobile Brain/Body Imaging:
Opportunities, Pitfalls, and Future
Directions.
Front. Public Health 6:39.
doi: 10.3389/fpubh.2018.00039

Assessment of the cortical role during bipedalism has been a methodological challenge. While surface electroencephalography (EEG) is capable of non-invasively measuring cortical activity during human locomotion, it is associated with movement artifacts obscuring cerebral sources of activity. Recently, statistical methods based on blind source separation revealed potential for resolving this issue, by segregating non-cerebral/artifactual from cerebral sources of activity. This step marked a new opportunity for the investigation of the brains' role while moving and was tagged mobile brain/body imaging (MoBI). This methodology involves simultaneous mobile recording of brain activity with several other body behavioral variables (e.g., muscle activity and kinematics), through wireless recording wearable devices/sensors. Notably, several MoBI studies using EEG–EMG approaches recently showed that the brain is functionally connected to the muscles and active throughout the whole gait cycle and, thus, rejecting the long-lasting idea of a solely spinal-driven bipedalism. However, MoBI and brain/muscle connectivity assessments during human locomotion are still in their fledgling state of investigation. Mobile brain/body imaging approaches hint toward promising opportunities; however, there are some remaining pitfalls that need to be resolved before considering their routine clinical use. This article discusses several of these pitfalls and proposes research to address them. Examples relate to the validity, reliability, and reproducibility of this method in ecologically valid scenarios and in different populations. Furthermore, whether brain/muscle connectivity within the MoBI framework represents a potential biomarker in neuromuscular syndromes where gait disturbances are evident (e.g., age-related sarcopenia) remains to be determined.

Keywords: mobile brain/body imaging, independent component analysis, corticomuscular coherence, neural drive, gait, electroencephalography, central pattern generators, age-related sarcopenia

CENTRAL PATTERN GENERATORS (CPGs) OR CORTICAL MECHANISMS? A LONG-LASTING (OPEN) QUESTION IN MOTOR CONTROL OF GAIT

Whether human locomotion is driven primarily by supraspinal or subcortical mechanisms within the central nervous system (CNS) is object of long-lasting debates. In mammals, muscle activation requires CNS inputs either dependently (1) or independently (2) from peripheral sensory feedback based on whether locomotion is actually performed or not. This finding is based on animal experimental data from the beginning of the nineteenth (3, 4) and twentieth centuries (5). These empirical findings forged the core of the CPGs, spinal interneuronal networks, theory (6). Since then and until recently, CPGs were considered playing the most crucial role in human locomotion. Briefly, CPGs model human locomotion (i.e., walking) as an action initiated by the brain, but yet are maintained (and constrained) in its steady-state execution by mostly spinal mechanisms with the interaction of peripheral afferent contributions (1). However, intentional gait modifications require motor programming in the premotor cortices (7) and, thus, indicate a role for supraspinal control of human walking. Here, we summarize recent studies on human walking showing that bipedalism is achieved by inputs and modifications from supraspinal, spinal, and peripheral structures (Figure 1). The corresponding contributory weights of the different structures that help in controlling different modes of locomotion (e.g., running, walking with or without cognitive dual-tasking), remain to be explored. Recent advances in technology lead to the hypothesis that the control of human bipedalism can be explored by applying experimental approaches that allow imaging of human brain dynamics in actively moving individuals.

A constant motor control of human bipedalism has already been hypothesized two centuries ago by scientists such as George Hayward, who wrote: “*The nerves convey the stimulus of volition to the muscles ... and the whole machine is thus put in motion under the guidance of the will*” (8). Nevertheless, at that time such a theory could not be demonstrated experimentally, given that a device able to record brain activity was not yet available.

ASSESSING THE BRAIN DURING MOVEMENT: OPPORTUNITIES AND PITFALLS

Only one century later Hans Berger recorded the first electroencephalography (EEG) from the human scalp (9). Since then and almost until the end of the 20th century, EEG has been involved in several studies on physiological and pathological neural mechanisms, however, it was not yet usable for assessing the supraspinal role in human locomotion. Each EEG electrode measures electrical potentials from a huge neuronal pool (e.g., from thousands of neurons) and this neuronal activity is spread out because of the volume conduction within the skull. Therefore, at the end each EEG electrode delivers only weak amplitudes of electrocortical

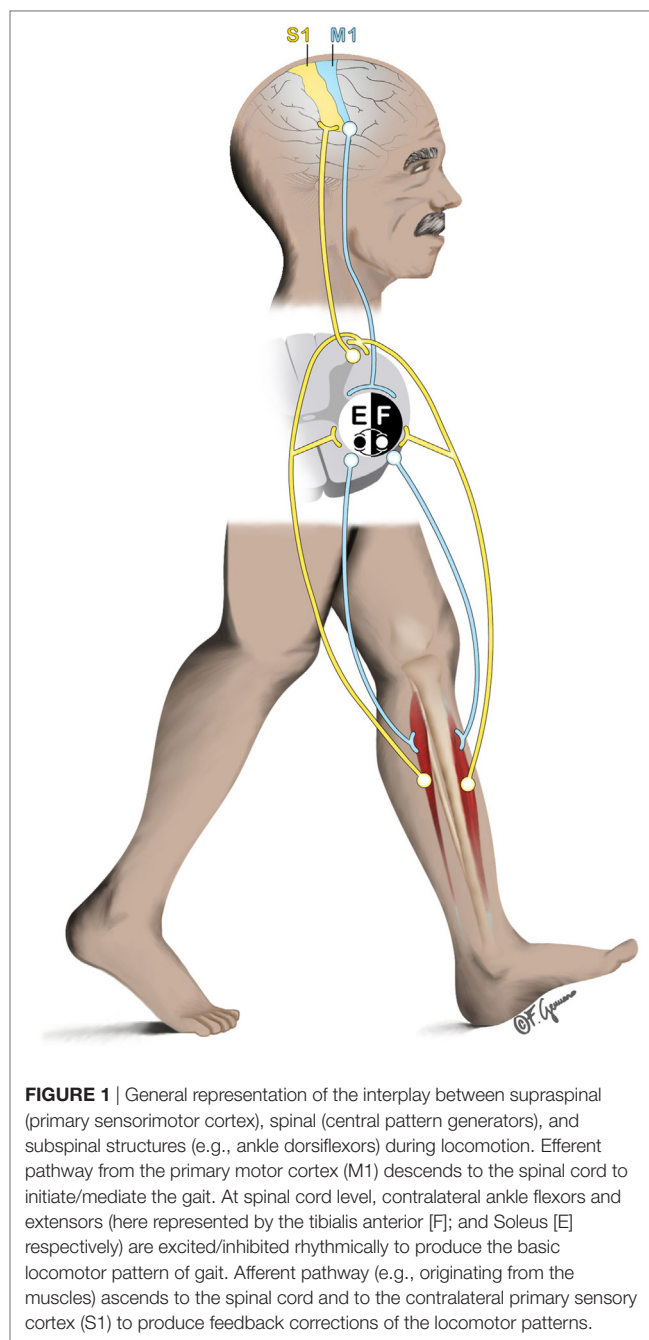


FIGURE 1 | General representation of the interplay between supraspinal (primary sensorimotor cortex), spinal (central pattern generators), and subspinal structures (e.g., ankle dorsiflexors) during locomotion. Efferent pathway from the primary motor cortex (M1) descends to the spinal cord to initiate/mediate the gait. At spinal cord level, contralateral ankle flexors and extensors (here represented by the tibialis anterior [F]; and Soleus [E] respectively) are excited/inhibited rhythmically to produce the basic locomotor pattern of gait. Afferent pathway (e.g., originating from the muscles) ascends to the spinal cord and to the contralateral primary sensory cortex (S1) to produce feedback corrections of the locomotor patterns.

signals which remain sensitive to electronic noise and artifacts (10). In fact, in the last century, a common goal of the scientific community in the motor control field focused only on experiments regarding the relationships between human locomotion and cognition (11). The movement-related artifacts/noise contaminating the EEG recordings in motion-related experiments possibly explains the lack of investigations in actively walking participants. However, recent technological developments give rise to the expectation that EEG- and movement artifacts-related problems during human locomotion might be overcome. We will, therefore, briefly discuss some of these recent developments. We

refer to a comprehensive overview of the theoretical and practical EEG and EEG-related principles (12, 13), since this topic is out of the scope of this work.

The interest in the supraspinal behavior during human locomotion has grown in the previous few decades and several studies started using functional near infrared spectroscopy (fNIRS) for the assessment of functional brain activation during human bipedalism (14, 15). fNIRS records the concentration levels of oxygenated hemoglobin (O_2Hb) and has the advantage of being less prone to movement artifacts contamination. However, using fNIRS in this context has some limitations as well. To name a few, fNIRS is not able to provide information about brain structure for anatomical reference, the separation of the hemodynamic changes originating either from cerebral tissue or extra-cerebral tissues/structures is difficult (16), and finally most fNIRS devices are composed of a few channels only (i.e., optodes). A multimodal approach where fNIRS and EEG are used in combination can be possible as well. Concurrent EEG-fNIRS measurements can be collected with relative ease (17) and allow simultaneous investigation of the brain at multiple spatial and temporal scales (16).

Electroencephalography allows the direct measurement of post-synaptic neuronal activity, with very high time resolution but low spatial resolution. However, in recent years several improvements to overcome the spatial resolution limitation of EEG have been made. Enhanced EEG source reconstruction techniques (18–23) in combination with advanced statistical methods such as clustering of independent components (24–27) (see next paragraph for more details about this topic) and measure projection analysis (28) are an example. These developments have enhanced the achievable spatial resolution quality of EEG (28). Furthermore, EEG devices are available in several settings and with a number of channels up to 256 electrodes, which allows coverage of the entire human scalp.

The application of statistical methods to segregate cerebral and non-cerebral sources (e.g., noise, muscle activity, and eye blinks/movements) from the EEG recordings (29) through blind source separation (BSS) constitutes a major improvement for the assessment of brain behavior during human movement in ecologically valid scenarios. This BSS method, known most commonly as independent component analysis (ICA) (30, 31), has demonstrated its capability to separate overlapping and linearly mixed sources (both cerebral and non-cerebral) from the EEG recordings into mutually independent sources. That is, EEG recordings can be cleaned from non-cerebral components while preserving the cerebral ones (32, 33). This “revolutionary” method to clean EEG recordings from contamination of movement artifacts has more recently evolved in more advanced methods such as adaptive mixture-independent component analysis (34).

MOBILE BRAIN/BODY IMAGING: A NEW PROMISING RESEARCH FIELD

This aforementioned development has kicked-off a new research field, tagged as mobile brain/body imaging (MoBI) (35, 36), that

translationally includes both knowledge from neuroscience and human movement sciences. MoBI introduces novel important opportunities allowing the investigation of the role of the CNS during human bipedal motion in natural environments (37, 38). Indeed, investigations using EEG approaches for studying human locomotion behavior has more recently shown an exponential increase, thus, unveiling several key aspects of cortical driven mechanisms of motor control in several human locomotion behavioral tasks, spanning from walking (39–46) to running (47) and from dancing (48) to cycling (49, 50). Even complex spatial navigation tasks (51) and virtual reality-based gait tasks (52) have been investigated with the help of this technique. Newer and deeper insights from more conventional types of analysis have been proposed, such as studies involving cognitive tasks (i.e., dual-task walking) in human bipedal motion (53–55).

A MoBI set-up allows an undefined number of body sensors to record human movement behavior concurrently with brain activity (e.g., by means of EEG). That is, the essence of the MoBI approach would require not only a mobile brain recording device but also simultaneous (and thus precisely triggered in time) several other measurement devices, in order to explore key aspects of the human locomotion linked to brain behavior. An example of such mobile wearable body sensors could be wireless surface electromyography (sEMG), 3D motion capture, inertial measurement units (IMUs), foot plantar pressure measurement systems, and/or eye tracker devices. A more comprehensive reading on wearable sensors options for MoBI studies can be found elsewhere (56).

BRAIN/MUSCLE CONNECTIVITY IN HUMAN LOCOMOTION: STANDPOINTS, LIMITATIONS, AND FUTURE DIRECTIONS

An important step in combining EEG with wearable body sensors has been performed by using sEMG. A recent MoBI study firstly showed that the motor cortex is actively committed in driving human locomotion such as walking (62). This was followed by several other similar studies (63–66). Together these studies represented the first direct and confirmatory evidence of supraspinal active controlling mechanisms, showing that brain activity is not solely constrained to a triggering role in human bipedal locomotion, but rather should be considered as being active during the whole motor execution phase, similar to the CPGs (67). This topic of investigation has been based on the assumption that the primary sensorimotor cortex (as assessed by means of EEG) is highly coupled (i.e., coherent) with muscle activity (as assessed by means of sEMG). That is, a measure of oscillatory synchronization between the primary sensorimotor cortex and spinal motor neurons activity (indirectly measured by sEMG), representing an actual measure of corticospinal interactions (68, 69). Coupled EEG–EMG analysis is often referred to as “corticomuscular coherence” (CMC) and has been first introduced by Baker in 1997 (70). CMC significant (71) values span from 0 to 1, where a higher number means higher coupling between EEG and EMG and, thus, a more efficient corticomuscular synchronization. Further

details regarding this brain/muscle connectivity measure can be found elsewhere (72–74).

The promising potential of using wearable sensors in combination with brain imaging devices, investigating the communication between supraspinal and subcortical sites with concurrent kinematic events, is shown by recent studies involving peripherally attached (i.e., to the limbs) IMUs coupled with magnetoencephalography. These studies have shown promising results in the sense that using such combined techniques (i.e., corticokinematic coherence, CKC) is capable to parallel CMC in assessing the neuronal communication between brain and muscle(s) (57–61). CKC is a good example of how wearable sensors in combination with brain imaging devices might be used for the assessment of meaningful human bipedalism behavior. CKC, currently not yet employed within a MoBI framework, might represent an important opportunity for future MoBI studies aiming to explore the brain–muscle communication during human locomotion. Indeed, IMUs are rather simple and quick to use as well as less prone to be contaminated by motion-related artifacts, compared to sEMG.

A comparable measure of CMC, referred to as “intramuscular coherence” or “EMG–EMG coherence”, takes into consideration the common synchronized oscillatory drive to a pair of sEMG placed over the same muscle (75). Intramuscular coherence is supposed to reflect the neural drive from the primary motor cortex to the muscles (75). EMG–EMG coherence has been found to be quite reliable during treadmill walking, however, although the derived coherence variables can be considered to be reliable measures, large changes are needed to indicate a real difference in an individual level (76).

It can be reasoned that CMC reliability as measured during human locomotion tasks (i.e., walking) is also promising; however, thorough investigations of the psychometric properties of the measurement approach are needed to substantiate or refute this assumption. We are currently far from having precise and accurate measurements of neuronal communication during human bipedal motion and available results from studies employing CMC (or EMG–EMG) techniques should be interpreted with prudence. The reproducibility and reliability of CMC measurements during human bipedal motion is an important issue not yet clarified on both group and individual levels and should be topic of future studies.

Another issue that needs to be resolved relates to the consistently reported efferent cortical role during the gait cycle (62, 65, 66). So far only one study evaluated the CMC during overground walking, reporting that in this more “ecological” scenario also the afferent pathway is involved in and throughout human locomotion (66). This is a standpoint of importance, given that in many clinical conditions where gait disturbances are present (e.g., muscle weakness, Parkinson’s disease), the entire feedback–feedforward motor control loop seems to be impaired. However, CMC should be regarded as a surrogate measure of the actual and direct neuronal communication taking place in humans. For example, it may well be that CMC cannot be found in a (healthy) subject, because of limitations either in applied study protocols, in the methods of analysis employed or, more generally, because of subject-to-subject variability. Obviously, this does not mean

absence of communication between brain and muscles; rather this is simply believed to be due to the fact that CMC applied during human bipedal motion assessment is still in its fledgling state of development and has several limitations that should be overcome.

Finally, future studies on CMC should consider to both establishing the reproducibility and reliability of CMC measurements as well as disentangling the causality in the connectivity measures (65, 66), possibly employing common CMC signal processing methods of analysis, thus enabling more consistent comparisons and to determine the most meaningful approach.

BRAIN/MUSCLE CONNECTIVITY DURING GAIT AS POTENTIAL NOVEL “BIOMARKER” IN CLINICAL SETTINGS

It has been shown that CMC has the potential to distinguish the presence of neuromuscular disorders such as in upper motor neuron disease (77). However, an important feature that future investigations should take into account is represented by using CMC during gait as a potential biomarker of clinical diseases where human locomotion is impaired. An important opportunity might be represented by the age-related progressive decline in muscle mass/strength, namely *sarcopenia* (78). Sarcopenia has a prevalence of about 10–20% in community-dwelling older adults above 65 years and goes up to 30–50% in those aged above 80 years (79–81). Sarcopenia, recently recognized as a geriatric syndrome by the Centers for Disease Control and Prevention (USA), requires better diagnostic methods for its determination (81). The potential relevance of using CMC while walking for detecting sarcopenia is driven by the fact that recent studies demonstrated that muscle atrophy is rather a relatively small contributor to the loss of muscle strength (82). Mounting evidence points to changes in neurologic function and/or the intrinsic force-generating properties of skeletal muscle as contributors to muscle weakness and motor dysfunction (83). Indeed, CMC has been defined as *the hallmark of aging* (84), able to distinguish younger from older adults based on fine motor (or motor-cognitive) tasks (85). Combining CMC measures with active walking within a MoBI framework can be assumed to provide meaningful information about the locomotor system in older adults (86).

CONCLUSION

In conclusion, the last two decades have opened a new and fascinating “door” on the motor control research field investigating neuronal communication in human locomotion. This field of research is still in its fledgling state, however, it is promising for revealing some aspects of the brain’s role in human locomotion. To increase the chances for replication both on group and individual human levels, studies using MoBI approaches in humans should specify parameters of the tests used, e.g., the exact procedures and instrumentation used, the duration of testing, and applied algorithms used for data analysis (87). An important feature is investigating CMC within the MoBI

framework as a potential “biomarker” in neuromuscular disorders (or syndromes), where the need of finding novel and better diagnostics is warranted.

AUTHOR CONTRIBUTIONS

FG has developed the conception and design of the manuscript under the lead of EB. FG drafted a first version of the manuscript. EB substantially revised the manuscript. Both FG and EB have read, revised, and approved the final version of the manuscript.

REFERENCES

- Patla AE, Calvert TW, Stein RB. Model of a pattern generator for locomotion in mammals. *Am J Physiol* (1985) 248(4 Pt 2):R484–94.
- Delcomyn F. Neural basis of rhythmic behavior in animals. *Science* (1980) 210(4469):492–8. doi:10.1126/science.7423199
- Flourens M-J-P. *Recherches Expérimentales Sur Les Propriétés et les Fonctions du Système Nerveux, Dans les Animaux Vertébrés [Experimental Studies on the Properties and Functions of the Nervous System in Vertebrate Animals]*. Paris: Chez Crevot (1824).
- Freusberg A. Reflexbewegungen beim Hunde. *Archiv für die gesamte Physiologie des Menschen und der Tiere* (1874) 9(1):358–91. doi:10.1007/bf01612347
- Sherrington CS. Flexion-reflex of the limb, crossed extension-reflex, and reflex stepping and standing. *J Physiol* (1910) 40(1–2):28–121. doi:10.1113/jphysiol.1910.sp001362
- Brown TG. On the nature of the fundamental activity of the nervous centres; together with an analysis of the conditioning of rhythmic activity in progression, and a theory of the evolution of function in the nervous system. *J Physiol* (1914) 48(1):18–46. doi:10.1113/jphysiol.1914.sp001646
- Takakusaki K. Neurophysiology of gait: from the spinal cord to the frontal lobe. *Mov Disord* (2013) 28(11):1483–91. doi:10.1002/mds.25669
- Hayward G. *Outlines of Human Physiology: Designed for the Use of the Higher Classes in Common Schools*. Boston, MA, US: Marsh, Capen & Lyon (1838).
- Berger H. Über das elektroencephalogramm des menschen. *Eur Arch Psychiatry Clin Neurosci* (1929) 87(1):527–70.
- Castermans T, Duvinage M, Cheron G, Dutoit T. Towards effective non-invasive brain-computer interfaces dedicated to gait rehabilitation systems. *Brain Sci* (2013) 4(1):1–48. doi:10.3390/brainsci4010001
- Lundin-Olsson L, Nyberg L, Gustafson Y. Stops walking when talking as a predictor of falls in elderly people. *Lancet* (1997) 349(9052):617. doi:10.1016/S0140-6736(97)24009-2
- Niedermeyer E, da Silva FL. *Electroencephalography: Basic Principles, Clinical Applications, and Related Fields*. Philadelphia: Lippincott Williams & Wilkins (2005).
- Nunez PL, Srinivasan R. *Electric Fields of the Brain: The Neurophysics of EEG*. USA: Oxford University Press (2006).
- EGgenberger P, Wolf M, Schumann M, de Bruin ED. Exergame and balance training modulate prefrontal brain activity during walking and enhance executive function in older adults. *Front Aging Neurosci* (2016) 8:66. doi:10.3389/fnagi.2016.00066
- Mirelman A, Maidan I, Bernad-Elazari H, Shustack S, Giladi N, Hausdorff JM. Effects of aging on prefrontal brain activation during challenging walking conditions. *Brain Cogn* (2017) 115:41–6. doi:10.1016/j.bandc.2017.04.002
- Quaresima V, Ferrari M. Functional near-infrared spectroscopy (fNIRS) for assessing cerebral cortex function during human behavior in natural/social situations: a concise review. *Organ Res Methods* (2016). doi:10.1177/1094428116658959
- Chen LC, Sandmann P, Thorne JD, Bleichner MG, Debener S. Cross-modal functional reorganization of visual and auditory cortex in adult cochlear implant users identified with fNIRS. *Neural Plast* (2016) 2016:4382656. doi:10.1155/2016/4382656
- Scherg M. Fundamentals of dipole source potential analysis. Auditory evoked magnetic fields and electric potentials. *Adv Audiol* (1990) 6:40–69.

ACKNOWLEDGMENTS

We thank the editors for inviting us to partake in this research topic by contributing with this work, which is based on an extension of an invited talk (Gennaro F, de Bruin ED. *EEG-EMG coherence during walking in older adults: A MoBI approach*) at the *Mini-Workshop on clinical applications of body mounted sensors* held on November 3, 2016 at the ARTORG Center for Biomedical Engineering of the University Bern (Bern, Switzerland). Moreover, we would like to thank Alexandra Schättin for the valuable comments on this manuscript.

- Hämäläinen MS, Ilmoniemi RJ. Interpreting magnetic fields of the brain: minimum norm estimates. *Med Biol Eng Comput* (1994) 32(1):35–42. doi:10.1007/BF02512476
- Pascual-Marqui RD, Michel CM, Lehmann D. Low resolution electromagnetic tomography: a new method for localizing electrical activity in the brain. *Int J Psychophysiol* (1994) 18(1):49–65. doi:10.1016/0167-8760(84)90014-X
- Van Veen BD, van Drongelen W, Yuchtman M, Suzuki A. Localization of brain electrical activity via linearly constrained minimum variance spatial filtering. *IEEE Trans Biomed Eng* (1997) 44(9):867–80. doi:10.1109/10.623056
- Groß J, Kujala J, Hämäläinen M, Timmermann L, Schnitzler A, Salmelin R. Dynamic imaging of coherent sources: studying neural interactions in the human brain. *Proc Natl Acad Sci U S A* (2001) 98(2):694–9. doi:10.1073/pnas.98.2.694
- Pascual-Marqui RD. Standardized low-resolution brain electromagnetic tomography (sLORETA): technical details. *Methods Find Exp Clin Pharmacol* (2002) 24(Suppl D):5–12.
- Makeig S, Westerfield M, Jung T-P, Enghoff S, Townsend J, Courchesne E, et al. Dynamic brain sources of visual evoked responses. *Science* (2002) 295(5555):690–4. doi:10.1126/science.1066168
- Onton J, Makeig S. Information-based modeling of event-related brain dynamics. *Prog Brain Res* (2006) 159:99–120. doi:10.1016/S0079-6123(06)59007-7
- Onton J, Westerfield M, Townsend J, Makeig S. Imaging human EEG dynamics using independent component analysis. *Neurosci Biobehav Rev* (2006) 30(6):808–22. doi:10.1016/j.neubiorev.2006.06.007
- Spadone S, de Pasquale F, Mantini D, Della Penna S. A K-means multivariate approach for clustering independent components from magnetoencephalographic data. *Neuroimage* (2012) 62(3):1912–23. doi:10.1016/j.neuroimage.2012.05.051
- Bigdely-Shamlo N, Mullen T, Kreutz-Delgado K, Makeig S. Measure projection analysis: a probabilistic approach to EEG source comparison and multi-subject inference. *Neuroimage* (2013) 72:287–303. doi:10.1016/j.neuroimage.2013.01.040
- Jung TP, Makeig S, Humphries C, Lee TW, McKeown MJ, Iragui V, et al. Removing electroencephalographic artifacts by blind source separation. *Psychophysiology* (2000) 37(2):163–78. doi:10.1111/1469-8986.3720163
- Bell AJ, Sejnowski TJ. An information-maximization approach to blind separation and blind deconvolution. *Neural Comput* (1995) 7(6):1129–59. doi:10.1162/neco.1995.7.6.1129
- Makeig S, Bell AJ, Jung T-P, Sejnowski TJ. Independent component analysis of electroencephalographic data. *Adv Neural Inf Process Syst* (1996):145–51.
- Kline JE, Huang HJ, Snyder KL, Ferris DP. Isolating gait-related movement artifacts in electroencephalography during human walking. *J Neural Eng* (2015) 12(4):046022. doi:10.1088/1741-2560/12/4/046022
- Snyder KL, Kline JE, Huang HJ, Ferris DP. Independent component analysis of gait-related movement artifact recorded using EEG electrodes during treadmill walking. *Front Hum Neurosci* (2015) 9:639. doi:10.3389/fnhum.2015.00639
- Palmer JA, Kreutz-Delgado K, Makeig S. AMICA: an adaptive mixture of independent component analyzers with shared components. *Tech. Report*. San Diego, CA: Swartz Center for Computational Neuroscience, University of California San Diego (2012).

35. Makeig S, Gramann K, Jung TP, Sejnowski TJ, Poizner H. Linking brain, mind and behavior. *Int J Psychophysiol* (2009) 73(2):95–100. doi:10.1016/j.ijpsycho.2008.11.008
36. Gramann K, Gwin JT, Ferris DP, Oie K, Jung TP, Lin CT, et al. Cognition in action: imaging brain/body dynamics in mobile humans. *Rev Neurosci* (2011) 22(6):593–608. doi:10.1515/RNS.2011.047
37. Pizzamiglio S, Naem U, Abdalla H, Turner DL. Neural correlates of single- and dual-task walking in the real world. *Front Hum Neurosci* (2017) 11:460. doi:10.3389/fnhum.2017.00460
38. Aspinnall P, Mavros P, Coyne R, Roe J. The urban brain: analysing outdoor physical activity with mobile EEG. *Br J Sports Med* (2015) 49:272–6. doi:10.1136/bjsports-2012-091877
39. Gwin JT, Gramann K, Makeig S, Ferris DP. Electrocranial activity is coupled to gait cycle phase during treadmill walking. *Neuroimage* (2011) 54(2):1289–96. doi:10.1016/j.neuroimage.2010.08.066
40. Haefeli J, Vögeli S, Michel J, Dietz V. Preparation and performance of obstacle steps: interaction between brain and spinal neuronal activity. *Eur J Neurosci* (2011) 33(2):338–48. doi:10.1111/j.1460-9568.2010.07494.x
41. Seeber M, Scherer R, Wagner J, Solis-Escalante T, Müller-Putz GR. EEG beta suppression and low gamma modulation are different elements of human upright walking. *Front Hum Neurosci* (2014) 8:380. doi:10.3389/fnhum.2014.00485
42. Bruijn SM, Van Dieën JH, Daffertshofer A. Beta activity in the premotor cortex is increased during stabilized as compared to normal walking. *Front Hum Neurosci* (2015) 9:593. doi:10.3389/fnhum.2015.00593
43. Bulea TC, Kim J, Damiano DL, Stanley CJ, Park H-S. Prefrontal, posterior parietal and sensorimotor network activity underlying speed control during walking. *Front Hum Neurosci* (2015) 9:247. doi:10.3389/fnhum.2015.00247
44. Salazar-Varas R, Costa Á, Iáñez E, Úbeda A, Hortal E, Azorín J. Analyzing EEG signals to detect unexpected obstacles during walking. *J Neuroeng Rehabil* (2015) 12(1):101. doi:10.1186/s12984-015-0095-4
45. Bradford JC, Lukos JR, Ferris DP. Electrocranial activity distinguishes between uphill and level walking in humans. *J Neurophysiol* (2016) 115(2):958–66. doi:10.1152/jn.00089.2015
46. Wagner J, Makeig S, Gola M, Neuper C, Müller-Putz G. Distinct β band oscillatory networks subserving motor and cognitive control during gait adaptation. *J Neurosci* (2016) 36(7):2212–26. doi:10.1523/JNEUROSCI.3543-15.2016
47. Gwin JT, Gramann K, Makeig S, Ferris DP. Removal of movement artifact from high-density EEG recorded during walking and running. *J Neurophysiol* (2010) 103(6):3526–34. doi:10.1152/jn.00105.2010
48. Ermutlu N, Yucedir I, Eskikurt G, Temel T, Isoglu-Alkac U. Brain electrical activities of dancers and fast ball sports athletes are different. *Cogn Neurodyn* (2015) 9(2):257–63. doi:10.1007/s11571-014-9320-2
49. Enders H, Cortese F, Maurer C, Baltich J, Protzner AB, Nigg BM. Changes in cortical activity measured with EEG during a high-intensity cycling exercise. *J Neurophysiol* (2016) 115(1):379–88. doi:10.1152/jn.00497.2015
50. Bigliassi M, Karageorghis CI, Wright MJ, Orgs G, Nowicky AV. Effects of auditory stimuli on electrical activity in the brain during cycle ergometry. *Physiol Behav* (2017) 177:135–47. doi:10.1016/j.physbeh.2017.04.023
51. Jungnickel E, Gramann K. Mobile Brain/Body Imaging (MoBI) of Physical Interaction with Dynamically Moving Objects. *Front Hum Neurosci* (2016) 10:306. doi:10.3389/fnhum.2016.00306
52. Wagner J, Solis-Escalante T, Scherer R, Neuper C, Müller-Putz G. It's how you get there: walking down a virtual alley activates premotor and parietal areas. *Front Hum Neurosci* (2014) 8:93. doi:10.3389/fnhum.2014.00093
53. De Sanctis P, Butler JS, Malcolm BR, Foxe JJ. Recalibration of inhibitory control systems during walking-related dual-task interference: a mobile brain/body imaging (MOBI) study. *Neuroimage* (2014) 94:55–64. doi:10.1016/j.neuroimage.2014.03.016
54. Malcolm BR, Foxe JJ, Butler JS, De Sanctis P. The aging brain shows less flexible reallocation of cognitive resources during dual-task walking: a mobile brain/body imaging (MoBI) study. *Neuroimage* (2015) 117:230–42. doi:10.1016/j.neuroimage.2015.05.028
55. Malcolm BR, Foxe JJ, Butler JS, Mowrey WB, Molholm S, De Sanctis P. Long-term test-retest reliability of event-related potential (ERP) recordings during treadmill walking using the mobile brain/body imaging (MoBI) approach. *Brain Res* (2017). doi:10.1016/j.brainres.2017.05.021
56. Reis PM, Hebenstreit F, Gabsteiger F, von Tscherner V, Lochmann M. Methodological aspects of EEG and body dynamics measurements during motion. *Front Hum Neurosci* (2014) 8:156. doi:10.3389/fnhum.2014.00156
57. Piitulainen H, Bourguignon M, De Tiege X, Hari R, Jousmäki V. Corticokinematic coherence during active and passive finger movements. *Neuroscience* (2013) 238:361–70. doi:10.1016/j.neuroscience.2013.02.002
58. Piitulainen H, Bourguignon M, De Tiege X, Hari R, Jousmäki V. Coherence between magnetoencephalography and hand-action-related acceleration, force, pressure, and electromyogram. *Neuroimage* (2013) 72:83–90. doi:10.1016/j.neuroimage.2013.01.029
59. Bourguignon M, Piitulainen H, De Tiege X, Jousmäki V, Hari R. Corticokinematic coherence mainly reflects movement-induced proprioceptive feedback. *Neuroimage* (2015) 106:382–90. doi:10.1016/j.neuroimage.2014.11.026
60. Bourguignon M, Whitmarsh S, Piitulainen H, Hari R, Jousmäki V, Lundqvist D. Reliable recording and analysis of MEG-based corticokinematic coherence in the presence of strong magnetic artifacts. *Neurophysiol Clin* (2016) 127(2):1460–9. doi:10.1016/j.clinph.2015.07.030
61. Smeds E, Vanhatalo S, Piitulainen H, Bourguignon M, Jousmäki V, Hari R. Corticokinematic coherence as a new marker for somatosensory afference in newborns. *Neurophysiol Clin* (2017) 128(4):647–55. doi:10.1016/j.clinph.2017.01.006
62. Petersen TH, Willerslev-Olsen M, Conway BA, Nielsen JB. The motor cortex drives the muscles during walking in human subjects. *J Physiol* (2012) 590(10):2443–52. doi:10.1113/jphysiol.2012.227397
63. Brantley JA, Luu TP, Ozdemir R, Zhu F, Winslow AT, Huang H, et al. Noninvasive EEG correlates of overground and stair walking. *38th Annual International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC)*. Orlando, FL: IEEE (2016). p. 5729–32. doi:10.1109/EMBC.2016.7592028
64. Winslow AT, Brantley J, Zhu F, Vidal JLC, Huang H. Corticomuscular coherence variation throughout the gait cycle during overground walking and ramp ascent: A preliminary investigation. *38th Annual International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC)* Orlando, FL: IEEE (2016). p. 4634–7. doi:10.1109/EMBC.2016.7591760
65. Artoni F, Fanciullacci C, Bertolucci F, Panarese A, Makeig S, Micera S, et al. Unidirectional brain to muscle connectivity reveals motor cortex control of leg muscles during stereotypic walking. *Neuroimage* (2017) 159:403–16. doi:10.1016/j.neuroimage.2017.07.013
66. Roeder L, Boonstra TW, Kerr GK. Dynamics of corticospinal motor control during overground and treadmill walking in humans. *bioRxiv* (2017). doi:10.1101/177915
67. Castermans T, Duvinage M. Corticomuscular coherence revealed during treadmill walking: further evidence of supraspinal control in human locomotion. *J Physiol* (2013) 591(6):1407–8. doi:10.1113/jphysiol.2012.247593
68. Schoffelen J-M, Oostenveld R, Fries P. Neuronal coherence as a mechanism of effective corticospinal interaction. *Science* (2005) 308(5718):111–3. doi:10.1126/science.1107027
69. Womelsdorf T, Schoffelen J-M, Oostenveld R, Singer W, Desimone R, Engel AK, et al. Modulation of neuronal interactions through neuronal synchronization. *Science* (2007) 316(5831):1609–12. doi:10.1126/science.1139597
70. Baker S, Olivier E, Lemon R. Coherent oscillations in monkey motor cortex and hand muscle EMG show task-dependent modulation. *J Physiol* (1997) 501(1):225–41. doi:10.1111/j.1469-7793.1997.225bo.x
71. Rosenberg J, Amjad A, Breeze P, Brillinger D, Halliday D. The Fourier approach to the identification of functional coupling between neuronal spike trains. *Prog Biophys Mol Biol* (1989) 53(1):1–31. doi:10.1016/0079-6107(89)90004-7
72. Mima T, Hallett M. Corticomuscular coherence: a review. *J Clin Neurophysiol* (1999) 16(6):501–11. doi:10.1097/00004691-199911000-00002
73. Bastos AM, Schoffelen J-M. A tutorial review of functional connectivity analysis methods and their interpretational pitfalls. *Front Syst Neurosci* (2015) 9:175. doi:10.3389/fnsys.2015.00175
74. Enders H, Nigg BM. Measuring human locomotor control using EMG and EEG: Current knowledge, limitations and future considerations. *Eur J Sport Sci* (2016) 16(4):416–26. doi:10.1080/17461391.2015.1068869
75. Hansen NL, Hansen S, Christensen LO, Petersen NT, Nielsen JB. Synchronization of lower limb motor unit activity during walking in human subjects. *J Neurophysiol* (2001) 86(3):1266–76. doi:10.1152/jn.2001.86.3.1266

76. van Asseldonk EH, Campfens SF, Verwer SJ, van Putten MJ, Stegeman DF. Reliability and agreement of intramuscular coherence in tibialis anterior muscle. *PLoS One* (2014) 9(2):e88428. doi:10.1371/journal.pone.0088428
77. Fisher KM, Zaaïmi B, Williams TL, Baker SN, Baker MR. Beta-band intermuscular coherence: a novel biomarker of upper motor neuron dysfunction in motor neuron disease. *Brain* (2012) 135(Pt 9):2849–64. doi:10.1093/brain/aww150
78. Clark BC, Manini TM. Sarcopenia≠ dynapenia. *J Gerontol A* (2008) 63(8):829–34. doi:10.1093/gerona/63.8.829
79. von Haehling S, Morley JE, Anker SD. An overview of sarcopenia: facts and numbers on prevalence and clinical impact. *J Cachexia Sarcopenia Muscle* (2010) 1(2):129–33. doi:10.1007/s13539-010-0014-2
80. Fielding RA, Vellas B, Evans WJ, Bhasin S, Morley JE, Newman AB, et al. Sarcopenia: an undiagnosed condition in older adults. Current consensus definition: prevalence, etiology, and consequences. International working group on sarcopenia. *J Am Med Direct Assoc* (2011) 12(4):249–56. doi:10.1016/j.jamda.2011.01.003
81. Falcon LJ, Harris-Love MO. Sarcopenia and the new ICD-10-CM code: screening, staging, and diagnosis considerations. *Fed Pract* (2017) 34(7):24–32.
82. Clark BC, Manini TM. What is dynapenia? *Nutrition* (2012) 28(5):495–503. doi:10.1016/j.nut.2011.12.002
83. Manini TM, Hong SL, Clark BC. Aging and muscle: a neuron's perspective. *Curr Opin Clin Nutr Metab Care* (2013) 16(1):21–6. doi:10.1097/MCO.0b013e32835b5880
84. Kamp D, Krause V, Butz M, Schnitzler A, Pollok B. Changes of cortico-muscular coherence: an early marker of healthy aging? *Age (Dordr)* (2013) 35(1):49–58. doi:10.1007/s11357-011-9329-y
85. Johnson AN, Shinohara M. Corticomuscular coherence with and without additional task in the elderly. *J Appl Physiol* (1985) (2012) 112(6):970–81. doi:10.1152/jappphysiol.01079.2011
86. Al-Yahya E, Dawes H, Smith L, Dennis A, Howells K, Cockburn J. Cognitive motor interference while walking: a systematic review and meta-analysis. *Neurosci Biobehav Rev* (2011) 35(3):715–28. doi:10.1016/j.neubiorev.2010.08.008
87. Bigdely-Shamlo N, Makeig S, Robbins KA. Preparing laboratory and real-world EEG data for large-scale analysis: a containerized approach. *Front Neuroinform* (2016) 10:7. doi:10.3389/fninf.2016.00007

Conflict of Interest Statement: The authors declare that the research has been conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

Copyright © 2018 Gennaro and de Bruin. This is an open-access article distributed under the terms of the Creative Commons Attribution License (CC BY). The use, distribution or reproduction in other forums is permitted, provided the original author(s) and the copyright owner are credited and that the original publication in this journal is cited, in accordance with accepted academic practice. No use, distribution or reproduction is permitted which does not comply with these terms.