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Prompt gamma spectroscopy retrieval algorithm for element and density measurements accelerated by cloud computing

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Prompt gamma ray in proton therapy is the product of a nuclear reaction between a proton and a target. The characteristic energies and intensities of prompt gamma lines can be used to determine the types of elements and their amounts in the target. In several previous experiments, it was demonstrated that no matter how complex the reaction cross-section is, once the energy of the incident proton and the irradiated element are determined, there is a definite linear relationship between the element concentration and the number of gamma-ray photons. However, this linear relationship is difficult to apply to medical imaging, and the nonlinear behavior of hydrogen has not been investigated so far. In this study, this linear relationship is extended to mixed elemental materials including a nonlinear case such as hydrogen, and a universal mathematical form, which is referred to as the prompt gamma spectroscopy retrieval algorithm (PGSRA), is developed. The basic assumption of the PGSRA is that the PGS of the sample material has a relationship with the molar gamma lines of the elements. For carbon and oxygen, this relationship is linear, while for hydrogen, this relationship is nonlinear. As the 2.23 MeV gamma line originates from neutron absorption radiation, the behavior of hydrogen is carefully investigated. The linear and nonlinear relationships are verified using Monte Carlo simulations with different combinations of carbon, oxygen, and hydrogen, such as PMMA, pentanediol, and ethanediol. The PGSRA developed in this work could be the first bridge between PGS and medical imaging.

KEYWORDS

proton therapy, prompt gamma spectroscopy retrieval algorithm, Monte Carlo, FLUKA, neutron absorption

1 Introduction

Prompt gamma (PG) is being widely investigated in proton and carbon ion therapy because it is a promising solution for online range verification [1, 2]. Different kinds of PG cameras were developed for 1D range measurement [3–6] and 3D image measurement [7–9]. Some of these cameras have already been tested in clinical trials [10, 11]. New PG timing systems, such as fast detectors based on CeBr₃ [12] and LaBr₃ [13], have been developed in recent years. Zhang *et al.* developed a new multi-slit PG imaging system based on BGO + SiPM [14, 15].

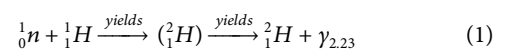
Monte Carlo code, such as FLUKA [16–18] and Geant4 [19, 20], are powerful tools for particle research. Some new ideas or new designs can be checked by conducting simulations on MC platforms; for example, the time-of-flight (TOF) method was adopted to study PG imaging using Geant4 [21, 22], and a new pixelated PG detector configuration was investigated using FLUKA [23]. Different configurations, such as multi-slit and knife-edge configurations, were compared using Geant4 [24]. Changran *et al.* investigated the Doppler shift effect for range verification using Geant4 [25, 26]. Recently, a new method for spatiotemporal emission reconstruction PG timing (SER-PGT) was developed and verified by FLUKA [27].

Protons deposit energy in matter through interactions when protons get into tissues during proton therapy. Proton–nuclear interactions involve both elastic and inelastic processes, including nuclear capture and nuclear scattering. For many scattering processes, the tissue nuclei remain intact and are left in an excited energy state. The decay of these excited nuclei typically produces a gamma ray with an energy ranging from 0 MeV to 11 MeV within a few nanoseconds of the proton–nucleus interaction, known as PG emission. The energy spectra of this PG emission depend on the specific nuclear energy states of the excited elemental nuclei, resulting in each element producing a unique spectrum, known as PG spectroscopy. Thus, tissues composed of different elements and elemental concentrations will produce different emission spectra during irradiation [28]. At present, prompt gamma spectroscopy (PGS) can be used to measure the beam range with high resolution [29–31]. In addition, Joost M. Verburg *et al.* investigated gamma lines and developed a novel optimization algorithm to determine the absolute range with a mean statistical precision of 1.1 mm [5, 11].

Range assessment is not the only capability of PGS. Similar to prompt gamma-ray neutron activation analysis (PGNAA) [32–35], the characteristic energies and intensities of gamma lines can be used to determine the types of elements and their amounts [36, 37]. The major difference between PGS and PGNAA is the kind of particle that initiates the nuclear reaction in the material. Verburg *et al.* assessed the complex cross-section and total photon yield for different incident proton energies on different target materials [35]. Polf *et al.* characterized how PG emission from tissue changes as a

function of carbon and oxygen concentrations [38, 39]. Paulo Martins *et al.* demonstrated a feasible technique for proton and ion beam spectroscopy (PIBS) that was capable of determining the elemental concentrations of irradiated tissues during particle therapy [40]. In the experiments of Polf *et al.* and Paulo Martins *et al.*, a linear relationship was demonstrated between the concentration of irradiated oxygen in tissue-equivalent samples and the total emission of PG radiation during irradiation by fixed energy protons.

Their experimental work demonstrated that no matter how complex the reaction cross-section is, once the energy of the incident proton and the irradiated element are determined, there is a definite relationship between the element content and the number of gamma-ray photons. However, this linear relationship is difficult to apply to medical imaging. These works did not extend the mathematical form of the linear relationship to more than one element. Our goal is to develop an algorithm that could be used to determine the content of multiple elements in the target, not just the concentration, from the PGS data obtained during irradiation. Additionally, a discussion on how to calculate the hydrogen amount as $\gamma_{2,23}$ intensity from the neutron (slow neutron) absorption reaction (Eq. 1), which is not the direct production of proton/carbon irradiation, was not presented in the aforementioned works. Thus, the $\gamma_{2,23}$ intensity is not a linear function of the hydrogen amount [41]. Jeyasingam *et al.* also measured PG-ray emissions from elements found in tissue; however, they also did not investigate the gamma lines from the neutron absorption reaction [42].



In the present study, the nonlinear behavior of the $\gamma_{2,23}$ intensity from different samples is first investigated. In addition, a retrieval algorithm is developed to measure the amounts of all elements in homogeneous materials, including PMMA, pentanediol, and ethanediol. Their chemical formulas and basic molecular structures are presented in Figure 1. As a feasibility study, all the irradiation and gamma-ray transport processes are simulated by using the FLUKA v4 which is currently distributed by the FLUKA CERN collaboration [43].

2 Materials and methods

2.1 Basic assumptions

From an ideal simulation shown in Figure 2, we used a proton beam to irradiate a PMMA molecule, which yields gamma-ray spectroscopy $\varphi(C_5H_8O_2)$ (left in blue). Similarly, we used a proton beam to irradiate one carbon nucleus and one oxygen nucleus, which yields gamma-ray spectroscopy $\varphi(C)$ (right in dark) and $\varphi(O)$ (right in red), respectively. Finally, we used a neutron to bombard a hydrogen nucleus to obtain gamma-ray spectroscopy

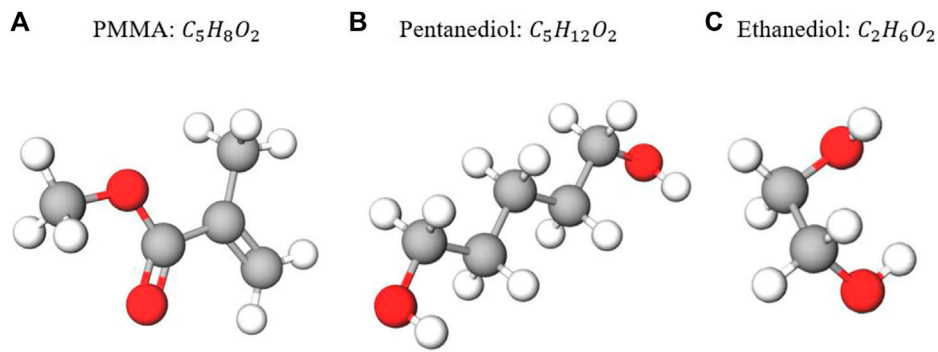


FIGURE 1

Chemical formulas and basic molecular structures of the three targets investigated in our feasibility study. The white spheres represent hydrogen atoms, the red spheres represent oxygen atoms, and the gray spheres represent carbon atoms. From (A–C): PMMA ($C_5H_8O_2$), pentanediol ($C_5H_{12}O_2$), and ethanediol ($C_2H_6O_2$).

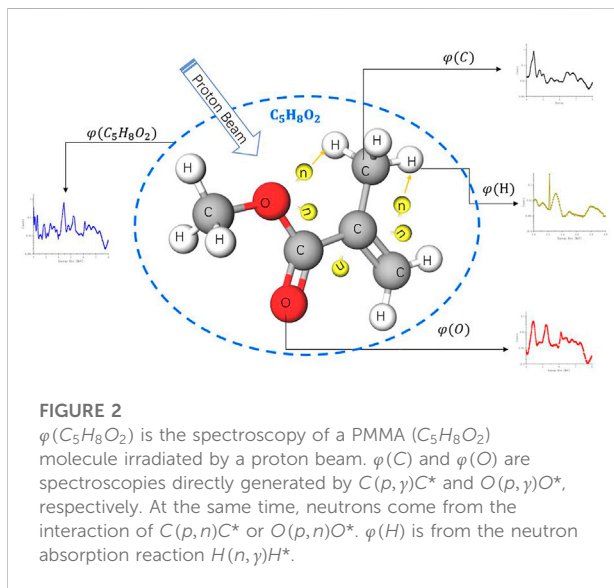


FIGURE 2

$\varphi(C_5H_8O_2)$ is the spectroscopy of a PMMA ($C_5H_8O_2$) molecule irradiated by a proton beam. $\varphi(C)$ and $\varphi(O)$ are spectroscopies directly generated by $C(p,\gamma)C^*$ and $O(p,\gamma)O^*$, respectively. At the same time, neutrons come from the interaction of $C(p,n)C^*$ or $O(p,n)O^*$. $\varphi(H)$ is from the neutron absorption reaction $H(n,\gamma)H^*$.

$\varphi(H)$ (right in yellow). Here, φ is spectroscopy from (p,γ) and (n,γ) reactions. There is a relationship between $\varphi(C_5H_8O_2)$ and $\varphi(C)$, $\varphi(O)$, $\varphi(H)$. In this section, we aim to formalize a mathematical form to describe this relationship.

Normally, the unit of φ is photon number per incident proton per molecule or per mol at different gamma lines. In this study, gamma-ray spectroscopy is the quantitative of the energy spectra of gamma ray from the interaction between the proton and the specific matter or element. Generally, the x -axis of a spectroscopy is the energy channel, while the y -axis is the gamma-ray count.

As experiments from Polf *et al.* and Paulo Martins *et al.* proved that there is a definite relationship between the element content and the number of gamma-ray photons, we formalize a

mathematical model from a phase-only perspective which could be solved by the numerical method in later sections. Thus, we assume a simple relationship, as in Eq. 2.

$$\varphi(C_{N_c}H_{N_H}O_{N_O}) = N_c\varphi(C) + N_O\varphi(O) + f(N_c, N_O, N_H)\varphi(H) \quad (2)$$

The spectroscopy of a target molecule is a sum of the spectroscopy from elemental carbon, oxygen, and hydrogen with corresponding weight ratios: N_c , N_O , and $f(N_c, N_O, N_H)$. The dominant factor is the number of element atoms in the molecule. From a microscopic point of view, the more atoms of an element in a molecule, the higher the probability is of emitting its characteristic gamma rays. Weight ratios N_c and N_O represent the numbers of carbon and oxygen, respectively, in the chemical formula; here, for example, $N_c = 5$ and $N_O = 2$. However, for hydrogen, the major gamma line at 2.23 MeV strongly relies on neutron yields based on the absorption reaction (Eq. 1). Thus, the spectroscopy of hydrogen depends not only on the number of hydrogen atoms but also on the number of neutrons that cause (n,γ) reactions, which in turn come from (p,n) reactions in other proton–nuclear interactions such as $C(p,n)C^*$ and $O(p,n)O^*$. Thus, the weight ratio f of hydrogen spectroscopy $\varphi(H)$ should be related to N_c , N_O , and N_H . Considering the different sources of neutrons in absorption reaction, we have Eqs 3–5:

$$\varphi(C_{N_c}H_{N_H}O_{N_O}) = N_c\varphi(C) + N_O\varphi(O) + f_c(N_c, N_O, N_H)\varphi(HC) + f_o(N_c, N_O, N_H)\varphi(HO), \quad (3)$$

$$f_c(N_c, N_O, N_H) = N_H \frac{N_c}{N_O + N_c} \frac{N_H}{N_O + N_c}, \quad (4)$$

$$f_o(N_c, N_O, N_H) = N_H \frac{N_O}{N_O + N_c} \frac{N_H}{N_O + N_c}. \quad (5)$$

The first two terms of Eq. 3 are the same as Eq. 2, as neutrons for the absorption reaction come from the interaction of $C(p, n)C^*$ and $O(p, n)O^*$. The third term of Eq. 2 hydrogen spectroscopy $\varphi(H)$ should be split into two parts: spectroscopy $\varphi(HC)$ originates from (n, γ) reactions where the neutrons come from $C(p, n)C^*$ reactions, and the spectroscopy $\varphi(HO)$ originates from (n, γ) reactions where the neutrons come from $O(p, n)O^*$ reactions. Correspondingly, their weight ratios Eq. 4 $f_c(N_c, N_o, N_H)$ and Eq. 5 $f_o(N_c, N_o, N_H)$ should be a nonlinear function of N_c , N_o , and N_H .

In Eq. 4, the dominant parameter is the number of hydrogen atoms N_H in the molecule. The ratio $\frac{N_c}{N_o+N_c}$ represents the factor of the neutron, that is, the neutron absorption reaction (Eq. 1), where the neutron is emitted from the $C(p, n)C^*$ reaction. The ratio $\frac{N_H}{N_o+N_c}$ is a hydrogen enhancement factor because when there are more hydrogens in a molecule with the same number of carbon or oxygen, the neutron absorption probability will increase. In Eq. 5, the dominant parameter is the number of hydrogen atoms N_H in the molecule, and the ratio $\frac{N_o}{N_o+N_c}$ represents the factor of the neutron emitted from the $O(p, n)O^*$ reaction. $\frac{N_H}{N_o+N_c}$ is a hydrogen enhancement factor same as in Eq. 4.

In Section 3, we will illustrate that for hydrogen, there is only one peak at 2.23 MeV in its PGS, and it does not contribute to the other characteristic gamma lines in the carbon and oxygen spectra. Thus, for an unknown material x we have the following changes: $C_{N_c}H_{N_H}O_{N_o} \rightarrow x$, $\varphi(HC) \rightarrow \varphi_{HC}^{2.23}$, $\varphi(HO) \rightarrow \varphi_{HO}^{2.23}$ in Eq. 3. And Eq. 3 can be mathematically separated into two equations (Eq. 6):

$$\begin{aligned} \varphi(x) - \varphi_x^{2.23} &= N_c \varphi(C) + N_o \varphi(O) \\ \varphi_x^{2.23} &= f_c \varphi_{HC}^{2.23} + f_o \varphi_{HO}^{2.23} \end{aligned} \quad (6)$$

In this article, we use φ to represent PG spectroscopy in a given material x or an element per molecule or per mol, and $\varphi_x^{2.23}$ represents the count at a given energy of 2.23 MeV in the material per molecule or per mol. The lower index is the material, and the upper index is the energy. $\varphi_{HC}^{2.23}$ and $\varphi_{HO}^{2.23}$ are 2.23 MeV gamma counts originating from carbon and oxygen per molecule or per mol. Eq. 1 to Eq. 6 are formalized based on a single molecule or 1 mol. In the next section, we will derive these equations to a large volume target.

2.2 PGS retrieval algorithm

In a real experiment, one cannot shoot a single molecule target with a single proton. If the target phantom has M mol molecules, then the elements' molar amount is

$$M_c = M^* N_c, \quad M_o = M^* N_o \quad \text{and} \quad M_H = M^* N_H$$

The total PG count from a phantom is

$$\psi_x^{FullEnergy} = M^* \varphi(x),$$

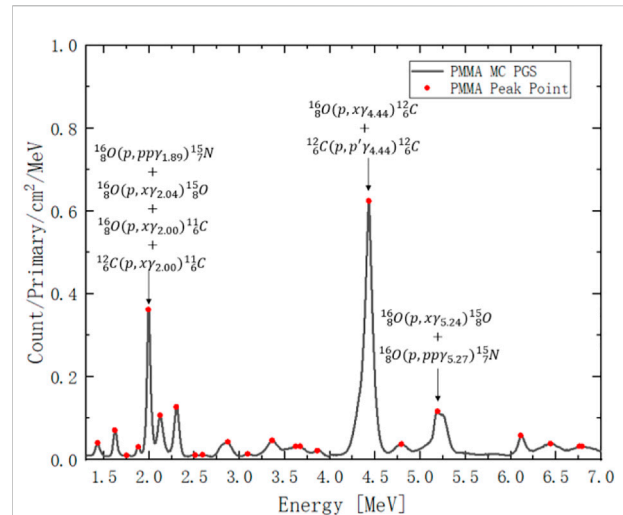


FIGURE 3
PGS spectrum from 150 MeV proton irradiation on PMMA. The red points are peak counts at a given gamma energy. The x-axis is gamma-ray energy channel from 1.3 MeV to 7 MeV. The y-axis is gamma-ray count per incident proton (primary) per unit cylinder surface area per MeV.

where ψ is total spectroscopy and φ is molar spectroscopy. The upper index *FullEnergy* means the gamma lines at every energy in consideration. For 2.23 MeV, the total gamma count of hydrogen is

$$\psi_x^{2.23} = M^* \varphi_x^{2.23}$$

In fact, $\psi_x^{2.23}$ is one peak point count at 2.23 MeV in $\psi_x^{FullEnergy}$. After both sides of Eq. 6 are multiplied by M , we obtain

$$\psi_x^{FullEnergy} - \psi_x^{2.23} = M_c \varphi(C) + M_o \varphi(O), \quad (7a)$$

$$\psi_x^{2.23} = F_c \varphi_{HC}^{2.23} + F_o \varphi_{HO}^{2.23}. \quad (7b)$$

Here, $\varphi(C)$ and $\varphi(O)$ are the PGS per mol carbon and oxygen, respectively. $\varphi_{HC}^{2.23}$ and $\varphi_{HO}^{2.23}$ are the PG counts per mol hydrogen with neutrons originating from carbon and oxygen, respectively. These molar PGS values can be measured or calculated from simple substances, such as hydrocarbons and water.

After both sides of Eq. 4 and Eq. 5 are multiplied by M , we obtain volume weight ratios Eq. 8 for F_c and Eq. 9 for F_o in Eq. 7b:

$$F_c = M^* f_c = M_H \frac{M_c}{M_o + M_c} \frac{M_H}{M_o + M_c}, \quad (8)$$

$$F_o = M^* f_o = M_H \frac{M_o}{M_o + M_c} \frac{M_H}{M_o + M_c}. \quad (9)$$

As shown in Figure 3, the dark curve is the MC simulated PGS from 150 MeV proton beam, which irradiate a PMMA cylinder, and the red points are the peaks in the PGS

spectrum. For example, the count at 2 MeV results from the contribution of 4 reactions; the first three reactions come from oxygen and the last one comes from carbon [44]. The count at 4.44 MeV also results from a contribution of both carbon and oxygen. The count at 5.25 MeV only comes from oxygen.

There are only two unknown variables M_c and M_O in Eq. 7a. Thus, for a binary linear equation, we need at least two peak points to solve the equation. From Figure 3, we always obtain more than 3 points from a PGS spectrum, and Eq. 7a can be solved by using the least squares method. These points are sorted into three different groups to compare the influence of the selection of different energy peaks on the results:

Low: low-energy peaks from 1.5 to 4 MeV.

High: high-energy peaks from 4 to 7 MeV.

Medium-high: peaks from medium energy 2 MeV to high energy 7 MeV.

To obtain a numerical solution, we discretize Eq. 7a:

$$\begin{bmatrix} \varphi_{\text{O}}^1 & \varphi_{\text{C}}^1 \\ \varphi_{\text{O}}^2 & \varphi_{\text{C}}^2 \\ \varphi_{\text{O}}^3 & \varphi_{\text{C}}^3 \\ \vdots & \vdots \\ \varphi_{\text{O}}^i & \varphi_{\text{C}}^i \\ \vdots & \vdots \end{bmatrix} \begin{bmatrix} M_C \\ M_O \end{bmatrix} = \begin{bmatrix} \psi_x^1 \\ \psi_x^2 \\ \psi_x^3 \\ \vdots \\ \psi_x^i \\ \vdots \end{bmatrix}, \quad (10)$$

$$\text{Object: } \min(Am - B), \quad (11)$$

where matrix $A = \begin{bmatrix} \varphi_{\text{O}}^1 & \varphi_{\text{C}}^1 \\ \varphi_{\text{O}}^2 & \varphi_{\text{C}}^2 \\ \varphi_{\text{O}}^3 & \varphi_{\text{C}}^3 \\ \vdots & \vdots \\ \varphi_{\text{O}}^i & \varphi_{\text{C}}^i \\ \vdots & \vdots \end{bmatrix}$ is the measured molar PGS point

of carbon and oxygen, and $B = \begin{bmatrix} \psi_x^1 \\ \psi_x^2 \\ \psi_x^3 \\ \vdots \\ \psi_x^i \\ \vdots \end{bmatrix}$ is the measured PGS point

of the sample material. Index i is the selected gamma energy point of PGS from the target phantom. Then, the unknown element molar number matrix $m = \begin{bmatrix} M_C \\ M_O \end{bmatrix}$ can be determined by the least square method.

The last step is to solve Eq. 7b and bring coefficients F_C and F_O into Eq. 7b; we have Eq. 12:

$$\psi_x^{2.23} = M_H \left(\frac{M_O}{M_O + M_C} \varphi_{HO}^{2.23} + \frac{M_C}{M_O + M_C} \varphi_{HC}^{2.23} \right) \frac{M_H}{M_O + M_C}. \quad (12)$$

Now, only M_H is an unknown variable, and the analytical solution of M_H is

$$M_H = (M_O + M_C) \sqrt{\frac{\psi_x^{2.23}}{M_O \varphi_{HO}^{2.23} + M_C \varphi_{HC}^{2.23}}}, \quad (13)$$

where $\psi_x^{2.23}$ is the peak point count at 2.23 MeV for target material x , which is determined by neutron distribution (energy, time, and lateral distribution) inside the phantom. $\varphi_{HC}^{2.23}$ and $\varphi_{HO}^{2.23}$ are the PG counts per mol hydrogen with neutrons originating from carbon and oxygen. If $\psi_x^{2.23}$, $\varphi_{HC}^{2.23}$ and $\varphi_{HO}^{2.23}$ are properly measured or calculated, we can get hydrogen molar amount M_H .

Finally, the target elements' molar amounts M_C , M_O and M_H are all retrieved. We refer to this method as the prompt gamma spectroscopy retrieval algorithm (PGSRA). In addition, PG can be used to measure the beam range in a target by using the TOF method [6] or a multi-slit camera [23, 45, 46]. Thus, the target volume and density can be measured.

$$V = S^*R, \quad (14)$$

where S is the lateral surface area and R is the proton range in the target. Density can be determined by Eq. 15:

$$\rho = \frac{Mass}{V} = \frac{12^*M_C + 16^*M_O + M_H}{S^*R}. \quad (15)$$

This mathematical algorithm is not limited to hydrogen, oxygen, and carbon. It can be extended to sulfur, nitrogen, or any other element. As a feasibility study, the focus of this study is hydrogen, oxygen, and carbon. We attempt to verify this algorithm on three molecules: PMMA ($C_5H_8O_2$), pentanediol ($C_5H_{12}O_2$), and ethanediol ($C_2H_6O_2$). The purpose is to retrieve the molar numbers of the elements and calculate the density of these samples.

2.3 Cloud computing

To improve the statistics, the run primary number is 5×10^7 for every MC simulation. The typical time consumption for a primary particle number of 10^6 is almost 2 h on a standalone computer (Intel Core (TM) i7-8550U CPU @ 1.8 GHz and 16 GB memory). It takes 100 h, which is approximately 1 week, to complete one simulation. Thus, we have to use a parallel method to reduce the time consumption [47]. It is logical to break down a large primary number into several smaller ones with valid random numbers. The Python script is Fluka_p_run.py. Every simulation takes several hours; therefore, we develop a special Python script (Status.py) that terminates cloud computing once the simulation is finished. Another function of the script is to monitor statuses such as the number of processes that are still running. This script is cost-effective and time-saving. Another useful script is KillAll.py, which is used to terminate all the jobs on the cloud if a problem is discovered. In this simulation, we use Amazon Web Service's HPC cluster instead of the traditional physical cluster.

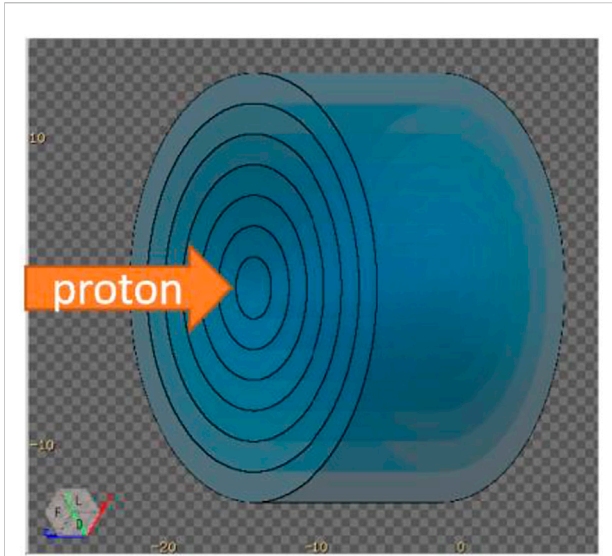


FIGURE 4
A water phantom with 7 layers ranging from a radii of 2 cm to 14 cm. The USRYIELD card was adopted to score the neutron yield between each layer.

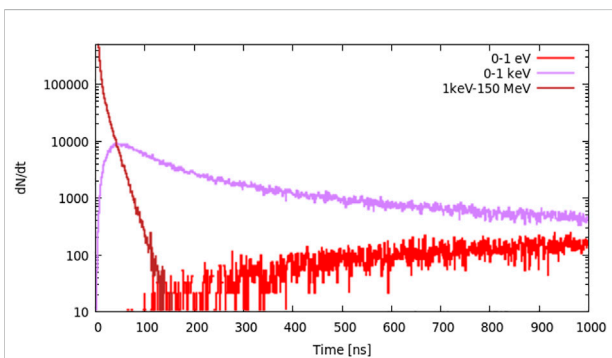


FIGURE 5
Neutron distribution in the layer where $R = 2$ cm; there are two slow neutron energy groups: 0–1 eV and 0–1 keV and one fast neutron group: 1 keV–150 MeV.

2.4 Neutron distribution

As Eq. 13 described, neutron distribution is the key to the nonlinear solution of PGSRA. First, we must figure out where the neutrons are generated and where the capture reactions take place. We do not consider the hydrogen atoms that are far away from the beam path in lateral direction as they can reduce the accuracy of the algorithm, and nowadays pencil beams are adopted in most proton therapy centers. In practice, we are not likely to put a detector in the target to measure the locations of the (n, γ) reaction. We can roughly determine the location of the neutron by its time of flight from inside the target to detector

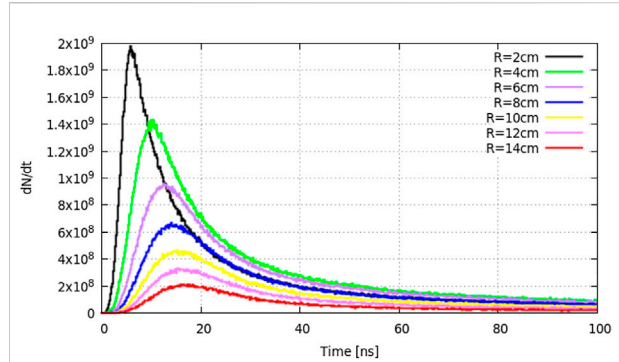


FIGURE 6
Neutron time-of-flight distribution from $R = 2$ cm to $R = 14$ cm for the 0–100 keV energy group.

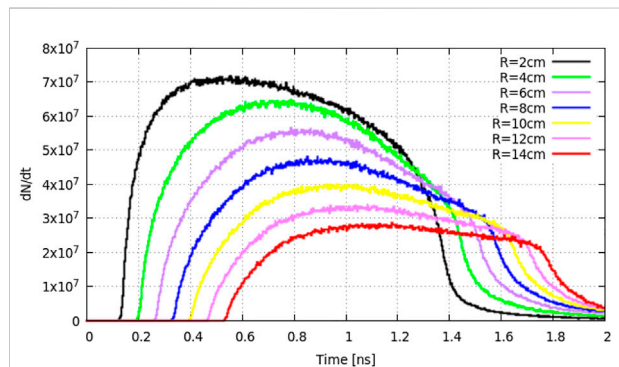


FIGURE 7
Time-of-flight distribution from $R = 2$ cm to $R = 14$ cm for the 0–10 MeV group.

outside. Thus, second, we calculate the time-of-flight for the neutron in different lateral layers in the target phantom. Based on data from the EXFOR library [48], slow neutrons (energy below ~ 10 keV) have a higher cross-section (~ 1 mb) for absorption reactions (Eq. 1). Thus, third, we need to determine the neutron distribution in energy. By the way, we also calculate the TOF of gamma photons in different layers in the same setup as neutrons.

A water phantom with 7 layers ranging from a radii of 2 cm to 14 cm was irradiated by 150 MeV protons, as shown in Figure 4. The USRYIELD card was adopted to score the neutron yield at different energies and time of flight for each radius. In this section, water is chosen as the material for calculation because the human body is mostly composed of water, which can be used as a rough estimation of the neutron distribution. All the calculation results in this section will finally give the recommended radius value of the phantom, which will be used in all the following simulations.

For the $R = 2$ cm layer, we set two slow neutron energy groups: 0–1 eV and 0–1 keV and one fast neutron group: 1 keV–150 MeV.

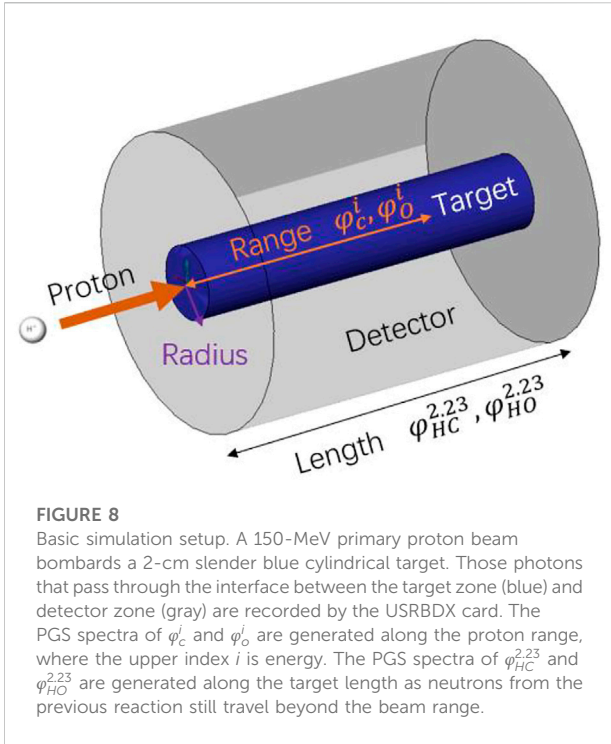


FIGURE 8
Basic simulation setup. A 150-MeV primary proton beam bombards a 2-cm slender blue cylindrical target. Those photons that pass through the interface between the target zone (blue) and detector zone (gray) are recorded by the USBDX card. The PGS spectra of φ_c^i and φ_o^i are generated along the proton range, where the upper index i is energy. The PGS spectra of $\varphi_{HC}^{2,23}$ and $\varphi_{HO}^{2,23}$ are generated along the target length as neutrons from the previous reaction still travel beyond the beam range.

From Figure 5, we can see that high-energy neutrons are generated immediately after the protons reach the target, and the slow neutron (0–1 keV group) yield increases rapidly and peaks at approximately 50 ns. The amount of 0–1 eV neutrons is much smaller than that from 0 to 1 keV neutrons before 200 ns.

The neutron (0–100 keV group) time-of-flight (TOF) distribution from $R = 2$ cm to $R = 14$ cm is shown in Figure 6. The neutron yield increases gradually and peaks at approximately 5 ns when $R = 2$ cm. As neutrons travel to the outside layers, the peak time increases and the neutron yield decreases. Thus, we choose $R = 2$ cm as the target radius for the absorption reaction region.

Correspondingly, we score the TOF of gamma photons (0–10 MeV group) in each layer from $R = 2$ cm to $R = 14$ cm. As shown in Figure 7, most photons are generated in the center layer $R = 2$ cm from 0.1 ns to 1.4 ns. The outside layers will start generating photons slightly later, within 0.6 ns, as neutron and other secondary particles require a short time to travel in the lateral direction in the water phantom. Thus, we will set an $R = 2$ cm slender cylindrical target in the feasibility study in the following simulation work.

2.5 MC simulations

To verify the retrieval algorithm in Section 2.2, a group of simulations are performed by using the FLUKA 4.0 code [16–18]. Figure 8 shows the basic simulation setup: one 150 MeV primary proton beam bombards a slender

TABLE 1 Parameters for the MC simulation of combinations of carbon and hydrogen.

Molecular formula	Number of carbon atoms	Number of hydrogen atoms	Density (g/cm ³)	Range (cm)	Length (cm)	Radius (cm)	USBDX area (cm ²)	Range volume (cm ³)	Target volume (cm ³)	Range mass (g)	Target mass (g)	Molecular molar mass (g/mol)	Molecular molar amount in range	Hydrogen molar amount in target
H0C	1	0	1	17.98	20.00	2	251.33	225.94	251.33	225.94	251.33	12	18.83	0.00
H1C	1	1	1	16.39	18.00	2	226.19	205.96	226.19	205.96	226.19	13	15.84	17.40
H2C	1	2	1	15.25	18.00	2	226.19	191.64	226.19	191.64	226.19	14	13.69	32.31
H3C	1	3	1	14.27	18.00	2	226.19	179.32	226.19	179.32	226.19	15	11.95	45.24
H4C	1	4	1	13.47	18.00	2	226.19	169.27	226.19	169.27	226.19	16	10.58	56.55
H5C	1	5	1	12.78	18.00	2	226.19	160.60	226.19	160.60	226.19	17	9.45	66.53
H6C	1	6	1	12.38	18.00	2	226.19	155.57	226.19	155.57	226.19	18	8.64	75.40
H8C	1	8	1	11.84	18.00	2	226.19	148.79	226.19	148.79	226.19	20	7.44	90.48
H10C	1	10	1	11.22	18.00	2	226.19	140.99	226.19	140.99	226.19	22	6.41	102.82
H12C	1	12	1	10.81	18.00	2	226.19	135.84	226.19	135.84	226.19	24	5.66	113.10
H15C	1	15	1	10.36	18.00	2	226.19	130.19	226.19	130.19	226.19	27	4.82	125.66
H20C	1	20	1	9.77	18.00	2	226.19	122.77	226.19	122.77	226.19	32	3.84	141.37

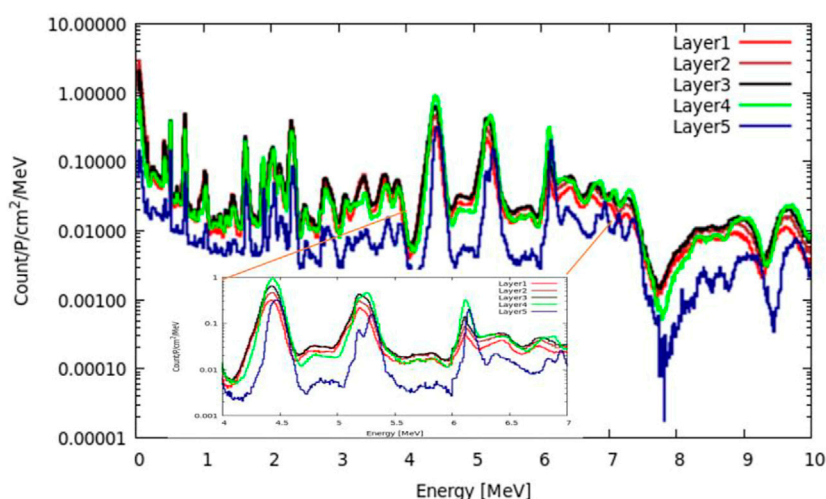


FIGURE 9
Gamma spectra at different depths.

cylindrical target. The primary beam is Gaussian with FWHM = 5 mm and zero momentum spread. The radius of the target is 2 cm. The target length is larger than the beam range, as shown in columns 5 and 6 of Table 1. As the 150 MeV proton range in H0C is 17.98 cm, its length is set to 20 cm to cover a short neutron flight path. The lengths of H1C ~ H20C and H0O ~ H20O are set to 18 cm. There is a virtual gamma detector (FLUKA scorer) around the target surface, and all the photons from the target to the scorer are recorded by the USRBDX card in the range of 0–10 MeV with 1,000 energy bins. USRBDX is a virtual detector for a boundary crossing fluence or current estimator [16].

This setup means that we ignore the energy difference of proton travel through the target in the beam direction. In fact, the proton beam enters and loses energy as it travels. Nuclei near the front face of the target experience higher energy protons than those toward the back of the target. The reaction probabilities change as a function of energy, so different reactions dominate at different depths in the target. We divide the 20-cm water target into five layers and obtain the gamma spectra at different depths by using 5 USRBDXs, each of which is 4 cm. As shown in Figure 9, the characteristic gamma counts increase as protons travel along the target and suddenly decrease in layer 5. However, for this feasibility study, we only adopt one USRBDX to score spectra for the full length to simplify the calculation.

2.5.1 FLUKA setup for elemental molar PGS

The first group of simulations is completed to obtain molar spectroscopy results for carbon, oxygen, and hydrogen. Thus, two series of sample materials are simulated with 150 MeV proton irradiation. One series is hydrocarbons: C, HC, H₂C, H₃C, ..., H₂₀C, and the other is O, HO, H₂O, H₃O, ..., H₂₀O. Certainly, most of these

compounds do not exist in our natural world except H₂O and H₄C. However, in our feasibility MC simulations, FLUKA can set up different combinations of atoms by using the COMPOUND card, which defines a mixture of different atoms. To simplify the calculation, the densities of all sample materials are set to the same as water $\rho = 1 \text{ g/cm}^3$.

As the focus of this study is not on range measurement, we measure the range by scoring proton fluence along the beam axis when 90% of the primary protons have stopped in the target. The USRBIN card, with a Cartesian grid of $40 \times 40 \times 300$ voxels, is adopted for such a measurement. The USRBIN card can score the distribution of proton fluence or other quantities in a regular spatial structure.

Not all the material in the target can contribute to the PGS spectra scored by USRBDX. After all the protons stop in the target, there will be no gamma radiation directly induced by protons. However, after reaching the longitudinal depth of the proton range, there are still neutrons from previous reactions along the beam path that can produce 2.23 MeV gamma rays. Thus, to calculate the molar PGS values for carbon and oxygen, we should use the range mass; for hydrogen, we should use the target mass. All the discussed parameters are shown in Tables 1, 2.

2.5.2 FLUKA setup for PGS

The second group of simulations is completed to obtain full energy PGS spectra of PMMA, pentanediol, and ethanediol. The configuration is similar to that in Section 2.5.1. The only difference is that the COMPOUND card simultaneously contains carbon, oxygen, and hydrogen with different numbers of atoms. In addition, their densities are set to 1.18 g/cm^3 , 0.9939 g/cm^3 , and 1.1088 g/cm^3 , respectively, in

TABLE 2 Parameters for the MC simulation of combinations of oxygen and hydrogen.

Molecular formula	Number of oxygen atoms	Number of hydrogen atoms	Density (g/cm ³)	Range (cm)	Length (cm)	Radius (cm)	USRBDX area (cm ²)	Range volume (cm ³)	Target volume (cm ³)	Range mass (g)	Target mass (g)	Molecular molar mass (g/mol)	Molecular molar amount in range	Hydrogen molar amount in target
H0O	1	0	1	18.00	18.00	2	226.19	226.19	226.19	226.19	226.19	16	14.14	0.00
H1O	1	1	1	17.22	18.00	2	226.19	216.39	226.19	216.39	226.19	17	12.73	13.31
H2O	1	2	1	16.00	18.00	2	226.19	201.06	226.19	201.06	226.19	18	11.17	25.13
H3O	1	3	1	15.20	18.00	2	226.19	191.01	226.19	191.01	226.19	19	10.05	35.71
H4O	1	4	1	14.37	18.00	2	226.19	180.58	226.19	180.58	226.19	20	9.03	45.24
H5O	1	5	1	13.79	18.00	2	226.19	173.29	226.19	173.29	226.19	21	8.25	53.86
H6O	1	6	1	13.39	18.00	2	226.19	168.26	226.19	168.26	226.19	22	7.65	61.69
H8O	1	8	1	12.61	18.00	2	226.19	158.46	226.19	158.46	226.19	24	6.60	75.40
H10O	1	10	1	12.00	18.00	2	226.19	150.80	226.19	150.80	226.19	26	5.80	87.00
H12O	1	12	1	11.39	18.00	2	226.19	143.13	226.19	143.13	226.19	28	5.11	96.94
H15O	1	15	1	10.99	18.00	2	226.19	138.10	226.19	138.10	226.19	31	4.45	109.45
H20O	1	20	1	10.40	18.00	2	226.19	130.69	226.19	130.69	226.19	36	3.63	125.66

TABLE 3 Parameters for the MC simulation of the sample materials.

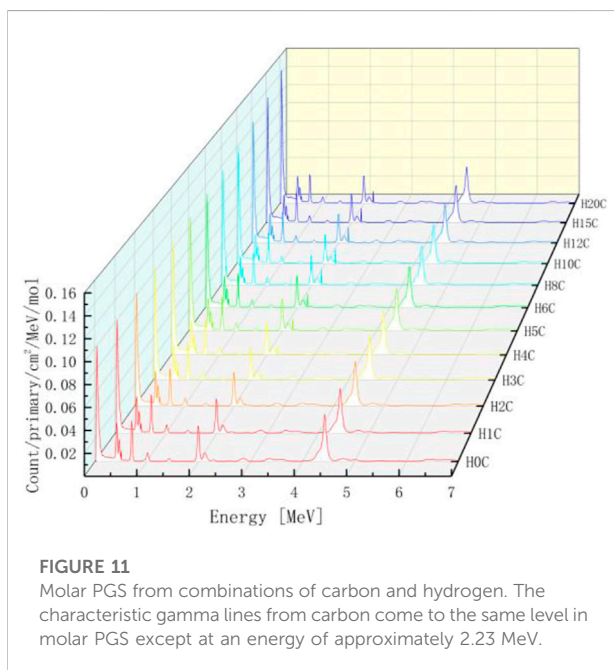
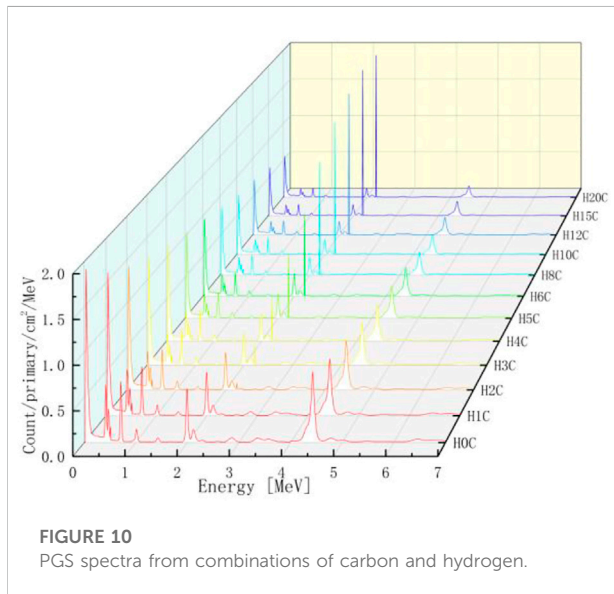
Sample material	Number of carbon atoms	Number of hydrogen atoms	Number of oxygen atoms	Density (g/cm ³)	Range (cm)	Length (cm)	Radius (cm)	USRBDX area (cm ²)	Range volume (cm ³)	Target volume (cm ³)	Range mass (g)	Target mass (g)	Molecular molar mass (g/mol)	Molecular molar amount in range	Hydrogen molar amount in target
C ₅ H ₈ O ₂	5	8	2	1.18	14.00	18.00	2	226.19	175.93	226.19	207.60	226.19	100	2.08	21.35
C ₅ H ₁₂ O ₂	5	12	2	0.9939	15.78	18.00	2	226.19	198.30	226.19	197.09	224.81	104	1.90	25.94
C ₂ H ₆ O ₂	2	6	2	1.1088	14.63	18.00	2	226.19	183.85	226.19	203.85	250.80	62	3.29	24.27

the MC simulations. All the discussed parameters are presented in Table 3.

3 Results

3.1 Element molar PGS

The PGS spectra from combinations of carbon and hydrogen bombarded by 150 MeV protons are shown in Figure 10.



Characteristic gamma lines from carbon decrease with an increasing number of hydrogen atoms, while 2.23 MeV gamma lines increase as the number of hydrogen atoms increases. This is consistent with our intuition that the carbon concentration is high in low hydrogen combinations and the opposite for hydrogen concentrations. In addition, 2.23 MeV lines from neutron absorption radiation will be investigated carefully later.

For every combination, the beam range, which decreases as the number of hydrogen atoms increases, is measured. As shown in Table 1, the range volume (column 9) and range mass (column 11) can be determined. Then, the PGS spectra are divided by the molecular molar amount in range, which is the molar PGS, as presented in Figure 11. The difference is that the characteristic gamma lines from carbon come to the same level in molar PGS except at an energy of approximately 2.23 MeV.

We extract peak gamma lines (2.00 MeV, 2.23 MeV, 2.88 MeV, 4.44 MeV, and 6.12 MeV) from Figures 10, 11. As shown on the left of Figure 12, the 2.00 MeV, 2.88 MeV, 4.44 MeV, and 6.12 MeV counts have a linear relationship with carbon concentration, which has been confirmed by experiments [40]. As shown on the right of Figure 12, the molar count curves of these selected gamma lines are at the same level except for 2.23 MeV. Thus, the basic assumption of a linear carbon term in Eq. 2 is reasonable.

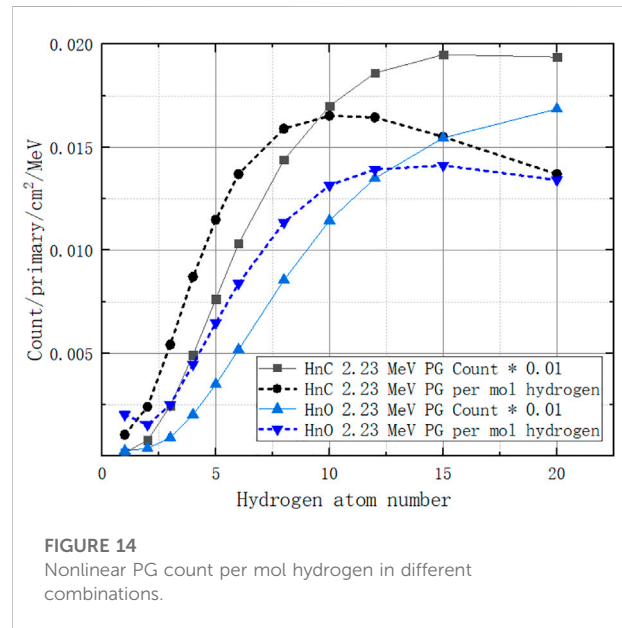
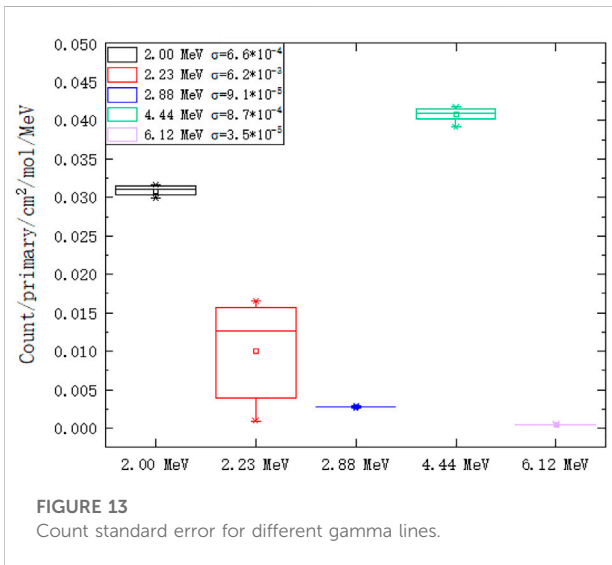
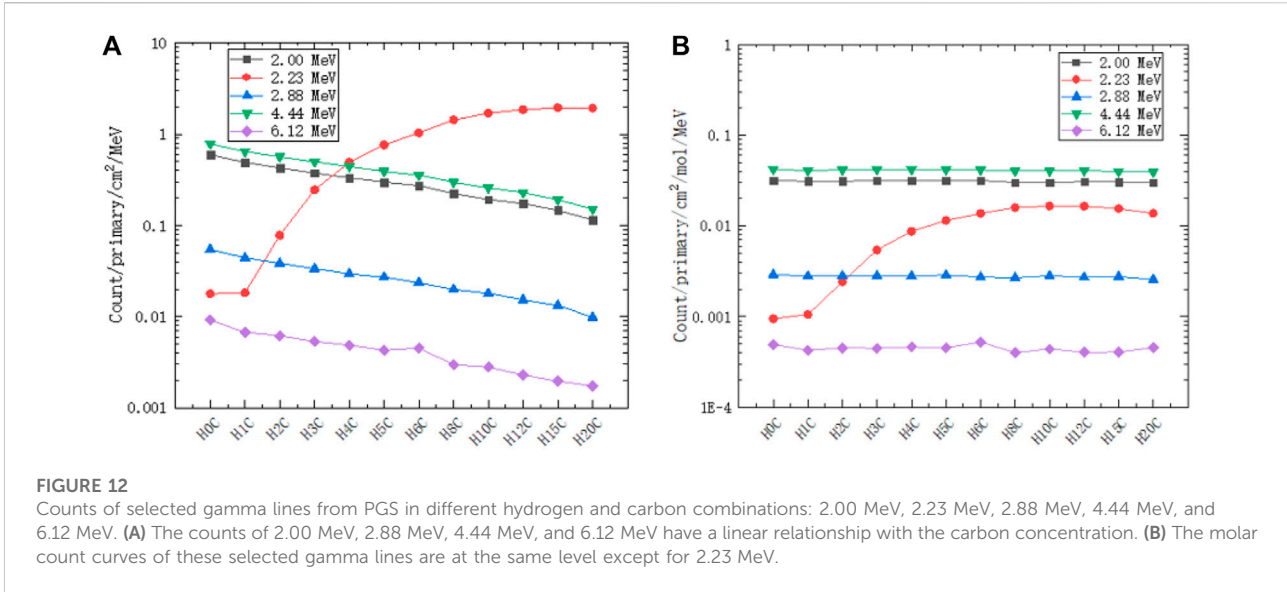
The molar count standard errors are 6.6×10^{-4} at 2 MeV, 6.2×10^{-3} at 2.23 MeV, 9.1×10^{-5} at 2.88 MeV, 8.7×10^{-4} at 4.44 MeV, and 3.5×10^{-5} at 6.12 MeV as shown in Figure 13. Thus, the count deviation for 2.23 MeV is at least an order of magnitude higher than that of the other gamma lines. We will analyze the nonlinear behavior in the next section.

The PGS spectra from combinations of oxygen and hydrogen bombarded by 150 MeV protons are analyzed by the same pattern as carbon in the supplementary material. While their behavior is similar to those from the combinations of carbon and hydrogen, their characteristic gamma lines are more abundant.

Thus, matrix A in Eq. 10 can be determined by the element molar PGS.

3.2 Molar PG count for hydrogen

We extract the 2.23 MeV gamma count from the PGS spectrum described in Section 3.1. Additionally, we obtain a nonlinear PG count per mol hydrogen with its number of atoms, as the dotted lines show in Figure 14. The count increases when the number of hydrogen atoms is 1–12 and then decreases. The reason is that the more hydrogens there are in a molecule, the higher the neutron absorption probability. However, the presence of too many hydrogens will stop neutrons from going further to the next molecule as energy is lost in the collision of neutrons and hydrogen nuclei. Thus, hydrogen appears to be an enhancer in low hydrogen combinations. The ratio term $\frac{N_H}{N_O + N_C}$ in Eqs 4, 5 is reasonable



when N_H is less than ~ 12 . $N_H = 11.5$ is the upper limit of human organ tissue from the ICRP 110 report as list in its ANNEX B section [49].

Here, we must choose a molar PG count values to assign $\varphi_{HC}^{2.23}$ and $\varphi_{HO}^{2.23}$ in Eq. 13. In principle, the PG counts corresponding to HC and HO should be the best option. However, most of the combinations with a large number of hydrogen atoms are not natural; in this study, we choose the 2.23 MeV molar count from HC and H_2O . That is,

$$\varphi_{HC}^{2.23} = 0.00105, \varphi_{HO}^{2.23} = 0.00154. \quad (16)$$

3.3 Element amount measurement by PGSRA

Figure 15 shows the full energy PGS spectra of PMMA, pentanediol, and ethanediol detected by the USBDX card during the virtual MC simulations described in Section 2.5.2. To solve Eq. 10, we select the peak points to assign matrix B . Most gamma lines are listed in Table 4. The MC simulated energy in column 3 is in good agreement with the experimental results [50].

These points are sorted into different groups:

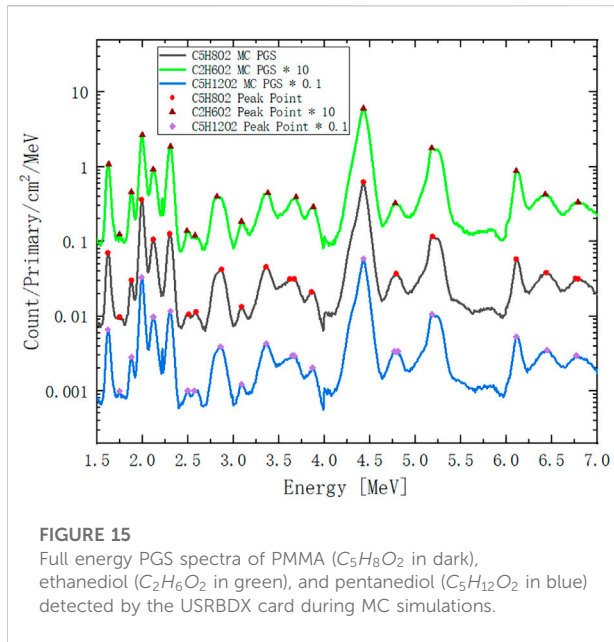


FIGURE 15
Full energy PGS spectra of PMMA ($C_5H_8O_2$ in dark), ethanediol ($C_2H_6O_2$ in green), and pentanediol ($C_5H_{12}O_2$ in blue) detected by the USBDX card during MC simulations.

All: All peaks from 1.5 to 7 MeV; energies lower than 1.5 MeV are not chosen in this algorithm, as some of these energies are not generated from pure (p, γ) channels. These gamma lines are not as distinct as those from Compton scattering.

Low: Low-energy peaks from 1.5 to 4 MeV.
High: High-energy peaks from 4 to 7 MeV.
Medium-high: Peaks of medium energy 2 MeV to high energy 7 MeV.

Every group will include at least 3 points, and thus, the numerical solution of the element molar amount matrix $m = \begin{bmatrix} M_C \\ M_O \end{bmatrix}$ can be determined by the least square method for each group.

Table 5 lists the numerical solutions of M_C and M_O for each group. The molar amount of carbon is approximately 10, and the ratio of M_C/M_O is close to 2.5. The last column is the error of M_C/M_O with respect to the atomic ratio N_C/N_O in a PMMA molecule. As a result, the solution of the medium-high group is the best solution, with smallest relative error of 0.78% as shown in Table 5 with bold number.

For pentanediol, the best solution is the high-energy group, as shown in Table 6 with bold number.

For ethanediol, the best solution is the high-energy group, as shown in Table 7 with bold number.

Medium- and high-energy points are preferred for the numerical solution as these characteristic gamma lines are more distinct. Now, M_C and M_O are determined, and $\psi_x^{2,23}$ can be extracted from the PGS spectra of the sample materials. $\phi_{HC}^{2,23}$ and $\phi_{HO}^{2,23}$ have been determined in Section 3.2. Then, we can calculate the hydrogen molar amount by using Eq. 13. The sample mass and density can be calculated by using Eq. 15.

TABLE 4 Gamma lines from proton reactions with oxygen and carbon. Experimental energy data, transition, reaction, and mean life from accelerated particle interactions [50].

Group	Energy experiment (MeV)	Energy MC (MeV)	Relative error (%)	Transition	Reaction	Mean life (s)
Deprecated	0.718	0.72	0.28	$^{10}B^{*0.718} \rightarrow$ g.s.	$^{12}C(p,x)^{10}B^*$ $^{16}O(p,x)^{10}B^*$	1.0×10^{-9} 1.0×10^{-9}
	1.022	1.02	0.20	$^{10}B^{*1.740} \rightarrow ^{10}B^{*0.718}$	$^{12}C(p,x)^{10}B^*$ $^{16}O(p,x)^{10}B^*$	7.5×10^{-15} 7.5×10^{-15}
	1.635	1.63	0.31	$^{14}N^{*3.948} \rightarrow ^{14}N^{*2.313}$	$^{16}O(p,x)^{14}N^*$	6.9×10^{-15}
Low	2.000	2.00	0.00	$^{11}C^{*2.000} \rightarrow$ g.s.	$^{12}C(p,x)^{11}C^*$	1.0×10^{-14}
	2.124	2.12	0.19	$^{11}B^{*2.125} \rightarrow$ g.s.	$^{12}C(p,x)^{11}B^*$	5.5×10^{-15}
	2.313	3.31	0.13	$^{14}N^{*2.313} \rightarrow$ g.s.	$^{16}O(p,x)^{14}N^*$	9.8×10^{-14}
	2.742	2.82	2.84	$^{16}O^{*8.872} \rightarrow ^{16}O^{*6.130}$	$^{16}O(p,p')^{16}O^*$	1.8×10^{-13}
	3.684	3.69	0.16	$^{13}C^{*3.685} \rightarrow$ g.s.	$^{16}O(p,x)^{13}C^*$	1.6×10^{-15}
	3.853	3.88	0.70	$^{13}C^{*3.854} \rightarrow$ g.s.	$^{16}O(p,x)^{13}C^*$	1.2×10^{-11}
	High	4.438	4.43	0.18	$^{12}C^{*4.439} \rightarrow$ g.s.	$^{12}C(p,p')^{12}C^*$ $^{16}O(p,x)^{12}C^*$
5.180		5.18	0.00	$^{15}O^{*5.181} \rightarrow$ g.s.	$^{16}O(p,x)^{15}O^*$	$< 4.9 \times 10^{-14}$
6.129		6.11	0.31	$^{16}O^{*6.130} \rightarrow$ g.s.	$^{16}O(p,p')^{16}O^*$	2.7×10^{-11}
6.476		6.43	0.71	$^{11}C^{*6.478} \rightarrow$ g.s.	$^{12}C(p,x)^{11}C^*$	$< 8.7 \times 10^{-15}$
6.741		6.76	0.28	$^{11}B^{*6.743} \rightarrow$ g.s.	$^{12}C(p,x)^{11}B^*$	4.3×10^{-20}
6.790		6.79	0.00	$^{11}B^{*6.792} \rightarrow$ g.s.	$^{12}C(p,x)^{11}B^*$	5.6×10^{-19}

TABLE 5 Numeric solution of PMMA.

$C_5H_8O_2$ group	M_C [mol]	M_O [mol]	M_C/M_O	M_C/M_O relative error (%)
All	10.1522	4.2419	2.3933	4.27
Low	10.1350	4.2509	2.3842	4.63
High	10.2351	4.2068	2.4330	2.68
Medium-high	10.3469	4.1066	2.5196	0.78

TABLE 6 Numeric solution of pentanediol.

$C_5H_{12}O_2$ group	M_C [mol]	M_O [mol]	M_C/M_O	M_C/M_O relative error (%)
All	9.2649	4.0280	2.3001	7.99
Low	9.1582	4.0814	2.2439	10.24
High	9.7719	3.8373	2.5466	1.86
Medium-high	9.5617	3.9140	2.4430	2.28

TABLE 7 Numeric solution of ethanediol.

$C_2H_6O_2$ group	M_C [mol]	M_O [mol]	M_C/M_O	M_C/M_O relative error (%)
All	6.3268	6.6354	0.9535	4.65
Low	6.1875	6.6743	0.9271	7.29
High	6.8350	6.7923	1.0063	0.63
Medium-high	6.6864	6.7517	0.9903	0.97

TABLE 8 Numeric solutions of M_H and density.

Sample material	Variable	PGSPA result	MC setup value	Relative error (%)
PMMA $\psi_{C_5H_8O_2}^{2,23} = 0.0349$	M_O [mol]	4.1066	4.1519	1.09
	M_C [mol]	10.3469	10.3798	0.32
	M_H [mol]	20.6003	21.3528	3.52
	Sample Mass [g]	210.4682	207.5964	1.38
	Density [g/cm³]	1.17	1.18	1.38
Pentanediol $\psi_{C_5H_{12}O_2}^{2,23} = 0.0365$	M_O [mol]	3.8373	3.7901	1.24
	M_C [mol]	9.7719	9.4754	3.13
	M_H [mol]	20.4229	22.7409	10.19
	Sample Mass [g]	199.0820	197.0877	1.01
	Density [g/cm³]	1.0040	0.99	1.01
Ethanediol $\psi_{C_2H_6O_2}^{2,23} = 0.0377$	M_O [mol]	6.7923	6.5758	3.29
	M_C [mol]	6.8350	6.5758	3.94
	M_H [mol]	19.8981	19.7273	0.87
	Sample Mass [g]	210.5943	203.8484	3.31
	Density [g/cm³]	1.1455	1.11	3.31

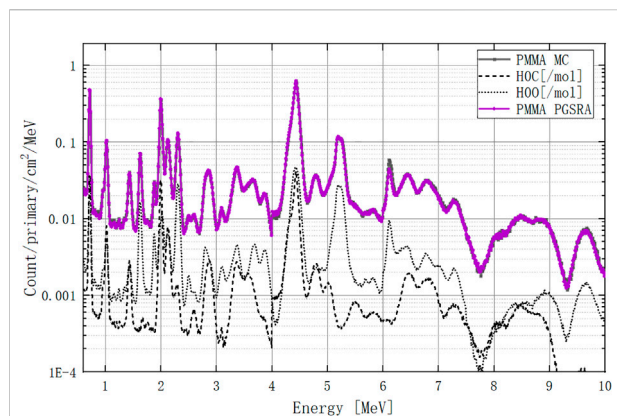


FIGURE 16

PMMA PGS spectrum at 0–10 MeV calculated by the retrieval algorithm. The dark curve is the MC-calculated PGS spectrum, and the purple curve is the PGSRA-calculated PGS spectrum. The carbon and oxygen molar PGS spectra are dashed lines.

The results are summarized in Table 8 and compared with the MC setup values from Table 3. The relative errors of the hydrogen molar amount are approximately 10% for PMMA and pentanediol. However, their densities are consistent with the setup values, and the relative errors are smaller than 2%. On the contrary, for ethanediol, the hydrogen amount relative error is only 0.87%, and the density relative error is 3.31%. This is because although there is a high atom number of hydrogen, it has much lower weight than carbon and oxygen in materials. Thus, density error is dominated by carbon and oxygen.

Finally, we can recalculate the PMMA PGS spectra by using our retrieval algorithm, as shown in Figure 16. In the 0–4 MeV range, all peaks are consistent with the MC curve. In the 4–7 MeV range, only the peak at 6.1 MeV shows a small deviation from the MC curve. The retrieved PGSs of pentanediol and ethanediol are in supplementary material.

4 Discussion and conclusion

Based on 3 basic assumptions: 1) the sample material has a relationship with its element molar gamma lines in PG spectroscopy, 2) for carbon and oxygen, this relationship is linear, and 3) for hydrogen, this relationship is nonlinear and is based on a neutron absorption reaction; an element retrieval algorithm is developed in the present study. The challenge is how to carefully deal with the nonlinear hydrogen 2.23 MeV gamma count. A series of simulations confirm that these assumptions are reasonable. The mathematical formulas of the PGSRA theoretically explain the linear relationship of the gamma count and element concentration detected by Polf *et al.* [38, 39] and Paulo *et al.* [40].

The element amount has been successfully calculated by the PGSRA for the following three sample materials: PMMA, pentanediol, and ethanediol. The relative errors of carbon and oxygen are smaller than 4% for all the sample materials. The relative error of hydrogen, based on its nonlinear behavior, is approximately 10%. In addition, the relative errors of the sample density are smaller than 3.5% for all the sample materials. This new retrieval algorithm is valid for predicting the element amount and density in an unknown material. It may be the first bridge between PGS and medical imaging.

Data availability statement

The original contributions presented in the study are included in the article. PGS spectra from combinations of oxygen and hydrogen, retrieval pentanediol PGS and ethanediol PGS are in the Supplementary Material, and further inquiries can be directed to the corresponding author.

Author contributions

J-L Wang: theoretical model, FLUKA simulation, and manuscript. X-GW: physics, prompt gamma analysis, and review. Z-FL: medical physics, proton therapy, and review. S-QX: data analysis. Z-HZ: detector. D-QH: neutron adsorption. AR: cloud computing. YZ: detector and physics. CL: nuclear reaction. T-XL: detector and physics. MZ: gamma detector. D-JD: data process. X-DW: data process. H-SR: data process.

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Conflict of interest

A Rusanov was employed by the company Elekta Limited.

The remaining authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.

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Supplementary material

The Supplementary Material for this article can be found online at: <https://www.frontiersin.org/articles/10.3389/fphy.2022.961162/full#supplementary-material>

References

- MacKay RI. Image guidance for proton therapy. *Clin Oncol* (2018) 30(5):293–8. doi:10.1016/j.clon.2018.02.004
- Knopf AC, Lomax A. *In vivo* proton range verification: A review. *Phys Med Biol* (2013) 58(15):R131–60. doi:10.1088/0031-9155/58/15/R131
- Min CH, Kim CH, Youn MY, Kim JW. Prompt gamma measurements for locating the dose falloff region in the proton therapy. *Appl Phys Lett* (2006) 89(18):183517. doi:10.1063/1.2378561
- Smeets J, Roellinghoff F, Prieels D, Stichelbaut F, Benilov A, Busca P, et al. Prompt gamma imaging with a slit camera for real-time range control in proton therapy. *Phys Med Biol* (2012) 57(11):3371–405. doi:10.1088/0031-9155/57/11/3371
- Verburg JM, Seco J. Proton range verification through prompt gamma-ray spectroscopy. *Phys Med Biol* (2014) 59(23):7089–106. doi:10.1088/0031-9155/59/23/7089
- Golnik C, Hueso-González F, Müller A, Dendooven P, Enghardt W, Fiedler F, et al. Range assessment in particle therapy based on prompt γ -ray timing measurements. *Phys Med Biol* (2014) 59(18):5399–422. doi:10.1088/0031-9155/59/18/5399
- Draeger E, Mackin D, Peterson S, Chen H, Avery S, Beddar S, et al. 3D prompt gamma imaging for proton beam range verification. *Phys Med Biol* (2018) 63(3):035019. doi:10.1088/1361-6560/aaa203
- Roellinghoff F, Richard MH, Chevallier M, Constanzo J, Dauvergne D, Freud N, et al. Design of a Compton camera for 3D prompt- γ imaging during ion beam therapy. *Nucl Instr Methods Phys Res Section A: Acc Spectrometers Detectors Associated Equipment* (2011) 648(Suppl. 1):20–3. doi:10.1016/j.nima.2011.01.069
- Panaino CMV, Mackay RI, Kirkby KJ, Taylor MJ. A new method to reconstruct in 3D the emission position of the prompt gamma rays following proton beam irradiation. *Sci Rep* (2019) 9(1):18820–13. doi:10.1038/s41598-019-55349-7
- Richter C, Pausch G, Barczyk S, Priegnitz M, Keitz I, Thiele J, et al. First clinical application of a prompt gamma based *in vivo* proton range verification system. *Radiother Oncol* (2016) 118(2):232–7. doi:10.1016/j.radonc.2016.01.004
- Hueso-González F, Rabe M, Ruggieri TA, Bortfeld T, Verburg JM. A full-scale clinical prototype for proton range verification using prompt gamma-ray spectroscopy. *Phys Med Biol* (2018) 63(18):185019. doi:10.1088/1361-6560/aad513
- Werner T, Berthold J, Hueso-González F, Koegler T, Petzoldt J, Roemer K, et al. Processing of prompt gamma-ray timing data for proton range measurements at a clinical beam delivery. *Phys Med Biol* (2019) 64(10):105023. doi:10.1088/1361-6560/ab176d
- Marcatili S, Collot J, Curtoni S, Dauvergne D, Hostachy JY, Koumeir C, et al. Ultra-fast prompt gamma detection in single proton counting regime for range monitoring in particle therapy. *Phys Med Biol* (2020) 65(24):245033–17. doi:10.1088/1361-6560/ab7a6c
- Zhang H, Fan P, Xu T, Wei Q, Ma T, Liu Y, et al. Scintillation detector design study for prompt gamma photon detection in proton therapy monitoring. In: 2017 IEEE Nucl Sci Symp Med Imaging Conf NSS/MIC 2017 - Conf Proc; 21–28 October 2017; Atlanta, GA, USA (2018). p. 7–10. doi:10.1109/NSSMIC.2017.8532768
- Zhang H, Fan P, Wang S, Xia Y, Xu T, Wei Q, et al. Design and performance evaluation of a BGO + SiPM detector for high-energy prompt gamma imaging in proton therapy monitoring. *IEEE Trans Radiat Plasma Med Sci* (2020) 4(2):184–93. doi:10.1109/trpms.2020.2972594
- Ferrari A, Sala PR, Fassò A, Ranft J. Fluka: A multi-particle transport code. *MC-INFN* (2005) 773. doi:10.2172/877507
- Böhlen TT, Cerutti F, Chin MPW, Fassò A, Ferrari A, Ortega P, et al. The FLUKA Code: Developments and challenges for high energy and medical applications. *Nucl Data Sheets* (2014) 120:211–4. doi:10.1016/j.nds.2014.07.049
- Kozłowska WS, Böhlen TT, Cuccagna C, Ferrari A, Fracchiolla F, Magro G, et al. FLUKA particle therapy tool for Monte Carlo independent calculation of scanned proton and carbon ion beam therapy. *Phys Med Biol* (2019) 64(7):075012. doi:10.1088/1361-6560/ab02cb
- Agostinelli S, Allison J, Amako K, Apostolakis J, Araujo H, Arce P, et al. GEANT4 - a simulation toolkit. *Nucl Instr Methods Phys Res Section A: Acc Spectrometers Detectors Associated Equipment* (2003) 506(3):250–303. doi:10.1016/S0168-9002(03)01368-8
- Cirrone GAP, Cuttone G, Di Rosa F, Mazzaglia SE, Romano F, Attili A, et al. Hadrontherapy: An open source, Geant4-based application for proton-ion therapy studies. In: IEEE Nuclear Science Symposium Conference Record; 24 October 2009 - 01 November 2009; Orlando, FL, USA (2009). p. 4186–9. doi:10.1109/NSSMIC.2009.5402279
- Biegun AK, Seravalli E, Lopes PC, Rinaldi I, Pinto M, Oxley DC, et al. Time-of-flight neutron rejection to improve prompt gamma imaging for proton range verification: A simulation study. *Phys Med Biol* (2012) 57(20):6429–44. doi:10.1088/0031-9155/57/20/6429
- Jacquet M, Marcatili S, Gallin-Martel ML, Bouly JL, Boursier Y, Dauvergne D, et al. A time-of-flight-based reconstruction for real-time prompt-gamma imaging in proton therapy. *Phys Med Biol* (2021) 66(13):135003–32. doi:10.1088/1361-6560/ac03ca
- Wang JL, Cruz LA, Lu M. Pixelated prompt gamma imaging detector for online measurement of proton beam: Monte Carlo feasibility study by FLUKA. *Radiat Detect Technol Methods* (2018) 2(1):4. doi:10.1007/s41605-017-0032-0
- Park JH, Kim SH, Ku Y, Lee HS, Kim CH, Shin DH, et al. Comparison of knife-edge and multi-slit camera for proton beam range verification by Monte Carlo simulation. *Nucl Eng Technol* (2019) 51(2):533–8. doi:10.1016/j.net.2018.10.002
- Han Y, Tang X, Geng C, Shu D, Gong C, Zhang X, et al. Investigation of *in vivo* beam range verification in carbon ion therapy using the Doppler shift effect of prompt gamma: A Monte Carlo simulation study. *Radiat Phys Chem Oxf Engl* 1993 (2019) 162:72–81. doi:10.1016/j.radphyschem.2019.04.036
- Geng C, Han Y, Tang X, Shu D, Gong C, Altieri S. Evaluation of using the Doppler shift effect of prompt gamma for measuring the carbon ion range *in vivo* for heterogeneous phantoms. *Nucl Instr Methods Phys Res Section A: Acc Spectrometers Detectors Associated Equipment* (2020) 959:163439. doi:10.1016/j.nima.2020.163439
- Pennazio F, Ferrero V, D'Onghia G, Garbolino S, Fiorina E, Marti Villarreal OA, et al. Proton therapy monitoring: Spatiotemporal emission reconstruction with prompt gamma timing and implementation with PET detectors. *Phys Med Biol* (2022) 67(6):065005. doi:10.1088/1361-6560/ac5765
- Polf JC, Peterson S, Ciangaru G, Gillin M, Beddar S. Prompt gamma-ray emission from biological tissues during proton irradiation: A preliminary study. *Phys Med Biol* (2009) 54(3):731–43. doi:10.1088/0031-9155/54/3/017
- Testa M, Bajard M, Chevallier M, Dauvergne D, Freud N, Henriquet P, et al. Real-time monitoring of the Bragg-peak position in ion therapy by means of single photon detection. *Radiat Environ Biophys* (2010) 49(3):337–43. doi:10.1007/s00411-010-0276-2
- Pausch G, Petzoldt J, Berthel M, Enghardt W, Fiedler F, Golnik C, et al. Scintillator-based high-throughput fast timing spectroscopy for real-time range verification in particle therapy. *IEEE Trans Nucl Sci* (2016) 63(2):664–72. doi:10.1109/TNS.2016.2527822

31. Dal Bello R, Magalhaes Martins P, Brons S, Hermann G, Kihm T, Seimetz M, et al. Prompt gamma spectroscopy for absolute range verification of ^{12}C ions at synchrotron-based facilities. *Phys Med Biol* (2020) 65(9):095010. doi:10.1088/1361-6560/ab7973
32. Idiri Z, Mazrou H, Amokrane A, Bedek S. Characterization of an Am-Be PGNAA set-up developed for *in situ* liquid analysis: Application to domestic waste water and industrial liquid effluents analysis. *Nucl Instr Methods Phys Res Section B: Beam Interactions Mater Atoms* (2010) 268(2):213–8. doi:10.1016/j.nimb.2009.10.185
33. Khelifi R, Amokrane A, Bode P. Detection limits of pollutants in water for PGNAA using Am-Be source. *Nucl Instr Methods Phys Res Section B: Beam Interactions Mater Atoms* (2007) 262(2):329–32. doi:10.1016/j.nimb.2007.06.003
34. Naqvi AA, Garwan MA, Nagadi MM, Maslehuddin M, Al-Amoudi OSB, Khateeb-ur-Rehman. Non-destructive analysis of chlorine in fly ash cement concrete. *Nucl Instr Methods Phys Res Section A: Acc Spectrometers Detectors Associated Equipment* (2009) 607(2):446–50. doi:10.1016/j.nima.2009.05.192
35. Naqvi AA, Al-Matouq FA, Khiari FZ, Khateeb-Ur-RehmanGondal MA, Isab AA. Optimization of a prompt gamma setup for analysis of environmental samples. *J Radioanal Nucl Chem* (2013) 296:215–21. doi:10.1007/s10967-012-2045-y
36. Jia W, Cheng C, Hei D, Ling Y, Wang H, Chen D. Method for correcting thermal neutron self-shielding effect for aqueous bulk sample analysis by PGNAA technique. *J Radioanal Nucl Chem* (2015) 304(3):1133–7. doi:10.1007/s10967-015-3962-3
37. Hei D, Jiang Z, Jia W, Cheng C, Wang H, Li J, et al. The background influence of cadmium detection in saline water using PGNAA technique. *J Radioanal Nucl Chem* (2016) 310(1):27–31. doi:10.1007/s10967-016-4767-8
38. Verburg JM, Shih HA, Seco J. Simulation of prompt gamma-ray emission during proton radiotherapy. *Phys Med Biol* (2012) 57(17):5459–72. doi:10.1088/0031-9155/57/17/5459
39. Polf JC, Panthi R, Mackin DS, McCleskey M, Saastamoinen A, Roeder BT, et al. Measurement of characteristic prompt gamma rays emitted from oxygen and carbon in tissue-equivalent samples during proton beam irradiation. *Phys Med Biol* (2013) 58(17):5821–31. doi:10.1088/0031-9155/58/17/5821
40. Magalhaes Martins P, Dal Bello R, Ackermann B, Brons S, Hermann G, Kihm T, et al. PIBS: Proton and ion beam spectroscopy for *in vivo* measurements of oxygen, carbon, and calcium concentrations in the human body. *Sci Rep* (2020) 10(1):7007–14. doi:10.1038/s41598-020-63215-0
41. Jia W, Cheng C, Shan Q, Hei D, Ling Y, Zhang Y, et al. Study on the elements detection and its correction in aqueous solution. *Nucl Instr Methods Phys Res Section B: Beam Interactions Mater Atoms* (2015) 342:240–3. doi:10.1016/j.nimb.2014.10.010
42. Jeyasugiththan J, Camero JN, Symons J, Jones P, Buffler A, Geduld D, et al. Measuring prompt gamma-ray emissions from elements found in tissue during passive-beam proton therapy. *Biomed Phys Eng Express* (2021) 7(2):025013. doi:10.1088/2057-1976/abe33d
43. Ahdida C, Bozzato D, Calzolari D, Cerutti F, Charitonidis N, Cimmino A, et al. New capabilities of the FLUKA multi-purpose code. *Front Phys* (2022) 9:1–14. doi:10.3389/fphy.2021.788253
44. Clegg AB, Foley KJ, Salmon GL, Segel RE. Gamma radiation from the medium energy proton bombardment of lithium, beryllium, boron, carbon and nitrogen. *Proc Phys Soc* (1961) 78(5):681–94. doi:10.1088/0370-1328/78/5/305
45. Lee HR, Kim SH, Park JH, Jung WG, Lim H, Kim CH. Prototype system for proton beam range measurement based on gamma electron vertex imaging. *Nucl Instr Methods Phys Res Section A: Acc Spectrometers Detectors Associated Equipment* (2017) 857:82–97. doi:10.1016/j.nima.2017.03.022
46. Park JH, Kim SH, Ku Y, Kim CH, Lee HR, Jeong JH, et al. Multi-slit prompt-gamma camera for locating of distal dose falloff in proton therapy. *Nucl Eng Technol* (2019) 51(5):1406–16. doi:10.1016/j.net.2019.03.008
47. Wang JL, Cruz LA, Wu QB, Wang Q, Wei Y, Wang HK. Radiation shielding design of a compact single-room proton therapy based on synchrotron. *Nucl Sci Tech* (2020) 31(1):1. doi:10.1007/s41365-019-0712-1
48. Otuka N, Dupont E, Semkova V, Pritychenko B, Blokhin AI, Aikawa M, et al. *Toward more complete and accurate experimental nuclear reaction data library (EXFOR) - international collaboration between nuclear reaction data centres (NRDC)*. New York: Nuclear Data Sheets (2014). p. 8–11.
49. Sowby FD. Annals of the ICRP 110. *Ann ICRP* (1981) 6(1):1. doi:10.1016/0146-6453(81)90127-5
50. Murphy RJ. *NUCLEAR DEEXCITATION GAMMA-RAY LINES FROM ACCELERATED PARTICLE INTERACTIONS benzion kozlovsky*. The Astrophysical Journal Supplement Series (2002). 2, p. 523–41. Published online.